

Porous nematic microfluidics for generation of umbilic defects and umbilic defect lattices

Jure Aplinc,¹ Stephen Morris,² and Miha Ravnik^{1,3,*}

¹*Faculty of Mathematics and Physics, University of Ljubljana, Jadranska 19, 1000 Ljubljana, Slovenia*

²*Department of Engineering Science, University of Oxford, Parks Road, Oxford OX1 3PJ, UK*

³*Jozef Stefan Institute, Jamova 39, 1000 Ljubljana, Slovenia*

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We demonstrate that porous nematic microfluidics is a potential route for the generation of nematic umbilic defects and regular umbilic defect lattices. By using numerical modelling we show that the mutual – backflow – coupling between the flow velocity and the orientation director field of nematic liquid crystal leads to formation of + umbilic defects at local peaks and to formation of – umbilic defects at the local saddles in the flow profile. The number of the flow peaks and the complexity of the flow saddles (i.e. the number of the valleys) is shown to be directly related to the strength of the umbilic defect, effectively relating the two fields at the geometrical level. The regular arrangement of the barriers in the porous channels is demonstrated to lead to formation of regular lattices of umbilic defects, including square, triangular and even Kagome. Experimental realisation of such systems is discussed, with particular focus towards microfluidic-tunable birefringent photonic band structures and lattices.

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I. INTRODUCTION

Microfluidics considers the flow of fluids in submillimeter-sized systems and typically under the influence of external forces [1]. The interest in microfluidics grew strongly in the last couple decades because of the rapid evolution of lab-on-a-chip systems [1, 2] which are 1000 times smaller compared with laboratory setups and are able to deal with very small volumes (1 nL or 1 pL) of samples [1]. At these volume scales, the typical volume forces (such as gravity and inertia) – which are prominent in our daily life – generally become less important and instead forces such as surface tension and shear stress become dominant. The Reynolds number (Re) is generally small at these scales, so the fluid flow is in the laminar regime, which is controllable and predictable [3, 4].

In addition to simple isotropic fluids, there is considerable fundamental and applied interest in the microfluidics of complex liquid crystalline fluids, as the internal structures of the fluid allow for novel mechanisms of manipulation, driving and steering [5–12]. Nematic liquid crystals are best known for their technological use in display devices, but are at the modern state-of-the-art level also capable of forming ferromagnetic fluids [13, 14], driving the colloidal self-assembly [15–18], transporting particles along topological defect lines [19] and manipulating the flow-of-light at the microscopic level [20, 21]. The distinction of nematic liquid crystals from isotropic fluids lies in the orientational ordering of liquid crystal molecules caused by their anisotropic shape. This anisotropy notably affects also the flow of nematic liquid

crystals, where the coupling between the (material) flow and the orientational order is called the backflow [22]. In the presence of flow velocity gradients, the backflow coupling causes the reorientation of the nematic director, i.e. it changes the average molecular orientation field. Typically, regimes of rotating director (flow tumbling regime) or steady state director with fixed angle between the director and flow gradient (flow aligning regime) are observed [23].

The lowest free energy state of a (non-flowing) nematic is a homogeneous director field with a uniform nematic degree of order. However, in most cases, such configuration is not compatible with the boundary conditions imposed by the surfaces or the external fields and the orientational order is frustrated. This frustration leads to formation of discontinuities in the director field, which are called defects [24–31]. Molecular orientation in the defect cores fluctuates rapidly and on average does not have a preferable direction of orientation. The vortex-like defects have accompanied liquid crystals since their discovery in 1889 by Lehmann [32], they are present also in a variety of fields of physics. Vortices attract a lot of attention because of their universal character, as they are solutions of the complex Ginzburg-Landau equation [33–35] that describes different systems such as fluids, superfluids [36], superconductors, fluidized anisotropic granular matter, optical dielectrics, magnetic media, and strings from the field theory [33–35]. Defects are found even in light polarization singularities [37–39], and gravitational lensing shear fields [40]. In particular defects in liquid crystals have proved to be a useful laboratory tool for studying defect behaviour in cosmology [41].

In contrast with the conventional defects in liquid crystals, with a discontinuity at the center, umbilic defects have a continuous core and the discontinuity emerges

* Email: miha.ravnik@fmf.uni-lj.si

only in the *projection* of the director field to a distinct plane perpendicular to the far field orientation [42]. These defects are also often interpreted as integer defects that have escaped in the third dimension. Liquid crystal umbilic defects are generally created by proper selection of anchoring, topology [43] and applied electric [34, 42, 44–49] or magnetic fields [50, 51] and even light pulses [52, 53]. Recently, generation of umbilics by a Poiseuille flow was demonstrated [50, 51] and anisotropic annihilation dynamics of umbilic defects was studied [54, 55]. It is important to notice that today the major attention is given to *singular* (i.e. not umbilic) topological defects, which were shown even to form knots, links, and accompany complex shaped colloidal particles; but much less attention is given to umbilics. The likely reasons are that (i) they are not fundamentally “topological” (i.e. can be continuously transformed into a homogeneous field) and (ii) they are not simple to generate and stabilise. However, the ability to spontaneously generate umbilic defects in a controlled manner would be particularly interesting in the development of advanced photonic materials that consist of a defect site within a well-defined periodic structure. The presence of this defect site leads to a so-called defect mode that can enable either the propagation or trapping of light in an otherwise forbidden band. Unlike the conventional topological defects that are observed in liquid crystals, these umbilic defects may enable extended light propagation through a structure and lead to other interesting optical phenomena not observed with their topological counterparts. Furthermore, through the creation of a lattice of umbilic defects it may be possible to create a photonic lattice of defects. And the idea of this paper is to show that umbilics can emerge naturally as steady-state structures in complex fluids and are actually elementary objects to emerge as a result of backflow coupling between the leadingly nonsingular nematic orientational order and the general flow profile characterised by multiple flow peaks and flow saddles.

In this paper, we demonstrate backflow driven formation of umbilic (nonsingular) defects and regular defect arrays within porous nematic microfluidic channels using numerical modelling. Umbilic defects of various strengths are controllably generated by setting different complex flow profiles, that distinctly include peak and saddle points. Umbilics of positive umbilic strength are found to emerge from multipeak flow profiles, with the number of flow peaks directly corresponding to the umbilic strength. Alternatively, umbilic defects of negative umbilic strength are found to emerge from saddle points in the flow profile, with the number of the valleys of the saddle determining the umbilic strength. By introducing microchannels with regular porosity, we demonstrate the formation of various umbilic defect lattices, notably including also Kagome lattice, which is an indication of the conceptual diversity of umbilic defect states that can be generated in such porous systems via the proposed microfluidic approach. Experimental realisation of um-

bilic states is outlined, with particular focus on the application of umbilic defect lattices as photonic elements, i.e. microfluidics tunable photonic crystals, where the effective dielectric constant of such microfluidics-generated photonic crystal could be tuned by the magnitude of the flow. Finally, the proposed work is an approach towards topology conditioned microfluidics and microrheology.

II. METHODS AND MODELLING

A strong approach for exploring the dynamics of nematic complex fluids and the related dynamic nematic structures is numerical modelling based on Berris-Edwards model of nematodynamics [56]. Such an approach can explore a wide phase-space, and gives good qualitative or even quantitative agreement with experiments. Within the Berris-Edwards model the orientational order of nematic liquid crystal is characterised by a symmetric and traceless order parameter tensor Q_{ij} and the flow of nematic is described by the velocity flow field u_i and density ρ . Time-evolution equations for the mutually – backflow – coupled orientational field and material flow are given as:

$$(\partial_t + u_k \partial_k) Q_{ij} - S_{ij} = \Gamma H_{ij}, \quad (1)$$

$$\begin{aligned} \rho(\partial_t + u_k \partial_k) u_i = & \partial_j \Pi_{ij} + \eta \partial_j [\partial_i u_j + \partial_j u_i \\ & + (1 - 3\partial_\rho P) \partial_k u_k \delta_{ij}], \end{aligned} \quad (2)$$

where ∂_t is derivative in time, ∂_i is derivative in the Cartesian spatial coordinate x, y, z , Γ is the liquid crystal rotational diffusion coefficient, η is the viscosity and Π_{ij} is the stress tensor

$$\begin{aligned} \Pi_{ij} = & -P \delta_{ij} + 2\xi(Q_{ij} + \delta_{ij}/3)(Q_{kl} H_{lk}) \\ & - \xi H_{ik}(Q_{kj} + \delta_{kj}/3) - \xi(Q_{ik} + \delta_{ik}/3) H_{kj} \\ & - \partial_i Q_{kl} \frac{\delta \mathcal{F}}{\delta \partial_j Q_{lk}} + Q_{ik} H_{kj} - H_{ik} Q_{kj}, \end{aligned} \quad (3)$$

where parameter ξ depends on the molecular details of a given liquid crystal. Summation over repeated indices is assumed. The relaxation to equilibrium of Q_{ij} is determined by the molecular field H_{ij} which originates from the equilibrium free energy \mathcal{F} of an elastic anisotropic fluid, $H_{ij} = -\frac{\delta \mathcal{F}}{\delta Q_{ij}} + \text{Tr} \frac{\delta \mathcal{F}}{\delta Q_{kl}} \delta_{ij}/3$, where

$$\begin{aligned} \mathcal{F} = & \int_V [L(\partial_k Q_{ij})^2/2 + A Q_{ij} Q_{ji}/2 + B Q_{ij} Q_{jk} Q_{ki}/3 \\ & + C(Q_{ij} Q_{ji})^2/4] dV, \end{aligned} \quad (4)$$

L is a single nematic elastic constant, and A, B, C are material constants. The advection term S_{ij} and effective compressibility term are defined as

$$S_{ij} = (\xi D_{ik} + \Omega_{ik})(Q_{kj} + S\delta_{kj}/2) + (Q_{ik} + S\delta_{ik}/2) \\ \times (\xi D_{kj} - \Omega_{kj}) - 2\xi(Q_{ij} + S\delta_{ij}/2)(Q_{kl}\partial_k u_l), \quad (5)$$

$$P = P_0\rho - L(\partial_k Q_{ij})^2/2, \quad (6)$$

where $D_{ij} = (\partial_j u_i + \partial_i u_j)/2$, $\Omega_{ij} = (\partial_j u_i - \partial_i u_j)/2$ and P_0 is the hydrostatic pressure.

We solve the dynamic equations for the flow u_i and the orientational order parameter Q_{ij} by using the hybrid lattice Boltzmann algorithm [6, 57, 58]. The time evolution for Q_{ij} is calculated by using the finite difference scheme in time, whereas the equation for u_i is solved by the D3Q15 lattice Boltzmann method [58]. The simulations are performed in a slice through the microchannel with a cubic lattice; typically $200 \times 200 \times 30$ mesh points. Along the channel (z), we assume periodic boundary conditions for both Q_{ij} and u_i , whereas at the channel walls we take no-slip boundary conditions for u_i and fixed in-plane boundary conditions for Q_{ij} . All calculations are performed in a low Reynolds numbers Re regime. Unless otherwise stated, the following values for material parameters are used: $L = 40$ pN, $A = -0.172$ MJ/m³, $B = -2.12$ MJ/m³, $C = 1.73$ MJ/m³, $\xi = 0.6$, $P_0 = 100$ kPa, $\Gamma = 7.29$ Pas, the mesh resolution $\Delta x = 10$ nm, time step $\Delta t = 0.34$ μ s, and body force $f = 0.01$ $\rho\Delta x/\Delta t^2$.

III. GEOMETRY-CONDITIONED NEMATIC MICROCHANNELS

Geometrical cross-section is the elementary variability of channels in microfluidic setups. Therefore, it is the natural first step in understanding the role of geometrical confinement in porous microfluidics, which effectively can be considered as if consisting of multiple sub-regions of various geometries and cross sections. Fig. 1 (a-d) shows the flow of nematic fluid pushed by a constant body-force along microchannels of different geometries, with surfaces imposing homogeneous alignment of the director along the channel axis z . The flow profile near the channel wall responds to the geometry of the channel, but becomes more circular-tube-like in the center of the channel, the response is very similar to the material flows of isotropic fluids. Differently, the nematic profile starts to deviate away from the homogeneous alignment imposed by the walls because of the coupling with the flow field (shear profile) in the central region of the channel (see Fig. 1 a-d) – and can be interpreted as a +1 umbilic defect. Notably, the director has no singular region, but is everywhere continuous and can be – from the standpoint of topology – virtually continuously transformed into a homogeneous field. The umbilic defect-type field profile emerges in the *projection* of the director on to the plane

perpendicular to the general director alignment direction (z axis), i.e. in the cross-section of the channel [26, 42]. The profile in this projected director also determines the strength (effectively, the winding number) of umbilic defects. The director deformation of the umbilic can be locally measured with the angle between deviated director and the axis z and is shown with colors in the third column of Fig. 1 (a-d). Maximum values of the flow velocity and director deformation both depend on microchannel geometry and surface of the channel cross section. For channels with equal cross section area, maximum flow velocity and maximum director deformation emerge in circular microchannel and decrease with the number of the edges.

In order to maximize the backflow coupling between the flow and nematic director – i.e make umbilic defects more pronounced by maximising the xy projection component of the nematic director – we vary the key two parameters of the system: (i) body force driving the flow and (ii) material parameter ξ , which depends on the molecular properties of the liquid crystal [26, 59]. Figure 1 (e) shows maximum velocity (reached in the center of the microchannel) and Fig. 1(f) maximum deformation of the director field (reached at the tip of the arrow depicted in the inset) as a function of tumbling parameter ξ and body force f for a square channel. Within a given channel, the maximum velocity proves to be linearly dependent on the body force f and weakly varies with the tumbling parameter ξ (Fig. 1 e). Both maximum velocity and director deformation are highest in the regime $\xi \sim 0.5$ (Fig. 1 f). The maximum angle of director deformation from the homogeneous configuration has a minimum at $\xi \sim 0.9$, where it drops for more than an order of magnitude. All the following simulations presented here are done at $\xi = 0.6$.

In terms of potential experiments to demonstrate the formation of these umbilic defects in the different geometries, a microfluidic device comprising a combination of cylindrical and rectangular capillaries would be required whereby the flow rate of the nematic is controlled by a syringe pump. This barriers could be pinned mutually and to the channel walls at some (large) distances, generating long regions of microchannels with effectively separate long cylindrical barriers that create regular pores. An optical polarising microscope and a high speed camera could then be used to monitor the formation and behaviour of the umbilic defect.

IV. POROUS NEMATIC MICROCHANNELS

Umbilic defects are observed to emerge when the nematic is pushed along the porous microchannels. The porous channels are set up as rectangular micro-channels with inserted cylindrical barriers, e.g. visualise long cylindrical fibres immersed in the channels (Fig. 2). The introduced barriers (i) increase the surface area where the flow velocity is imposed to be zero and (ii) decrease the

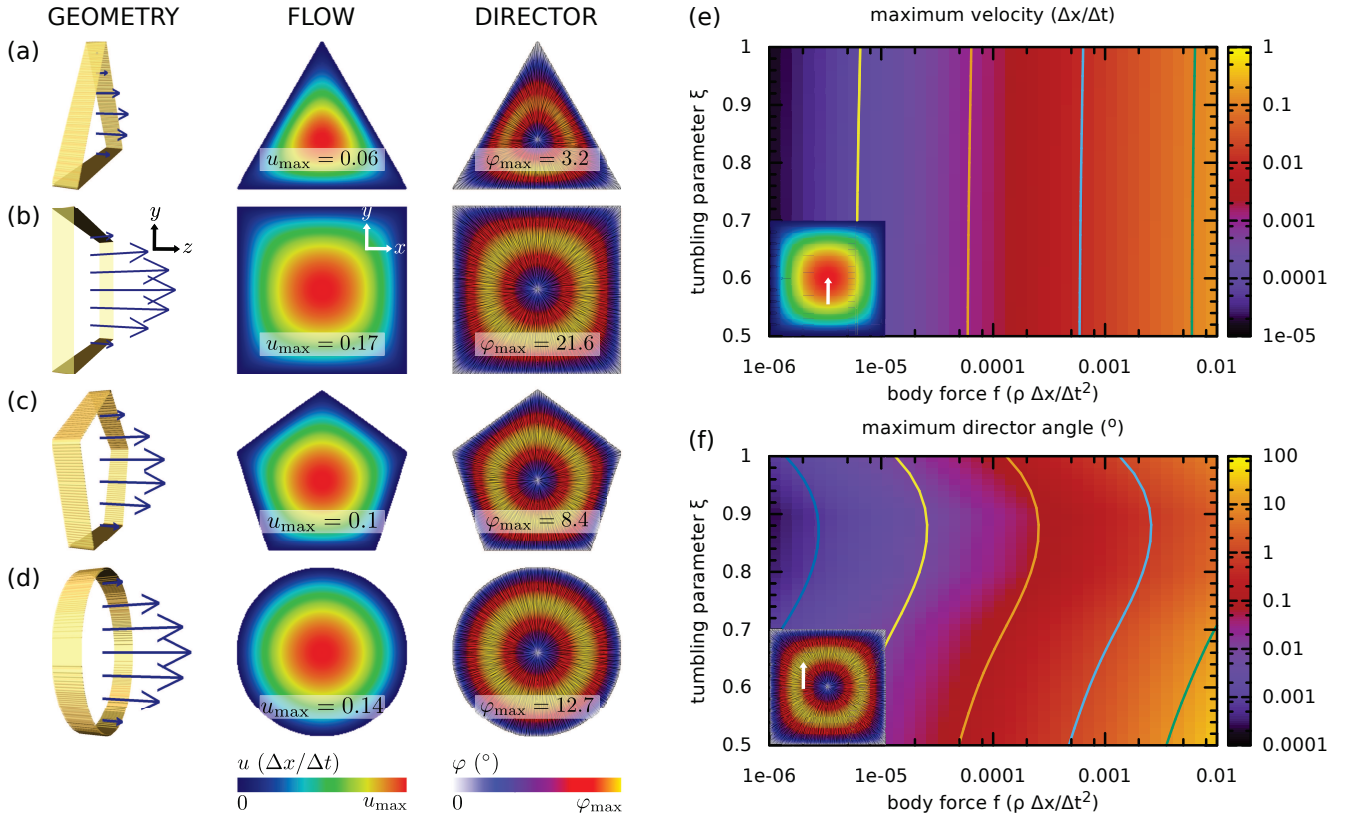


Figure 1. **Nematic liquid crystal flow in microchannels of different geometries driven with constant body force.** (a-d) Flow velocity and director deformation fields (angle between director and channel axis z) are indicated with colours; grey and white streamlines in bottom row show the projection of the director on the xy plane. Strong homogeneous planar anchoring in the direction of the channel axis z is imposed at the channel surfaces. Body-force $f = 1 \times 10^{-2} \rho \Delta x/\Delta t^2$. (e) Maximum velocity and (f) director deformation in square channel (both indicated with the white arrow) as a functions of tumbling parameter ξ and body force f .

fraction of the channel cross section accessible to the fluid – i.e. decrease the porosity of the channel. Consequently both the flow velocity and director deformation diminish, when the porosity of the microchannel is decreased. But more importantly, the porous barriers change the effective landscape of the microfluidic channel by introducing geometrical pores of various shapes and sizes, which cause the flow velocity to obtain multiple flow peaks and flow saddle points (Fig. 2 e). Effectively, both the material flow and the nematic distortion become locally compartmentalised by the pores into effective channel-like regions of different geometries. And it is the local flow peaks and saddles within such effective channel-like regions which generate the umbilic defects via the backflow mechanism (Fig. 2 e).

Figure 2 (a, b, c) shows the square microfluidic channel with one inserted cylindrical barrier. As the radius of the barrier is increased, the four maxima in the flow velocity become localised and flow saddle points between them become more pronounced. Similar is observed in the case of two (Fig. 2 d, e) and four (Fig. 2 f, g) barriers in the microchannel, generating different configurations of the local flow peaks and flow saddles. In such chan-

nels, the deformation of the director field is a result of competition between the surface alignment imposed by the channel surfaces and the flow shear, where the flow shear turns the director away from the direction imposed by the surfaces. We observe that a local maximum in the flow field yields an umbilic defect of strength $+1$ and a horse saddle point gives an umbilic defect of strength -1 (insets at Fig. 2 e). Director field in umbilic defect is tilted towards its core and is consequently continuous everywhere in space. A notable difference between regular defects in liquid crystals, called disclinations, and umbilic defects is that half integer (winding number) defect lines can occur in disclinations, but not in umbilic defect lines. Therefore, umbilics of strength $+1$ and -1 , that occur in our porous microchannels, are expectedly the lower elastic energy deformations.

The flow field in porous microfluidic channels was shaped by cylindrical barriers and only the two simplest flow profiles – i.e flow peaks and flow horse saddles – emerged, which gave umbilic defects of strengths $+1$ and -1 . However, by designing flow profiles with different symmetry beyond simple peaks and horse saddles, umbilic defects of higher umbilic strength can be created.

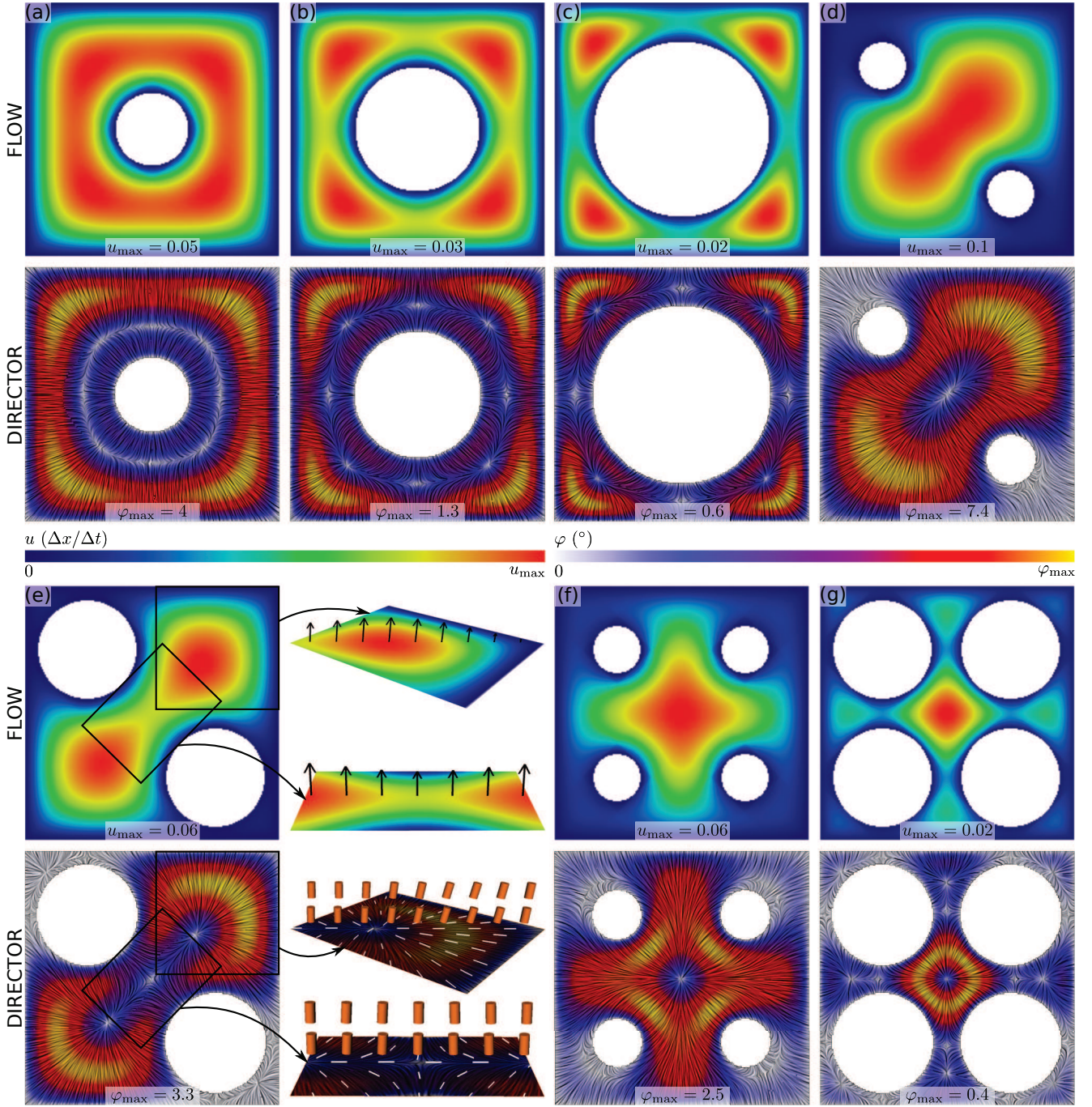


Figure 2. **Flow and director profiles in porous micro-channels.** Porous channels with (a, b, c) one, (d, e) two and (f, g) four cylindrical barriers. Umbilic defects in the director field of umbilic strength +1 emerge at local flow peaks (i.e. local maximum or minimum) and umbilics of umbilic strength -1 emerges in the flow saddle point.

We perform simulations in an (empty) square microchannel with predefined and fixed velocity profile of distinct symmetry and calculate the nematic orientation for such imposed shear-flow. Expectedly, a peak in the velocity field generates a +1 umbilic and a horse saddle a -1 umbilic (Fig. 3). Two peaks without a saddle point (a minimum and a maximum) generate umbilic of strength

+2, whereas a three-valley saddle (monkey saddle) and a four-valley saddle yield umbilics of strength -2 and -3 , respectively. As shown in Fig. 3, in a local core region, the -3 umbilic can decompose into one +1 umbilic defect and four -1 umbilics, keeping the umbilic strength conserved.

The direct relation between the shape of local flow

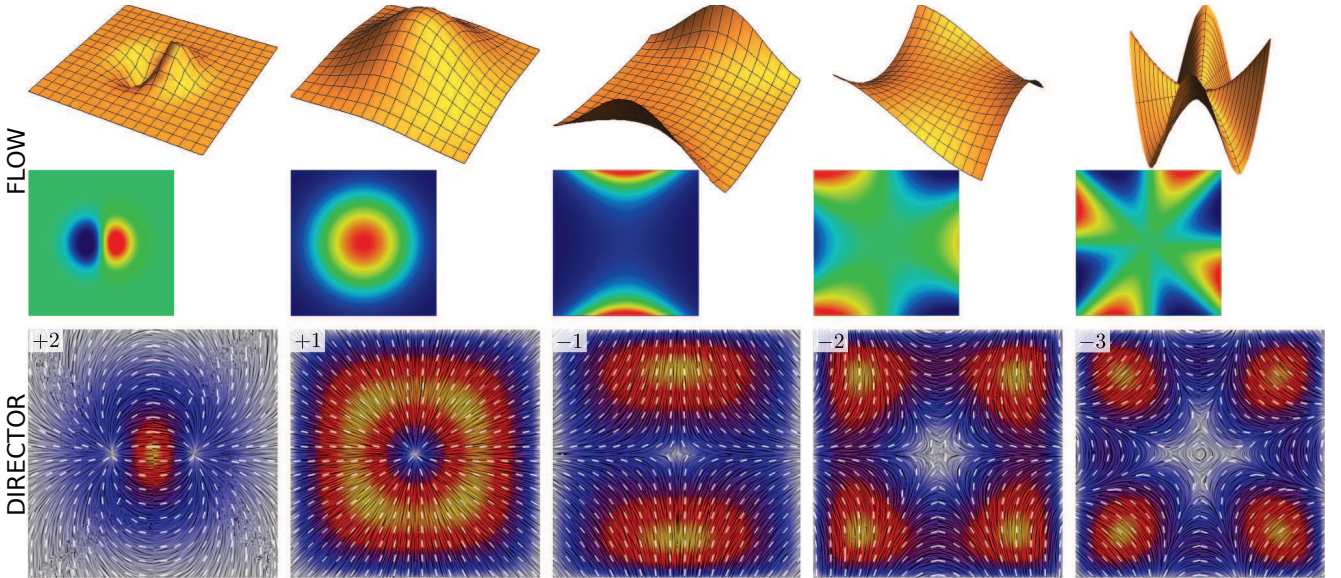


Figure 3. **Generation of umbilic defects of variable (high) umbilic strength.** A local peak in the velocity field generates a +1 umbilic, two peaks of different signs generate +2 umbilic. Umbilics of negative signs (-1 , -2 , -3) are generated if the velocity field has saddle point with two, three and four valleys, respectively. In the core region, the -3 umbilic can decompose into one +1 umbilic and four -1 umbilics.

profile and the generation of umbilic defects of various umbilic strengths can be shown also by simple analytical calculations. All numerical results in this paper are based on the Berris-Edwards model of nematodynamics. If one assumes incompressible nematic fluid, constant nematic degree of order ($S = \text{const.}$) and takes director \mathbf{n} instead of order parameter tensor \mathbf{Q} for the hydrodynamic variable (i.e. assuming uniaxial order parameter tensor $Q_{ij} = S(3n_i n_j - \delta_{ij})/2$), the Berris-Edwards model reduces to the Ericksen-Leslie hydrodynamic theory of nematic liquid crystal [25, 26]. Time evolution equation for Q_{ij} (Eq. 1) reduces to director equation [25]

$$I \frac{d}{dt} [\mathbf{n} \times \dot{\mathbf{n}}] = \mathbf{n} \times \mathbf{H} + \mathbf{\Gamma}. \quad (7)$$

where I is the moment of inertia per unit volume, and $\mathbf{\Gamma} = -\gamma_1 [\mathbf{n} \times \mathbf{N}] - \gamma_2 [\mathbf{n} \times \mathbf{D} \cdot \mathbf{n}]$ is the viscous torque, $\mathbf{N} = \dot{\mathbf{n}} - \boldsymbol{\omega} \times \mathbf{n}$ describes relative rotations of the director and $\gamma_1 = \alpha_3 - \alpha_2 > 0$, $\gamma_2 = \alpha_6 - \alpha_5 = \alpha_2 + \alpha_3$ are combinations of Leslie viscosities. At low-frequency excitations, the inertia term can be neglected and equation 7 reduces to

$$\mathbf{n} \times \mathbf{H} = \mathbf{n} \times (\gamma_1 \mathbf{N} + \gamma_2 \mathbf{D} \cdot \mathbf{n}). \quad (8)$$

which gives the connection between the nematic molecular field \mathbf{H} and the velocity gradient tensor \mathbf{D} :

$$\mathbf{H} = -\gamma_1 \boldsymbol{\omega} \times \mathbf{n} + \gamma_2 \mathbf{D} \cdot \mathbf{n}. \quad (9)$$

The latter coupling in Eq. 9 between the nematic director and the material flow shows that by imposing a distinct velocity profile, one can control the molecular field – i.e. the equilibrium alignment of the nematic.

We take a 2D Gaussian function ($-$) and a 2D Gaussian saddle ($+$) to resemble a local peak and a horse saddle in the velocity profile [60]:

$$\mathbf{u}(x, y) = a \exp \left(-\frac{x^2}{2c^2} \mp \frac{y^2}{2c^2} \right) \mathbf{e}_z, \quad (10)$$

where the parameter a determines the height of the function peak and c (the standard deviation) controls the width of the Gaussian peak. We calculate the velocity gradient tensor D_{ij} using predefined profiles (Eq. 10) which yields the corresponding molecular field as:

$$\mathbf{H} = \gamma_1 \boldsymbol{\omega} \times \mathbf{n} + \frac{1}{2c^2} \gamma_2 u_z(x, y) \begin{pmatrix} -xn_z \\ \mp yn_z \\ -xn_x \mp yn_y \end{pmatrix}. \quad (11)$$

Indeed, for the Gaussian velocity profile, the corresponding molecular field has rotational symmetry around axis z , whereas for the Gaussian saddle-shaped velocity profile, the corresponding normalised molecular field has a C_4 symmetry which corresponds to the symmetry of the -1 umbilic. In equilibrium, the director must be at each point parallel to the molecular field [26]. Furthermore, if normalising the molecular fields calculated from Gaussian saddle velocity field in the xy plane for visualisation reasons, they show the profile exactly similar to the director profiles of umbilic defects projected on the xy plane. So the symmetry and the shape of the normalised molecular field equals the symmetry of the outcoming umbilic defects. Such simplified Ericksen-Leslie analytical approach works well also for umbilics of higher strengths, reproducing the symmetry and roughly the projection of their director profile.

V. MICROCHANNELS WITH REGULAR POROSITY AS GENERATORS OF UMBILIC LATTICES

With the knowledge on mutual coupling between the flow profiles and nematic orientation, different regular and irregular configurations of umbilic defects can be created, notably including diverse umbilic defect lattices. We use rectangular microfluidic channels and impose porosity with cylindrical barriers arranged into three regular configurations: triangular, square and hexagonal lattice. Generally, we observe that the flow field in such microchannels with cylindrical barriers has locally only two basic profiles, namely local peaks or local horse saddles (Fig. 4), which generate the basic ± 1 umbilic defects. Performing the study in finite-size channels, the flow field is affected by the confining microchannel walls, where surface effects can distort and affect the lattice of the umbilics.

Figure 4 (a, b) shows the microchannel with triangular lattice of barriers where depending on the barrier radius, we observe formation of two different lattices of the umbilic defects. In thin barrier regime, $+1$ umbilics form triangular lattice and -1 umbilics a square lattice. However, if the barriers are thick compared to the interspaces between them, $+1$ umbilics form hexagonal lattice and -1 umbilics arrange into a Kagome lattice. Both types of umbilic defects in porous microchannel with square lattice of barriers (Fig. 4 c) form lattices of the same symmetry. If the barriers are arranged into a hexagonal lattice (Fig. 4 d) umbilic defects of strength $+1$ form triangular and -1 umbilics a Kagome lattice.

To generalise the results, the mutual – backflow – coupling between the flow field and nematic orientational ordering is shown as an interesting novel way for creating birefringent defect lattices in complex fluids via direct microfluidic approach. By controlling the symmetry and size of the porous barriers in the channels, one can design various umbilic arrangements and lattices ranging from simple square, to triangular and even Kagome. As objects, the umbilic defects are inherently birefringent and could be used for manipulating the flow of light at various levels and frequency scales, depending on the pore (barrier) design and size. Also umbilic defects, could be used as switchable and controllable objects for trapping and guiding inclusions – such as colloidal particles – in the microchannels, relevant in field of microtransport and mixing. By further designing and changing the surface conditions at the porous barriers (e.g. make the surfaces to impose homeotropic anchoring), the formation of umbilic defects could be complemented also by the emergence of singular defects (such as $+1/2$ and $-1/2$ disclination lines) which would add a further variability to the material.

Creating the umbilic defect lattices from an experimental point of view is by no means trivial. However, we propose that this may be achieved using direct laser writing to create cylindrical polymer channels in a nematic

liquid crystal device that consisted of reactive mesogens and photo-initiator. With the use of two-photon polymerisation it should be possible to create well defined polymer cylinders that are located at precise positions within the device. Furthermore, with the use of adaptive optics it should also be possible to form the structures in-situ and with the aid of a spatial light modulator an array of these cylinders in any one of the potential configurations (i.e. square, triangular, or hexagonal) could be created. To induce flow, a piezoelectric transducer would be connected to the nematic liquid crystal device. Work is currently underway to realise the appearance of stable umbilic defects in porous nematic microfluidic devices.

Cylindrical barriers may have different refractive index than the surrounding liquid crystal, which is birefringent and given by the director orientation. Regular lattices of barriers and umbilic defects of different symmetries thus form complex composite birefringent photonic crystal materials, where one contribution to the band structure is determined by the 2D periodic lattice of umbilic defects, whereas the second contribution emerges from the regular lattice of the cylindrical barriers. Flow rate and the barrier size -beside the material constants- are direct parameters that could be used to tune the optical bands and band gaps of these photonic materials as they affect the effective dielectric contrast of the photonic crystal. We should comment that the effects of bulk-heating are generally small in such complex liquid crystal geometries, where the aimed effects come from the heating via surfaces [61]. More generally, such photonic crystal materials may offer a novel -microfluidics based- approach towards tunable soft matter photonic materials. Additional interesting variability of these materials could open by also applying external fields, including electric and magnetic.

VI. CONCLUSION

We introduce porous nematic microfluidics as a controllable system for generating complex regular configurations of nematic umbilic defects, ranging from individual umbilics to umbilic lattices, such as square, triangular and even Kagome. With their complex spatial variation of birefringence, the generated porous umbilic systems are novel photonic materials of conceptually different design: essentially, the umbilics produce optical lattices of *some* symmetry within the optical lattices of the barriers with *another* symmetry, which may be used as a novel route to tunable photonics based on materials with inherently multiple underlying symmetries. Specifically, we perform hybrid lattice Boltzmann simulations of driven nematic liquid crystal flow in rectangular microchannels with inserted cylindrical barriers, and also clearly discuss the experimental realisation of such systems. The porous barriers inside the microfluidic channel change the effective landscape of the channel, creating narrow and wide regions for the flow to pass, which results in the forma-

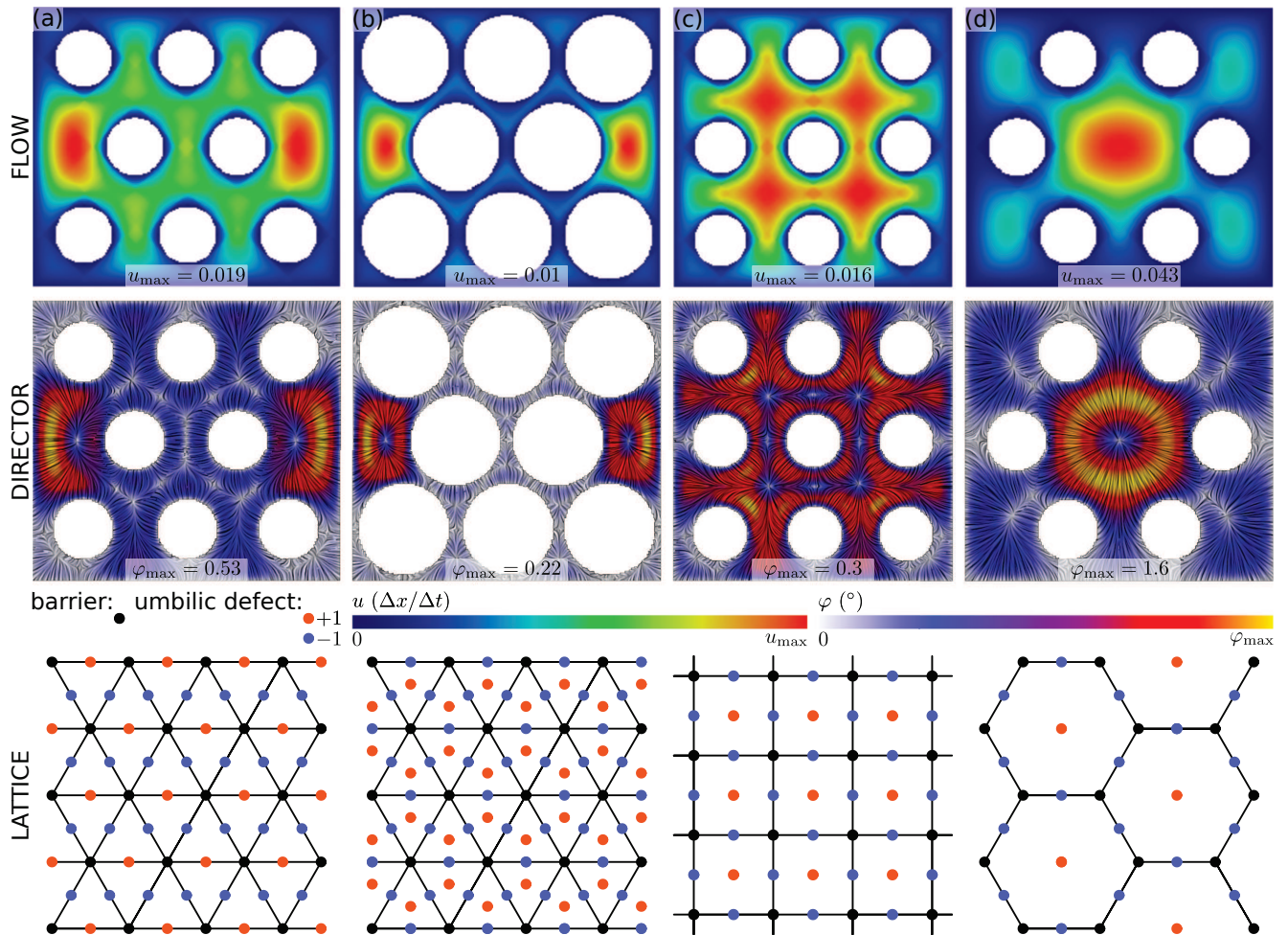


Figure 4. **Porous nematic micro-channels as generators of umbilic defect lattices.** Porous micro-channels with cylindrical barriers arranged into (a, b) triangular, (c) square and (d) hexagonal lattice. Triangular lattice of barriers (a, b) can generate two possible lattices of the umbilics, depending on the diameter of the cylindrical barriers. In the thin cylinders regime (a), triangular lattice of $+1$ umbilics form and rectangular lattice of -1 umbilics. In the thick cylinders regime (b), hexagonal lattice of $+1$ umbilics form, and Kagome lattice of -1 umbilics. (c) For the square lattice of barriers, both types of umbilics form square lattices. (d) For hexagonal lattice of barriers, $+1$ form triangular lattice and -1 umbilics Kagome lattice. Bottom panels show generalisation of the observed umbilic patterns from finite sized channels to (infinite) periodic umbilic lattice structure; black dots indicate barrier positions, orange dots show $+1$ and blue dots -1 umbilic defects.

tion of local peaks and saddles in the flow field, which in turn results in the formation of the umbilic defects, i.e. geometrically distinct spatial variations of birefringence. Umbilic defects of umbilic strength $+1$ form at local flow peaks, whereas umbilics of umbilic strength -1 emerge at horse saddle points. Furthermore, we show that umbilics of higher umbilic strength can be formed via controlling the geometry of the flow velocity profile, which is an interesting generalisation that provides direct insight into the actions of the backflow mechanism with relevance in various complex fluids, notably including active nematics. Finally, this work is an approach towards realising microfluidically tunable optical and photonic materials

and may find relevance in diverse systems with internal order, ranging from flexible polymers under shear to active fluids.

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