

## 1. Extended Data

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Extended Data Fig. 1	<b>Membrane porosity following treatment with Tat-trimer</b>	Extended_Data_Figure_1_NC_HEM-19091918B	<b>Extended Data Fig. 1. Membrane porosity following treatment with Tat-trimer.</b> (a, b) Addition of 40 $\mu$ M propidium iodide (PI) 20 min after addition of 1 $\mu$ M trimer; image at 30 min after start of experiment. Cells treated with tri-Tat A (a) co-stain with PI; cells treated with tri-cTat B (b) are PI negative. (c) Average fluorescence intensity of PI per cell, 45 min after the start of the experiment (n=25). Cells treated with tri-Tat A show significantly higher PI uptake, indicative of pore formation. (d) Cells treated with tri-Tat A (solid line) or tri-cTat B (dotted line) for 60 min and metabolic activity as an indicator of cell viability assessed using MTT assay after 1 h, 2 h, 4 h, 3 days (n=3 biologically independent experiments). Data presented as mean $\pm$ standard deviation. Scale bar: 20 $\mu$ m.

## 2. Supplementary Information:

### A. Flat Files

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Supplementary Information	Yes	Supporting.Information.NCHEM-19091918B.pdf	Supporting Information
Reporting Summary	Yes	nr-reporting-summary_NCHEM-19091918B.pdf	
Peer Review Information	No	<i>OFFICE USE ONLY</i>	

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Source Data Fig. 1	SourceData.Fig1.xls	Statistical Source Data for main Figures and Extended Data Figures
Source Data Fig. 2	SourceData.Fig2.xls	Statistical Source Data for main Figures and Extended Data Figures
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Source Data Fig. 6	SourceData.Fig6.xls	Statistical Source Data for main Figures and Extended Data Figures
Source Data Extended Data Fig. 1	SourceData.ExFig1.xls	Statistical Source Data for main Figures and Extended Data Figures

## **Tricyclic Cell-Penetrating Peptides for Efficient Delivery of Functional Antibodies into Cancer Cells**

Ole Tietz<sup>1</sup>, Fernando Cortezon-Tamarit<sup>1</sup>, Rod Chalk<sup>2</sup>, Sarah Able<sup>1</sup>, Katherine Vallis<sup>1\*</sup>

<sup>1</sup> CRUK/MRC Oxford Institute for Radiation Oncology, Department of Oncology, University of Oxford, Old Road Campus Research Building, Roosevelt Drive, Oxford, OX3 7DQ, United Kingdom.

<sup>2</sup> Centre for Medicines Discovery, University of Oxford, Old Road Campus Research Building, Roosevelt Drive, Oxford, OX3 7DQ, United Kingdom.

**CONTACT:** \* telephone: +44 (0)1865 2 25850; e-mail: [katherine.vallis@oncology.ox.ac.uk](mailto:katherine.vallis@oncology.ox.ac.uk)

## **Abstract**

The intracellular environment hosts a large number of cancer and other disease relevant human proteins. Targeting these with internalised antibodies would allow therapeutic modulation of hitherto undruggable pathways, such as those mediated by protein-protein interactions (PPI). However, one of the major obstacles in intracellular targeting is the entrapment of biomacromolecules in the endosome. Here we report an approach to delivering antibodies and antibody fragments into the cytosol and nucleus of cells using trimeric cell-penetrating peptides (CPP). Four trimers, based on linear and cyclic sequences of the archetypal CPP Tat, are significantly more potent than monomers and can be tuned to function by direct interaction with the plasma membrane or escape from vesicle-like bodies. These studies identify a tricyclic Tat construct that enables intracellular delivery of functional IgG antibodies and Fab fragments that bind intracellular targets in the cytosol and nuclei of live cells at effective concentrations as low as 1  $\mu$ M.

## 1 **Introduction**

2 Agents that can deliver exogenous cargo into live cells are highly sought after and  
3 find wide application in cell biology; furthermore, effective intracellular targeting is  
4 crucial in the development of novel diagnostic and therapeutic agents.<sup>1</sup> Intracellular  
5 delivery of functional monoclonal antibodies would allow the utilization of previously  
6 undruggable but therapeutically relevant targets, such as the large number of  
7 intracellular protein-protein interactions (PPI).<sup>2</sup> Despite advances in the field,  
8 intracellular delivery remains a formidable challenge due to toxicity or limited efficacy  
9 of current vehicles. Cargo has been delivered into cells using viral and non-viral  
10 carriers, as well as physical techniques such as electroporation; each approach  
11 presents distinct strengths and weaknesses in the context of *in vitro*, *ex vivo* and *in*  
12 *vivo* applications.<sup>3</sup> Polycationic non-viral carriers, such as polymers, lipid particles,  
13 and cell-penetrating peptides (CPPs), have been studied extensively over the past  
14 three decades as a means of transporting pharmaceuticals into cells.<sup>4-7</sup> The archetypal  
15 CPP Tat has been used extensively in the design of intracellularly targeted  
16 therapeutics; however, endocytic entrapment is recognized as a significant  
17 hindrance to intracellular delivery.<sup>8-13</sup> Low level leakage of Tat delivered cargos from  
18 endosomes is typically too inefficient to lend itself to most intracellular targeting  
19 applications.

20 A number of recent studies have attempted to address this problem.<sup>14,15</sup>  
21 Cyclized Tat and oligoarginine conjugated to GFP (cTat-GFP) were found to access  
22 the cytosol and nucleus by direct translocation across the cell membrane.<sup>16,17</sup> Linear  
23 oligoarginine was used as a reagent to deliver a range of cargos, including enzymes,  
24 nanobodies and antibodies, into cells by direct interaction with the plasma  
25 membrane.<sup>18</sup> A CPP specifically designed to be endosomolytic (L17E) was shown to

26 facilitate the escape of cargo from the endosome.<sup>19</sup> A significant barrier to utilization  
27 of these approaches in translational *in vivo* applications is the relatively high  
28 concentration needed to achieve desirable results *in vitro* (>10  $\mu$ M). Importantly,  
29 typical dosing of clinically used immunotherapeutics (10 mg/kg) results in peak  
30 antibody plasma concentrations of only 2  $\mu$ M or less, emphasizing the need for CPP  
31 delivery technology with activity at  $\sim$  1  $\mu$ M.<sup>20</sup> The observation that Tat and other  
32 CPPs cluster prior to internalization,<sup>21,22</sup> as well as recent insights into the  
33 relationship between charge density of polycationic agents and efficacy of delivery,<sup>23-</sup>  
34 <sup>25</sup> led to the hypothesis addressed in the current report, that prearranging Tat  
35 peptides into multimeric clusters on a defined chemical scaffold would increase their  
36 efficacy. This hypothesis is lent credence by the observation that branched  
37 multimers of Tat, on peptide scaffolds or connected by disulphide bonds, results in  
38 increased intracellular delivery.<sup>26-28</sup> Particular attention in this area of research has  
39 been given to bridged dimers of Tat and oligoarginine.<sup>29-31</sup> Furthermore, cyclization  
40 of individual peptides has been shown to improve efficacy of uptake.<sup>14</sup>

41 Here we report the design and synthesis of four Tat trimers based on linear and  
42 cyclic sequences of Tat peptide, arranged on two different tetrakis core structures,  
43 which were evaluated *in vitro* using live cell confocal microscopy. The results  
44 indicate that the geometry of the synthetic core structure affects efficacy of delivery  
45 and that replacing linear Tat with a cyclized variant alters the mechanism of uptake.  
46 We identify a tricyclic lead structure and demonstrate delivery of functional  
47 antibodies and antibody fragments into the cytosol of HeLa cells which bind  
48 intracellular actin fibrils and fluorescent protein expressed in the cytosol and nuclei of  
49 live cells.

50

## 51 **Results**

52

### 53 **Synthesis of Tat trimers**

54 Four Tat trimers were designed using two different scaffolds furnished with either  
55 linear or cyclic Tat (cTat) peptide. These were chosen to determine (1) whether Tat  
56 trimers are more effective than monomers, (2) whether scaffold geometry affects the  
57 efficacy of Tat trimers, and (3) whether trimers based on cyclic sequences behave  
58 differently from trimers based on linear peptide. Tat-trimers were synthesized by  
59 copper catalysed 2+3 cyclo-addition between azide and alkyne functionalized  
60 components. The synthesis of trimers **tri-Tat A** and **tri-cTat A** is based on an azide  
61 functionalized scaffold A (**2**, Fig. 1a) and the synthesis of trimers **tri-Tat B** and **tri-**  
62 **cTat B** is based on an alkyne functionalized scaffold B (**10**, Fig. 1f). Linear Tat (49-  
63 57) peptide (RKKRRQRRR), modified with a hexynoyl (alkyne) (**3**) or an azido-  
64 pentanoyl (azide) (**11**) at the N-terminus was used to synthesize **tri-Tat A (8)** and **tri-**  
65 **Tat B (16)**, as well as monomeric control **mono-Tat (18**, Supplementary Scheme 3).  
66 Cyclic Tat was custom designed to match the linear sequence; azide / alkyne  
67 functionality was added by including either an azide modified lysine (K(N<sub>3</sub>)) residue  
68 or propargyl glycine (Pra) at the N-terminus. Peptides were cyclized by addition of  
69 glutamic acid to the C-terminus for head to tail cyclisation to the N-terminus to  
70 generate cyclic Pra-RKKRRQRRRG (**4**) and K(N<sub>3</sub>)RKKRRQRRRG (**12**). These  
71 peptides were used to synthesize cyclic trimers **tri-cTat A (9)** and **tri-cTat B (17)**, as  
72 well as monomeric cyclic control **mono-cTat (19**, Supplementary Scheme 3). Tat-  
73 trimers were labeled with AlexaFluor488 (AF488) for further study. Photophysical  
74 properties of peptide trimers were found to be similar to AF488 alone (Fig. 1;  
75 Supplementary Figs. 1 and 2). *In silico*

76 generated three-dimensional representations of all four trimers are shown as ball  
77 and stick models in Figure 1.

78

### 79 **Uptake of trimers in HeLa and CHO cells**

80 The cellular uptake and intracellular distribution of Tat-trimers and monomeric  
81 controls was investigated by performing live cell confocal microscopy of HeLa  
82 (human, cervical cancer) and CHO (Chinese hamster, epithelial) cells incubated with  
83 Tat conjugates (1  $\mu$ M) in serum-free DMEM (60 min). Following washing, images  
84 were acquired using a Zeiss 780 confocal microscope fitted with an incubation  
85 chamber (Fig. 2). In accordance with observations that free Tat in the cytosol readily  
86 enters the nucleus and strongly binds to nucleoli,<sup>32</sup> homogenous staining of  
87 cytoplasm and nucleoli were considered as indicative of cells having accumulated  
88 free conjugate, not confined to endosomes, for quantification purposes. The results  
89 show that **mono-Tat** (1  $\mu$ M) is not taken up by HeLa or CHO cells (Fig. 2a). In  
90 contrast **tri-Tat A**, shows homogenous cytosolic uptake and nucleolar staining at this  
91 concentration (Fig. 2b). This effect is not due to the increased total amount of Tat  
92 peptide, as experiments with 10  $\mu$ M **mono-Tat** indicate no cytosolic uptake or  
93 nucleolar staining (Supplementary Fig. 3). The uptake and intracellular distribution of  
94 **tri-Tat A** is similar in live HeLa and CHO cells (Fig. 2b,d,e). Interestingly,  
95 experiments with **tri-Tat B** showed no evidence of cytosolic uptake or nucleolar  
96 staining in either HeLa or CHO cells (Fig. 2c,e). Experiments in HeLa cells  
97 transfected with the early endosomal marker rab5a tagged with RFP (rab5a-RFP)  
98 confirm that the intracellular punctuate fluorescence displayed by **tri-Tat B** is due to  
99 endosomal entrapment (Supplementary Fig. 5).

100 Similar to **mono-Tat**, and despite reports that cyclic Tat is more effective in  
101 comparison to linear Tat,<sup>14,17</sup> **mono-cTat** is not taken up into HeLa or CHO cells  
102 (Fig. 2f). It is probable that differences between monomeric linear and cyclic Tat are  
103 only observed above certain threshold concentrations and thus not observed at 1  $\mu$ M  
104 or 10  $\mu$ M (Supplementary Fig. 3b). In contrast, **tri-cTat A** (1  $\mu$ M) shows homogenous  
105 cytosolic and nucleolar staining (Fig. 2g), although the staining intensity is lower than  
106 that observed with linear **tri-Tat A**, and transduction efficiency is slightly reduced  
107 (Fig. 2i,j). Interestingly, **tri-cTat B** appears to be more effective at cellular  
108 transduction in comparison to **tri-cTat A** both by average fluorescence intensity per  
109 cell and percentage of transduced cells. As cell transduction and amount of trimer  
110 delivered into the cell differ for linear versus cyclic trimers, we propose that cyclic  
111 trimers enter the cytosol by a different mechanism from linear trimers. These initial  
112 experiments identified linear **tri-Tat A** and cyclic **tri-cTat B** as the most promising  
113 lead compounds.

114

#### 115 **Time course of uptake in HeLa cells.**

116 To better understand the mechanism by which **tri-Tat A** and **tri-cTat B** enter the  
117 cytosol and the nucleus, we investigated the uptake kinetics of the conjugates during  
118 the first 15 min after their addition to HeLa cells using confocal live cell microscopy.

119 **Tri-Tat A** or **tri-cTat B** (1  $\mu$ M) were added to the cells and images acquired from 1  
120 min to 15 min at 60 sec intervals (Fig. 3a,b). The two trimers show distinct uptake  
121 patterns in HeLa cells. To better understand the difference in uptake kinetics, we  
122 drew cross sectional profile plots through representative cells treated with **tri-Tat A**  
123 (Fig. 3c) and **tri-cTat B** (Fig. 3d). These plots reveal initial strong association of **tri-**  
124 **Tat A** with the membrane, indicated by two signals on either end of the plot, and no

125 fluorescence in the cytosol; fluorescence signal then spreads from the membrane  
126 into the cytosol. In contrast, **Tri-cTat B** displays little association with plasma  
127 membrane and instead forms large vesicular bodies in the cytosol; fluorescence  
128 signal then spreads from these vesicles into the cytosol. To investigate whether  
129 findings in individual cells also apply to larger populations, we extended the plot  
130 profile analysis by designating regions of interest (ROI) corresponding to plasma  
131 membrane, cytosol (excluding endosomes), nucleus, and nucleoli along the cross  
132 section, using information from brightfield images.<sup>33</sup> Average fluorescence intensities  
133 for each ROI, at each time point, in five cells per treatment group were calculated  
134 and plotted in Fig. 3, e–h. **Tri-Tat A** shows significant, approximately three-fold,  
135 stronger association with the plasma membrane ( $p < 0.05$  for  $t = 1$  to 15 min; Fig 3e).  
136 While the cytosolic signal of **tri-cTat B** gradually increases over time, cells treated  
137 with **tri-Tat A**, show little cytosolic accumulation (significantly lower than **tri-cTat B**  
138 from 4 to 7 min ( $p < 0.05$ ), until signal increases rapidly after  $\sim 12$  min and exceeds  
139 **tri-cTat B** signal by a factor of 2 at 15 min ( $p = 0.08$ , SI Table S2) (Fig. 3f). Similar  
140 patterns are observed for accumulation in the nucleus and nucleoli (Fig. 3g, h).  
141 These observations are consistent with different mechanisms of cell entry for the two  
142 trimers. **Tri-Tat A** translocates directly across the membrane, rather than or in  
143 addition to entry into the cytosol via endosomal escape, while the route of cell entry  
144 for **tri-cTat B** is the formation of vesicle-like bodies followed by vesicular escape.

145 To assess membrane integrity, 40  $\mu\text{M}$  propidium iodide (PI; a cell impermeable  
146 dye), was added to HeLa cells 20 min after the addition of the peptide trimer. Cells  
147 with free **tri-Tat A** in the cytosol also contain PI (Extended Data Fig. 1a), indicating  
148 that transient pores are formed, once a critical peptide to membrane lipid ratio is  
149 reached,<sup>21</sup> allowing the influx of PI into the cell (Supplementary Fig. 6). The amount

150 of PI in cells, as measured by average fluorescence signal in the cytosol and  
151 nucleus, is significantly higher in cells treated with **tri-Tat A** than **tri-cTat B**  
152 ( $p < 0.0001$ ; Extended Data Fig. 1b, c), indicating that the cyclic peptide trimer does  
153 not form pores in the plasma membrane. Co-localization of **tri-cTat B** and rab5a  
154 confirms that the intracytoplasmic vesicle-like structures are endosomes; rab5a  
155 associates with endosomes before release of cargo into the cytosol (Supplementary  
156 Fig. 5).

157 Toxicity is a concern with potent intracellular delivery agents. We used the MTT  
158 assay to measure the metabolic activity of HeLa cells treated with 1  $\mu\text{M}$  **tri-Tat A** or  
159 **tri-cTat B** for 60 min (Extended Data Fig. 1d). **Tri-cTat B** shows little acute toxicity  
160 (cells 94.3% viable, 4 h post-treatment), and no chronic toxicity (cells 96.5% viable, 3  
161 days post-treatment). **Tri-Tat A** is slightly more toxic, which is consistent with the  
162 observation that the trimer forms membrane pores (cells 84.4% viable, 4 h post-  
163 treatment; 80.2% viable, 3 days post-treatment). The favourable uptake mechanism  
164 and low toxicity of **tri-cTat B** led us to investigate this agent for its potential to  
165 transport biomacromolecular cargos into cells.

166

### 167 **Co-delivery of antibodies and antibody fragments.**

168 Access to the cytosol by mechanisms that are independent of transmembrane  
169 pore formation constitutes a preferred method of co-delivery due to reduced  
170 cytotoxicity. Treatment of HeLa cells with 500 nM AF647-labelled non-specific  
171 mouse Fab fragment and 1  $\mu\text{M}$  **tri-cTat B** for 30 min resulted in successful delivery  
172 of Fab into cytosol and nucleus of 50% of cells in a typical experiment (Fig. 4a, d).  
173 Successful delivery of Fab and its release from endosomes is indicated by  
174 homogenous staining of cytosol and nucleus by Fab-AF647; the persistence of some

175 punctuate signal indicates that endosomal escape is incomplete. AF647 is only  
176 observed in cells that have been transduced with **tri-cTat B** showing that Fab  
177 internalisation depends on the action of the CPP (Supplementary Fig. 7). The time  
178 course of Fab uptake by **tri-cTat B** (Fig. 4c) follows a similar pattern as **tri-cTat B**  
179 itself (Fig. 3b, d). **Tri-cTat B** and Fab form large vesicle-like bodies that release their  
180 contents into the cytosol of the cell; unambiguous cytosolic staining by Fab is  
181 observed from 23 min. Interaction between peptide trimer and biomacromolecule,  
182 mediated by charge-charge interactions is likely to be important for the accumulation  
183 of both in endosomes and subsequent release and delivery of cargo into cells.  
184 Delivery of relatively  $\beta$ -sheet rich, neutrally charged recombinant RFP was  
185 unsuccessful (Supplementary Fig. 10) possibly due to a lack of association between  
186 **tri-cTat B** and cargo (Supplementary Fig. 11). On the other hand, interaction with  
187 the intended cargo diminishes the efficacy of the peptide trimer due to charge  
188 masking, emphasising the need to maintain an appropriate peptide to cargo ratio for  
189 a given macromolecule.

190 Experiments to explore the efficiency of **tri-cTat B** in the presence of serum-  
191 supplemented medium underline this principle. While **tri-cTat B** continues to function  
192 in the presence of serum, the number of transduced cells diminishes (61%, serum  
193 free; 42%, serum) but can be restored by increasing **tri-cTat B** concentration to 2  $\mu$ M  
194 (79%); Supplementary Fig. 9. Whole IgG co-delivery by **tri-cTat B** is possible, but  
195 less efficient than the delivery of Fab, with 20% of cells showing homogenous AF647  
196 staining in cytosol and nucleus (Fig. 4b, d). This is likely due to the larger size of  
197 antibodies and to the observation that antibodies have a greater tendency to  
198 aggregate in the presence of **tri-cTat B** compared to Fab fragments. There was no

199 cellular uptake of Fab or IgG in the absence of **tri-cTat B** or in the presence of  
200 **mono-Tat / mono-cTat** (Supplementary Fig. 8).

201 We next investigated whether it is possible to deliver functional antibodies and  
202 antibody fragments into the cytosol and nuclei of cells.  $\beta$ -actin was chosen as a  
203 proof-of-principle target protein because of its abundance in the cell and formation of  
204 distinctive subcellular stress fibres (Supplementary Fig. 13). To clearly identify actin  
205 stress fibres, HeLa cells were transfected with red fluorescent protein fused to actin  
206 (actin-RFP) before being incubated with  $\beta$ -actin antibody (mouse IgG<sub>2b</sub>) or  $\beta$ -actin  
207 Fab fragment (mouse) conjugated to AF647 plus **tri-cTat B** for 30 min. After  
208 washing, cells were left for 60 min to allow IgG / Fab to bind to actin filaments. Figure  
209 6a shows a representative cell transfected with actin-RFP (shown in orange, O),  
210 transduced with **tri-cTat B** and co-delivered  $\beta$ -actin Fab-AF647 (shown in red, R).  
211 Figure 6b shows the co-delivery of  $\beta$ -actin IgG-AF647 into a similarly treated cell. To  
212 enable objective quantification of co-localization between  $\beta$ -actin stress fibres and  
213 IgG / Fab fragment (white arrows), a co-localization threshold algorithm was used in  
214 selected ROI.<sup>34</sup> Pearson's and Manders' coefficients were obtained under Costes'  
215 automatic threshold<sup>35</sup> and the co-localized pixels are shown as a mask of yellow  
216 pixels of constant intensity (co-localization panels). The significance of the co-  
217 localization parameters (Pearson's and Manders' coefficients) was evaluated using  
218 the confined displacement algorithm (CDA).<sup>34,36</sup> This analysis indicates that 4 to 8%  
219 of RFP signal in ROIs co-localizes with IgG / Fab; while one third of IgG / Fab signal  
220 co-localizes with  $\beta$ -actin RFP (Supplementary Table 1), resulting in statistically  
221 significant correlation in the areas indicated (white arrows, yellow mask). These  
222 results indicate that  $\beta$ -actin Fab and IgG antibodies retain their ability to bind actin  
223 stress fibres in the cytoplasm of cells.

224 We went on to investigate whether functional antibodies can be delivered to the  
225 nucleus using **tri-cTat B**. HeLa cells were transfected with a histone-RFP fusion  
226 protein and then incubated with **tri-cTat B** and an anti-RFP IgG (mouse, IgG<sub>1</sub>; Fig.  
227 5c). The antibody enters the nucleus and co-localizes with RFP (white arrows). Co-  
228 localization analysis of the ROI indicates that approximately half of the RFP signal  
229 co-localizes with IgG and >45% of IgG signal co-localizes with RFP, resulting in a  
230 significant correlation (Supplementary Table 1). It was also shown that anti-RFP IgG  
231 can bind actin-RFP stress fibres in the cytoplasm (Supplementary Figures 14 and  
232 15), resulting in higher target occupancy (> 30%; Supplementary Table S1)  
233 compared to that achieved with  $\beta$ -actin-Fab-AF647. Some of the internalised  
234 antibody and Fab remains confined to vesicles that mainly localize in the perinuclear  
235 region. Trafficking of IgG and Fab to the nucleoli was observed, an off-target effect  
236 mediated by charge-charge association with **tri-cTat B** (Supplementary Fig. 17).  
237 Delivery of anti-RFP Fab fragment into the cytoplasm and nucleus of cells was  
238 accomplished, but co-localization could not be demonstrated, due to low affinity of  
239 the Fab fragment for RFP protein (Supplementary Fig. 12).

240 The proximity ligation assay (PLA; Duolink®) which allows optical detection of  
241 protein-protein interactions (PPI) was used to show that co-localization of CPP  
242 internalised antibodies and targeted RFP-tagged proteins results from specific  
243 interaction of the two. Samples are first incubated with antibodies against the two  
244 target proteins and then incubated with secondary antibodies with attached  
245 oligonucleotides that form a circular DNA structure only when the two primary  
246 antibodies are within 40 nm of each other. The circular DNA is amplified through  
247 addition of a complementary sequence that incorporates a fluorophore and thus  
248 reveals the presence of the PPI and its subcellular localization.<sup>37</sup> PLA detects

249 protein-protein interactions in their native form compared to other techniques such as  
250 co-immunoprecipitation, which requires disruption of the cell structure, or FRET,  
251 which requires extensive data processing. Here, the interaction between an anti-  
252 H2B-AF488, co-delivered to the cytosol and nuclei of HeLa cells using **tri-cTat B**  
253 lacking a fluorophore label (cTat<sub>3</sub>-alkyne, **14**), and an H2A.Z antibody, introduced in  
254 the cells after permeabilization, is observed. Proximity detection by secondary  
255 antibody mediated oligonucleotide ligation followed by rolling-circle amplification  
256 (RCA) reveals red spots in the nuclei of cells that also show nuclear accumulation of  
257 internalised H2B-AF488 IgG (Fig. 6a). The PLA signal in cells incubated with H2B-  
258 AF488 IgG plus **tri-cTat B** and then with H2A.Z IgG was significantly higher than in  
259 cells incubated with either H2B-AF488 or H2A.Z IgG alone (Fig. 6b;  $p < 0.0001$ ).  
260 Additional controls with a non-specific IgG and a  $\beta$ -actin IgG were performed by  
261 incubation of the cells as well as co-delivery of the antibodies using cTat<sub>3</sub>-alkyne. In  
262 all cases, it can be observed that the number of PLA signals in the nuclei remains  
263 significantly higher (Fig. 6b;  $p < 0.0001$ ) than in the incubated or co-delivered antibody  
264 controls. This provides evidence that anti-H2B IgG delivered into the nucleus by **tri-**  
265 **cTat B** is functional and binds the H2B/H2A.Z dimer that constitutes part of the  
266 nucleosome octamer. These results validate the findings of the co-localisation  
267 experiments and show that antibodies and antibody fragments delivered into the  
268 cytosol and nucleus using **tri-cTat B** retain their ability to bind target proteins.

269

270

## 271 **Discussion**

272 The arrangement of Tat peptides into multimeric clusters on a defined chemical  
273 scaffold provides delivery agents that are significantly more effective than previously

274 reported CPPs. The significant difference in transduction efficiency between the  
275 linear trimers **tri-Tat A** and **tri-Tat B** is surprising, but broadly consistent with reports  
276 suggesting that higher charge density leads to more effective uptake into cells.<sup>23-25</sup>  
277 The interaction between trimer geometry and cell surface clusters might account for  
278 differences in uptake efficacy between different cell lines and raises the possibility of  
279 enhancing uptake into specific cell types by altering CPP cluster geometry. The  
280 effect of multimerization on binding efficacy to cell surface proteins has recently been  
281 demonstrated.<sup>38</sup>

282 Despite reports that cyclisation of CPPs can increase efficacy by up to two  
283 orders of magnitude,<sup>39</sup> cyclic trimers **tri-cTat A** and **tri-cTat B** did not show  
284 significantly improved uptake into the cytoplasm and nuclei of cells compared to  
285 linear Tat trimers. Instead, cyclisation of Tat peptide on the trimer scaffold leads to a  
286 shift in mechanism from direct interaction with the plasma membrane to vesicular  
287 escape. A model, proposed by Pei and co-workers,<sup>14</sup> argues that there is no  
288 mechanistic difference between linear and cyclic peptides of the same sequence and  
289 postulates an exclusively quantitative difference. The results of the current study,  
290 however, suggest that there is a qualitative difference in mechanism of uptake;  
291 trimerization of linear peptides and their cyclic equivalents adds a further element of  
292 complexity to the behaviour of CPPs *in vitro*. Two features of **tri-cTat B** uptake are  
293 broadly consistent with the proposals of Pei *et al*: (1) the formation of large vesicle-  
294 like bodies containing trimer and (2) the persistence of those vesicles while peptide  
295 spreads freely into the cytosol and nucleus.<sup>14,39</sup>

296 The data presented in this report indicate that, rather than gaining access to the  
297 cytosol by a single pathway, CPPs may be able to bind different cell surface  
298 components and are apt to switch between uptake mechanisms to find the most

299 energetically favourable path into the cell. Our results show that it is possible to alter  
300 the mechanism of uptake by changing the geometry of conformation of Tat trimers,  
301 while leaving amino acid sequence and net charge unaltered.

302 It has been shown previously that endosomal escape is an efficient and non-  
303 toxic mechanism for intracellular cargo delivery.<sup>19,29-31</sup> Successful co-delivery of  
304 antibodies and antibody fragments using **tri-cTat B**, is consistent with this. Our  
305 results further suggest that an appropriate peptide to cargo ratio is crucial for  
306 successful co-delivery. Charge-charge association between peptide and cargo is  
307 necessary for the formation of endosomes containing both agents followed by  
308 release, but also leads to charge masking and reduced efficacy of the CPP. These  
309 opposing effects need to be balanced for efficient delivery of macromolecules into  
310 cells. The relative structural homogeneity of antibodies and their fragments<sup>40</sup>  
311 warrants the optimization of delivery protocols that are broadly applicable to these  
312 classes of cargo. Co-delivery of structurally diverse proteins is more challenging, as  
313 the results for RFP demonstrate. However, the absence of charge-charge interaction  
314 is likely to be a considerable advantage for covalently linked peptide-cargo  
315 conjugates, where high efficiency of delivery can be maintained, as previously  
316 demonstrated.<sup>16</sup>

317 The co-localization of protein targets and targeting agents in live cells provides  
318 insight into the efficacy of immunoglobulins in intracellular environments. While the  
319 fraction of cargo bound to target is high at 30% to 50%, the fraction of target  
320 occupied by cargo is dependent on the nature and abundance of the target.  $\beta$ -actin  
321 is a high abundance protein ( $>10 \mu\text{M}$ ), with only a small fraction expressed as RFP  
322 fusion protein (in the experimental conditions shown in Figure 6). Intracellular cargo  
323 concentrations are at least 1 magnitude lower than target concentration;

324 consequently, target occupancy is low (<10%). In contrast, histone-RFP expression  
325 is low, leading to relatively low abundance of RFP in the nucleus; as a result, higher  
326 target occupancy is observed (~ 45%). Indeed, using anti-RFP IgG, instead of anti- $\beta$ -  
327 actin IgG, to target actin increases target occupancy to >30 %, due to the low  
328 abundance of RFP in stress fibres. These observations, combined with the sub  
329 nanomolar affinity of immunoglobulins for their targets, suggest that this approach  
330 might be most suited for the development of therapeutics against low abundance  
331 targets.

332 Proximity ligation assays detected binding of H2B-AF488 IgG, internalised in  
333 the presence of tri-cTat B, to the H2B/H2A.Z dimer that constitutes the histone  
334 octamer in the nucleus, demonstrating successful nuclear targeting and validating  
335 co-localization data. The mechanism by which antibodies enter the nucleus is not  
336 known; our data points to continuing interaction between tri-cTat B and IgG cargo in  
337 the cytosol of cells. It is possible that this association allows nuclear delivery of cargo  
338 using the nuclear localization sequence of the Tat peptide. Large cargos such as  
339 pathogens and pre-ribosomes (some up to 40 nm in diameter) are able to cross from  
340 the cytoplasm into the nucleus, suggesting that, based on size, whole IgGs which  
341 have a length of approximately 15 nm, could also do so.<sup>41,42</sup> The ability of antibodies  
342 to enter the nucleus has been reported previously, particularly anti-DNA  
343 autoantibodies.<sup>43,44</sup> Notably, a few fluorescent spots are located outside the nucleus  
344 in the proximity ligation assay (Fig. 6a). Histones, like other proteins, are synthesised  
345 in the cytoplasm, and are then transported into the nucleus as dimers (including  
346 H2A.Z-H2B).<sup>45,46</sup> Therefore, a small amount of H2B and H2A.Z dimer does exist in  
347 the cytoplasm and was detectable in the proximity ligation assay following tri-cTat B-  
348 mediated internalisation of H2B-AF488 IgG.

349           **Tri-cTat B** is an efficient non-viral delivery agent allowing the rapid, non-toxic  
350 transport of biomacromolecular cargo into cells. This approach has some important  
351 advantages over viral delivery methods, which are limited to nucleic acid delivery  
352 and can trigger host immune responses, as well as mechanical delivery methods,  
353 which frequently lead to loss of cytoplasmic content, can excessively damage  
354 organic molecules, denature proteins, and are less amenable to *in vivo* translation.<sup>3</sup>  
355 The successful targeting of actin stress fibres using  $\beta$ -actin antibodies and Fab  
356 fragments, as well as intranuclear RFP using an IgG, raises the possibility of using  
357 immunoagents against therapeutic targets inside the cytoplasm and nucleus to affect  
358 previously undruggable disease relevant pathways. In summary **tri-cTat B** can be  
359 used as an effective delivery agent to address the challenge of targeting intracellular  
360 therapeutic targets. Furthermore, the structure-activity insights reported here will aid  
361 the development of novel CPP multimers with tailored mechanistic properties.  
362

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372

373 **Author Contributions**

374 Dr. Ole Tietz: design, conception, synthesis of Tat trimers; design, conception,  
375 acquisition of microscopy studies; data analysis; writing of manuscript; Dr. Fernando  
376 Cortezon-Tamarit: acquisition and analysis of microscopy data, PLA assay; Sarah  
377 Able: synthesis of IgG and Fab conjugates; Dr. Rod Chalk: mass Spectrometry of  
378 Tat trimers; Prof. Katherine Vallis: conception and design; funding acquisition; study  
379 supervision. All authors reviewed and revised the final manuscript.

380

381 **Competing interests statement**

382 The authors declare no competing interests.

383

384 **Data availability statement**

385 The authors declare that all the data supporting the findings of this study are  
386 available within the Article, the Supplementary Information, or the Source Data.

387 Alternatively the data is also available from the corresponding authors upon  
388 reasonable request.

## 389 Figure legends

390

391 **Fig. 1. Synthesis of Trimer Tat constructs.** Synthesis of tri-Tat A and tri-cTat A (a), tri-Tat B and tri-  
392 cTat B (f). *In silico* generated ball and stick models of linear Tat trimers suggest that they adopt coiled  
393 helices which arrange in a more compact conformation in tri-Tat A. Cyclic peptides adopt tighter  
394 helices, due to the C-terminus being forced towards the centre of the molecule. In all four trimers,  
395 peptides align in an off-parallel fashion, with arginine side chains pointing outwards. Hydrogens  
396 removed for clarity, Carbon – grey, Oxygen – red, Nitrogen – blue, Sulphur – orange; geometry of  
397 trimer conjugates optimized using a Dreiding-like forcefield; the peptide backbones highlighted from  
398 N-terminus (blue) to C-terminus (red); the central carbon of the tetrakis core highlighted in yellow.  
399 Fluorescence excitation and emission spectra of trimer (black line) compared to AF488 (dotted line); y  
400 axis - normalized fluorescence intensity (A.U.); x axis – wavelength (nm).

401

402 **Fig. 2. Live cell confocal microscopy of linear and cyclic Tat trimers in HeLa and CHO cells.** (a,  
403 f) 1  $\mu$ M mono-Tat (a) or mono-cTat (f) are not taken up into HeLa or CHO cells. (b, g, h) 1  $\mu$ M linear  
404 tri-Tat A (b) cyclic tri-cTat A (g) and tri-cTat B (h) are taken up into the cytosol and nucleoli of HeLa  
405 and CHO cells. (c) 1  $\mu$ M linear tri-Tat B is only taken up into endosomes of HeLa and CHO cells. (d, i)  
406 Quantification of average fluorescence intensity per cell in cells treated with linear (d) or cyclic (i)  
407 constructs. (e, j) Quantification of the percentage of transduced cells (scored as positive when  
408 showing homogenous cytoplasmic and nucleolar fluorescence) in cells treated with linear (e) or cyclic  
409 (i) constructs. Data presented as mean  $\pm$  standard deviation; n-numbers identical for treatment groups  
410 analysed in graphs d/e and i/j. BF = Brightfield image. Scale bar: 20  $\mu$ m.

411

412 **Fig. 3. Continuous live cell confocal microscopy of trimers in HeLa cells.** (a) Time course uptake  
413 of 1  $\mu$ M tri-Tat A; and (b) 1  $\mu$ M tri-cTat B. (c, d) Cross-sectional profile plot through a representative  
414 cell treated with 1  $\mu$ M tri-Tat A (c) and 1  $\mu$ M tri-cTat B (d); surface plot (middle) composed of cross-  
415 sectional profiles from 1 min to 15 min (y-axis: fluorescence intensity (AU); x-axis: distance along the  
416 cross section (mm); z-axis: time (min); colour added for clarity to denote y-axis values – dark blue 0-  
417 199 AU, orange – 200-399 AU, grey – 400-599 AU, yellow – 600-799 AU, light blue >800 AU). Tri-Tat  
418 A fluorescence moves from the plasma membrane inwards (c), while tri-cTat B fluorescence moves  
419 from a focal point in the cell outwards (d). (e-h) Time course analysis of cross-sectional profiles (1 –  
420 15 min) through n=5 cells examined over 3 independent experiments treated with tri-Tat A (solid lines)  
421 and tri-cTat B (dotted lines), where regions of interest (ROIs) corresponding to the membrane (e),  
422 cytosol (f), nucleus (g), and nucleoli (h) are defined and average fluorescence intensity reported. Tri-  
423 cTat B shows significantly different membrane association and uptake kinetics into cellular  
424 compartments compared to tri-Tat A. Data presented as mean  $\pm$  standard deviation. Scale bar: 20  
425  $\mu$ m.

426 **Fig. 4. Co-delivery of antibodies and antibody fragments in live HeLa cells using tri-cTat B.** (a,  
427 b) Post-wash live cell confocal microscopy images of HeLa cells treated with 500 nM mouse Fab  
428 fragment AF647 conjugate (Fab-AF647) and 1  $\mu$ M tri-cTat B for 30 min (a) or 166 nM mouse IgG  
429 AF647 conjugate (IgG-AF647) and 1  $\mu$ M tri-cTat B for 45 min (b) show homogenous distribution of  
430 Fab in cytosol and nucleus of cells with green nucleoli staining typical of tri-cTat B delivery; (c)  
431 Continuous live-cell confocal microscopy of trimers in HeLa cells treated with 500 nM Fab-AF647  
432 (red) and 1  $\mu$ M tri-cTat B (green); (d) quantification of the percentage of cells transduced with cargo  
433 (IgG-AF647 or Fab-AF647 - scored as positive when showing homogenous cytoplasmic and nucleolar  
434 fluorescence). Data presented as mean  $\pm$  standard deviation. Scale bar: 20  $\mu$ m.

435

436 **Fig. 5. Co-delivery of functional antibodies and antibody fragments in live HeLa cells.** HeLa  
437 cells were transfected with actin-RFP (a, b) or histone-RFP (c). 90 min post-wash live cell confocal  
438 microscopy images of cells treated with (a) 500 nM anti- $\beta$ -actin mouse Fab-AF647 conjugate ( $\beta$ -actin-  
439 Fab-AF647) and 1  $\mu$ M tri-cTat B for 30 min show co-localization of Fab (red) with actin stress fibres  
440 (orange); (b) 166 nM anti- $\beta$ -actin mouse IgG<sub>2b</sub> AF647 conjugate ( $\beta$ -actin-IgG-AF647) and 1  $\mu$ M tri-  
441 cTat B for 30 min show co-localization of antibody with actin stress fibres; (c) 166 nM anti-RFP mouse  
442 IgG<sub>1</sub> AF647 conjugate (RFP-IgG-AF647) and 1  $\mu$ M tri-cTat B for 30 min show co-localization of  
443 antibody with RFP fused to histone in the nucleus. G = green channel (tri-cTat B); O = orange channel  
444 (RFP fusion protein); R = red channel (AF647); Co-localization panel: co-localized pixels are shown  
445 as a mask of yellow pixels of constant intensity and all results shown present a significant correlation  
446 and are co-localized; BF = brightfield; scale bar: 20  $\mu$ m.

447

448 **Fig. 6. Proximity ligation assays (PLA).** PLA were performed in HeLa cells using an H2B-AF488  
449 antibody and a histone H2A.Z antibody. H2B-AF488 (166 nM) was co-delivered into cells using cTat<sub>3</sub>-  
450 alkyne (2  $\mu$ M, 1h incubation at 37 °C, 5% CO<sub>2</sub>). Negative controls consisted in the co-delivery of a  
451 mouse non-specific (NS) antibody and an antibody against  $\beta$ -actin (166 nM IgG, 2  $\mu$ M cTat<sub>3</sub>-alkyne, 1  
452 h incubation at 37 °C, 5% CO<sub>2</sub>) and in the incubation of non-specific,  $\beta$ -actin, H2B-AF488 and H2A.Z,  
453 antibodies after fixation and permeabilization of the cells and. a) Confocal microscopy images  
454 showing Hoechst 33342 stained nuclei (blue), PLA signals (red) and an overlay of the fluorescent  
455 channels. b) The number of PLA signals was quantified in the nuclei using CellProfiler and  
456 represented using Origin in at least 50 cells (IgG incubation controls: No abs, n=57; NS, n=55;  $\beta$ -  
457 actin, n= 76; H2B, n=55; H2A.Z, n=100. IgG codelivery controls: NS, n= 87;  $\beta$ -actin, n=90. PLA  
458 delivery, n=98) over three independent experiments. Data presented as mean  $\pm$  SD. A. One way  
459 analysis of variance (ANOVA) with Tukey's test correction were employed in statistical analysis.  
460 \*\*\*\*p<0.0001. Scale bars: 20  $\mu$ m.

461

462 **References**

- 463 1 Carter, P. J. & Lazar, G. A. Next generation antibody drugs: pursuit of the 'high-  
464 hanging fruit'. *Nature Reviews Drug Discovery* **17**, 197-223, (2018).
- 465 2 Verdine, G. L. & Walensky, L. D. The challenge of drugging undruggable  
466 targets in cancer: lessons learned from targeting BCL-2 family members. *Clin.*  
467 *Cancer. Res.* **13**, 7264-7270, (2007).
- 468 3 Stewart, M. P. *et al.* In vitro and ex vivo strategies for intracellular delivery.  
469 *Nature* **538**, 183-192, (2016).
- 470 4 Samal, S. K. *et al.* Cationic polymers and their therapeutic potential. *Chem.*  
471 *Soc. Rev.* **41**, 7147-7194, (2012).
- 472 5 Brooks, H., Lebleu, B. & Vivès, E. Tat peptide-mediated cellular delivery: back  
473 to basics. *Adv. Drug Del. Rev.* **57**, 559-577, (2005).
- 474 6 Peraro, L. & Kritzer, J. A. Emerging methods and design principles for cell-  
475 penetrant peptides. *Angew. Chem. Int. Ed. Engl.* **57**, 11868-11881, (2018).
- 476 7 Pei, D. & Buyanova, M. Overcoming endosomal entrapment in drug delivery.  
477 *Bioconj. Chem.* **30**, 273-283, (2019).
- 478 8 Fu, A., Tang, R., Hardie, J., Farkas, M. E. & Rotello, V. M. Promises and pitfalls  
479 of intracellular delivery of proteins. *Bioconj. Chem.* **25**, 1602-1608, (2014).
- 480 9 Fawell, S. *et al.* Tat-mediated delivery of heterologous proteins into cells. *Proc.*  
481 *Natl. Acad. Sci. USA.* **91**, 664-668, (1994).
- 482 10 Cornelissen, B. *et al.* Imaging DNA damage in vivo using  $\gamma$ H2AX-targeted  
483 immunoconjugates. *Cancer Res.* **71**, 4539-4549, (2011).
- 484 11 Singh, K., Ejaz, W., Dutta, K. & Thayumanavan, S. Antibody delivery for  
485 intracellular targets: emergent therapeutic potential. *Bioconj. Chem.* **30**, 1028-  
486 1041, (2019).

- 487 12 Brock, R. The uptake of arginine-rich cell-penetrating peptides: putting the  
488 puzzle together. *Bioconj. Chem.* **25**, 863-868, (2014).
- 489 13 Madani, F., Lindberg, S., Langel, U., Futaki, S. & Gräslund, A. Mechanisms of  
490 cellular uptake of cell-penetrating peptides. *J. Biophys.* **2011**, 414729, (2011).
- 491 14 Dougherty, P. G., Sahni, A. & Pei, D. Understanding cell penetration of cyclic  
492 peptides. *Chem. Rev.* **119**, 10241-10287, (2019).
- 493 15 Milletti, F. Cell-penetrating peptides: classes, origin, and current landscape.  
494 *Drug Discov. Today* **17**, 850-860, (2012).
- 495 16 Nischan, N. *et al.* Covalent attachment of cyclic TAT peptides to GFP results in  
496 protein delivery into live cells with immediate bioavailability. *Angew. Chem. Int.*  
497 *Ed. Engl.* **54**, 1950-1953, (2015).
- 498 17 Herce, H. D. *et al.* Cell-permeable nanobodies for targeted immunolabelling  
499 and antigen manipulation in living cells. *Nature Chem* **9**, 762-771, (2017).
- 500 18 Schneider, A. F. L., Kithil, M., Cardoso, M. C., Lehmann, M. & Hackenberger,  
501 C. P. R. Cellular uptake of large biomolecules enabled by cell-surface-reactive  
502 cell-penetrating peptide additives. *Nature Chem* **15**, 1, (2021).
- 503 19 Akishiba, M. *et al.* Cytosolic antibody delivery by lipid-sensitive endosomolytic  
504 peptide. *Nature Chem* **9**, 751-761, (2017).
- 505 20 Ovacik, M. & Lin, K. Tutorial on monoclonal antibody pharmacokinetics and its  
506 considerations in early development. *Clin. Transl. Sci.* **11**, 540-552, (2018).
- 507 21 Kauffman, W. B., Fuselier, T., He, J. & Wimley, W. C. Mechanism matters: A  
508 taxonomy of cell penetrating peptides. *Trends Biochem. Sci.* **40**, 749-764,  
509 (2015).

- 510 22 Herce, H. D. & Garcia, A. E. Molecular dynamics simulations suggest a  
511 mechanism for translocation of the HIV-1 TAT peptide across lipid membranes.  
512 *Proc. Natl. Acad. Sci. USA.* **104**, 20805-20810, (2007).
- 513 23 Lawrence, M. S., Phillips, K. J. & Liu, D. R. Supercharging proteins can impart  
514 unusual resilience. *J. Am. Chem. Soc.* **129**, 10110-10112, (2007).
- 515 24 Cronican, J. J. *et al.* Potent delivery of functional proteins into mammalian cells  
516 in vitro and in vivo using a supercharged protein. *ACS Chem. Biol.* **5**, 747-752,  
517 (2010).
- 518 25 Freire, J. M., Almeida Dias, S., Flores, L., Veiga, A. S. & Castanho, M. A. R. B.  
519 Mining viral proteins for antimicrobial and cell-penetrating drug delivery  
520 peptides. *Bioinformatics* **31**, 2252-2256, (2015).
- 521 26 Tung, C.-H., Mueller, S. & Weissleder, R. Novel branching membrane  
522 translocational peptide as gene delivery vector. *Biorg. Med. Chem.* **10**, 3609-  
523 3614, (2002).
- 524 27 Angeles-Boza, A. M., Erazo-Oliveras, A., Lee, Y.-J. & Pellois, J.-P. Generation  
525 of endosomolytic reagents by branching of cell-penetrating peptides: tools for  
526 the delivery of bioactive compounds to live cells in cis or trans. *Bioconj. Chem.*  
527 **21**, 2164-2167, (2010).
- 528 28 Fu, J., Yu, C., Li, L. & Yao, S. Q. Intracellular delivery of functional proteins and  
529 native drugs by cell-penetrating poly(disulfide)s. *J. Am. Chem. Soc.* **137**,  
530 12153-12160, (2015).
- 531 29 Erazo-Oliveras, A. *et al.* Protein delivery into live cells by incubation with an  
532 endosomolytic agent. *Nat. Methods* **11**, 861-867, (2014).

- 533 30 Erazo-Oliveras, A. *et al.* The late endosome and Its lipid BMP act as gateways  
534 for efficient cytosolic access of the delivery agent dfTAT and Its  
535 macromolecular cargos. *Cell Chem Biol* **23**, 598-607, (2016).
- 536 31 Najjar, K. *et al.* Unlocking endosomal entrapment with supercharged arginine-  
537 rich peptides. *Bioconj. Chem.* **28**, 2932-2941, (2017).
- 538 32 Kez, C., Lin, H., Peter, D. W. & Arwyn, T. J. Endocytosis, intracellular traffic and  
539 fate of cell penetrating peptide based conjugates and nanoparticles. *Curr.*  
540 *Pharm. Des.* **19**, 2878-2894, (2013).
- 541 33 Jonkman, J., Brown, C. M., Wright, G. D., Anderson, K. I. & North, A. J.  
542 Tutorial: guidance for quantitative confocal microscopy. *Nat. Protoc.* **15**, 1585-  
543 1611, (2020).
- 544 34 Herbert, A. Available from:  
545 <http://www.sussex.ac.uk/gdsc/intranet/microscopy/UserSupport/AnalysisProtoc>  
546 [ol/imagej/colocalisation](http://www.sussex.ac.uk/gdsc/intranet/microscopy/UserSupport/AnalysisProtoc/ol/imagej/colocalisation),
- 547 35 Costes, S. V. *et al.* Automatic and quantitative measurement of protein-protein  
548 colocalization in live cells. *Biophys. J.* **86**, 3993-4003, (2004).
- 549 36 Ramirez, O., García, A., Rojas, R., Couve, A. & Härtel, S. Confined  
550 displacement algorithm determines true and random colocalization in  
551 fluorescence microscopy. *J. Microsc.* **239**, 173-183, (2010).
- 552 37 Söderberg, O. *et al.* Direct observation of individual endogenous protein  
553 complexes in situ by proximity ligation. *Nat. Methods* **3**, 995-1000, (2006).
- 554 38 Rouet, R. *et al.* Receptor-mediated delivery of CRISPR-Cas9 endonuclease for  
555 cell-type-specific gene editing. *J. Am. Chem. Soc.* **140**, 6596-6603, (2018).
- 556 39 Qian, Z. *et al.* Discovery and mechanism of highly efficient cyclic cell-  
557 penetrating peptides. *Biochemistry* **55**, 2601-2612, (2016).

558 40 Liu, H., Gaza-Bulseco, G., Faldu, D., Chumsae, C. & Sun, J. Heterogeneity of  
559 monoclonal antibodies. *J. Pharm. Sci.* **97**, 2426-2447, (2008).

560 41 Delavoie, F., Soldan, V., Rinaldi, D., Dauxois, J. Y. & Gleizes, P. E. The path of  
561 pre-ribosomes through the nuclear pore complex revealed by electron  
562 tomography. *Nat Commun* **10**, 497, (2019).

563 42 Paci, G., Zheng, T., Caria, J., Zilman, A. & Lemke, E. A. Molecular  
564 determinants of large cargo transport into the nucleus. *Elife* **9**, (2020).

565 43 Avrameas, A., Ternynck, T., Nato, F., Buttin, G. & Avrameas, S. Polyreactive  
566 anti-DNA monoclonal antibodies and a derived peptide as vectors for the  
567 intracytoplasmic and intranuclear translocation of macromolecules. *Proc. Natl.*  
568 *Acad. Sci. USA.* **95**, 5601-5606, (1998).

569 44 Gordon, R. E., Nemeth, J. F., Singh, S., Lingham, R. B. & Grewal, I. S.  
570 Harnessing SLE autoantibodies for intracellular delivery of biologic  
571 therapeutics. *Trends Biotechnol.* **39**, 298-310, (2021).

572 45 Bernardes, N. E. & Chook, Y. M. Nuclear import of histones. *Biochem. Soc.*  
573 *Trans.* **48**, 2753-2767, (2020).

574 46 Placek, B. J., Harrison, L. N., Villers, B. M. & Gloss, L. M. The H2A.Z/H2B  
575 dimer is unstable compared to the dimer containing the major H2A isoform.  
576 *Protein Sci.* **14**, 514-522, (2005).

577

578 **Methods**

579 *Methods and additional data also available in supporting information.*

580

581 **Synthesis of Tat-conjugates.**

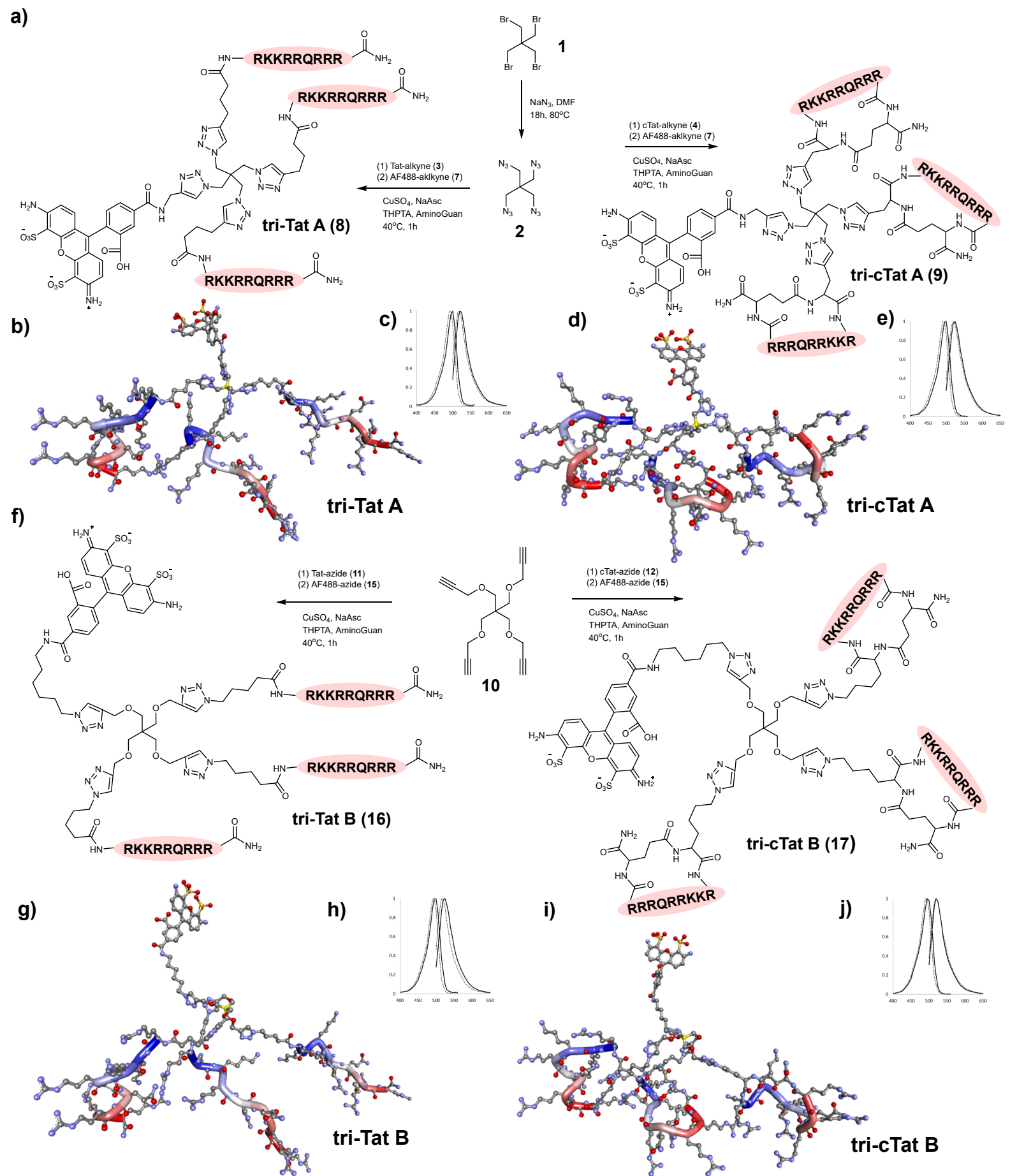
582 Peptide and fluorophores were conjugated to tetrakis scaffolds via copper-catalysed  
583 azide alkyne cycloaddition reactions (CuAAC), using azide / alkyne starting materials  
584 and 1 eq. CuSO<sub>4</sub>, 5 eq. tris((1-hydroxy-propyl-1H-1,2,3-triazol-4-yl)methyl)amine  
585 (THPTA), 2 eq. sodium L-ascorbate, 3 eq. aminoguanidine hydrochloride per  
586 cycloaddition, followed by HPLC purification and analysis by mass spectrometry.  
587 Azide functionalized scaffold A (1,3-diazido-2,2-bis(azidomethyl)propane, **2**) was  
588 used to synthesize **Tri-Tat A** and **tri-cTat A**; alkyne functionalized scaffold B  
589 (tetakis(2-propynyloxymethyl)methane, **10**) was used to synthesize **tri-Tat B** and **tri-**  
590 **cTat B**. Linear Tat (49-57) peptide (RKKRRQRRR), modified with a hexynoyl  
591 (alkyne) (**3**) or an azido-pentanoyl (azide) (**11**) functional group at the N-terminus  
592 was obtained from International Peptides Inc., Louisville, KY, USA. Cyclic Tat was  
593 custom designed to match the linear peptide and synthesized by Cambridge  
594 Peptides, Birmingham, UK. Azide / alkyne functionality was added by including either  
595 an azide modified lysine (K(N<sub>3</sub>)) residue or propargyl glycine (Pra) at the N-terminus.  
596 Peptides were cyclized by addition of glutamic acid to the C-terminus for head to tail  
597 cyclisation to the N-terminus to generate cyclic Pra-RKKRRQRRRG (**4**) and  
598 K(N<sub>3</sub>)RKKRRQRRRG (**12**).

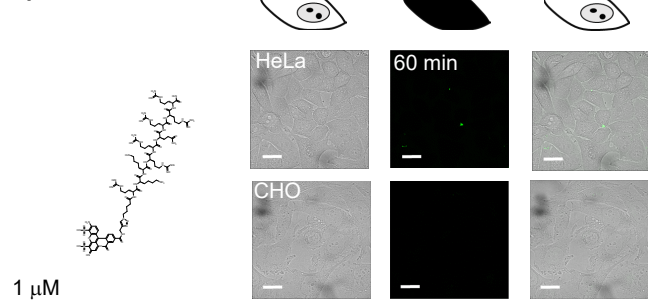
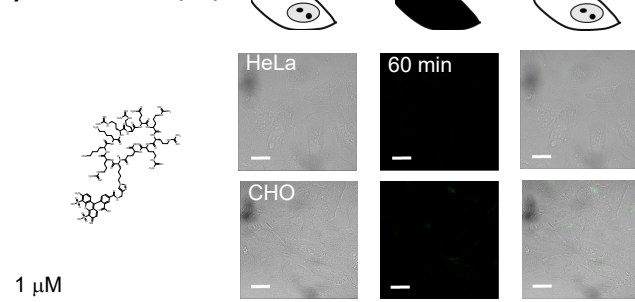
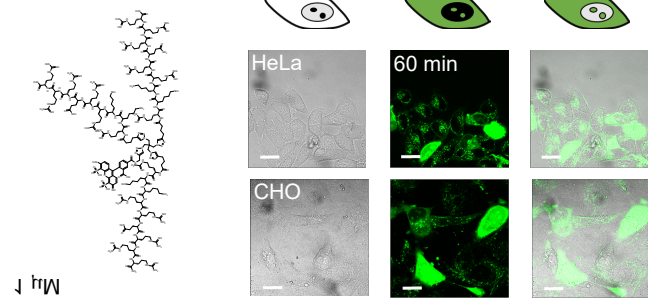
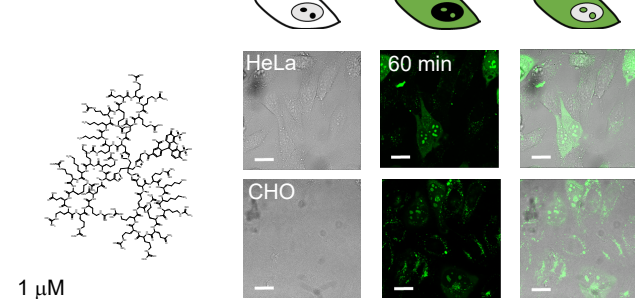
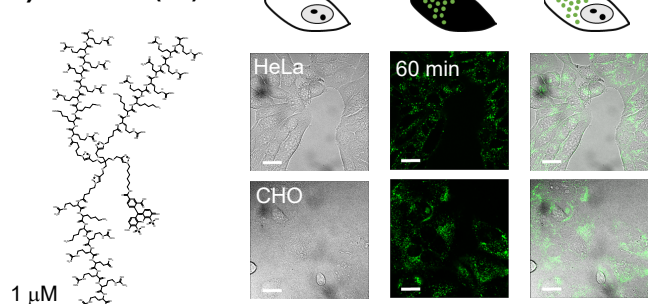
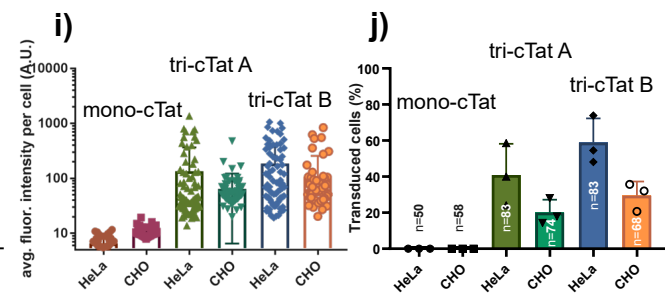
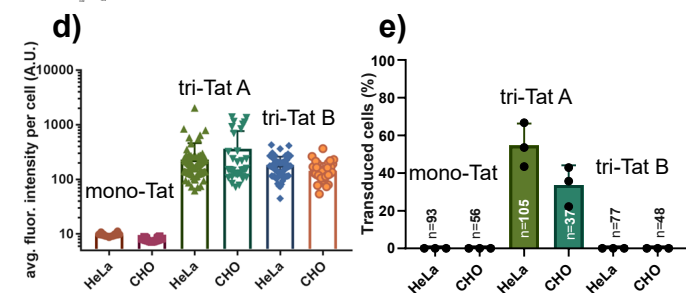
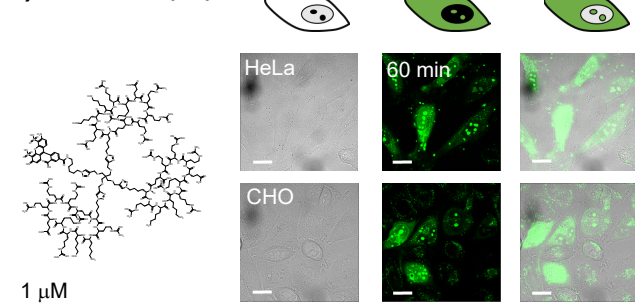
599

600 **Live cell confocal microscopy.**

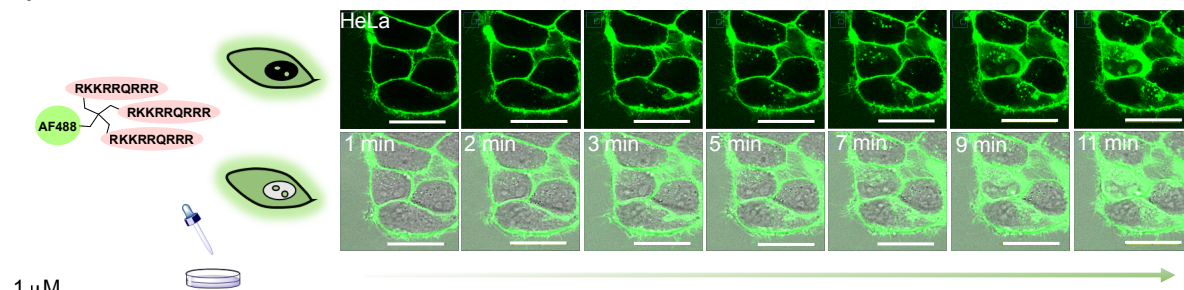
601 HeLa (obtained from ATCC; CCL-2) and CHO (obtained from institute repository)  
602 cells were cultured in DMEM supplemented with 10% FBS and penicillin /

603 streptomycin. For post-wash experiments, Tat conjugate was added to the cells in  
604 serum-free medium, cells incubated at 37 °C in an atmosphere of 5% CO<sub>2</sub>, culture  
605 medium removed at the desired time point, cells washed and transferred to the  
606 microscope for imaging. For time course or pre-wash experiments, cells were  
607 transferred to the microscope (incubation chamber at 37 °C, 5% CO<sub>2</sub>) and Tat  
608 conjugate added directly to cell medium and cells imaged at desired time points. Co-  
609 delivery experiments were conducted by adding peptide trimer immediately followed  
610 by cargo into serum free medium. Samples were visualised using a Zeiss LSM 780  
611 inverted confocal microscope fitted with a XLmultiS1 incubation chamber and Plan-  
612 Apochromat 63x / 1.40 Oil DIC M27 objective. Images were analysed using ImageJ  
613 software. Digital adjustments and image processing are consistent for all  
614 experiments, unless otherwise stated in the figure legend. Statistical analyses were  
615 carried out using GraphPad Prism 7 or Origin software and all data used for  
616 statistical analysis consists of measurements from distinct cells. Where applicable a  
617 parametric, unpaired, two-tailed t-test was used for statistical testing.

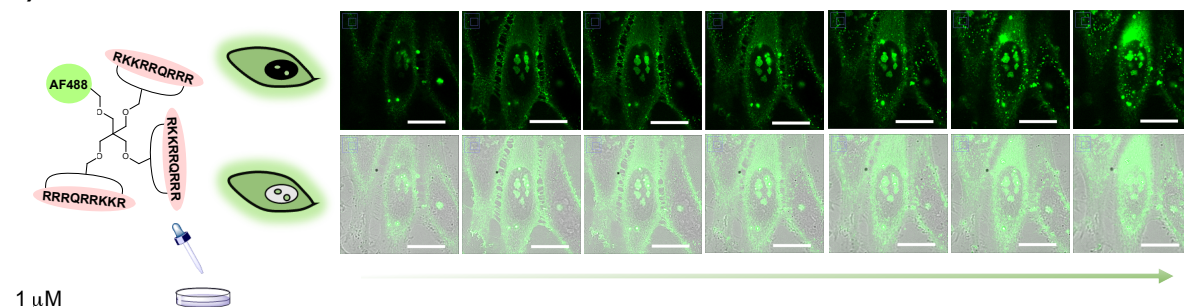


**a) mono-Tat (18)****f) mono-cTat (19)****b) tri-Tat A (8)****g) tri-cTat A (9)****c) tri-Tat B (16)****h) tri-cTat B (17)**

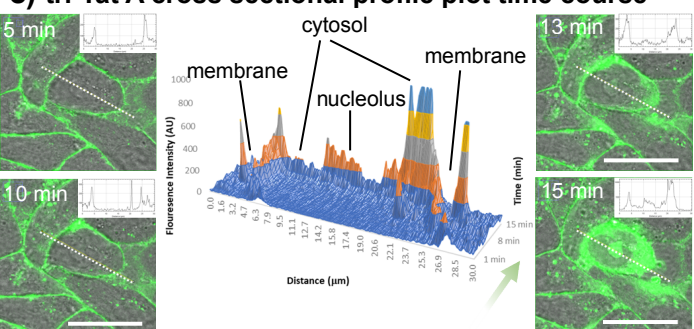
**a) tri-Tat A time course**



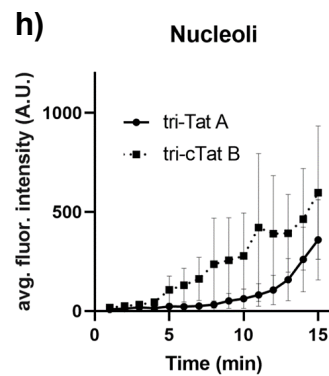
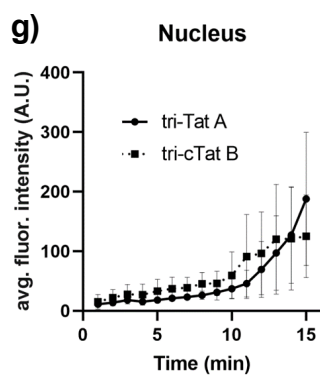
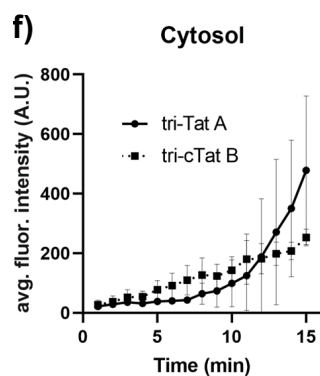
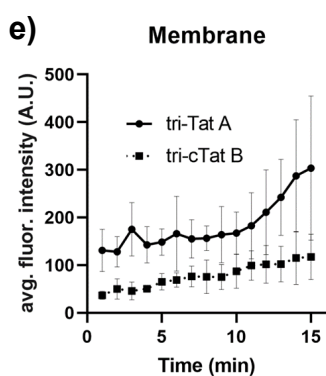
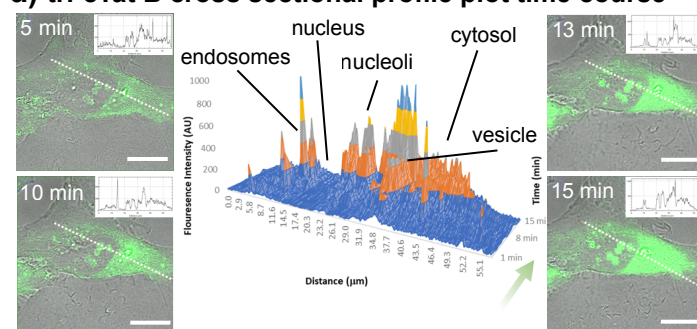
**b) tri-cTat B time course**

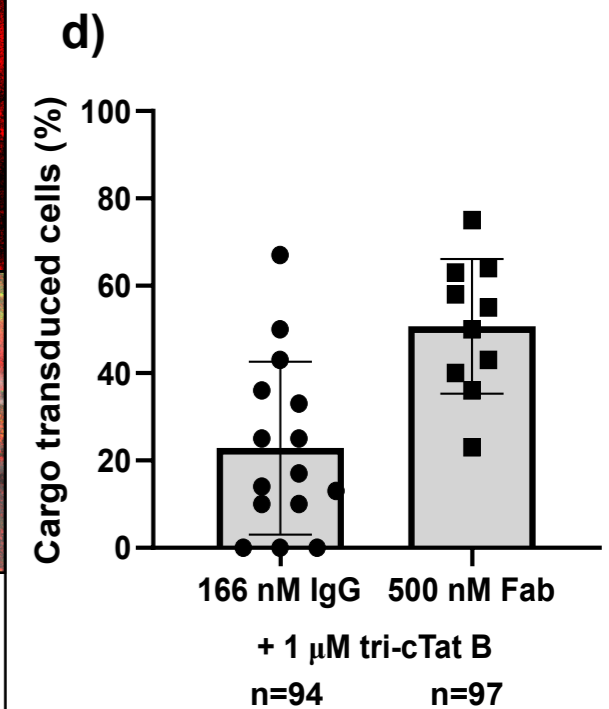
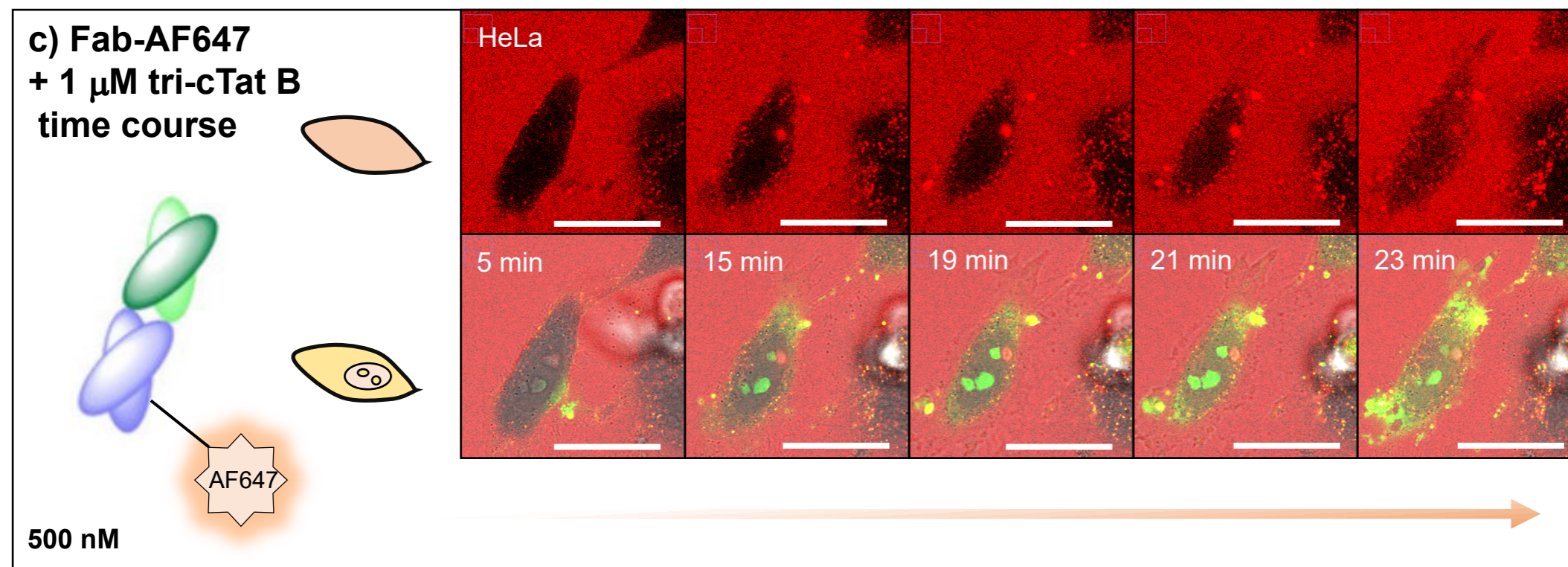
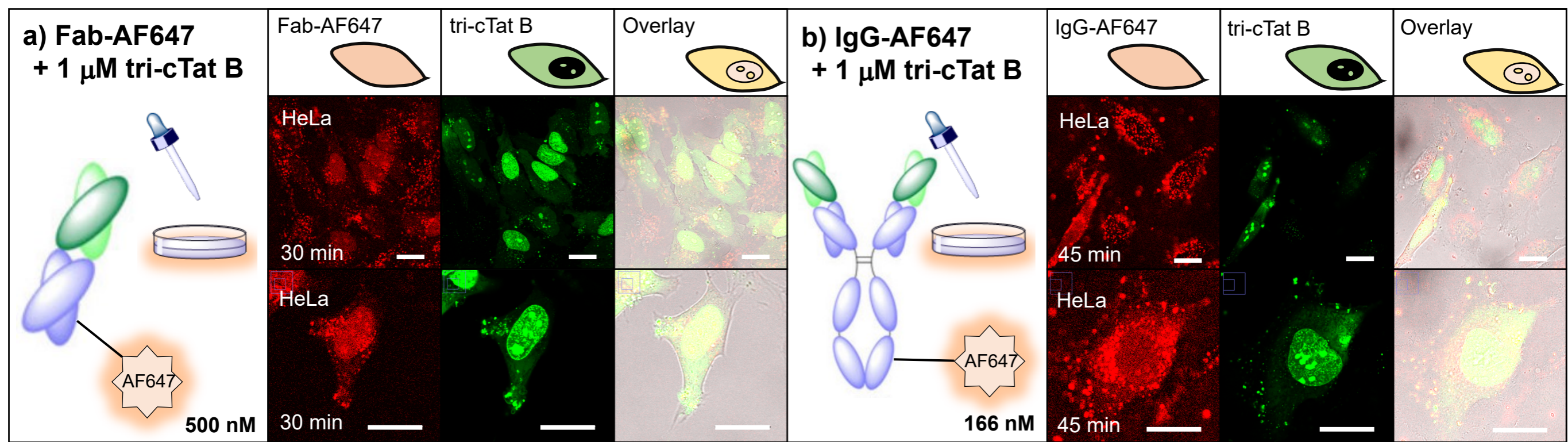


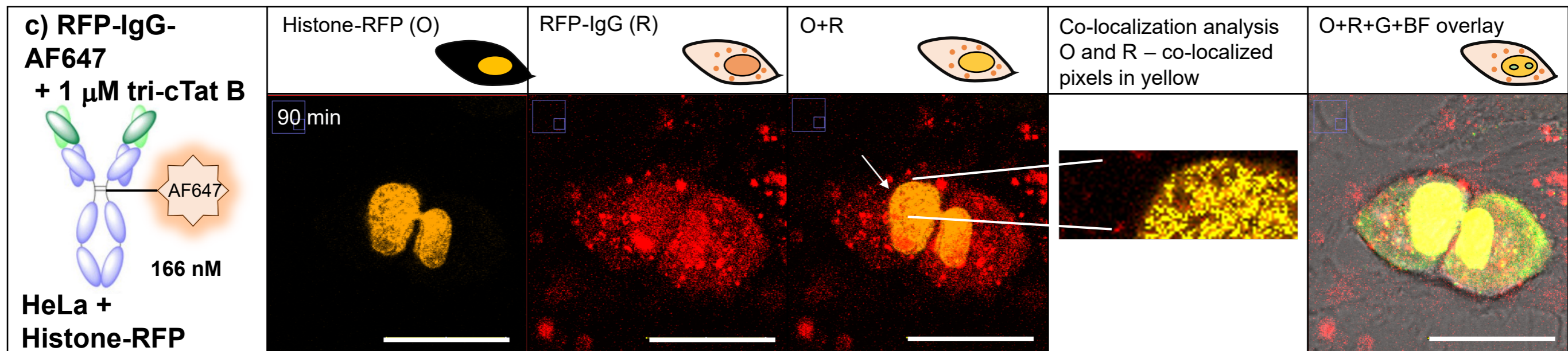
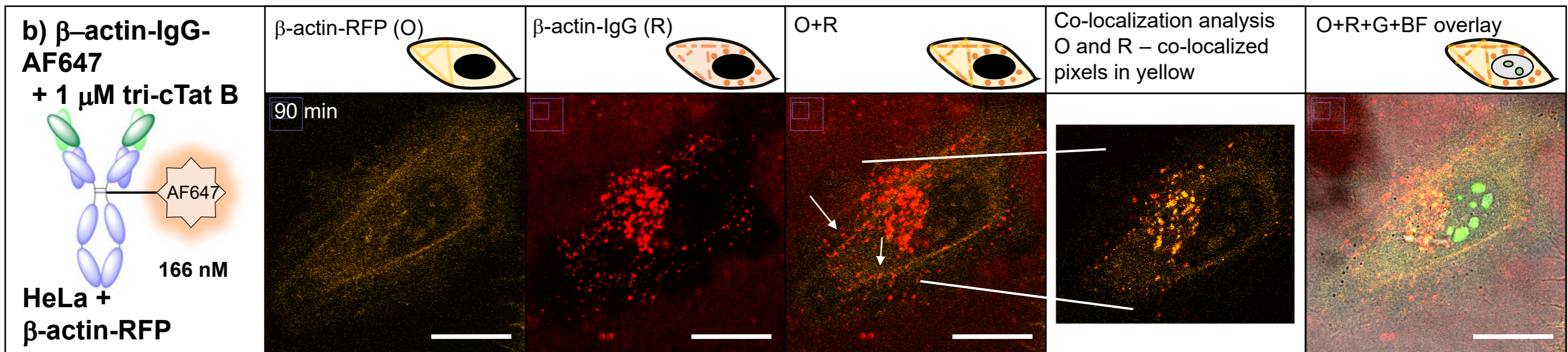
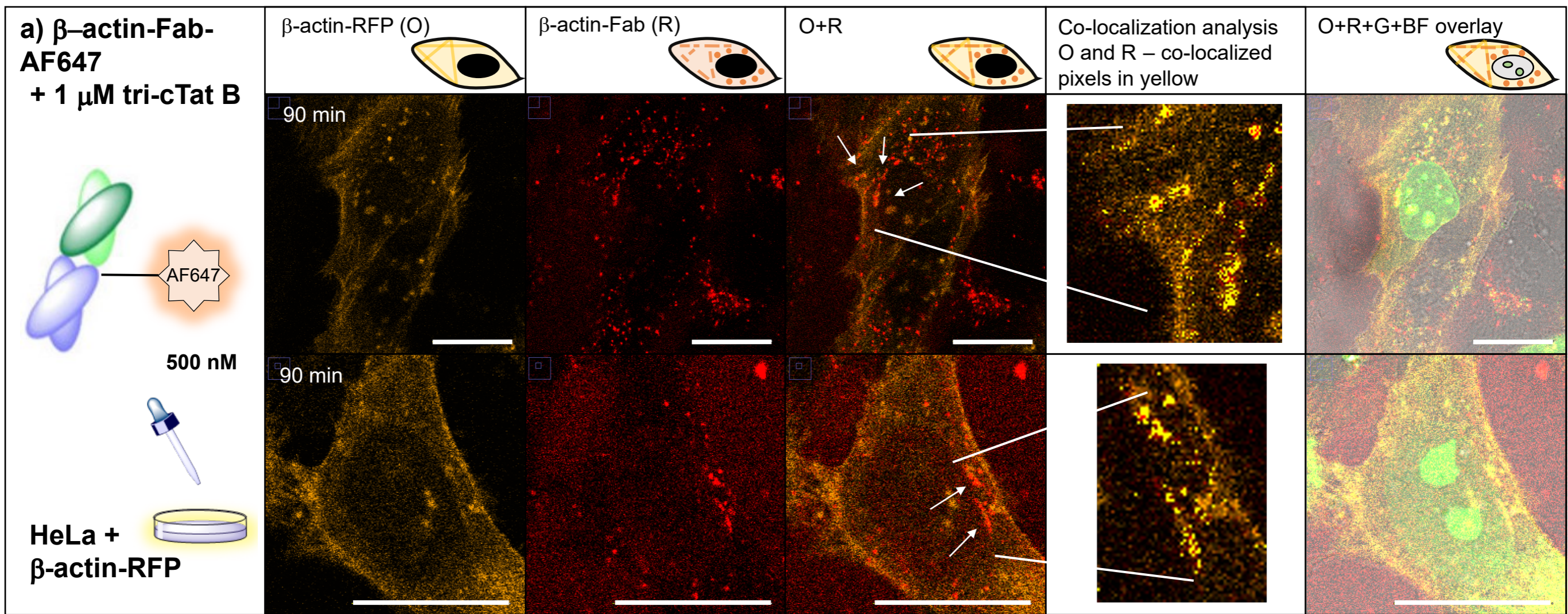
**c) tri-Tat A cross sectional profile plot time course**



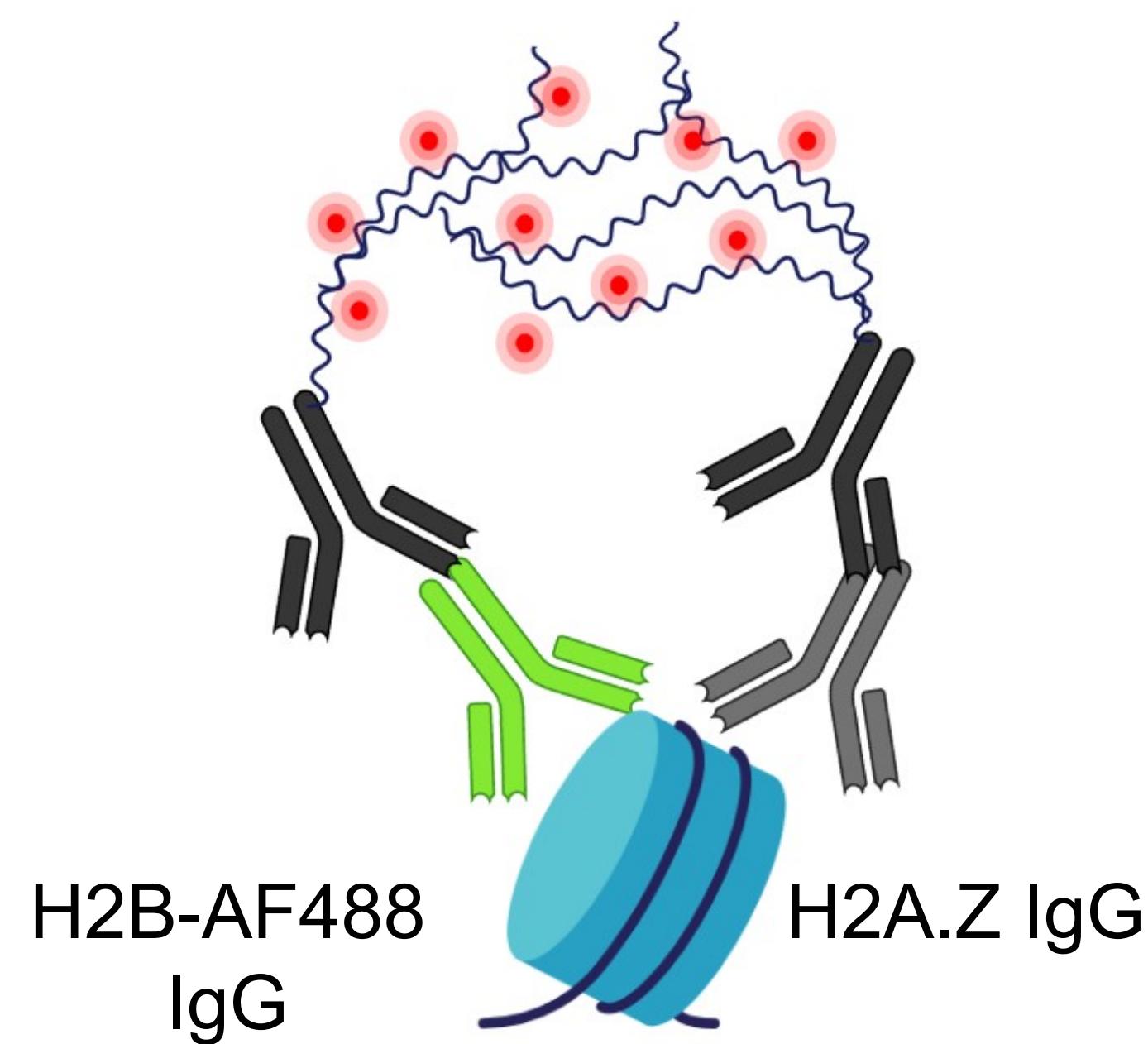
**d) tri-cTat B cross sectional profile plot time course**



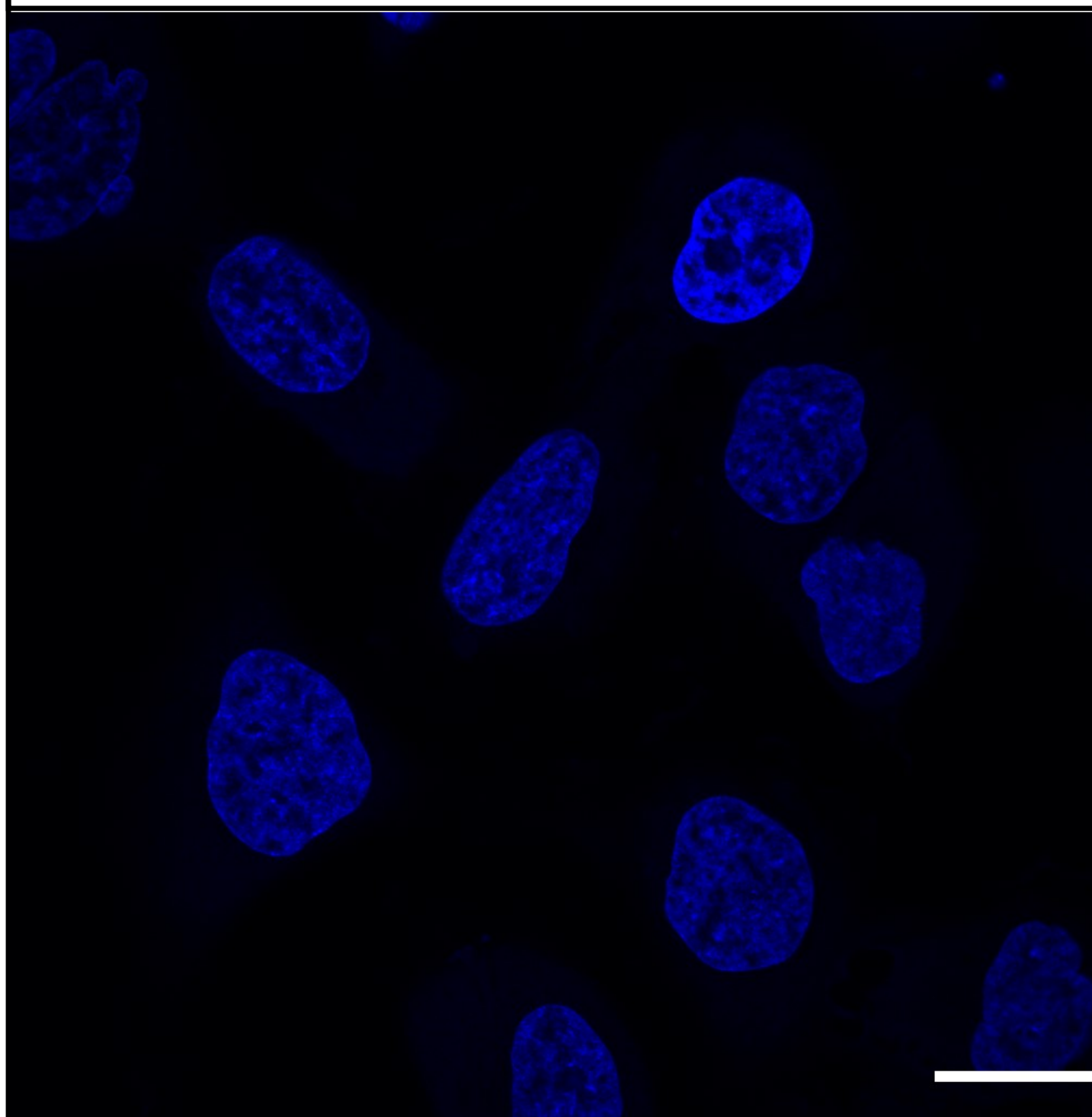




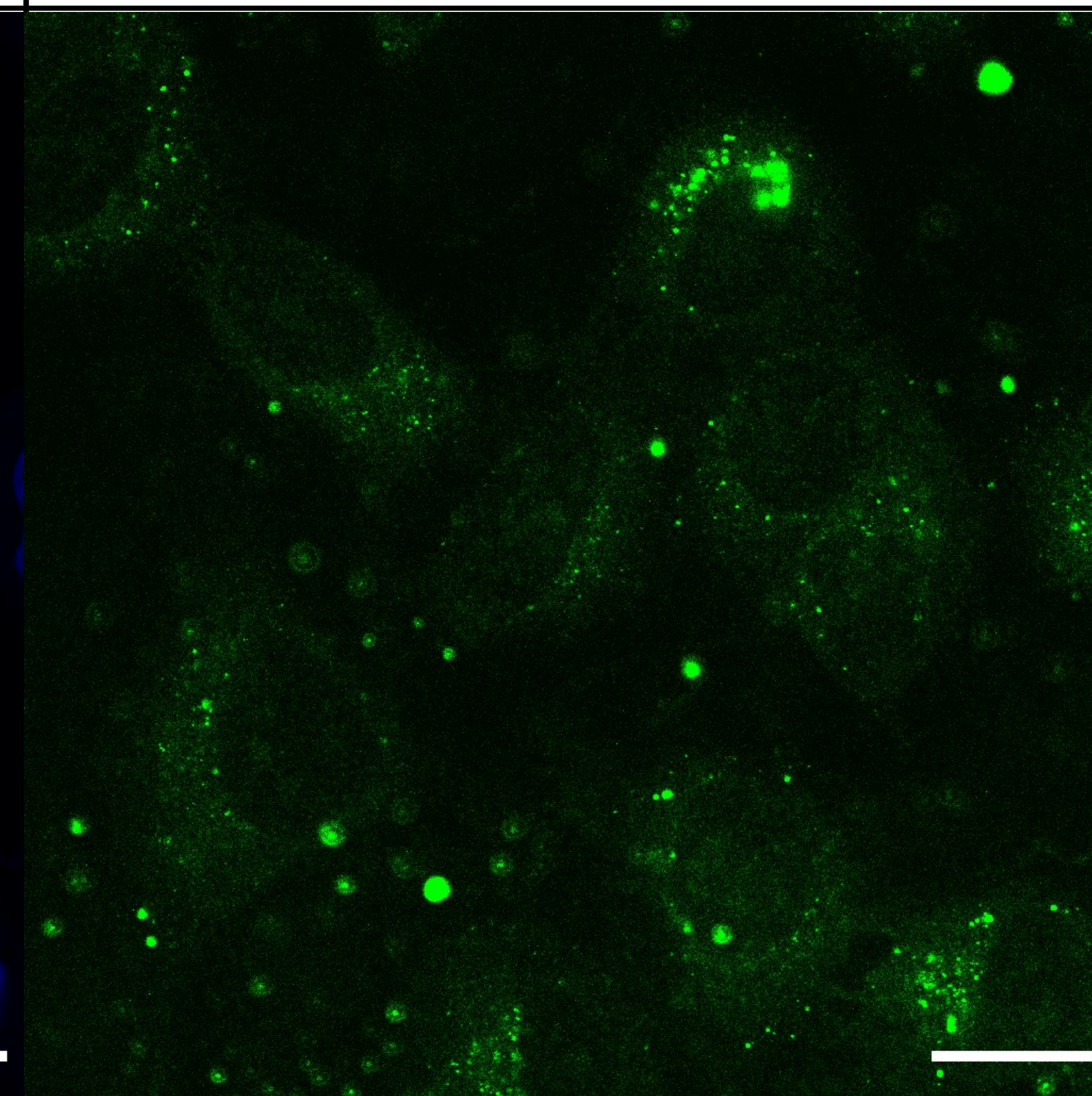
**a) Proximity Ligation assay (PLA) images**



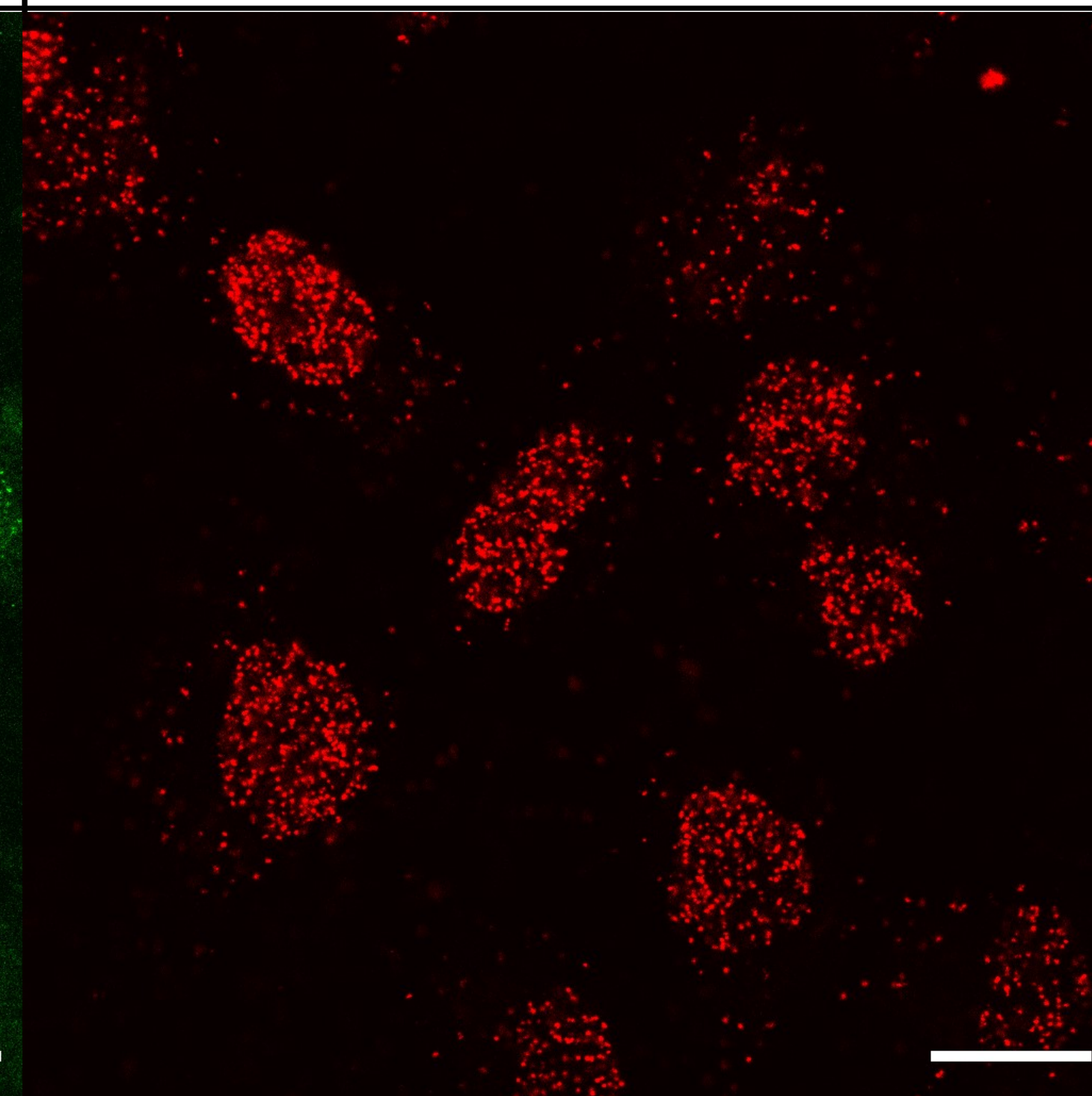
Hoechst (nuclear stain)



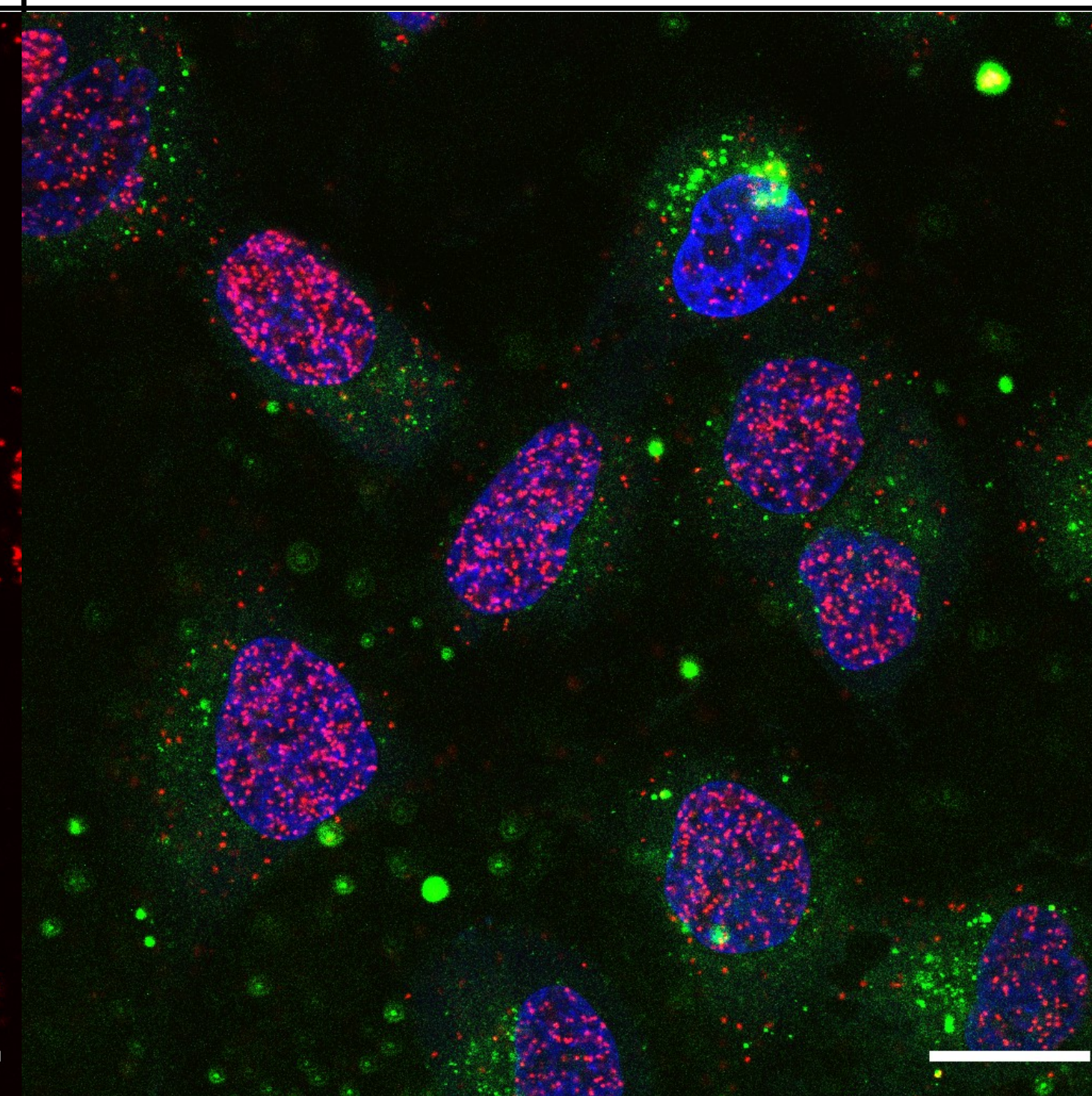
H2B-AF488 IgG



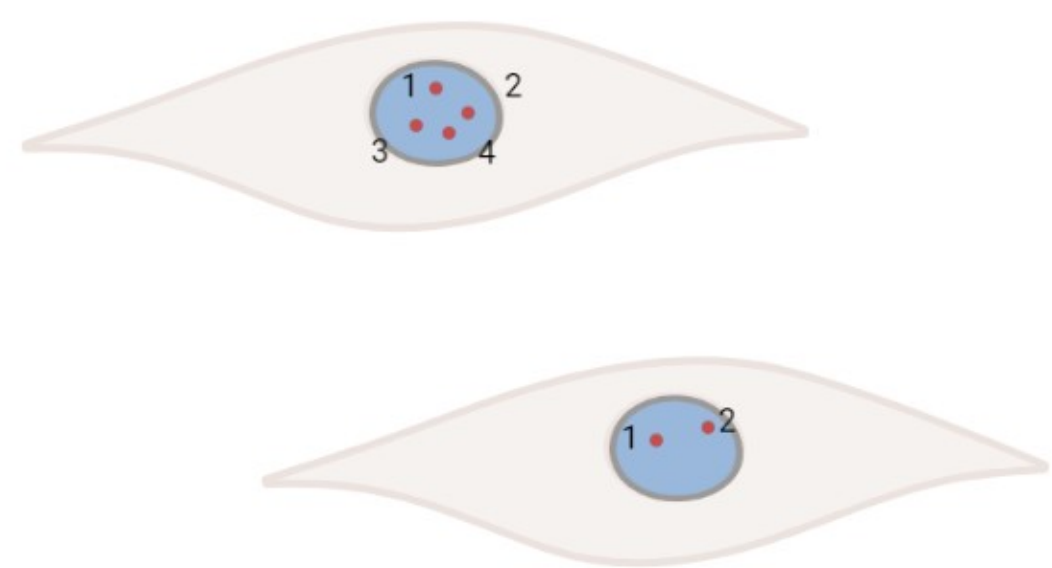
PLA signal



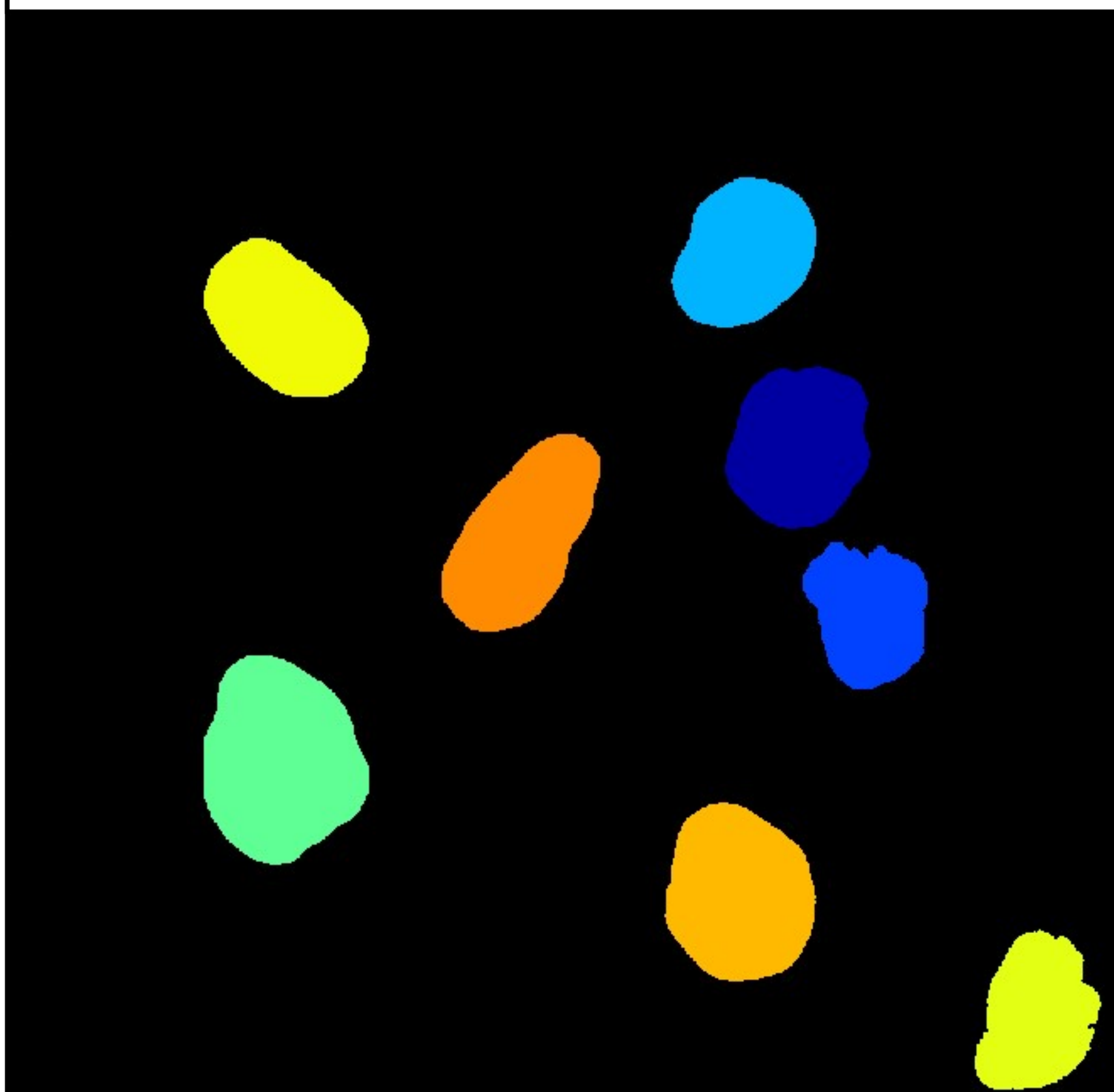
Overlay



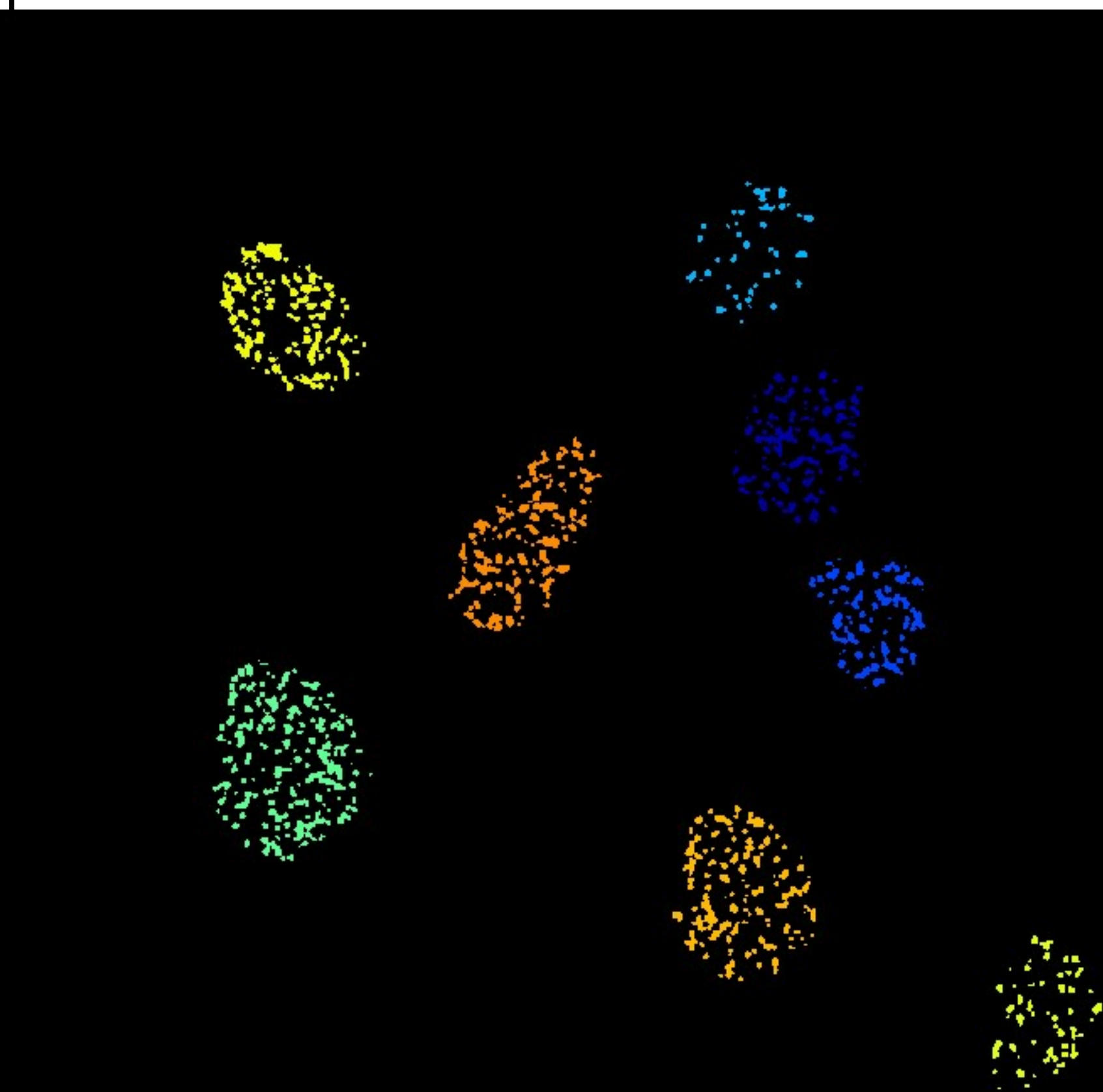
**b) Quantification of PLA signals**



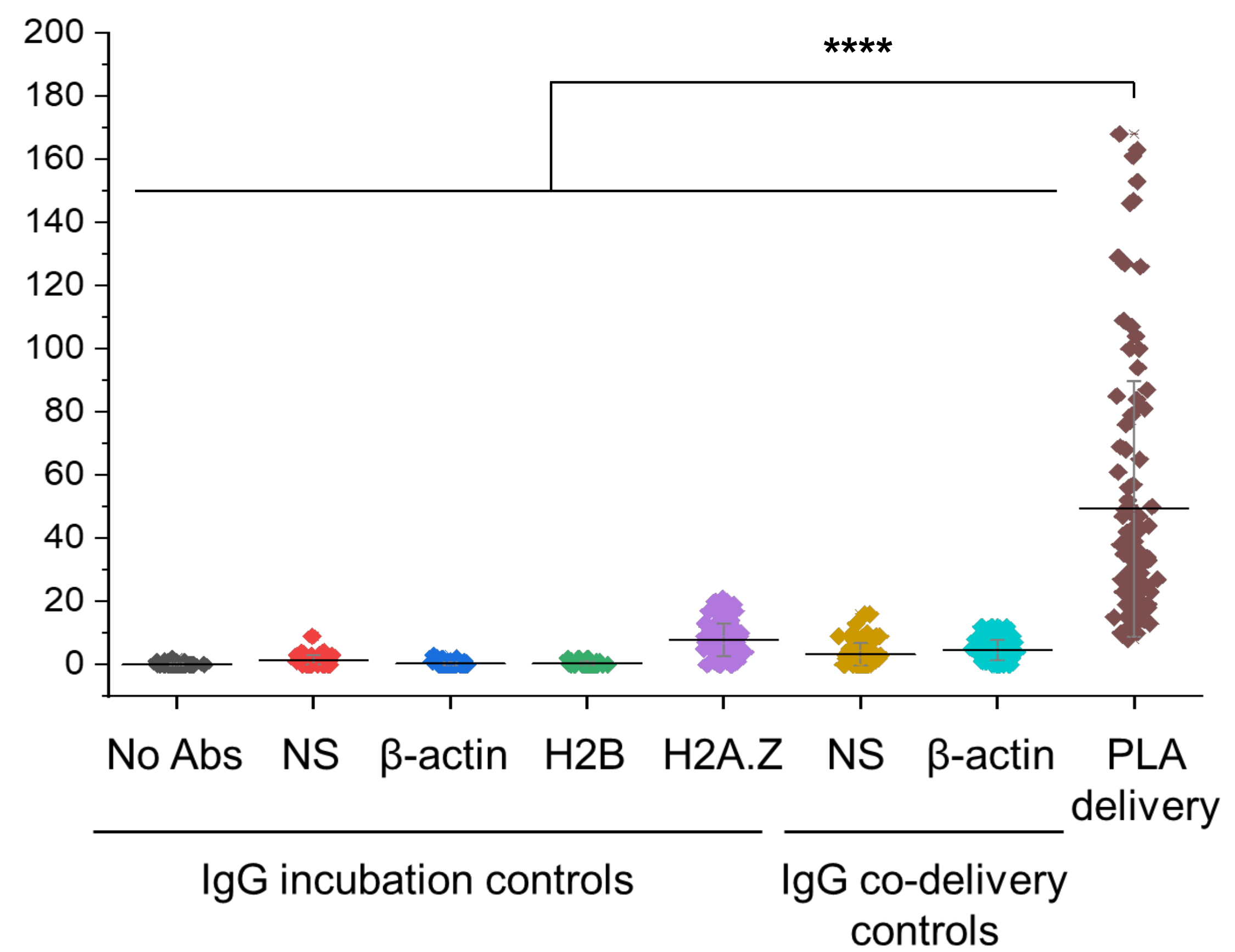
Mask of nuclei



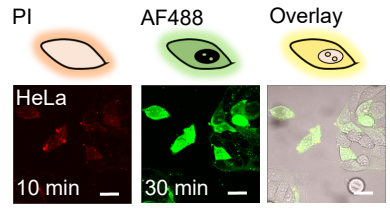
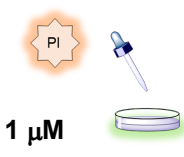
PLA labelled by nuclei



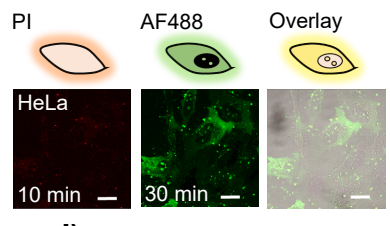
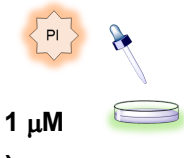
Number of PLA signals per nuclei



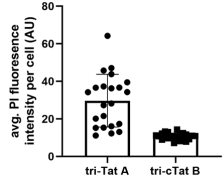
**a) tri-Tat A +PI**



**b) tri-cTat B +PI**



**c)**



**d)**

