

# Unraveling Subcellular Ultrastructure with Cyclically Multiplexed Expansion Microscopy

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## Abstract:

Despite advances in fluorescence microscopy, spectral overlap and limited resolution hinder the dense mapping of the cellular ultrastructure. To overcome these challenges, we developed Cy-ExM, a high-plex imaging strategy that integrates optimized cryo-fixation for antigen preservation, expansion microscopy, and iterative immunofluorescence labeling. Using oblique plane microscopy, we perform three-dimensional super-resolution imaging of 20 biological targets encompassing the full cellular volume of individual mammalian cells.

## Main Text:

The spatial organization of proteins and organelles within eukaryotic cells governs a vast amount of fundamental biological processes such as replication, metabolism, and intra- and extracellular signaling. Fluorescence microscopy is a widely applicable method for visualizing subcellular structures because it provides high molecular specificity and relatively rapid, multi-target imaging, whereas electron microscopy excels at revealing ultrastructural and cellular context but is generally lower throughput and, in conventional implementations, depends on broad-spectrum contrast mechanisms such as heavy metal staining<sup>1</sup>. Nonetheless, spectral overlap and the limited availability of orthogonal antibody pairs constrain the number of molecular targets that can be simultaneously visualized in fluorescence microscopy. While spectral imaging and unmixing techniques can computationally separate overlapping fluorophores, their accuracy diminishes at low photon counts where noise is non-negligible. As a result, modern multiplexed imaging approaches, such as t-CyCIF<sup>2</sup>, IBEX<sup>3</sup>, and CODEX<sup>4</sup>, have adopted cyclic labeling strategies to dramatically expand the number of visualized targets. Together, these methods have provided critical insights into physiological and pathological states, particularly in tissue contexts<sup>5</sup>.

However, understanding cellular function requires imaging molecular structures at cellular and sub-cellular scales, where key biological processes such as protein complex assembly, cytoskeletal organization, and organelle interactions occur. Super-resolution light microscopy has greatly advanced our ability to visualize biological structures at sub-diffraction-scales<sup>6</sup>, but practical limitations hinder its

40 application in multiplexed imaging. Techniques like localization microscopy and stimulated emission  
41 depletion rely on specialized fluorophores, and their inherently slow acquisition speeds constrain imaging  
42 to shallow 3D volumes<sup>7</sup>. Even with state-of-the-art DNA-PAINT-based multiplexing methods, imaging is  
43 typically limited to about a dozen targets and shallow (~1 micron) imaging depths<sup>8</sup>. Overcoming these  
44 challenges requires an integrated imaging strategy that combines volumetric super-resolution with high-  
45 plex molecular detection in thick specimens, enabling a more comprehensive understanding of cellular  
46 organization.

47 One promising strategy for multiplexed, nanoscale imaging involves embedding specimens in a  
48 hydrogel scaffold that simultaneously stabilizes the sample mechanically and renders it optically  
49 transparent. However, embedding and polymerization steps, often coupled with proteolytic softening to  
50 relax tissue mechanics, can mask or remove antigens, reducing sensitivity across a range of molecular  
51 targets<sup>9</sup>. Immunostaining can be performed either before or after hydrogel embedding, but each approach  
52 requires a distinct workflow and involves trade-offs in labeling efficiency, signal retention, and  
53 multiplexing capacity (See **Supplementary Note 1**). Despite these challenges, techniques such as  
54 CLARITY<sup>10</sup>, SWITCH<sup>11</sup>, and Expansion Microscopy<sup>12</sup>, have been adapted for cyclic labeling strategies.  
55 To date, however, most cyclic ExM-style applications have emphasized synaptic marker panels and  
56 synapse classification<sup>12</sup>, in part because extending these workflows to comprehensive, cell-biological  
57 mapping of diverse organelles and protein assemblies requires substantially higher preservation of  
58 ultrastructure and epitope integrity across repeated processing steps. In practice, cumulative losses in  
59 antigenicity, structural distortions introduced during mechanical homogenization, and signal dilution in  
60 expanded gels have limited broad application to multi-organelle nanoscale mapping. Consequently, a cell-  
61 biologically focused approach that fully integrates cyclic multiplexing with expansion microscopy while  
62 preserving ultrastructure across cycles has yet to be demonstrated.

63 To overcome these limitations, we introduce Cyclically Multiplexed Expansion Microscopy (Cy-  
64 ExM), a strategy for high-sensitivity, nanoscale, three-dimensional visualization of subcellular  
65 architectures. Our method combines cryofixation by guillotine-based plunge-freezing, which minimizes  
66 specimen damage (**Figure S1**), with acetone-based freeze substitution, protein entanglement, and heat-  
67 induced denaturation to relax intermolecular interactions and mechanically homogenize the specimen for  
68 isotropic expansion<sup>13</sup> (**Figure 1a-b, Supplementary Note 2**). Although denaturation disrupts native  
69 protein conformation, it maintains the relative spatial arrangement of proteins and minimizes antigen loss  
70 compared with conventional chemical fixation and expansion workflow<sup>14</sup> (**Figure S2**). Leveraging this  
71 approach, specimens routinely achieved 4.2-fold linear expansion and were compatible with volumetric  
72 imaging on both conventional fluorescence microscopes (**Figure 1c**) and an inverted oblique plane  
73 microscope (OPM) optimized for large, aqueous samples, with a large field of view and a high numerical  
74 aperture (NA 1.1) water-dipping objective<sup>15</sup>. Combined, our sample preparation, labeling, and OPM  
75 achieved ~95 nm lateral and ~290 nm axial resolution prior to deconvolution, and ~70 nm lateral by ~220  
76 nm axial resolution after deconvolution, respectively, while enabling iterative multiplexed mapping of up  
77 to 20 targets. Relative to standard immunofluorescence, Cy-ExM revealed significantly greater structural  
78 detail, including the visualization of mitochondrial cristae and continuous, well-resolved microtubule  
79 filaments throughout the cytoskeletal network in mouse embryonic fibroblast (MEF) cells (**Figure 1d-g**,  
80 **Figure S3**).

81 Importantly, this protocol enabled repeated cycles of labeling and volumetric imaging of the same  
82 specimen (**Figure 1h**) while preserving subcellular architecture and maintaining a reproducible 4.2×

83 linear expansion coefficient across successive rounds. We used nuclear DNA staining as a robust  
84 fiduciary marker to quantify expansion repeatability and confirm preservation of fine nuclear features  
85 (e.g., nucleoli) across cycles (**Figure S4**). To further evaluate the fidelity of iterative labeling, cryo-fixed  
86 MEFs were embedded in a swellable hydrogel, denatured, and partially expanded (~2×) for  
87 immunolabeling of peroxisomes, DNA, and microtubules, and then fully expanded (4.2×) for volumetric  
88 imaging (**Figure 1i-k, Movie S1, Tables S1 and S2**). After the first round of imaging (**Figure 1i**),  
89 antibodies were gently stripped using  $\beta$ -mercaptoethanol to reduce disulfide bonds and facilitate antibody  
90 removal<sup>12</sup>; complete loss of antibody signal in the stripped state confirmed effective stripping (**Figure 1j**).  
91 Cells were then re-labeled with the same antibody set and re-imaged (**Figure 1k**).

92 Although visual inspection showed strong agreement across labeling rounds, we next quantified  
93 how faithfully subcellular features aligned in 3D by quantitatively evaluating registration accuracy  
94 between rounds using the same marker sets. Registration was performed using the microtubule channel,  
95 which is distributed throughout the cellular interior and is sufficiently dense to robustly constrain the  
96 registration transform. To ensure accurate alignment between rounds, we applied a pyramidal registration  
97 routine that increased in complexity over successive steps: beginning with simple translation, followed by  
98 rigid body, similarity, and ultimately two rounds of affine registration (**Figure S5a; Methods**).  
99 Registration accuracy in 3D was evaluated using quantitative metrics, including normalized cross-  
100 correlation, mutual information, and structural similarity index (**Supplementary Note 3**). Decomposition  
101 of the affine matrix showed that round-to-round transformations were small, with near-zero rotation and  
102 shear, and only slight anisotropic scaling (**Table S3**). While affine alignment achieved strong global  
103 consistency, quantitative similarity metrics showed little additional improvement following non-linear  
104 warping (**Table S4**). Nevertheless, inspection of the registered volumes revealed subtle but spatially  
105 localized misalignments that were not captured by global intensity and structure-based metrics. These  
106 residual local distortions were effectively corrected by applying a modest non-linear warp (**Figure S5b-c,**  
107 **Movie S2**), suggesting that non-linear registration primarily refines local geometric consistency rather  
108 than improving global similarity scores, and resulting in high-fidelity alignment between individual  
109 imaging rounds.

110 To determine whether this level of accuracy was maintained across the entire cyclic workflow, not  
111 just between two rounds, we next evaluated the consistency of registration and labeling across five Cy-  
112 ExM cycles. Image registration was performed using the microtubule channel, and registration accuracy  
113 was independently assessed in the mitochondria channel, which was not used during alignment, by  
114 detecting mitochondrial puncta and computing mutual nearest-neighbor-paired distances as a target  
115 registration error (TRE)-like proxy (**Figure S6**). Using this approach, we observed a root mean square  
116 displacement of ~124 nm across cycles (**Table S5**). Nearest-neighbor pairing provides a straightforward  
117 estimate of residual misalignment, but for spatially heterogeneous targets such as mitochondria, incorrect  
118 correspondences can occur when nearby puncta are ambiguously matched. To obtain a more conservative,  
119 globally consistent estimate, we additionally matched mitochondrial features using descriptor-based  
120 correspondences and robustly fit a global similarity transform to the resulting pairs, estimating the TRE  
121 proxy from inlier matches. This approach yielded a mean cross-validated TRE proxy of 91 and 100 nm,  
122 after linear and nonlinear registration, respectively. Together, these analyses indicate that Cy-ExM  
123 preserves high spatial fidelity across iterative cycles, with residual inter-round misalignment on the order  
124 of ~100 nm throughout the entire field of view.

125 We next quantified round-to-round staining variability with a spinning disk confocal microscope  
126 using a 20× NA 0.75 air objective (**Figure S7**). Peroxisome signal was quantified by measuring the  
127 background-corrected mean intensity within regions of interest for seven cells; after stripping, the  
128 peroxisome intensities dropped to near-background levels (i.e., comparable to regions outside the cell),  
129 yielding signal-to-noise values close to unity. Notably, peroxisome labeling intensity did not  
130 monotonically decrease across cycles; instead, it increased from rounds 1–4 and then modestly decreased  
131 in round 5 while remaining higher than rounds 1–3, consistent with cycle-dependent changes in staining  
132 efficiency rather than cumulative antigen loss. Consistent with this interpretation, a cycle-permutation  
133 experiment showed that antigenicity was independent of labeling order (**Figure S8**), indicating that  
134 epitopes remain accessible even when targets are stained in late rounds. Because antibodies are gently  
135 removed using redox chemistry and the specimen is mechanically reinforced by the hydrogel, the  
136 apparent labeling quality was not sensitive to staining order, as judged by consistent staining patterns and  
137 low background across cycles. Consequently, we hypothesized that Cy-ExM should tolerate cycle counts  
138 comparable to established cyclic immunofluorescence workflows (e.g., 10-20 cycles, depending on tissue  
139 resilience<sup>2,3,16</sup>). To evaluate this, we simulated a high-cycle experiment by subjecting a gel to ten  
140 consecutive rounds of stripping, consisting of 45 minutes in  $\beta$ -mercaptoethanol at 95°C, with staining and  
141 imaging performed at the beginning, middle, and end of the workflow. Cells were labeled for actin  
142 filaments, microtubules, mitochondrial matrix, endoplasmic reticulum (ER), and DNA, and all structures  
143 remained well preserved even after ten rounds of stripping (**Figure S9**).

144 To demonstrate the feasibility and practical utility of Cy-ExM, we next applied the method to  
145 visualize 20 distinct molecular targets within the same MEF cell across eleven iterative imaging cycles  
146 (**Figure 2a-b, Movie S3, Table S6**). This multiplexed dataset captured the major cellular organelles,  
147 including the ER, Golgi apparatus, mitochondria, lysosomes, and peroxisomes, as well as nuclear  
148 components such as the nuclear envelope, nuclear pore complexes, and fibrillar in. In addition to  
149 membrane-bound organelles, cytoskeletal networks comprising actin filaments, vimentin, and  
150 microtubules, were robustly resolved, reflecting the broad epitope compatibility enabled by cryo-fixation  
151 and post-expansion labeling. Analysis of the full dataset confirmed that geometric stability was  
152 maintained across labeling cycles at scale: decomposition of affine transforms revealed highly consistent  
153 round-to round alignment with minimal variability in scale and shear, and non-linear warping remained  
154 modest, indicating limited cumulative distortion (**Table S7**). Given the multiplexing demonstrated here,  
155 Cy-ExM enables direct comparison of multiple cellular structures within the same cell, avoiding reliance  
156 on population-averaged measurements across separate specimens<sup>17</sup>. To illustrate this capability, we  
157 organized datasets acquired from distinct cells into functionally coherent views of subcellular architecture  
158 (**Figure 2c-f, Movie S3 and S4**), highlighting distinct regions of interest in which targets were grouped  
159 by primary biological role, including the secretory pathway, cytoskeletal network, metabolic organelle  
160 network, and nuclear architecture. This integrative representation preserves the full molecular context of  
161 each structure while maintaining sufficient spatial resolution to resolve nanoscale features, such as  
162 individual NUP p62 nuclear pore complexes within the nuclear envelope (**Figure 2f, Figure S10**).  
163 Together, these capabilities position Cy-ExM as a practical route toward constructing high-content  
164 nanoscale atlases of cellular ultrastructure, enabling systematic mapping and quantitative analysis of  
165 organelle organization and interactions within a single, intact cell.

166 One compelling application of Cy-ExM is to quantify coordinated spatial organization of proteins  
167 and organelles within single cells. To test this, we compared the radial distributions of multiplexed

168 markers from the nuclear boundary to the cell periphery by computing per-marker intensity profiles  
169 normalized by cell size (**Figure 3a–b; Methods**). Because distances are normalized, these profiles  
170 provide a rotationally invariant, shape-independent representation of spatial organization that enables  
171 direct comparisons across cells. Markers associated with the same organelles exhibited similar radial  
172 profiles, and clustering of these profiles recovered expected groupings of mitochondrial, nuclear, and  
173 cytoskeletal components (**Figure 3c; Figure S10**). These relationships were reproducible across  
174 independent cells (**Figure 3d**), demonstrating that Cy-ExM supports quantitative, single-cell comparisons  
175 of subcellular organization and provides a practical framework for testing how organelle organization  
176 changes across cell states and perturbations.

177 Taken together, these results establish Cy-ExM as a high-fidelity platform for high-cycle, three-  
178 dimensional multiplexed imaging that preserves ultrastructural context, antigenicity, and spatial fidelity  
179 across repeated labeling rounds (**See Supplementary Note 4, Limitations and Future Directions**). By  
180 integrating cryo-preserved sample preparation with expansion microscopy and iterative immunolabeling,  
181 Cy-ExM enables quantitative, whole-cell volumetric super-resolution maps of multi-protein organization  
182 using standard fluorescence microscopes. We anticipate that this combination of ultrastructural  
183 preservation and multiplexed nanoscale readouts will make it possible to construct systematic atlases of  
184 subcellular architecture and to measure how organelle organization and compartmental co-organization  
185 evolve in increasingly complex specimen contexts.

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## 198 **Author Contributions**

199 S.G.: Methodology, Validation, Formal Analysis, Investigation, Writing (original draft, review,  
200 and editing), Visualization. B.-J.C.: Methodology, Investigation, Writing (review and editing). Q.S.:  
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204 Investigation, Writing (review and editing). K.M.D.: Conceptualization, Methodology, Software, Formal  
205 Analysis, Writing (original draft, review, and editing), Resources, Visualization, Supervision, Project  
206 Administration, Funding Acquisition.

## 207 Declaration of Interests

208 K.M.D. is a founder of Discovery Imaging Systems, LLC. K.M.D. and R.F. have a patent covering  
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210

## 211 Declaration of generative AI and AI-assisted technologies in the manuscript preparation process

212 During the preparation of this work the authors used ChatGPT in to improve grammar and  
213 readability of the text. After using this service, the authors reviewed and edited the content as needed and  
214 takes full responsibility for the content of the published article.

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## FIGURE CAPTIONS

282  
283 **Figure 1. Cyclically Multiplexed Expansion Microscopy Workflow.** (a-b) Overview of sample  
284 preparation for Cy-ExM. (a) Cultured cells were rapidly plunge-frozen in liquid ethane at  $-180^{\circ}\text{C}$  and  
285 freeze-substituted into acetone at  $-80^{\circ}\text{C}$  to preserve ultrastructure and antigenicity. (b) After rehydration,  
286 cells were chemically anchored with formaldehyde and acrylamide, embedded in a swellable hydrogel,  
287 denatured at  $95^{\circ}\text{C}$  to expose epitopes, and isotropically expanded in deionized water. (c) Depth-encoded  
288 maximum-intensity projection of a cryo-fixed,  $4.2\times$  expanded MEF undergoing mitosis, in which color  
289 indicates the axial (Z) position. (d-g) Representative images of cultured MEFs processed using a single  
290 round of the Cy-ExM workflow. (d) Mitochondria channel only (cyan). (e) Microtubules channel only  
291 (orange). (f) Merged view of microtubules (orange) and mitochondria (cyan). (g) Magnified inset  
292 corresponding to the boxed region in (f). (h) The full Cy-ExM workflow: visualization of cellular  
293 ultrastructure was performed by iterative post-expansion indirect immunofluorescence, volumetric  
294 imaging with an oblique plane or spinning disk confocal microscope, and antibody stripping using  $\beta$ -  
295 mercaptoethanol. (i-k) Example of iterative imaging across rounds. Cells were first labeled for  
296 peroxisomes, microtubules, and nuclei and imaged; antibodies were then stripped, nuclei were re-stained  
297 and re-imaged as a reference; cells were subsequently re-labeled for peroxisomes, microtubules, and  
298 nuclei and imaged again. Deconvolved maximum-intensity projections are shown. All scale bars are  
299 corrected for the expansion factor.

300  
301 **Figure 2. Twenty-plex volumetric Cy-ExM imaging of subcellular organization.** (a) Maximum-  
302 intensity projections (MIPs) of all 20 cellular targets imaged in the same cell using the Cy-ExM  
303 workflow; individual channels are displayed with inverted lookup tables to enhance visibility of fine  
304 structural features (target labels indicated above each panel). Inter-round registration was performed using  
305 the microtubule channel as the structural reference. (b) Corresponding merged MIPs of the same cell are  
306 shown as two composite subpanels, each displaying 10 targets (lookup tables indicated by colored dots).  
307 (c-f) Data from a different cell, with targets grouped into four functional classes: (c) secretory pathway,  
308 (d) cytoskeletal components, (e) metabolic organelle network, and (f) nuclear organization. All images  
309 were acquired volumetrically using an oblique plane microscope and deconvolved prior to visualization.  
310 Scale bars: (a)  $10\ \mu\text{m}$ ; (b)  $20\ \mu\text{m}$ ; (c-e)  $5\ \mu\text{m}$ ; (f)  $2\ \mu\text{m}$  (all corrected for the expansion factor).

311  
312 **Figure 3. Quantifying co-organization of subcellular architectures using normalized radial signal**  
313 **distributions.** (a) Analysis workflow: the cell and nuclear volumes are segmented to compute a 3D  
314 normalized distance field ( $r$ ), where  $r = 0$  corresponds to the nuclear boundary and  $r = 1$  to the cell  
315 periphery, enabling calculation of a rotationally invariant, shape-normalized signal distribution,  $I(r)$ .  
316 Representative renderings of the 3D distance field and an  $x$ - $y$  midslice are shown, with example  $r = 0$  and  
317  $r = 1$  contours indicated. (b) Normalized signal distributions,  $I(r)$ , for 20 markers in the same cell shown  
318 in Figure 2c-f. (c) Ward hierarchical clustering of the radial signal distributions from the single-cell 20-  
319 plex dataset, displayed as a dendrogram and heatmap of  $I(r)/\text{mean}(I(r))$ . (d) Two additional segmented  
320 cells (shown in Figure 2a-b) and the corresponding Ward hierarchical clustering of their radial signal  
321 distributions (Cell 1 and Cell 2), demonstrating reproducible organization patterns across cells.

322  
323

## ONLINE METHODS

324  
325

### *Cell culture*

326 Mouse embryonic fibroblasts (MEFs) cells were cultured under standard conditions in Dulbecco's  
327 Modified Eagle's Medium (DMEM, Gibco) supplemented with 10% fetal bovine serum (FBS, Gibco),  
328 100 U/mL penicillin, and 100 µg/mL streptomycin. The cells were maintained at 37°C in a humidified  
329 incubator with 5% CO<sub>2</sub> and cultured in a 12-well plate on 5-mm glass coverslips pre-rinsed with 70%  
330 ethanol.

331

### *Chemical fixation*

332 To compare fixation methods (**Figure S2**), MEF cells were rinsed with 1× Phosphate-Buffered Saline  
333 (PBS) and incubated in: (a) 4% paraformaldehyde (PFA) at RT for 15 min, (b) 4% PFA supplemented  
334 with 0.2% Glutaraldehyde (GA) at RT for 15 min, (c) pre-heated 37°C PEM buffer [80 mM PIPES, 5 mM  
335 EGTA, 2 mM MgCl<sub>2</sub>, (pH: 6.8)], supplemented with 0.3% Triton-X and 0.125% GA for 30 s, fixed in a  
336 PEM<sup>18</sup> buffer supplemented with 2% PFA for 15 min at 37°C and washed three times with 1× PBS, 2 min  
337 each, or (d) -20°C chilled methanol for 5 min. In all other cases, the cells were subjected to cryofixation.

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### *Cryofixation*

340 Cells were cryo-fixed by plunge freezing followed by solvent fixation during freeze substitution using an  
341 established, slightly modified protocol<sup>14</sup>. Briefly, a glass coverslip with adherent cells was held vertically  
342 with forceps and gently blotted with cotton-tipped applicators. Using a homemade pneumatic plunge  
343 freezing device, the coverslip was then rapidly plunged into liquid ethane that was chilled in a liquid N<sub>2</sub>-  
344 filled Vitrobot dewar (Thermofisher). Next, the coverslip was quickly immersed in liquid nitrogen and  
345 transferred into an Eppendorf tube pre-cooled in liquid nitrogen and containing 1.5 mL of frozen acetone.  
346 The tubes were stored in liquid nitrogen until further processing. For freeze substitution, the tubes with  
347 coverslips were left overnight in a metal block that was cooled with dry ice and liquid nitrogen in a cold  
348 room, allowing gradual warming to -80°C and thawing of the acetone. Next day, the dry ice was removed,  
349 and the tubes were incubated in the metal block with lids open at room temperature for ~1 h until the  
350 acetone reached 0°C, completing solvent fixation. Samples were then rehydrated through successive  
351 ethanol:water baths in the following gradients: 100% (x2), 95% (x2), 70%, 50%, and 25% EtOH, and  
352 finally 1× PBS, for 5 min each. Rehydrated samples were stored at 4°C in 1× PBS with 0.02% (w/v)  
353 sodium azide (NaN<sub>3</sub>) to prevent microbial and fungal growth.

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### *Ultrastructure Expansion Microscopy*

356 Cryo-fixed cells were rinsed three times with 1× PBS to remove NaN<sub>3</sub> and underwent anchoring in 1×  
357 PBS containing 1.4% formaldehyde (FA, Sigma-Aldrich) and 2% acrylamide (AA, Bio-Rad) for 3 h at  
358 37°C without agitation. Cells were then incubated in a monomer solution [23% sodium acrylate (SA,  
359 AmBeed), 10% AA, 0.1% N,N'-methylenebisacrylamide (BIS, Sigma-Aldrich), 5%  
360 Tetramethylethylenediamine (TEMED, Bio-Rad), 1× PBS and Mili-Q water] for 30 min on ice to ensure  
361 uniform monomer infusion of the cells. After monomer infusion, the glass coverslips were placed cell-  
362 side down onto an ice-cooled (4°C) gelation chamber containing ~15 µL monomer solution with 0.5%  
363 ammonium persulfate (APS, Bio-Rad) for 10 min. After initial polymerization on ice, the samples were  
364 transferred to 37°C and incubated for 45 min under humidified conditions for complete gel formation. To  
365 relax native protein assemblies and enable uniform expansion, hydrogels were next transferred to a vial  
366

367 containing denaturation buffer [200mM SDS, 200mM NaCl, 50mM Tris-Base, and Mili-Q water, (pH 9)],  
368 and incubated for 1.5 h in preheated 95°C oven or thermoblock. At this stage, gels expanded ~twofold and  
369 detached spontaneously from the coverslips. Finally, hydrogels were immersed in Mili-Q water for at  
370 least 1 h, with water exchanged every 20 min or left overnight at RT to ensure complete physical  
371 expansion and removal of denaturation agents. The size of the hydrogel was measured to calculate the  
372 macro-scale expansion factor, after which it was transferred to 1× PBS to partially shrink prior to  
373 labeling. For storage, hydrogels were cut into smaller pieces and stored at 4 °C in 1× PBS containing  
374 0.02% (w/v) NaN<sub>3</sub> to prevent microbial and fungal growth.

375

### 376 *Highly Multiplexed Labeling of Expanded Cells*

377 All incubations were performed at room temperature with constant agitation unless otherwise specified.  
378 To enhance epitope accessibility and improve signal-to-noise, hydrogels shown in **Figure 2** and  
379 **Supplementary Figure 10** were pre-treated in denaturation buffer supplemented with 100 μM β-  
380 mercaptoethanol (BME) and incubated at 95 °C for ~30 min. Prior to labeling, partially expanded  
381 (~2×) hydrogels were blocked in 3% bovine serum albumin (BSA) and 0.01% Triton X-100 in 1× PBS.  
382 All samples were labeled via indirect immunofluorescence or covalently reactive small-molecule  
383 fluorescent dyes (e.g., NHS-ester conjugates). Specifically, samples were concurrently immunolabeled  
384 with mix of previously centrifuged primary antibodies raised against distinct host species (**Table S1**)  
385 diluted at 1:50 - 1:1000 (v/v) in staining buffer, which consists of PBST [0.01% Triton-X in PBS]  
386 supplemented with 1% BSA, for 2.5 h at 37 °C. After primary antibodies incubation, samples were  
387 washed three times with an excess of PBST for 20 min each. Hydrogels were then protected from light  
388 and incubated in staining buffer containing a mix of highly cross-adsorbed secondary antibodies (**Table**  
389 **S2**), each diluted 1:500 (v/v), for 2 h at 37 °C, followed by a repetition of the washing steps. For nuclear  
390 staining, DAPI (0.3 μM, Thermo Fisher Scientific Cat# 62248) was used. For antibody stripping,  
391 hydrogels were incubated in 3 mL of denaturation buffer supplemented with 100 μM BME at 95 °C  
392 for 45 min and washed for at least 1 h with an excess of 1× PBS to remove detached antibodies. Blocking  
393 and immunostaining were followed by antibody stripping and repeated over eleven iterative rounds  
394 (**Table S6**). In each round, the microtubule network was relabeled to provide a consistent structural  
395 reference for multi-target image registration.

396

### 397 *Pre-imaging gel processing*

398 To enable iterative, volumetric imaging of defined regions of interest, expanded gels were oriented with  
399 the cellular surface facing downward and trimmed into irregular shapes matching the dimensions of the  
400 imaging dish (u-Slide 8 Well High Glass Bottom, Idibi Cat #80807). This approach minimized lateral  
401 drift and ensured consistent repositioning across imaging rounds. After removing excess water, hydrogels  
402 were placed directly onto the glass surface without Poly-D-lysine or other adhesives, as these fragile gels  
403 can tear or deform when mechanically mounted. For extended imaging sessions, gels were optionally  
404 secured by affixing the edges to a glass-bottom dish (MatTek Cat #P35G-1.5-14-C) using a small amount  
405 of hot glue applied outside the field of view

406

### 407 *Spinning Disk Confocal Microscope*

408 Cells shown in **Figure 1c**, **Supplementary Fig. 1, 4, and 6-9** were imaged using a Nikon CSU-W1 SoRa  
409 inverted spinning disk confocal microscope (Nikon Instruments), equipped with a SoRa super-resolution

410 module. The system features a dual-disk scan head, a piezo Z-drive for rapid volumetric acquisition, a  
411 motorized XY stage for multi-position imaging and tiling, and Nikon's Perfect Focus System to maintain  
412 focus stability throughout extended acquisitions. Excitation was provided by 405, 445, 488, 514, 561, and  
413 640 nm laser lines. Emitted fluorescence was detected using a Hamamatsu ORCA-Fusion sCMOS camera  
414 (C14440-20UP). Imaging was performed using multiple infinity-corrected objectives from Nikon,  
415 covering a broad range of magnifications. Depending on the application, an air-immersion Plan Fluor  $\lambda$   
416 20 $\times$ /0.75 objective (working distance (WD): 1.0 mm, MRD00205) was used for larger field-of-view  
417 imaging. Higher-resolution imaging was performed using oil-immersion objectives, including a Plan  
418 Fluor 40 $\times$ /1.30 objective (WD: 0.24 mm, MRH01401), a Plan Apo  $\lambda$  60 $\times$ /1.40 objective (WD: 0.13 mm,  
419 MRD01605), and a Plan Apo  $\lambda$  100 $\times$ /1.45 objective (WD: 0.13 mm, MRD01905). All objectives were  
420 designed for a standard cover glass thickness of 0.17 mm, providing a high numerical aperture for  
421 subcellular imaging. Z-stacks were acquired using step sizes of 0.9  $\mu$ m, 0.3  $\mu$ m, or 0.2  $\mu$ m, as appropriate  
422 for the axial resolution and sampling requirements.

423

#### 424 *Oblique Plane Microscope*

425 A custom-built oblique plane microscope (OPM) was used for imaging cells in **Figures 1d–k, i–k, 2,**  
426 **Supplementary Figures 2, 3, 5, and 10.** The OPM system was constructed in an inverted geometry and  
427 optimized for high-resolution imaging of aqueous specimens<sup>15</sup>. The sample was illuminated obliquely at  
428 45° using a water immersion objective (25 $\times$ , NA 1.1, MRD77220, Nikon). Fluorescence was collected  
429 through the same primary objective in an epi-fluorescence format and relayed to a secondary objective  
430 (20 $\times$ , NA 0.8, UPLXAPO20X, Olympus). The emission was then redirected at a 45° angle by a custom  
431 glass-tipped tertiary objective (AMS-AGY v2, 54-18-9, Applied Scientific Instrumentation) and projected  
432 onto an sCMOS camera (ORCA-Flash4.0, C13440-20CU, Hamamatsu) via a tube lens (AC508-300-A-  
433 ML, Thorlabs). The effective isotropic pixel size of 150 nm after shear/rotation was previously validated  
434 empirically by imaging calibration specimens of known dimensions (e.g., fluorescent bead samples and  
435 stage micrometer/grid standards) and confirming the expected scaling in all axes<sup>15</sup>. Excitation was  
436 provided by 405, 488, 561, and 640 nm laser lines. The system was controlled with custom LabView  
437 software interfaced through National Instruments I/O hardware (National Instruments). Z-stacks were  
438 acquired using step sizes of 0.21  $\mu$ m or 0.32  $\mu$ m.

439

#### 440 *Imaging Parameters*

441 Unless otherwise noted, all cells were volumetrically imaged in their 4.2 $\times$  expanded state to capture the  
442 full extent of their three-dimensional structure. All detailed acquisition settings, including objective types,  
443 laser powers, emission filters, Z-step sizes, and other camera configurations, are listed in **Table S8**.

444

#### 445 *Computing, Image Analysis, and Image Registration*

446 All computational analyses were performed on a SLURM-managed high-performance computing cluster.  
447 Hardware specifics are not critical to the results; for completeness, analyses were run on Red Hat  
448 Enterprise Linux 9.4 nodes with 512 GB RAM and dual Intel Xeon Gold 6354 CPUs (72 logical CPUs).  
449 Image-processing, registration, and analysis routines were implemented in Python (version  $\geq$ 3.11).  
450 JupyterLab was used for interactive development, while long-running registration and analysis pipelines  
451 were executed as SLURM scripts. Images from each staining cycle were registered using the Advanced  
452 Normalization Tools Python interface (ANTsX/ANTsPy)<sup>19</sup>. Initial alignment was performed with the

453 ‘TRSAA’ transformation method, which sequentially applies Translation, Rigid, Similarity, and two  
454 Affine transformations to achieve a high-quality affine mapping. This step was configured with multi-  
455 resolution iterations set to (1000, 500, 250, 100) to robustly converge. To further refine the alignment and  
456 correct residual non-linear deformations, we performed an elastic (non-linear) registration step using a  
457 smoothly varying deformation field. This procedure applied moderate flow smoothing and minimal total-  
458 field regularization and was executed at a single resolution level to ensure that only local, fine-scale  
459 adjustments were introduced. Additional dependencies included volumetric file I/O using tiff file, image  
460 processing via scikit-image and SimpleITK, and plotting using matplotlib and seaborn. All custom image-  
461 processing and registration routines are publicly available on GitHub  
462 (<https://github.com/TheDeanLab/clearex>), with a versioned and archived release to be deposited on  
463 Zenodo upon manuscript acceptance.

464

#### 465 *Highly Multiplexed Image Processing*

466 The raw image volumes were geometrically transformed to a standard orientation via shearing and  
467 rotation operations implemented in MATLAB as previously reported<sup>20</sup>. Registered z-stacks were imported  
468 into ImageJ (v1.54r) as separate grayscale images and merged into a single hyperstack, with each slice  
469 assigned as an individual channel. All channels were pseudo-colored by applying individual lookup tables  
470 (LUTs), and linear intensity ranges were manually adjusted using Brightness/Contrast. The final images  
471 were exported as 16-bit TIFF files for **Figure 2a** preparation. The 20-plexed visualization of cellular  
472 structures (**Fig. 2b**) was performed in napari (0.6.6), where channel-specific colormaps were individually  
473 applied. Opacity, intensity scaling, and gamma correction were manually adjusted to enable simultaneous  
474 visualization of dense cellular structures, and images were exported at full spatial resolution for  
475 downstream figure assembly.

476

#### 477 *Analysis of Staining Intensity*

478 To evaluate fluctuations in staining intensity across imaging rounds, peroxisomes and nuclei were  
479 repetitively labeled, imaged, and stripped. Imaging was performed using a spinning disk confocal  
480 microscope with constant acquisition settings between rounds. Three-dimensional image stacks were  
481 converted to maximum intensity projections, and each round was registered to the initial round (chosen as  
482 reference) using the TRSAA algorithm implemented in ANTsX/ANTsPy. Regions of interest of identical  
483 size were then selected from each cell within the field of view, and the background-corrected mean  
484 intensity was extracted for quantitative comparison across cycles.

485

#### 486 *Nuclei Size Quantification*

487 For nuclear area measurements (**Figure S4e and g**), nuclei were stained with SYTOX Green (0.167  $\mu\text{M}$ ,  
488 Invitrogen Cat# S7020) during each imaging round. Nuclei were imaged before and after full (4.2 $\times$ )  
489 expansion using a spinning disk confocal microscope, ensuring that each Z-stack encompassed the entire  
490 nuclear volume. Maximum intensity projections were generated in ImageJ (v1.54r) to produce 2D  
491 representations suitable for area quantification. Segmentation of individual nuclei was performed using  
492 Cellpose with default nuclei-segmentation parameters. Nuclei area was calculated by summing the pixels  
493 within each nucleus mask and converting pixel counts to physical units using the native pixel dimensions  
494 of the raw images. Measurements are reported in  $\mu\text{m}^2$ . For estimation of nuclear “diameter,” we report an  
495 operational linear size estimate measured along a single user-defined axis across each nucleus (i.e., a one-

496 dimensional line measurement rather than a fitted equivalent diameter). Nuclear areas (**Fig. S3e**) and  
497 diameters (**Fig. S3g**) were visualized in RStudio (R version 4.4.0) using the dplyr, tidyr, ggplot2, and  
498 ggpubr packages.

499

#### 500 *Mitochondria Detection*

501 Images were preprocessed with background subtraction and intensity rescaling. Candidate puncta were  
502 detected using Difference-of-Gaussians algorithm implemented in Skikit-image. The nominal object size  
503 was parameterized by a Gaussian-equivalent FWHM of 5 pixels, with a multi-scale search. Detection  
504 thresholds were set on a per-image basis, reflecting round-dependent intensity differences. Detected  
505 object coordinates were stored in row/column coordinates for subsequent pairing.

506

#### 507 *Nearest-Neighbor-Based Target Registration Error Estimate*

508 To estimate registration accuracy independently of the reference channel, we quantified a target-  
509 registration-error (TRE) proxy by (i) registering imaging rounds using the microtubule channel and (ii)  
510 measuring residual point-to-point misalignment on mitochondrial puncta, which were not used to compute  
511 the registration transforms. To expedite analysis, volumetric tiff stacks were reduced to 2D maximum-  
512 intensity projections. Five staining rounds were analyzed, and registration was performed pairwise using  
513 round 1 as the fixed reference and rounds 2–5 as moving images. This included the ANTsPy TRSAA  
514 transform, which applies a pyramidal sequence of transforms to obtain a robust mapping between rounds.  
515 The resulting transform was then applied to both microtubules and mitochondria. To correct residual local  
516 distortions, a deformable registration was performed on the TRSAA-aligned microtubules using a  
517 nonlinear registration (type “SyNOnly”). For mitochondria, we applied the affine TRSAA transform  
518 followed by the SyN deformation field; in ANTsPy this was implemented using the standard transform  
519 list ordering (SyN transforms listed before TRSAA) when resampling the original moving mitochondria  
520 image.

521

522 Mitochondrial puncta were detected independently in the fixed mitochondria MIP and in each  
523 transformed mitochondria MIP under both transform conditions. To estimate a TRE proxy, puncta were  
524 paired between the fixed and transformed mitochondria images using mutual nearest-neighbor (MNN)  
525 matching. Specifically, a k-d tree was constructed for each point set, each moving point was assigned its  
526 nearest fixed neighbor, and each fixed point its nearest moving neighbor. Pairs were retained only if the  
527 association was mutual (moving to fixed and fixed to moving). Pairing was evaluated with multiple  
528 distance gates (unlimited, 10 px, 5 px, 3 px) to characterize sensitivity to the matching threshold. For each  
529 condition and round, we summarized the distribution of paired distances by mean, median, standard  
530 deviation, 95th percentile (P95), maximum, and RMS distance. Distances were corrected for specimen  
531 expansion using an effective pixel size of 38.7 nm.

532

#### 533 *Descriptor- and RANSAC-based Target Registration Error Estimate*

534 To obtain a more conservative estimate of residual misalignment that is not driven by local, ambiguous  
535 nearest-neighbor assignments, we complemented mutual nearest-neighbor pairing with a descriptor- and  
536 RANSAC-based landmark matching approach. Here, “globally consistent” refers to correspondences that  
537 are jointly explainable by a single best-fit similarity transform (translation/rotation/scale) between rounds,  
538 rather than independent local pairings. Mitochondrial puncta coordinates (detected as described above)

539 were treated as candidate landmarks for feature matching between imaging rounds. For each pairwise  
540 comparison, maximum-intensity projections were used, and images were cropped to a common  
541 overlapping field of view when necessary to ensure identical dimensions prior to matching. Binary BRIEF  
542 descriptors were computed at mitochondrial landmark locations, and putative correspondences were  
543 identified by matching descriptors using Hamming distance. Because descriptor matching can include  
544 spurious pairs, RANSAC was used to robustly fit a similarity-transform model and reject outliers,  
545 retaining only inlier landmark pairs consistent with a single global transform. The similarity transform  
546 was then refit using all inliers. To avoid reporting an optimistically biased fit error, we computed a cross-  
547 validated TRE-like proxy by repeatedly fitting the similarity transform on a subset of inlier  
548 correspondences and evaluating residual distances on held-out inliers; the root mean square of these held-  
549 out residuals was used as the final descriptor-based registration accuracy estimate.

550

### 551 *Antibody Signal Distribution Analysis*

552 Cells and nuclei were individually segmented with CDC42 as a diffuse cytoplasmic marker, and DAPI as  
553 a nuclei marker using u-Segment3D<sup>21</sup> and pretrained Cellpose<sup>22</sup> 2D segmentation models. The distance  
554 transform was computed using u-Unwrap3D<sup>23</sup> and is the Fast-Marching Method solution to the Eikonal  
555 equation with the nuclei mask as a source term, and the cell mask as a boundary condition<sup>21</sup>. We  
556 normalize the distance transform by dividing by the maximum value after masking out the cell exterior  
557 and nuclear interior regions. The normalized distance,  $r \in (0,1)$  was then equipartitioned into 50  
558 intervals. The signal distribution of each antibody was constructed as the median voxel intensity in each  
559 interval. To group signal distributions, we constructed the pairwise Pearson correlation matrix and applied  
560 hierarchical clustering to the matrix with a Euclidean metric and Ward linkage.

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## SUPPLEMENTARY FIGURE CAPTIONS

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**Figure S1. Impact of Freezing Kinetics on Cellular Integrity.** Representative spinning disk confocal images of 4.2× expanded and N-hydroxysuccinimide ester stained MEF cells subjected to: (a) rapid guillotine plunge freezing and (b) hand operated freezing. Insets squares highlight selected cells shown at higher magnification. Cracks and ruptures in cellular architecture were more frequently observed following hand-operated freezing, as seen in panel b. Imaging was performed using 20×, 40×, and 100× objectives. Maximum intensity projections are shown. Scale bars: 20 μm (corrected for the expansion factor).

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**Figure S2. Comparison of Fixation Methods.** Deconvolved, maximum intensity projections of microtubules (anti-α-Tubulin, Sigma-Aldrich Cat# T9026, RRID:AB\_477593) and mitochondria (anti-TOM20, Proteintech Cat# 11802-1-AP, RRID:AB\_2207530) in 4.2× expanded MEF cells subjected to: (a–d) 4% paraformaldehyde (PFA) fixation, (e–h) 4% PFA + 0.2% glutaraldehyde (GA) fixation, (i–l) cytoskeleton-preservation-optimized fixation<sup>18</sup>, (m–p) 100% methanol fixation, (q–t) and cryofixation by guillotine-style plunge-freezing. Red squares in merged images correspond to zoomed regions of interest shown in (c, g, k, o, s). Images acquired with a custom-built oblique plane microscope. All scale bars are corrected for the expansion factor. While traditional fixation methods are effective for select structures, cryofixation offers the most comprehensive preservation of native cellular architecture, effectively maintaining the native architecture of cytoskeletal compartments as well as membrane-bound organelles. Methanol, for example, is commonly used for cytoskeletal preservation but can induce depolymerization of microtubules and actin filaments. Aldehyde-based fixatives such as PFA form covalent crosslinks that may mask epitopes and necessitate additional antigen retrieval steps. In contrast, cryofixation preserves proteins in their native state without chemical modification, resulting in superior epitope accessibility and antigenicity for high-resolution immunofluorescence imaging.

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**Figure S3. Enhanced resolution in expanded cells visualized by Cy-ExM.** (a) Non-expanded and (b) expanded MEF cells stained for DNA (SYTOX Orange, Invitrogen Cat# S11368) and the outer mitochondrial membrane (anti-TOMM20, Abcam Cat# ab232589, RRID:AB\_3065091). Representative but distinct cells are shown in each condition. Cells were imaged volumetrically using an oblique plane microscope. Deconvolved maximum intensity projections are shown for standard immunofluorescence (a) and for cells processed with a single round of the Cy-ExM workflow (b). Insets highlight representative subcellular features, demonstrating improved spatial resolution and structural detail following 4.2× expansion. Scale bars: 10 μm (overview), 1 μm (insets), corrected for the expansion factor.

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**Figure S4. Validation of expansion consistency and iterative labeling workflow.** (a) Schematic illustrating the iterative labeling workflow used in Cy-ExM. (b) Macroscopic gel conditioning across rounds. Representative images of the same hydrogel alternating between full expansion in deionized water and partial shrinkage in 1× PBS during staining. The apparent ~2× change in gel diameter reflects this reversible water/PBS conditioning and is shown to illustrate handling during iterative cycles; it is not the 4.2× cellular expansion factor used for imaging. (c–d) Spinning disk confocal images of the same population of MEF cells stained for DNA (SYTOX Green, Invitrogen Cat# S7020), acquired before (c) and after (d) full 4.2× expansion. (e) Quantification of expansion repeatability across labeling rounds by measuring nuclear area in the fully

606 expanded state. Green lines link corresponding nuclei across rounds to visualize consistency.  
607 (f) Example of three randomly selected nuclei tracked and iteratively imaged over five expansion rounds;  
608 yellow lines denote positions used for diameter measurements.  
609 (g) Measured nuclear diameters of the three nuclei across rounds, confirming consistent expansion. Line  
610 colors correspond to the artificially assigned nuclear colors shown in (f).  
611 The  $4.2\times$  linear expansion factor was calculated from nuclear area as the square root of the area in the  
612 expanded state divided by the area in the unexpanded state. All imaging was performed under identical  
613 acquisition conditions for each round. All scale bars are corrected for the expansion factor.

614

615 **Figure S5. Registration Strategy, Deformation Quantification, and Overlay of Registration Results.**

616 (a) Schematic of the registration pipeline. Samples were sequentially aligned using translation, rigid body,  
617 similarity, and affine transforms, followed by a non-linear warp registration to correct for local  
618 distortions. (b) Vector plot illustrating local deformations from the warp field for a representative 2D  
619 section of the image. (c) Result of the registration routine enabling precise alignment of the microtubule  
620 network across independent labeling rounds. Original image in top left corner (first staining, red) and  
621 registered overlay (first and second staining, red + cyan) are shown, with inset squares. All scale bars  
622 were corrected for the expansion factor.

623

624 **Figure S6. Multi-round registration accuracy assessed by microtubule-guided alignment and  
625 independent mitochondrial landmark matching.**

626 Five imaging rounds are shown (rows), with each column depicting a successive stage of the registration workflow. Left: raw overlays of microtubules  
627 (orange) and mitochondria (cyan). Second column: microtubule channel after linear registration to round  
628 1. Third column: mitochondria channel after applying the linear transform, with detected mitochondrial  
629 puncta overlaid; cyan and lime circles denote puncta detected in the fixed (round 1) and transformed  
630 moving images, respectively. Fourth column: microtubule channel after both linear and nonlinear  
631 registration. Fifth column: mitochondria channel after applying the combined linear and non-linear  
632 transforms, with matched puncta displayed as in the third column. Round 1 serves as the fixed reference  
633 and is therefore identical across conditions. Imaging was performed with a spinning disk confocal  
634 microscope at 40x magnification.

635

636 **Figure S7. Iterative peroxisome imaging validates registration accuracy and stripping efficiency.**

637 (a)  $4.2\times$  expanded MEF cells stained for DNA (SYTOX Green, Invitrogen Cat# S7020) and peroxisomes  
638 (anti-PMP70, Thermo Fisher Scientific Cat# PA1-650, RRID:AB\_2219912) were iteratively imaged  
639 across five rounds of the Cy-ExM workflow. Shown is the same colony of cells in the labeled state (left)  
640 and after successful antibody removal (right). For each round, identical labeling conditions were used  
641 (antibody concentration, incubation time, and temperature), followed by overnight expansion in deionized  
642 water. In the image from Round 1, dashed-line squares indicate the regions of interest (ROIs) where  
643 fluorescence signal intensity was consistently measured in each round. Imaging was performed on a  
644 spinning disk confocal microscope using a  $20\times$  objective, with unchanged acquisition settings. For  
645 peroxisomes: 640 nm laser at 60 mW and 200 ms exposure was applied every time, ensuring  
646 reproducibility for average signal intensity quantification shown in (b). Scale bars:  $20\ \mu\text{m}$  (corrected for  
647 the expansion factor).

648

649 **Figure S8. Cycle permutation confirms antigen stability across rounds.** (a) Schematic of the  
650 permutation experiment workflow. (b) Cells embedded in hydrogel A were expanded and stained for  
651 DNA (DAPI, Thermo Scientific Cat# 62248) and the Golgi apparatus (anti-GOLGA2/GM130,  
652 Proteintech Cat# 11308-1-AP, RRID:AB\_2115327), while (c) cells in hydrogel B were simultaneously  
653 stained for DNA (DAPI) and the endoplasmic reticulum (ER; anti-calnexin, Abcam Cat# ab22595,  
654 RRID:AB\_2069006). Following  $\beta$ -mercaptoethanol (BME) treatment to remove antibodies, the hydrogels  
655 were re-stained in the opposite configuration: hydrogel A for DNA and ER, and hydrogel B for DNA and  
656 Golgi, using the same antibodies and labeling conditions. Insets in (d) and (g) highlight a MEF  
657 undergoing late cytokinesis (telophase-to-G1 transition), a stage characterized by organelle reorganization  
658 and nuclear reassembly during daughter cell separation. The cell contains two nascent daughter nuclei  
659 connected by a persistent cytoplasmic bridge, consistent with incomplete abscission. (d) reveals extensive  
660 ER continuity across the bridge, suggesting active ER remodeling, while (g) shows a fragmented Golgi  
661 apparatus distributed around the daughter nuclei, consistent with Golgi vesiculation during mitotic exit.  
662 All scale bars are corrected for the expansion factor: 20  $\mu\text{m}$  (b, c, e, f) and 10  $\mu\text{m}$  (d, g). Images were  
663 acquired using a spinning disk confocal microscope with a 20 $\times$  objective under identical acquisition  
664 settings.

665  
666 **Figure S9. Benchmarking Cy-ExM across repeated labeling cycles.** (a) Schematic of the experiment:  
667 hydrogels with MEF cells were subjected to 10 Cy-ExM cycles, each including: 1 h blocking, 2.5 h  
668 incubation in primary antibody staining solution, 1 h of washing, 2 h incubation in secondary antibody  
669 staining solution, followed by 2 h of physical expansion in water, and 45 min of  $\beta$ -mercaptoethanol  
670 treatment in 95  $^{\circ}\text{C}$ . Two hydrogels were independently stained: first (b) for microtubules (anti- $\alpha$ -Tubulin,  
671 Sigma-Aldrich Cat# T9026, RRID:AB\_477593), endoplasmic reticulum (anti-calnexin, Abcam Cat#  
672 ab22595, RRID:AB\_2069006) and DNA (DAPI, Thermo Scientific Cat# 62248), while the second gel (c)  
673 was stained for microtubules (anti- $\alpha$ -Tubulin, Selleckchem Cat# F1566), mitochondria (anti-HSP60,  
674 Abcam Cat# ab46798, RRID:AB\_881444), actin filaments (anti- $\beta$ -actin, Sigma-Aldrich Cat# A1978,  
675 RRID:AB\_476692) and DNA (DAPI). Hydrogels were imaged every 5 rounds using a spinning disk  
676 confocal microscope with a 20 $\times$  objective under identical acquisition settings. Scale bars: 50  $\mu\text{m}$   
677 (corrected for the expansion factor).

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679 **Figure S10. Fourteen-plex Cy-ExM imaging of subcellular organization in a MEF cell.** (a–d)  
680 Maximum-intensity projections (MIPs) from the same cell with targets grouped by biological function: (a)  
681 secretory pathway, (b) cytoskeletal components, (c) metabolic organelle network, and  
682 (d) nuclear organization. (e) Corresponding single-channel MIPs for each of the 14 targets shown  
683 individually; colors in (e) match the merged images corresponding to the functional classes in (a–d). All  
684 samples were processed using the Cy-ExM workflow and imaged volumetrically using an oblique plane  
685 microscope. Scale bar: 5  $\mu\text{m}$  (corrected for the expansion factor).

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## SUPPLEMENTARY MOVIE CAPTIONS

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**Supplementary Movie 1. Three-dimensional volume rendering of peroxisomes, microtubules, and nuclei.** Data were deconvolved and geometrically reoriented to correct the oblique plane microscopy imaging geometry (shear/deskew) and rotated into the standard viewing perspective of an inverted microscope (see **Methods**). Volumetric imaging was performed using an oblique plane microscope. Scale bar: 5  $\mu\text{m}$ .

**Supplementary Movie 2. Z-stack rendering of the registered microtubule network across two independent immunolabeling rounds.** The overlay of the first staining (red) with the registered second staining, after antibody stripping (cyan) demonstrates the accuracy of the registration routine and capability to repeatedly target the same cellular component. Imaged volumetrically using an oblique plane microscope. Scale bar: 5 microns.

**Supplementary Movie 3. Three-dimensional visualization of a 20-plex Cy-ExM dataset.** Three-dimensional rendering of 20 distinct cellular targets from a single cell, grouped according to their primary biological function, including nuclear/nucleolar components, mitochondria, secretory pathway organelles, endomembrane trafficking compartments, cytoskeletal structures, and adhesion-related proteins. The volume is displayed as an attenuated maximum-intensity projection with additive blending to highlight spatial relationships among molecular assemblies throughout the cellular volume. Colored bars adjacent to each label indicate the per-channel intensity look-up table used for visualization. Data were imaged volumetrically using an oblique plane microscope.

**Supplementary Movie 4. Two-dimensional Z-flythrough of a 20-plex Cy-ExM dataset grouped by biological function.** A 20-target Cy-ExM dataset from a single cell is shown as a sequence of 2D optical sections. Targets are grouped by primary biological function (nuclear, mitochondria, secretory pathway organelles, endomembrane trafficking, and cytoskeletal structures) to facilitate interpretation of subcellular organization across depth. The current Z position is annotated in the upper-left corner of the movie. Colored bars adjacent to each label indicate the per-channel intensity look-up table used for visualization. Data were acquired volumetrically using an oblique plane microscope.

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## SUPPLEMENTARY TABLES

**Table S1. Primary antibodies and dyes used in this study.** The table lists targets, clone information, host species and isotype, stock concentration, working dilution, vendor, and catalog number for each reagent. Abbreviations: host—Ra, rabbit; C, chicken; M, mouse; Rt, rat; stock concentration—ND, not determined.

Primary antibody	Targeted structure	Clone	Host / Isotype	Stock Conc. [mg/mL] / (dilution used)	Vendor	Catalog no.	RRID
Calnexin	Endoplasmic reticulum	Polyclonal	Ra / IgG	0.9 / (1:250)	Abcam	ab22595	AB_2069006
CDC42	Rho GTPase	Polyclonal	C / IgY	1 / (1:125)	Invitrogen	PA5-20764	AB_1115325
CDK9	Transcriptional complexes	1G6B3	M / IgG1	1 / (1:200)	Proteintech	67256-1-Ig	AB_3085038
CLTC	Endocytic vesicles	1B3D7	M / IgG1	1.5 / (1:250)	Proteintech	66487-1-Ig	AB_2881852
DAPI	Nucleus (DNA)	---	---	1 / (1:1000)	ThermoFisher	62248	N/A
DRP1	Mitochondria fission sites	Polyclonal	Ra / IgG	0.5 / (1:200)	Proteintech	26187-1-AP	AB_2880417
EEA1	Early endosomes	Polyclonal	Ra / IgG	1 / (1:200)	Invitrogen	PA1-063A	AB_2096819
Fascin	Filopodia / actin bundles	55K-2	M / IgG1, kappa	0.0504 / (1:100)	Dako	M3567	AB_2278596
FBL	Nucleolus / fibrillar	Polyclonal	Ra / IgG	0.25 / (1:150)	Proteintech	16021-1-AP	AB_2105788
GM130	Golgi apparatus (cis-Golgi)	M342	M / IgG1	0.25 / (1:250)	Invitrogen	MA5-47668	AB_2942649
GM130	Golgi apparatus (cis-Golgi)	Polyclonal	Ra / IgG	0.6 / (1:250)	Proteintech	11308-1-AP	AB_2115327
HSP60	Mitochondrial matrix	Polyclonal	Ra / IgG	0.9 / (1:200)	Abcam	ab46798	AB_881444
Lamin A/C	Nuclear envelope	Polyclonal	C / IgY	ND / (1:200)	Invitrogen	PA5-143574	AB_2942803
Lamin A/C	Nuclear envelope	4C11	M / IgG2a	0.007 / (1:200)	Cell Signaling	4777	AB_1054575
Lamin B1	Nuclear envelope	Polyclonal	Ra / IgG	0.7 / (1:200)	Proteintech	12987-1-AP	AB_2136290
LAMP2	Lysosomes	241893A7	Ra / IgG	1 / (1:150)	Proteintech	84474-5-RR	N/A
NHS-Ester	Total proteins	---	---	2 / (1:2000)	Sigma-Aldrich	07376	N/A
NUP p62	Nuclear pores	53	M / IgG2b	0.25 / (1:250)	BD	610497	AB_397863
PCNA	DNA replication foci	PC10	M / IgG2a	0.079 / (1:125)	Cell Signaling	2586	AB_2160343
PEX14	Peroxisomes	Polyclonal	Ra / IgG	0.6 / (1:250)	Proteintech	10594-1-AP	AB_2252194
PMP70	Peroxisomes	Polyclonal	Ra / IgG	1 / (1:300)	Invitrogen	PA1-650	AB_2219912
RPA32	DNA repair foci	4E4	Rt / IgG1	0.262 / (1:125)	Cell Signaling	2208	AB_2238543
RPS6	Ribosomes	1C3E10	M / IgG2a	1.5 / (1:150)	Proteintech	66886-1-Ig	AB_2882218
SYTOX Green	Nucleus (DNA)	---	---	~3.5 (1:30000)	Invitrogen	S7020	N/A
SYTOX Orange	Nucleus (DNA)	---	---	~3.5 (1:50000)	Invitrogen	S11368	N/A
TOM20	Outer mitochondrial membrane	Polyclonal	Ra / IgG	0.25 / (1:200)	Proteintech	11802-1-AP	AB_2207530
TOMM20	Outer mitochondrial membrane	EPR15581-54	Ra / IgG	1.034 / (1:200)	Abcam	ab232589	AB_3065091
Vimentin	Intermediate filaments	Polyclonal	C / IgY	ND / (1:200)	Invitrogen	PA1-10003	AB_2216267
Vinculin	Focal adhesions	7F9	M / IgG1, kappa	0.5 / (1:125)	Invitrogen	14-9777-82	AB_2573028
WGA	Glycoconjugates	---	---	1 / (1:50)	Biotium	29022-1	N/A
$\alpha$ -Tubulin	Microtubules	G9A12	Rt / IgG2a	2 / (1:200)	Selleckchem	F1566	N/A
$\alpha$ -Tubulin	Microtubules	DM1A	M / IgG1	ND / (1:200)	Sigma-Aldrich	T9026	AB_477593
$\beta$ -Actin	Actin filaments	AC-15	M / IgG1	2 - 2.5 / (1:250)	Sigma-Aldrich	A1978	AB_476692
$\beta$ -Catenin	Adherens junctions	L87A12	M / IgG1	ND / (1:150)	Cell Signaling	2698	AB_1030945

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725 **Table S2. Summary of secondary antibodies used in the study.** Listed are the host species and  
 726 reactivity, conjugation, clonality, stock concentrations and working dilutions, as well as the vendor and  
 727 catalog numbers for each secondary antibody.

Host & Reactivity	Conjugation	Clonality	Isotype	Stock Conc. (dilution used)	Vendor	Catalog Number	RRID
Donkey anti-Rat	Alexa Fluor 488	Polyclonal	IgG	2 mg/mL (1:500)	Invitrogen	A-21208	AB_2535794
Donkey anti-Chicken	Alexa Fluor 488		IgG		Invitrogen	A-78948	AB_2921070
Donkey anti-Mouse	CF555		IgG		Biotium	20037	AB_1085438
Donkey anti-Rabbit	Alexa Fluor 674		IgG		Invitrogen	A-31573	AB_2536183

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730 **Table S3. Affine registration metrics.** Reported values include shear, rotation, and scale parameters, as  
 731 well as the mean, median, and maximum displacement measured for the non-linear warp transform. Data  
 732 were acquired with the oblique plane microscope.

Rotation (Degrees)		
Z (Yaw) = 0.3	Y (Pitch) = 0.01	X (Roll) = -0.25
Scale (Amplitude)		
Z = 1.03	Y = 1.07	X = 1.03
Shear (Degrees)		
XY = 0.18	XZ = 0.08	YZ = 0.03
Warp Displacement (nm)		
Mean = 77.53	Median = 58.28	Max = 558.13

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735 **Table S4. Quantitative evaluation of registration accuracy using intensity- and structure-based**  
736 **similarity metrics.** Normalized cross-correlation (NCC) and Mattes mutual information (MI) were  
737 computed using the ANTsPy package with regular sampling and a 50% voxel sampling fraction.  
738 Structural similarity index (SSIM) was computed using the scikit-image package. Metrics are reported for  
739 raw (unregistered) data, after linear (affine) registration, and after additional non-linear registration for  
740 each imaging channel. While linear registration substantially improved global similarity metrics, non-  
741 linear registration did not further increase these global similarity metrics. SSIM likewise showed no  
742 improvement with non-linear warping and, in this dataset, decreased after registration, consistent with  
743 SSIM's sensitivity to intensity scaling, background differences, and local contrast changes introduced by  
744 interpolation and resampling. Together, these results suggest the interpretation that non-linear registration  
745 primarily corrects localized geometric distortions that may not be captured by global intensity-based  
746 similarity measures.

**Normalized Cross-Correlation (NCC)**

<b>Channel</b>	<b>Raw Data</b>	<b>Linearly Registered</b>	<b>Nonlinearly Registered</b>
DNA	0.598	0.626	0.626
Microtubules	0.127	0.581	0.581
Peroxisomes	0.011	0.075	0.075

**Mattes Mutual Information (MI)**

<b>Channel</b>	<b>Raw Data</b>	<b>Linearly Registered</b>	<b>Nonlinearly Registered</b>
DNA	0.101	0.133	0.133
Microtubules	0.040	0.094	0.094
Peroxisomes	0.0006	0.0028	0.0028

**Structural Similarity Index (SSIM)**

<b>Channel</b>	<b>Raw Data</b>	<b>Linearly Registered</b>	<b>Nonlinearly Registered</b>
DNA	0.9649	0.9682	0.9944
Microtubules	0.4774	0.8194	0.9403
Peroxisomes	0.4774	0.8192	0.9404

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750 **Table S5. Independent estimates of registration error using mitochondrial landmarks across**  
751 **iterative imaging rounds.** Registration accuracy was quantified in the mitochondrial channel after  
752 microtubule-guided registration. For each moving round (2–5) relative to round 1, a target-registration-  
753 error-like proxy was computed using (i) mutual nearest-neighbor pairing of detected mitochondrial  
754 puncta and reporting the RMS paired distance, and (ii) a descriptor-based RANSAC approach that fits a  
755 global similarity transform to inlier matches, reporting both the inlier RMS residual and a cross-validated  
756 RMS residual on held-out inliers. Metrics are shown for linear registration alone and for combined linear  
757 plus non-linear registration. Distances are reported in nanometers.

	<b>Nearest-Neighbor</b>		<b>RANSAC</b>
<b>Linear Registration</b>	<b>RMS (nm)</b>	<b>RMS (nm)</b>	<b>Cross-Validated RMS (nm)</b>
Round 2	124	97	108
Round 3	124	93	97
Round 4	130	88	85
Round 5	118	70	74
Mean	124	87	91
<b>Non-Linear Registration</b>			
Round 2	122	99	113
Round 3	127	95	107
Round 4	131	84	89
Round 5	117	85	92
Mean	124	91	100

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760 **Table S6. Multiplexed labelling experimental design for visualization of subcellular organization.**  
 761 Experimental design showing the antibody host species, fluorophore excitation channels (405, 488, 555,  
 762 and 647 nm), and corresponding targets imaged across eleven labeling rounds. The 488 nm or 555 nm  
 763 channel was used as a registration channel throughout all cycles. At the bottom, the number of targets  
 764 visualized per channel is summarized, along with the total number of distinct labels imaged across the full  
 765 multiplexing experiment.

<b>Iteration</b>	<b>405</b>	<b>488: chicken / rat</b>	<b>561: mouse</b>	<b>640: rabbit</b>
Round 1	Nucleus [DAPI, #62248]	Microtubules [ $\alpha$ -Tubulin, #F1566]	Actin filaments [ $\beta$ -actin, #A1978]	Endoplasmic reticulum [Calnexin, #ab22595]
Round 2		Microtubules [ $\alpha$ -Tubulin, #F1566]	Nuclear pores [NUP p62, #610497]	Nuclear envelope [Lamin B1, #12987-1-AP]
Round 3		Microtubules [ $\alpha$ -Tubulin, #F1566]	Focal adhesions [Vinculin, #14-9777-82]	Early endosomes [EEA1, #PA1-063A]
Round 4		Intermediate filaments [Vimentin, #PA1-10003]	Microtubules [ $\alpha$ -Tubulin, #T9026]	Mitochondrial membrane [TOM20, #11802-1-AP]
Round 5		Rho GTPase [CDC42, #PA5-20764]	Microtubules [ $\alpha$ -Tubulin, #T9026]	Lysosomes [LAMP2, #84474-5-RR]
Round 6		Microtubules [ $\alpha$ -Tubulin, #F1566]	Endocytic vesicles [CTLC, #66487-1-Ig]	Peroxisomes [PEX14, #10594-1-AP]
Round 7		Microtubules [ $\alpha$ -Tubulin, #F1566]	Adherens junctions [ $\beta$ -catenin, #2698]	Mitochondria fission sites [DRP13, #26187-1-AP]
Round 8		Microtubules [ $\alpha$ -Tubulin, #F1566]	—	Golgi apparatus [GM130, #11308-1-AP]
Round 9		Microtubules [ $\alpha$ -Tubulin, #F1566]	---	Fibrillarin [FBL, #16021-1-AP]
Round 10		Microtubules [ $\alpha$ -Tubulin, #F1566]	---	Mitochondrial matrix [HSP60, #ab46798]
Round 11		Glycoconjugates [WGA, #29022-1]	Microtubules [ $\alpha$ -Tubulin, #T9026]	---
<i>targets visualized</i>	<i>1</i>	<i>4</i>	<i>6</i>	<i>10</i>
$\Sigma$			<i>21</i>	

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769 **Table S7. Quantitative registration parameters across iterative imaging rounds.** Reported values  
 770 summarize the decomposition of affine and non-linear registration transforms between round 1 and  
 771 subsequent imaging rounds. Parameters include translation ( $\mu\text{m}$ ), rotation (degrees), scale (unitless), and  
 772 shear (degrees) derived from the affine transform, as well as the mean, maximum, and standard deviation  
 773 of the displacement field from the non-linear warp. Mean and standard deviation values across rounds are  
 774 provided to quantify the magnitude and variability of round-to-round geometric transformations.

	Translation (microns)			Rotation (Degrees)		
	Z	Y	X	Z (Yaw)	Y (Pitch)	X (Roll)
<i>Round 2</i>	0.049	-0.778	0.157	-3.14	-1.04	-0.31
<i>Round 3</i>	0.051	-2.121	1.445	-7.97	-1.52	-0.08
<i>Round 4</i>	0.683	1.859	-0.879	5.56	-1.55	-0.53
<i>Round 5</i>	1.111	-0.639	-1.005	-1.99	4.77	1.24
<i>Round 6</i>	0.102	-0.450	-0.467	-1.63	-1.34	-1.03
<i>Round 7</i>	0.246	-1.267	-0.728	-3.5	-1.36	-0.85
<i>Round 8</i>	0.076	-0.601	-1.114	-1.84	-1.39	-0.57
<i>Round 9</i>	0.107	-0.193	-1.819	-0.36	-0.89	-1.17
<i>Round 10</i>	0.245	-0.560	-0.811	-1.34	-1.36	-0.71
<i>Round 11</i>	3.751	11.932	9.240	-2.91	-1.62	-0.33
<i>Mean</i>	0.642	0.718	0.402	-1.91	-0.73	-0.43
<i>Std. Dev.</i>	1.145	4.065	3.225	3.34	1.95	0.68

	Shear (Degrees)			Scale (Amplitude)		
	XY	XZ	YZ	Z	Y	X
<i>Round 2</i>	-0.54	1.23	0.06	0.943	1.013	1.0192
<i>Round 3</i>	-0.33	1.58	0.19	0.916	1.0017	1.0116
<i>Round 4</i>	-0.25	1.72	0.24	0.822	1.0031	1.0155
<i>Round 5</i>	1.15	4.56	-0.22	0.582	0.993	1.0042
<i>Round 6</i>	-1.06	1.58	0.03	0.982	1.0058	1.0191
<i>Round 7</i>	-1.02	1.00	-0.05	0.968	0.9979	1.0120
<i>Round 8</i>	-0.69	1.47	0.07	1.006	1.0052	1.0196
<i>Round 9</i>	-1.12	0.58	-0.02	1.080	1.0071	1.0146
<i>Round 10</i>	-0.76	1.01	-0.11	0.975	1.0059	1.0116
<i>Round 11</i>	-0.58	1.5	-0.12	0.934	1.0003	1.0117
<i>Mean</i>	-0.52	1.62	0.007	0.920	1.0033	1.0139
<i>Std. Dev.</i>	0.66	1.09	0.14	0.136	0.0055	0.0048

	Warp Amplitude ( $\mu\text{m}$ )			
	Minimum	Mean	Std. Deviation	Maximum
<i>Round 2</i>	0.0	0.139	0.137	0.849
<i>Round 3</i>	0.0	0.143	0.143	0.873
<i>Round 4</i>	0.0	0.140	0.117	0.700
<i>Round 5</i>	0.0	0.171	0.135	0.831
<i>Round 6</i>	0.0	0.150	0.150	0.908
<i>Round 7</i>	0.0	0.147	0.136	0.849
<i>Round 8</i>	0.0	0.152	0.142	0.858
<i>Round 9</i>	0.0	0.121	0.101	0.636
<i>Round 10</i>	0.0	0.146	0.143	0.862
<i>Round 11</i>	0.0	0.142	0.129	0.836
<i>Mean</i>	0.0	0.145	0.133	0.820
<i>Std. Dev.</i>	0.0	0.012	0.015	0.084

776 **Table S8. Imaging Parameters.** Detailed summary of imaging conditions used on the pinning disk  
 777 confocal microscope (SoRa) and oblique plane microscope (OPM), including objective specifications  
 778 (immersion type and magnification), physical pixel size ( $\mu\text{m}$ ), wavelengths (nm), emission filter type, z-  
 779 step size ( $\mu\text{m}$ ), exposure time (ms), and labels used.

Figure	Setup	Objective	Pixel size ( $\mu\text{m}$ )	Excitation Wavelength (nm)	Emission filter	Step size ( $\mu\text{m}$ )	Exp. time (ms)	Labels
1c	SoRa	Nikon CFI Plan Apochromat Lambda 100X Oil	0.07	488	525/50	0.2	200	#F1566
1d-g	OPM	Nikon CFI75 Apo 25XC W	0.15	561 640	598/25 647LP	0.32	100	#T9026 #11802-1-AP #S7020
1i-k	OPM	Nikon CFI75 Apo 25XC W	0.15	561 640	598/25 647LP	0.21	100	#T9026 #PA1-650
2	OPM	Nikon CFI75 Apo 25XC W	0.15	see Table S6	525/50 598/25 647LP	0.32	50 - 100	see Table S6
		Nikon CFI Plan Apochromat Lambda 20X	0.32			0.9		
S1	SoRa	Nikon CFI Plan Fluor 40X Oil	0.16	640	700/76	0.3	100	#07376
		Nikon CFI Plan Apochromat Lambda 100X Oil	0.07			0.2		
S2	OPM	Nikon CFI75 Apo 25XC W	0.15	561 640	598/25 647LP	0.32	100	#T9026 #11802-1-AP
S3	OPM	Nikon CFI75 Apo 25XC W	0.15	561 640	598/25 BLP01-647R	0.32	100	#S11368 #ab232589
S4	SoRa	Nikon CFI Plan Apochromat Lambda 20X	0.32	488	525/50	0.9	300	#S7020
S5	OPM	Nikon CFI75 Apo 25XC W	0.15	561	598/25	0.21	100	#T9026
S6	SoRa	Nikon CFI Plan Fluor 40X Oil	0.16	561 640	603/54 700/76	0.3	200 200	#T9026 #11802-1-AP
S7	SoRa	Nikon CFI Plan Apochromat Lambda 20X	0.32	488 640	525/50 700/76	0.9	200	#S7020 #PA1-650
S8b, f, g	SoRa	Nikon CFI Plan Apochromat Lambda 20X	0.32	405 640	460/50 700/76	0.9	200	#62248 #11308-1-AP
S8c-e	SoRa	Nikon CFI Plan Apochromat Lambda 20X	0.32	405 640	460/50 700/76	0.9	200	#62248 #ab22595
S9b	SoRa	Nikon CFI Plan Apochromat Lambda 20X	0.32	405 561 640	460/50 603/54 700/76	0.9	200	#62248 #T9026 #ab22595
S9c	SoRa	Nikon CFI Plan Apochromat Lambda 20X	0.32	488 561 640	525/50 603/54 700/76	0.9	200	#F1566 #A1978 #ab46798
S10	OPM	Nikon CFI75 Apo 25XC W	0.15	See Table S6	525/50 598/25 647LP	0.32	50 - 100	see Table S6

780 \*For the full list of host-complementary secondary antibodies used in all experiments, see **Table S2**.

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## SUPPLEMENTARY NOTES

### Supplementary Note 1 – Strategies for Multiplexed Immunostaining in Expansion Microscopy.

Expansion Microscopy (ExM) has rapidly evolved since its first description, providing a powerful means to achieve nanoscale imaging with conventional microscopes. The original protocol, however, relied on pre-expansion labeling combined with harsh proteolytic digestion, which destroyed most proteins and left only covalently anchored fluorophores as “phantoms” of the original structures<sup>24</sup>. While effective for visualization of a limited number of targets (typically on the order of a few), this approach was inherently incompatible with highly multiplexed labeling strategies. To address these limitations, numerous ExM variants have been developed with alternative gel chemistries, denaturation strategies, and labeling schemes, greatly broadening its utility for imaging single cells, tissue sections, and even entire organisms.

Today, immunostaining in ExM generally falls into two camps: pre-expansion labeling, in which targets are stained before gelation and expansion, and post-expansion labeling, where staining is performed after the specimen has been expanded. To perform multiplexing in a format compatible with pre-expansion immunostaining, the sample must be stained simultaneously with all primary antibodies prior to embedding. Because the number of orthogonal antibody pairs is limited (e.g., goat, mouse, rabbit, etc.), alternative readout mechanisms are required. The most common strategy is to use oligo-conjugated antibodies, where the attached DNA sequence can be decoded in a cyclic format after expansion<sup>25</sup>. Often, antibody conjugation must be performed independently, increasing experimental complexity. While this enables multiplexing, direct immunofluorescence provides only limited signal amplification, which is particularly important in ExM because fluorophore density is defined per unit volume; since the number of labeled molecules is fixed while the specimen volume increases by the cube of the linear expansion factor ( $E^3$ ), the effective fluorophore concentration decreases proportionally ( $\propto 1/E^3$ ). Some improvement can be achieved by increasing labeling stoichiometry per target (e.g., using pre-complexed primary antibodies with labeled secondary reagents such as  $F(ab')_2$  fragments or nanobodies) or by adopting branched-DNA hybridization schemes to boost readout signal. And, if the oligo is further modified to include a primary amine, it can be covalently incorporated into the hydrogel during polymerization<sup>24</sup>, ensuring retention of the readout sequence throughout expansion. To prevent the hydrogel from shrinking during secondary oligo hybridization, which requires salt-containing buffers, samples are in some implementations embedded in a secondary, non-expandable hydrogel; however, this introduces diffusion barriers for sequential labeling and alters the refractive index, exacerbating spherical aberrations.

In contrast, post-expansion labeling offers several advantages for multiplexed imaging. Because staining is performed after gelation, trapped or nonspecifically bound fluorophores can be washed away, reducing background. The porous nature of the expanded gel also facilitates deep and uniform antibody penetration<sup>26</sup>, even for large complexes such as IgG (~150 kDa, ~14.5 nm), a feature particularly beneficial for labeling tissues and organs where diffusion barriers are significant and labeling time is greatly reduced. Importantly, indirect pre-expansion immunofluorescence (primary + secondary antibodies) introduces a linkage error of ~15–20 nm in the unexpanded state, which scales proportionally with the expansion factor; post-expansion labeling minimizes this error and is further compatible with smaller affinity reagents such as Fab fragments or nanobodies, making it especially valuable when performing iterative ExM. A key consideration for post-expansion labeling is the preservation of

825 antigenicity, as the gelation and denaturation steps can disrupt epitopes and reduce labeling efficiency.  
826 The primary methods for integrating proteins into the hydrogel are through covalent anchoring with AcX  
827 or polymer entanglement. However, covalent anchoring can mask epitopes and reduce labeling efficiency,  
828 whereas polymer entanglement, used here, retains proteins while better preserving epitope accessibility.

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### 830 **Supplementary Note 2 – Considerations for Fixation and Mechanical Relaxation in ExM.**

831 Expansion microscopy workflows, whether relying on pre- or post-expansion labeling, share critical  
832 dependencies on how specimens are fixed and mechanically relaxed, as these steps directly govern protein  
833 retention, antigen accessibility, and ultimately the quality of downstream labeling. Fixation with different  
834 ratios of paraformaldehyde (PFA) and acrylamide (AA) represents a trade-off between epitope  
835 preservation, protein retention, and fluorescence stability: higher PFA increases crosslinking and protein  
836 retention but often masks epitopes, whereas lower PFA or delayed AA introduction improves antigen  
837 accessibility, as demonstrated in eMAP<sup>13</sup> and U-ExM<sup>27</sup>. Similarly, the step used to relax tissue mechanics,  
838 whether proteolysis with proteinase K or heat/SDS denaturation, has major consequences for labeling.  
839 Proteolysis efficiently softens tissues but removes many proteins, limiting downstream detection, while  
840 heat-based denaturation preserves more protein content, albeit with a risk of partial epitope disruption.  
841 Thus, regardless of whether labeling occurs before or after expansion, careful balancing of fixation  
842 chemistry and relaxation method is critical for maximizing both retention and accessibility of antigens. To  
843 preserve the maximum number of proteins, we applied an U-ExM<sup>14,27</sup>-inspired workflow, which relies on  
844 mild heat denaturation of the specimen and allows for detection of antigens in the post-expansion state.

845

### 846 **Supplementary Note 3 – Quantitative Evaluation of Registration Accuracy.**

847 To assess the fidelity of image alignment across iterative labeling cycles, we employ a suite of  
848 complementary registration metrics that capture both geometric and intensity-based correspondence  
849 between volumes. These methods are briefly summarized below.

850

851 Target Registration Error (TRE). TRE is a landmark-based metric that directly measures geometric  
852 misalignment. It is defined as the 3D Euclidean distance between corresponding image features after  
853 applying the registration transform. Specifically, given N landmark pairs, each with coordinates  $(x_i, y_i, z_i)$   
854 in the reference image and corresponding coordinates  $(x'_i, y'_i, z'_i)$  in the moving (transformed) image, the  
855 TRE for each pair is calculated as:

856

$$\text{TRE}_i = \sqrt{(x_i - x'_i)^2 + (y_i - y'_i)^2 + (z_i - z'_i)^2}$$

857

858 TRE reflects how well independent structures align following registration and is typically summarized  
859 using mean, median, and range. This provides a direct and interpretable measure of how precisely  
860 structures are aligned across rounds. In this work, because landmark correspondence is inferred from  
861 puncta matching rather than a known a priori, the reported values represent a TRE-like proxy rather than a  
862 ground-truth TRE.

863

864 Normalized Cross-Correlation (NCC). NCC quantifies the linear correlation between voxel intensities in  
865 the two volumes and is calculated as the Pearson correlation coefficient across all voxel pairs. For two  
866 images  $I_1$  and  $I_2$  with N voxels each:

$$\text{NCC} = \frac{1}{N} \sum_v \frac{(I_1(v) - \bar{I}_1)(I_2(v) - \bar{I}_2)}{\sigma_{I_1} \sigma_{I_2}}$$

867 NCC ranges from  $-1$  to  $1$ , where  $1$  indicates perfect alignment of structural intensities and  $0$  indicates no  
868 correlation. In high-resolution fluorescence microscopy of the same target structure, well-registered  
869 volumes typically achieve NCC values above  $0.9$ . Because it assumes a linear relationship between  
870 intensity values, NCC underperforms when fluctuations in the expansion coefficient or staining efficiency  
871 result in intensity differences between the two images (see **Figure S6**).

872

873 Mutual Information (MI). MI is an information-theoretic measure of how much knowing the intensity in  
874 one image reduces uncertainty about the other. Unlike NCC, MI does not assume a linear relationship and  
875 is well-suited for variably scaled data, such as those arising from differences in the expansion coefficient  
876 between imaging rounds. Like NCC, MI remains sensitive to fluctuations in staining efficiency<sup>28</sup>. It is  
877 calculated from the joint intensity histogram of the two volumes:

$$\text{MI}(I_1, I_2) = \sum_{i,j} p(i, j) \log \left( \frac{p(i, j)}{p_1(i)p_2(j)} \right)$$

878 where  $p(i, j)$  is the joint probability of observing intensity  $i$  in image  $I_1$  and  $j$  in  $I_2$ , and  $p_1$  and  $p_2$  are the  
879 marginal distributions. MI increases when structural alignment leads to a more peaked joint histogram and  
880 decreases when images are misaligned. While absolute MI values are less interpretable, improvements in  
881 MI after registration indicate enhanced alignment.

882

883 Structural Similarity Index (SSIM). SSIM evaluates perceptual similarity between images by comparing  
884 local patterns of luminance, contrast, and structural texture. For local windows centered at each voxel:

885

$$\text{SSIM} = \frac{(2\mu_F \mu_G + C_1)(2\sigma_{FG} + C_2)}{(\mu_F^2 + \mu_G^2 + C_1)(\sigma_F^2 + \sigma_G^2 + C_2)}$$

886

887 where  $\mu$ ,  $\sigma$ , and  $\sigma_{FG}$  are local means, standard deviations, and cross-covariance terms, respectively, and  
888  $C_1$ ,  $C_2$  are stability constants. SSIM results range from  $-1$  to  $1$ : a value of  $1$  indicates perfect structural  
889 similarity, while  $-1$  represents perfect anti-correlation (e.g., an image and its negative). SSIM is  
890 particularly useful for assessing registration accuracy in high-resolution microscopy data, where  
891 preserving local spatial relationships is critical. Using the default implementation in Scikit-image, we  
892 compute SSIM over 3D neighborhoods to capture structural alignment in volumetric datasets.

893

## 894 **Supplementary Note 4 - Limitations and Future Directions**

### 895 Limitations

896 Despite its advantages, Cy-ExM has several limitations that warrant consideration. First, antibody  
897 compatibility remains a bottleneck, and certain epitopes may be sensitive to cryo-fixation or expansion-  
898 associated processing. Because our workflow relies on indirect immunofluorescence, each cycle requires  
899 orthogonal primary–secondary antibody pairs, which constrains panel design and multiplexing depth per  
900 round. This limitation could be alleviated by adopting direct labeling strategies (e.g., directly conjugated  
901 primaries) or using pre-complexed Fab–antibody assemblies to expand the number of usable channels  
902 without increasing cross-reactivity. Second, although Cy-ExM preserves antigenicity for many targets,

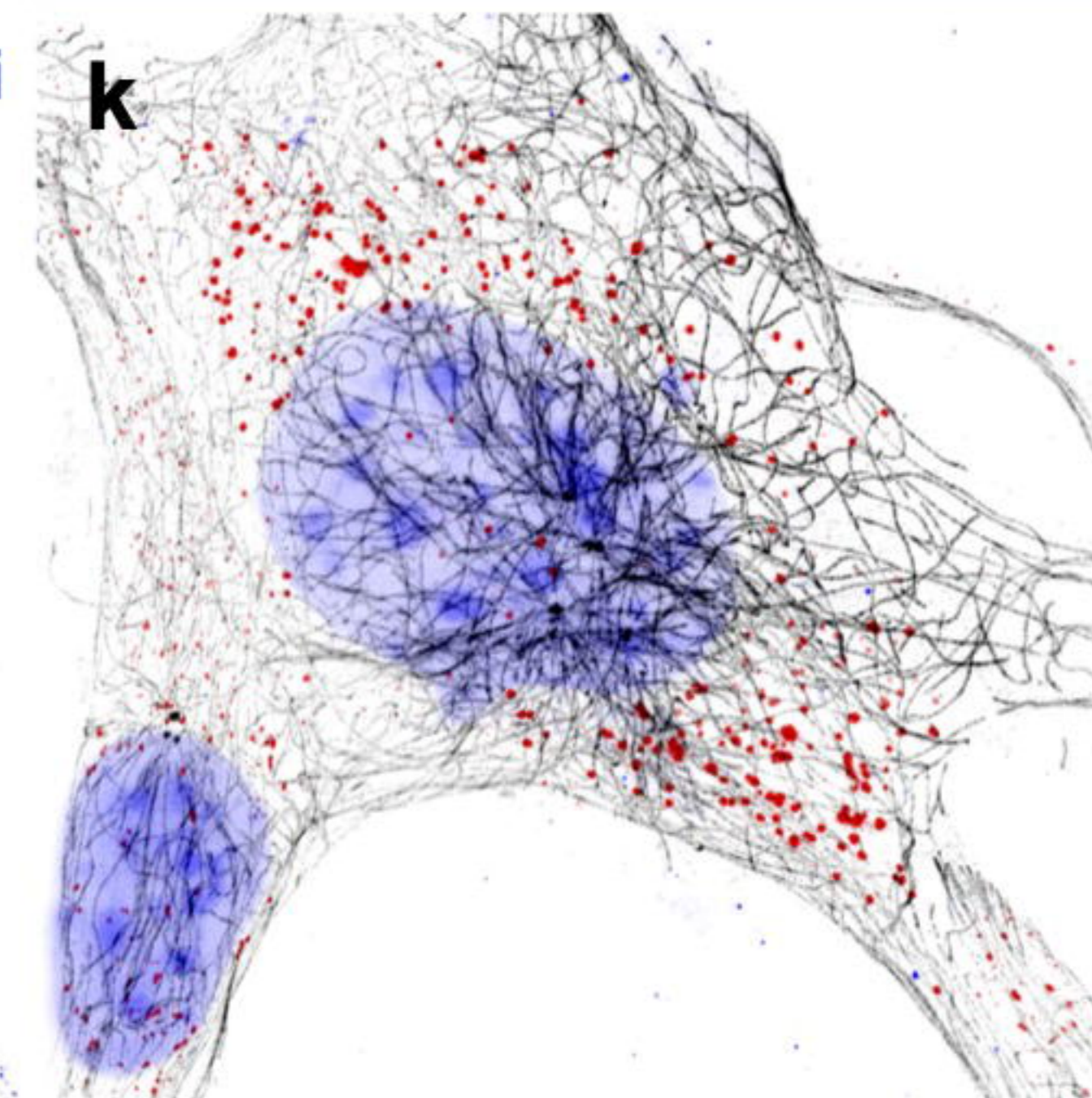
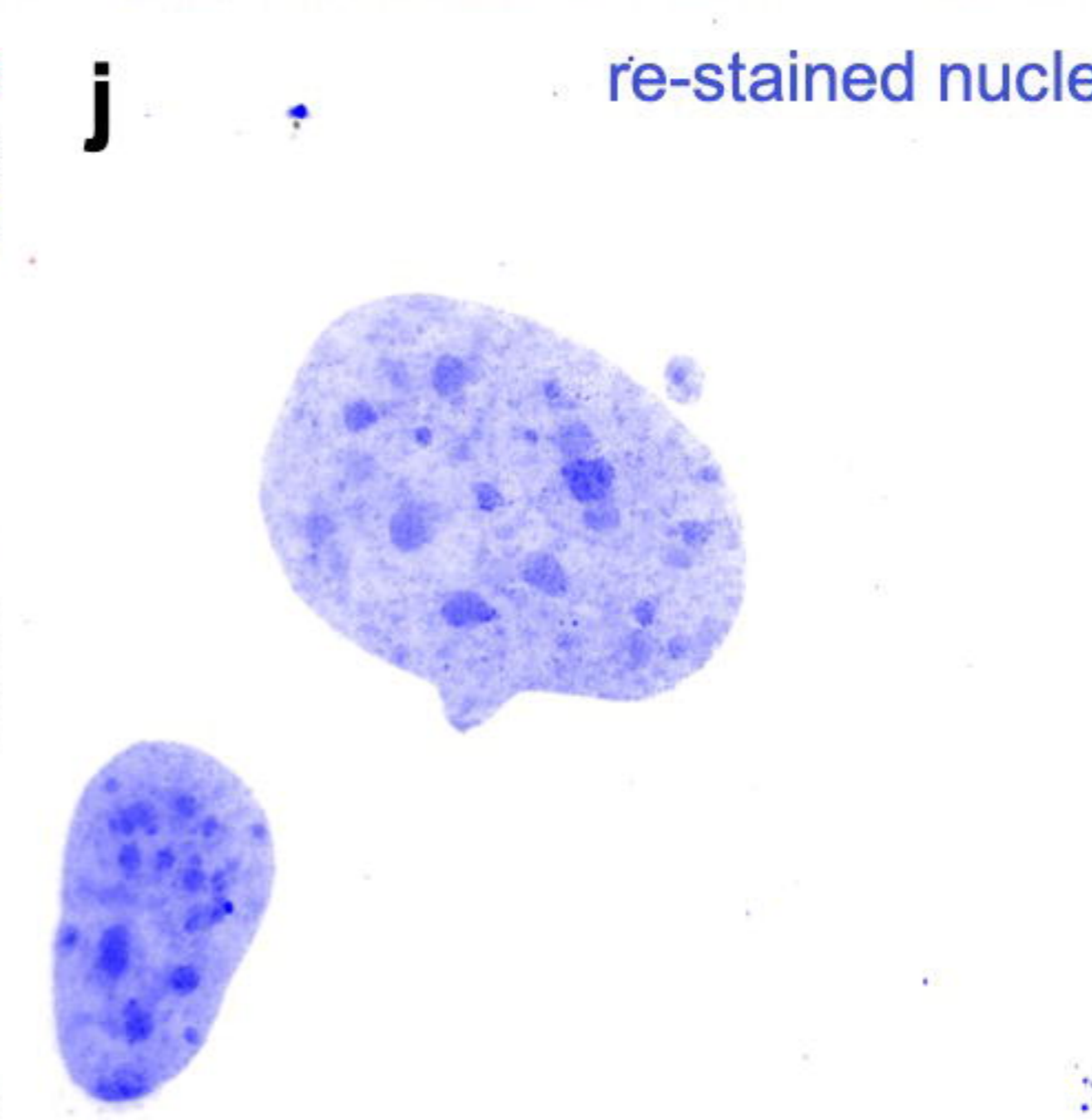
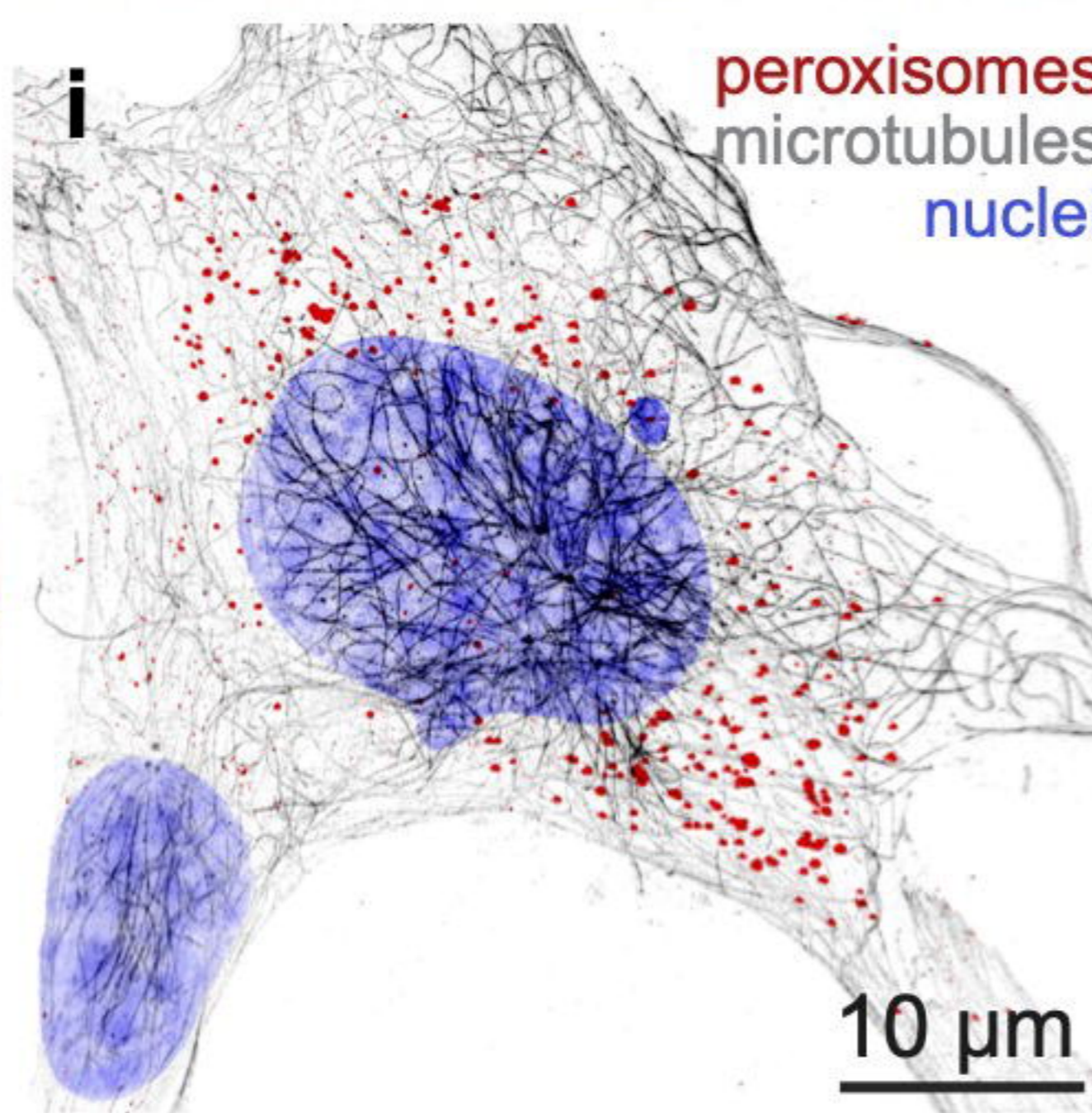
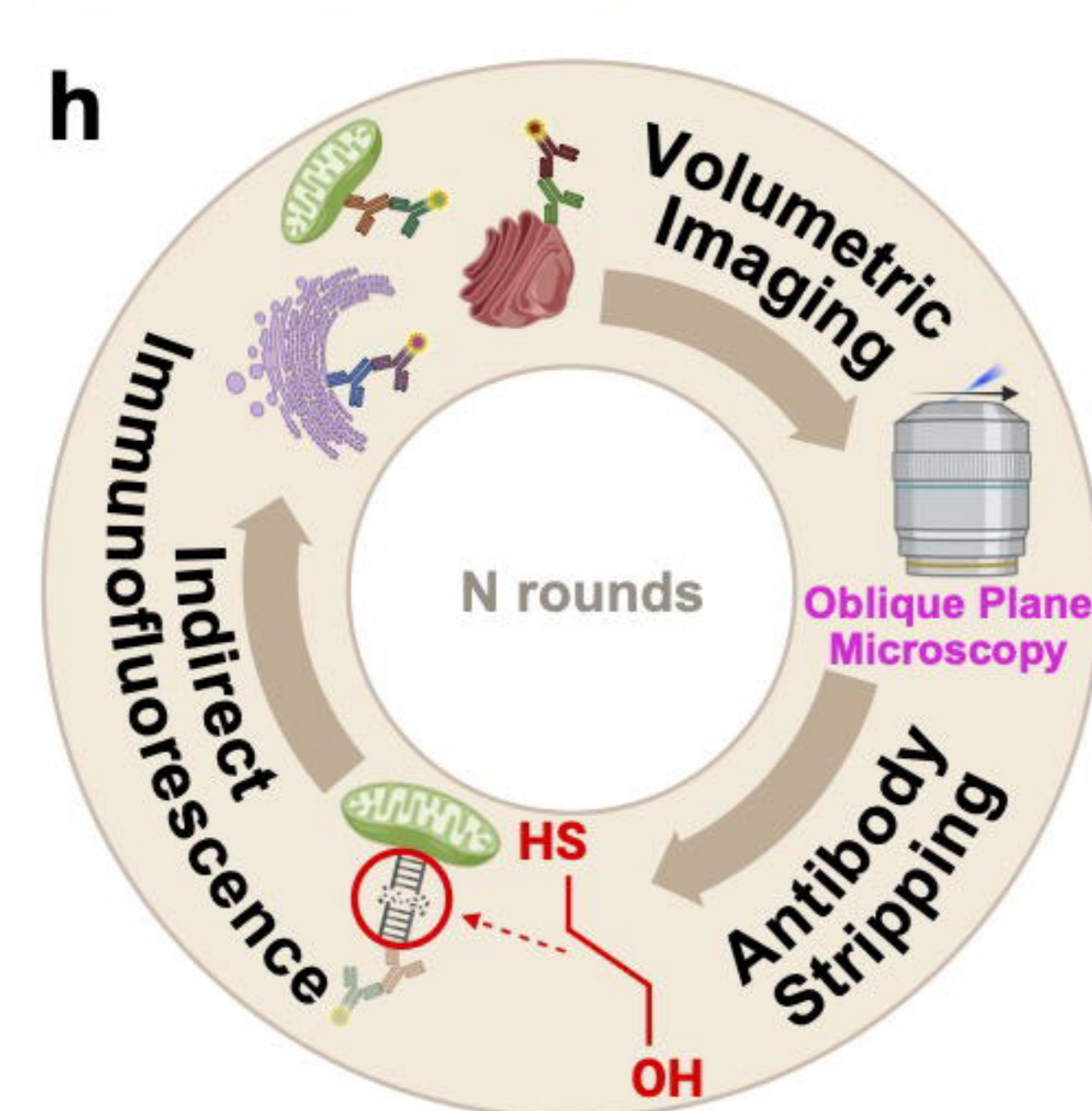
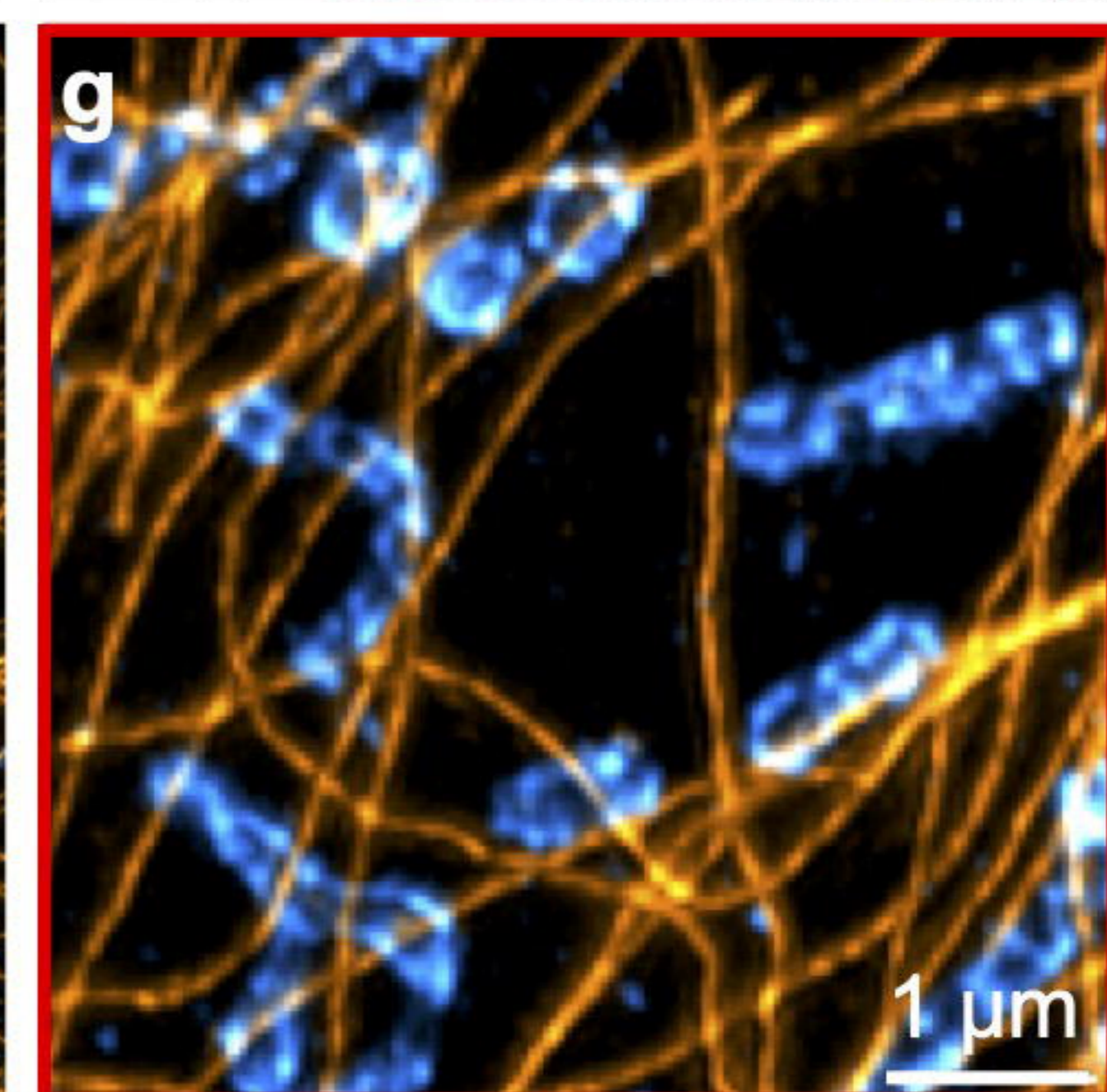
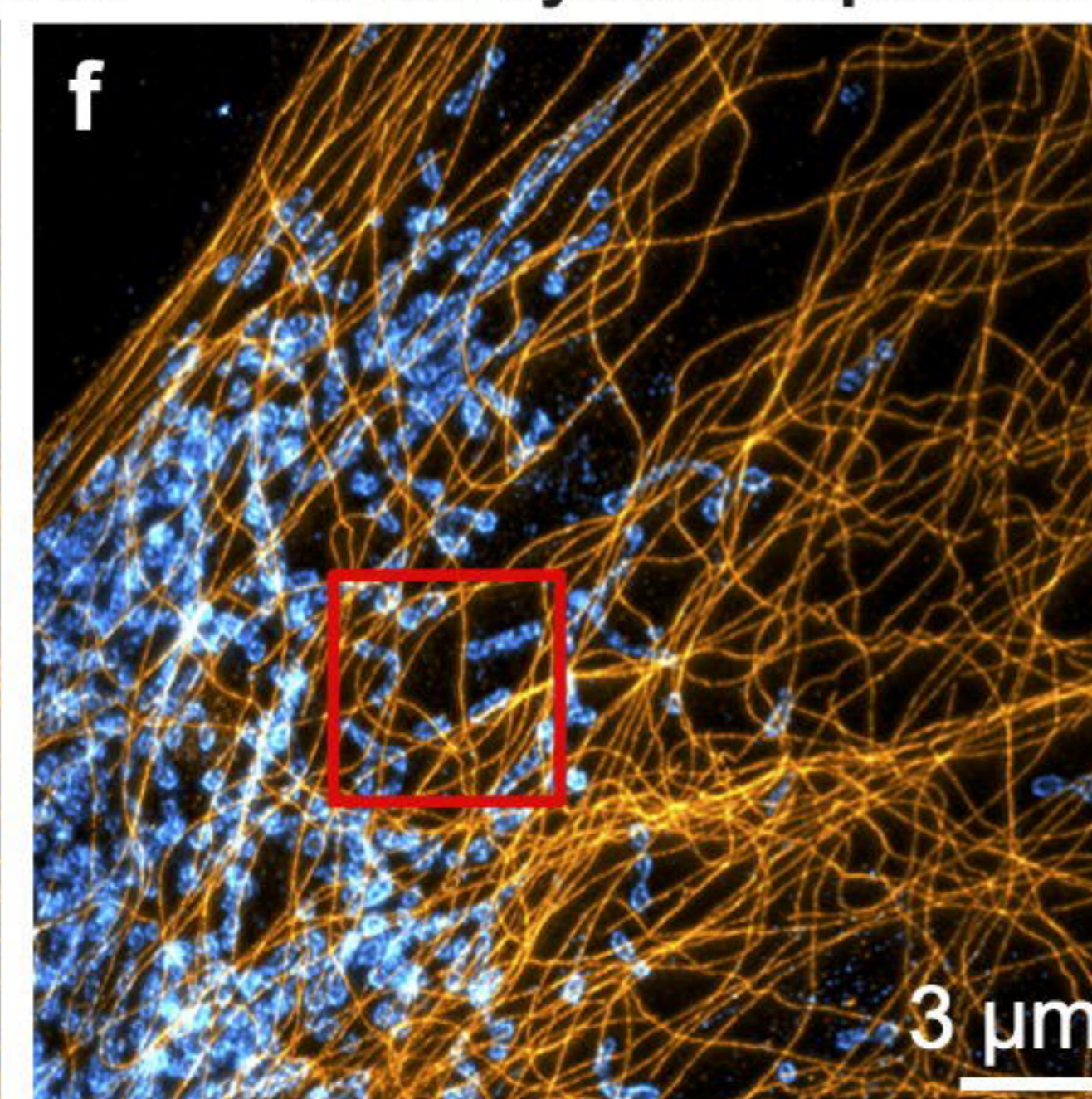
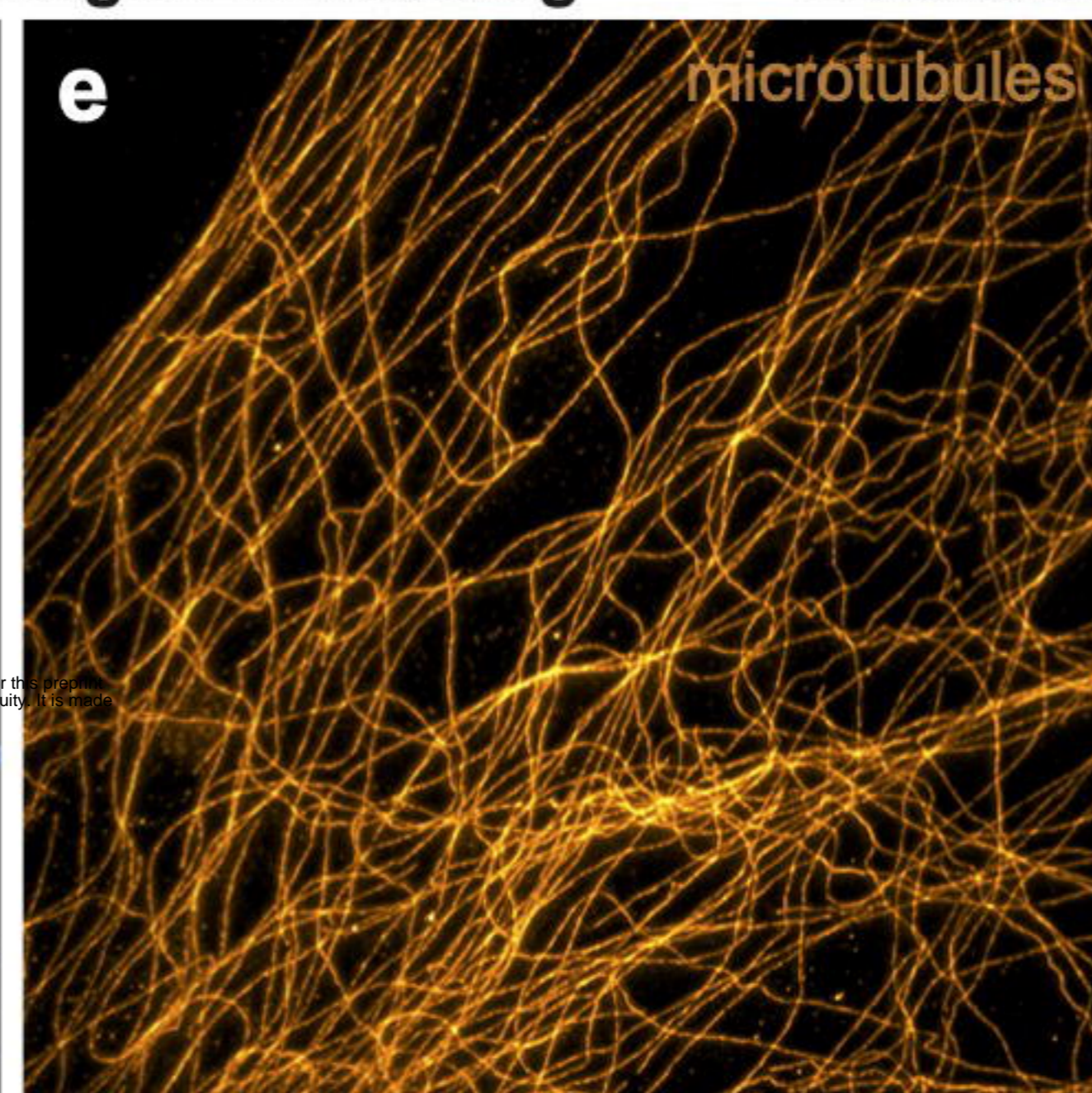
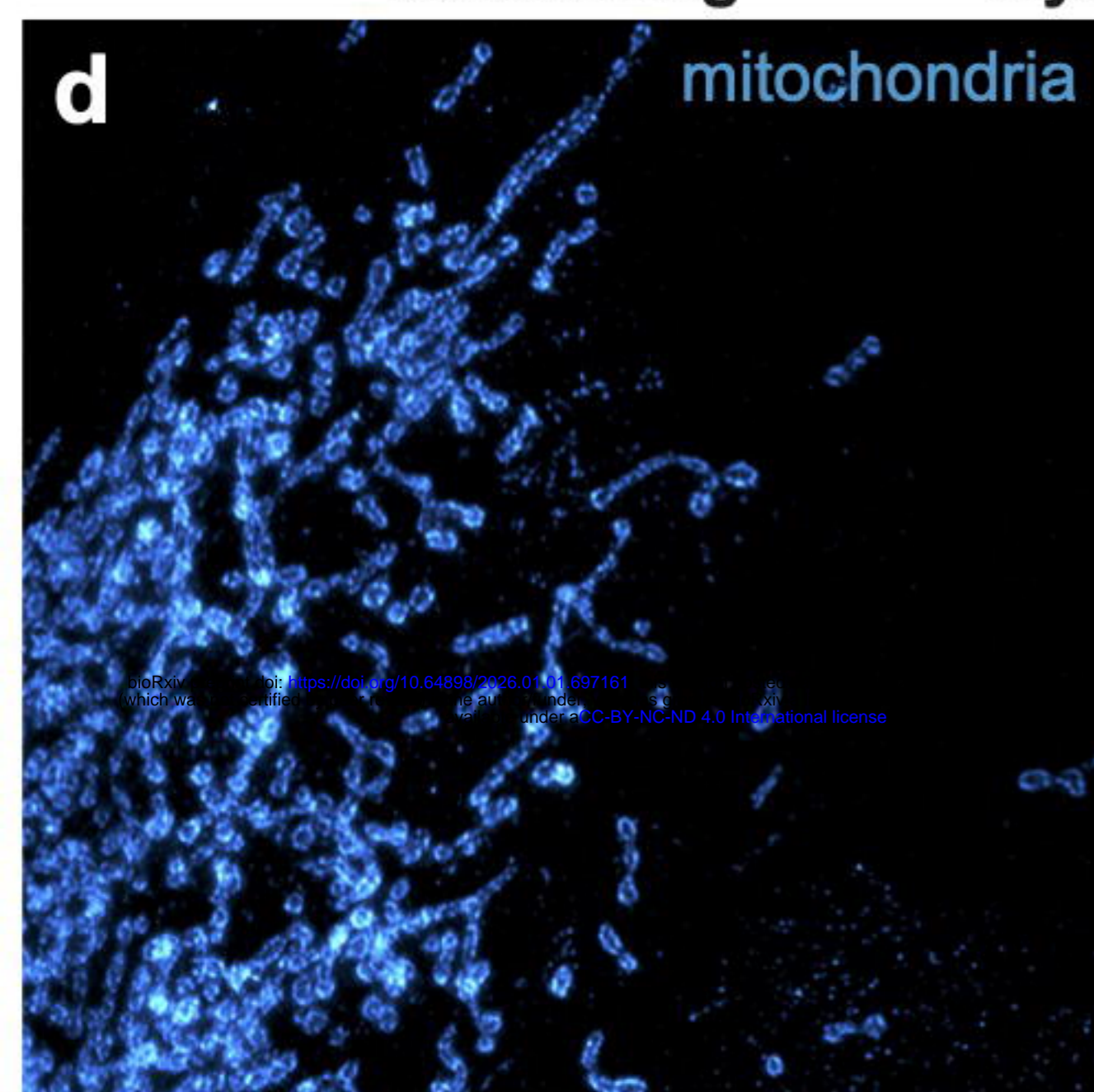
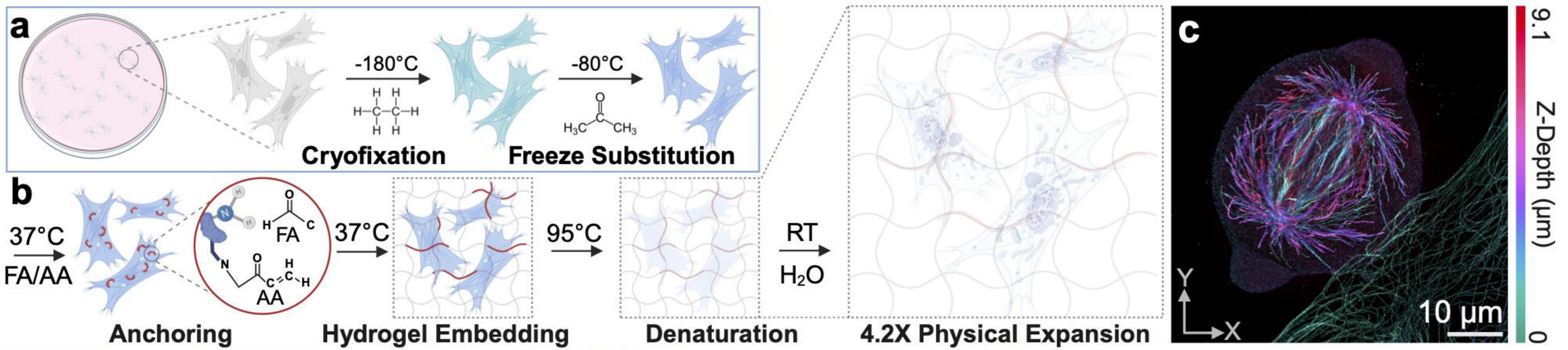
903 fluorescent proteins are variably preserved during cryo-fixation and denaturation; when intrinsic  
904 fluorescence is critical, additional optimization or post-expansion immunostaining is likely required.  
905 Third, while  $\beta$ -mercaptoethanol provides a relatively gentle mechanism for antibody removal, repeated  
906 reduction cycles may still affect the stability of particularly sensitive epitopes or labeling chemistries, and  
907 the practical ceiling on cycle number may depend on target class and specimen type. Finally, nanoscale  
908 3D imaging across multiple cycles generates large volumetric datasets, necessitating substantial storage  
909 and computational resources as well as automated workflows for registration, segmentation, and  
910 downstream analysis. Addressing these limitations through expanded labeling chemistries, continued  
911 optimization of fixation/denaturation/stripping conditions, and more efficient computational pipelines will  
912 further broaden the applicability and scalability of Cy-ExM.

913

#### 914 Future directions

915 Looking ahead, Cy-ExM establishes a foundation for several promising extensions. Combining  
916 our cyclic workflow with iterative expansion microscopy could push effective resolution into the ~20 nm  
917 regime, enabling more detailed mapping of protein nanodomains, cytoskeletal architectures, and organelle  
918 interfaces. Future implementations could also substantially increase the molecular information captured  
919 per cycle by integrating automated fluidics, broadband illumination sources, tunable emission filters,  
920 ultra-narrowband fluorophores, and improved spectral unmixing algorithms. Together, these advances  
921 could move Cy-ExM toward substantially higher multiplexing depth (e.g., ~80-plex and potentially >100-  
922 plex, depending on channel allocation, fluorophore performance, and cycle count) while maintaining  
923 image fidelity. In addition, the approach should be adaptable to more complex biological specimens,  
924 including organoids and tissue sections, particularly when paired with cryo-preservation strategies that  
925 maintain subcellular detail at depth. Ultimately, the ability to visualize molecular organization across  
926 dozens of targets within intact 3D specimens holds promise for systematically characterizing how  
927 subcellular protein architecture varies across cell types and states, and how compartment-level  
928 organization relates to biological function across cellular, organelle, and tissue scales.

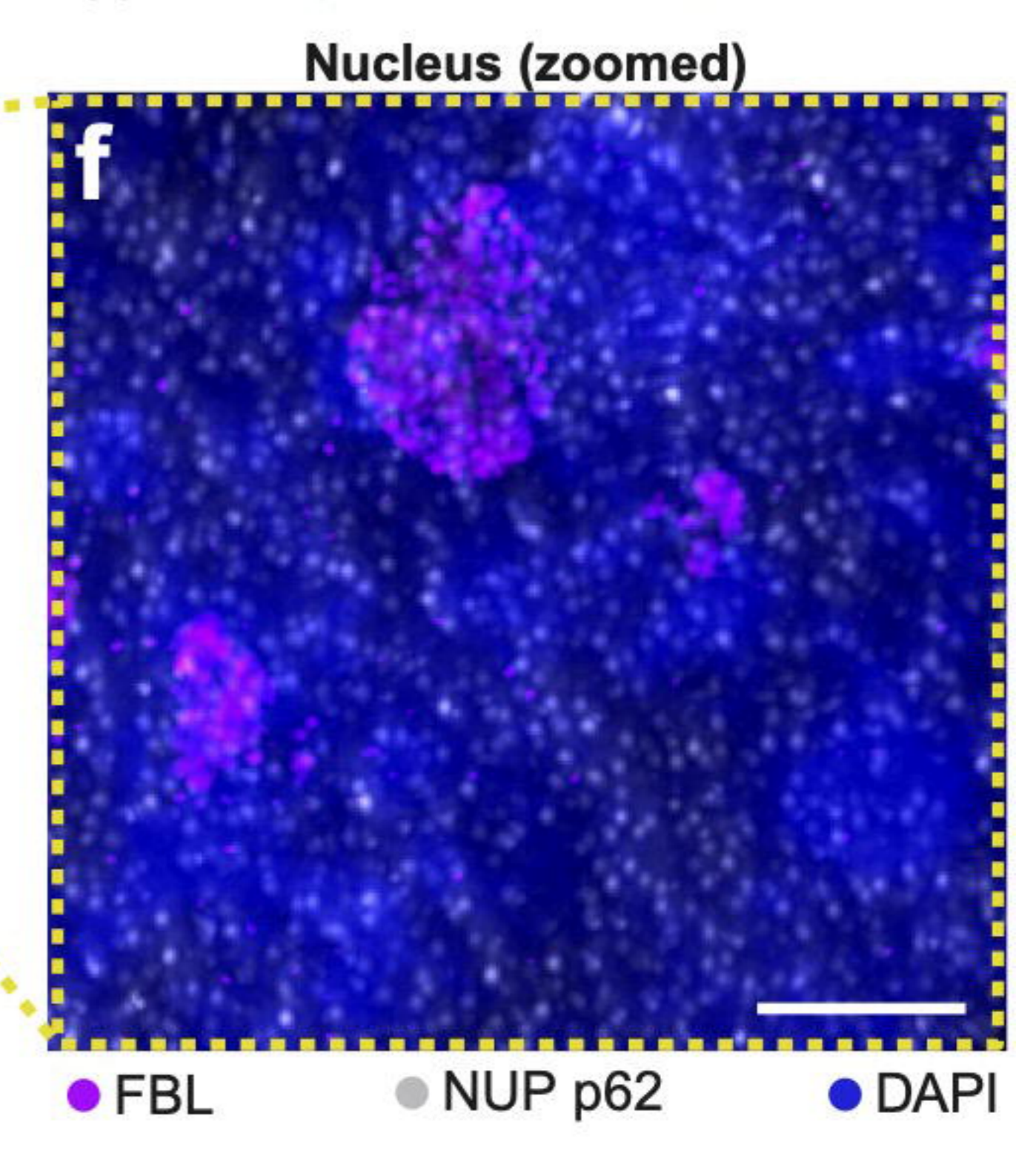
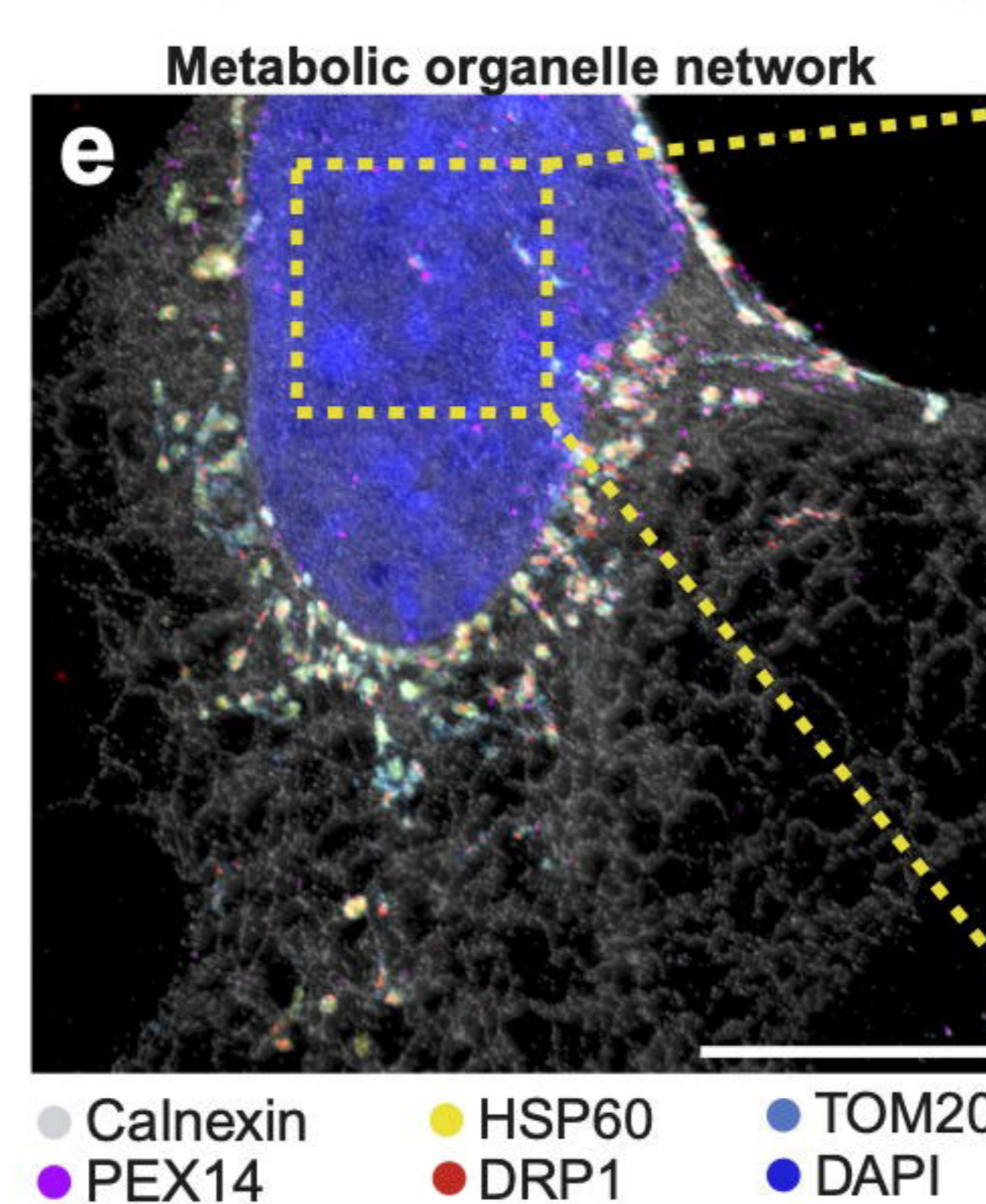
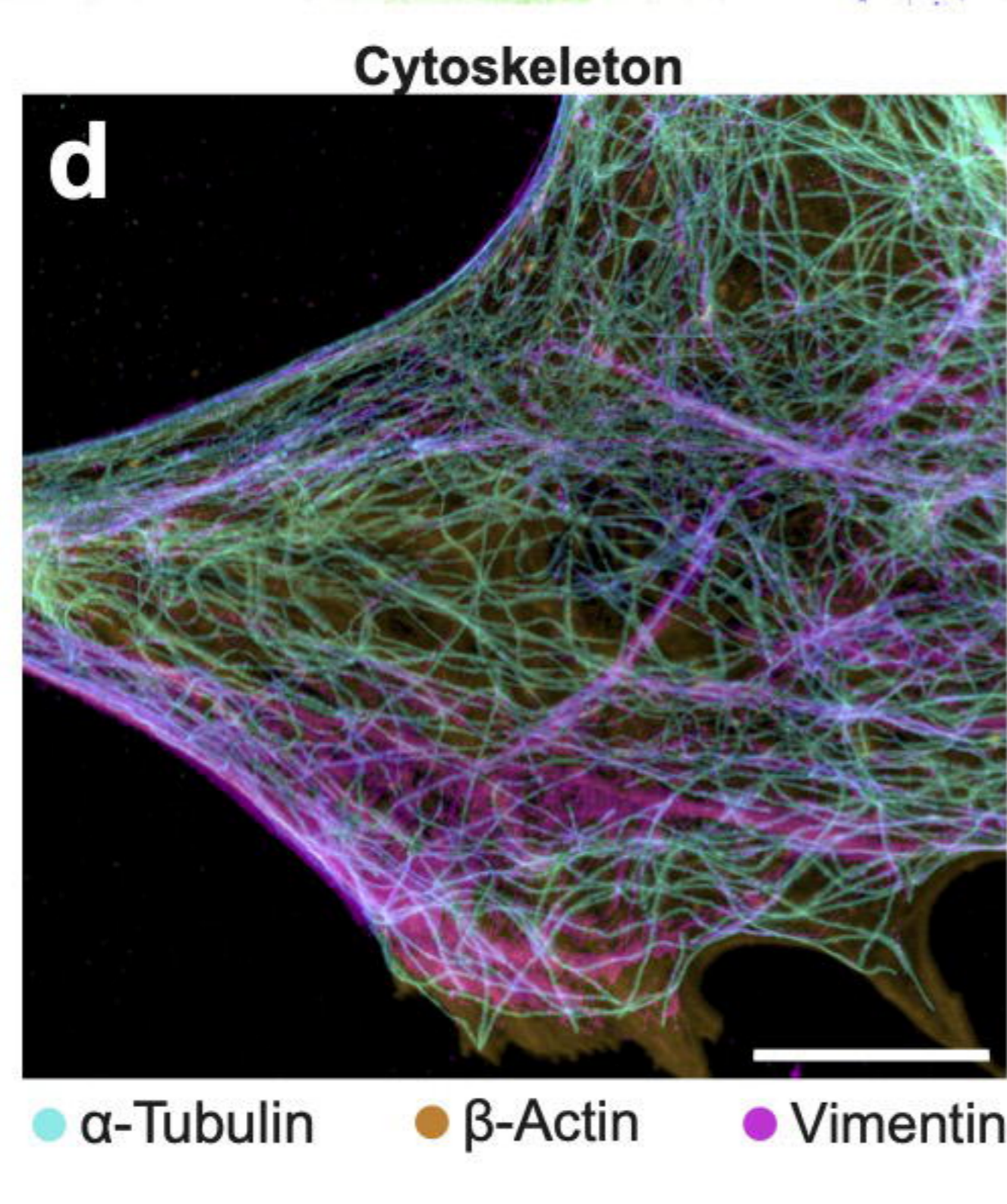
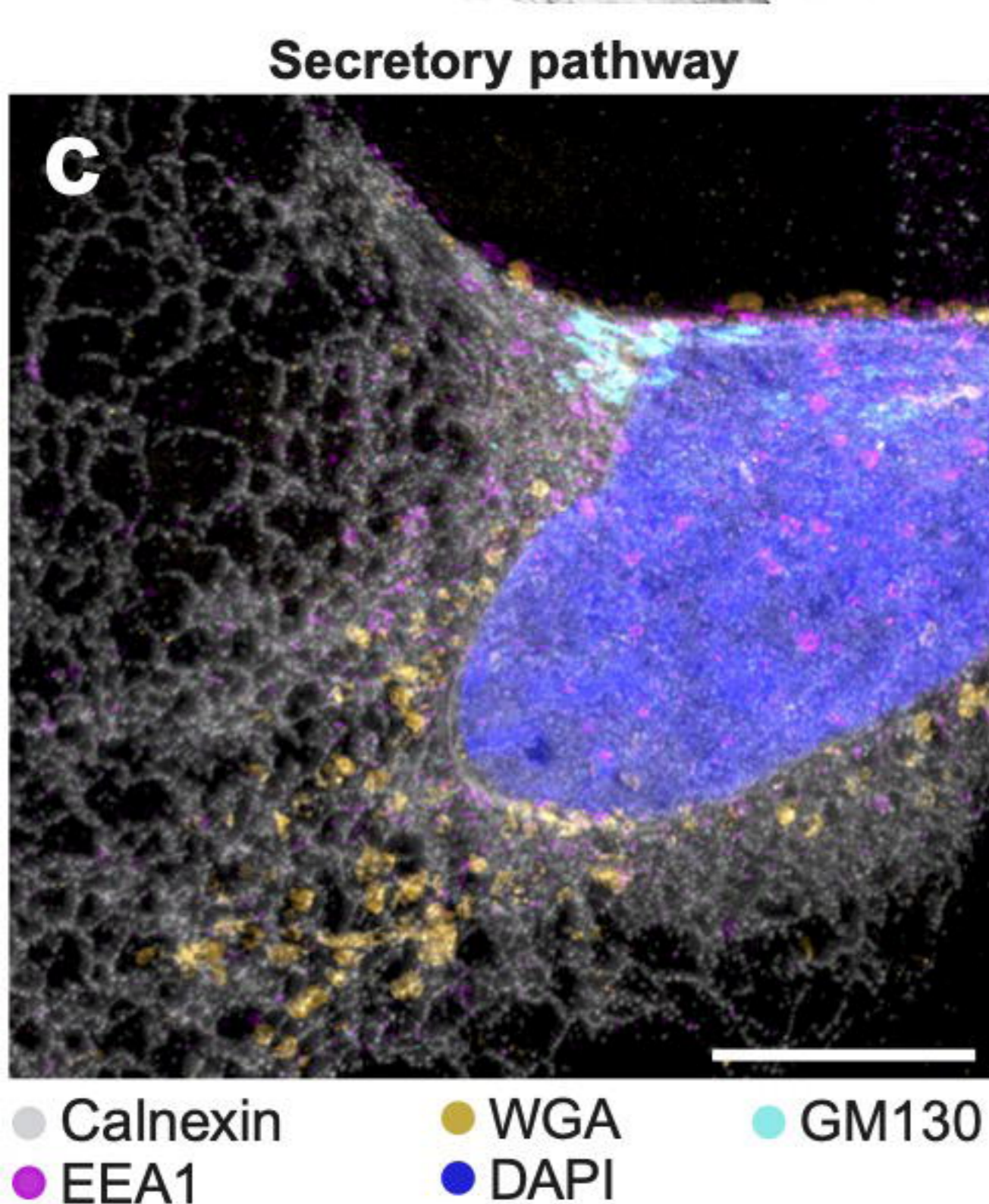
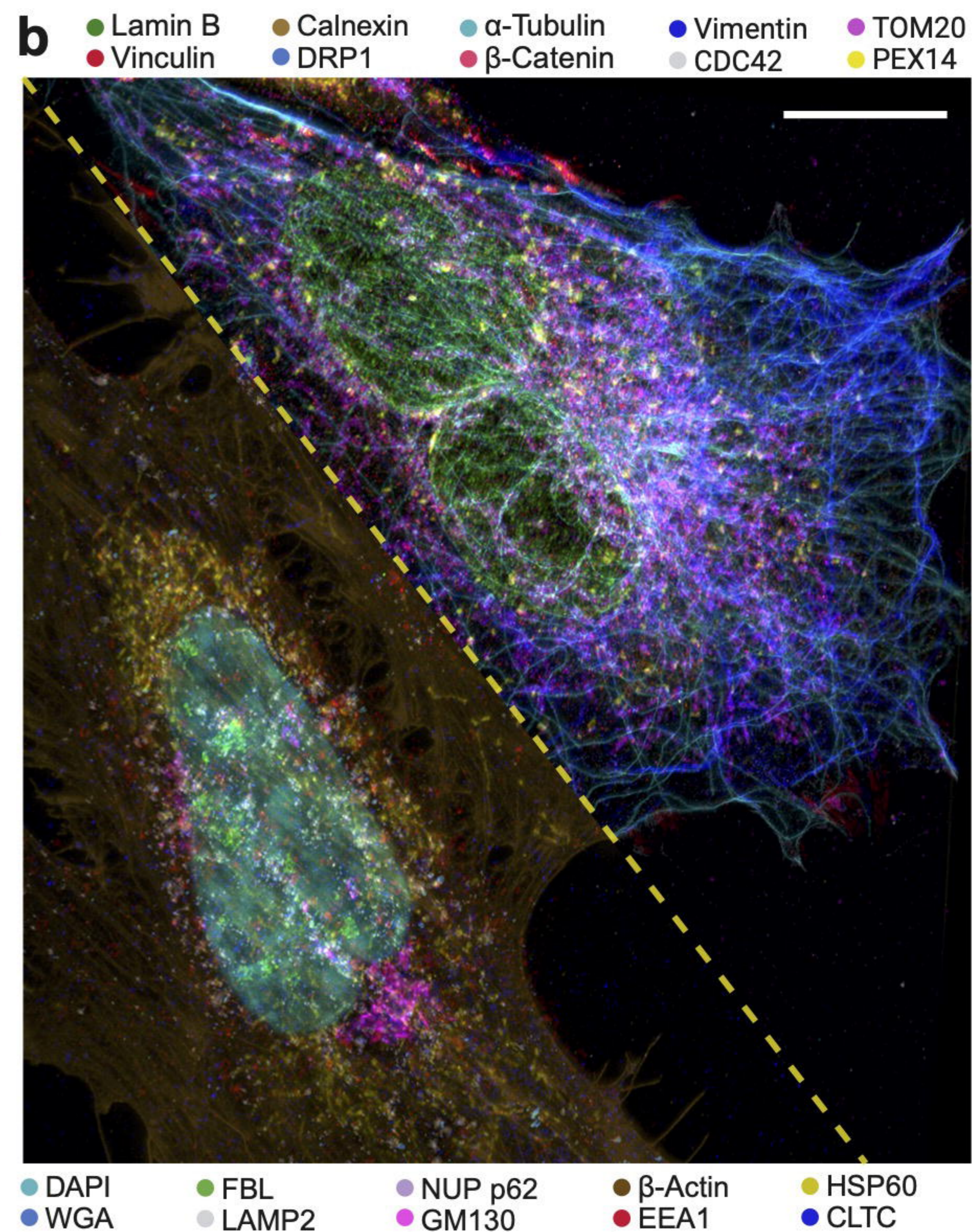
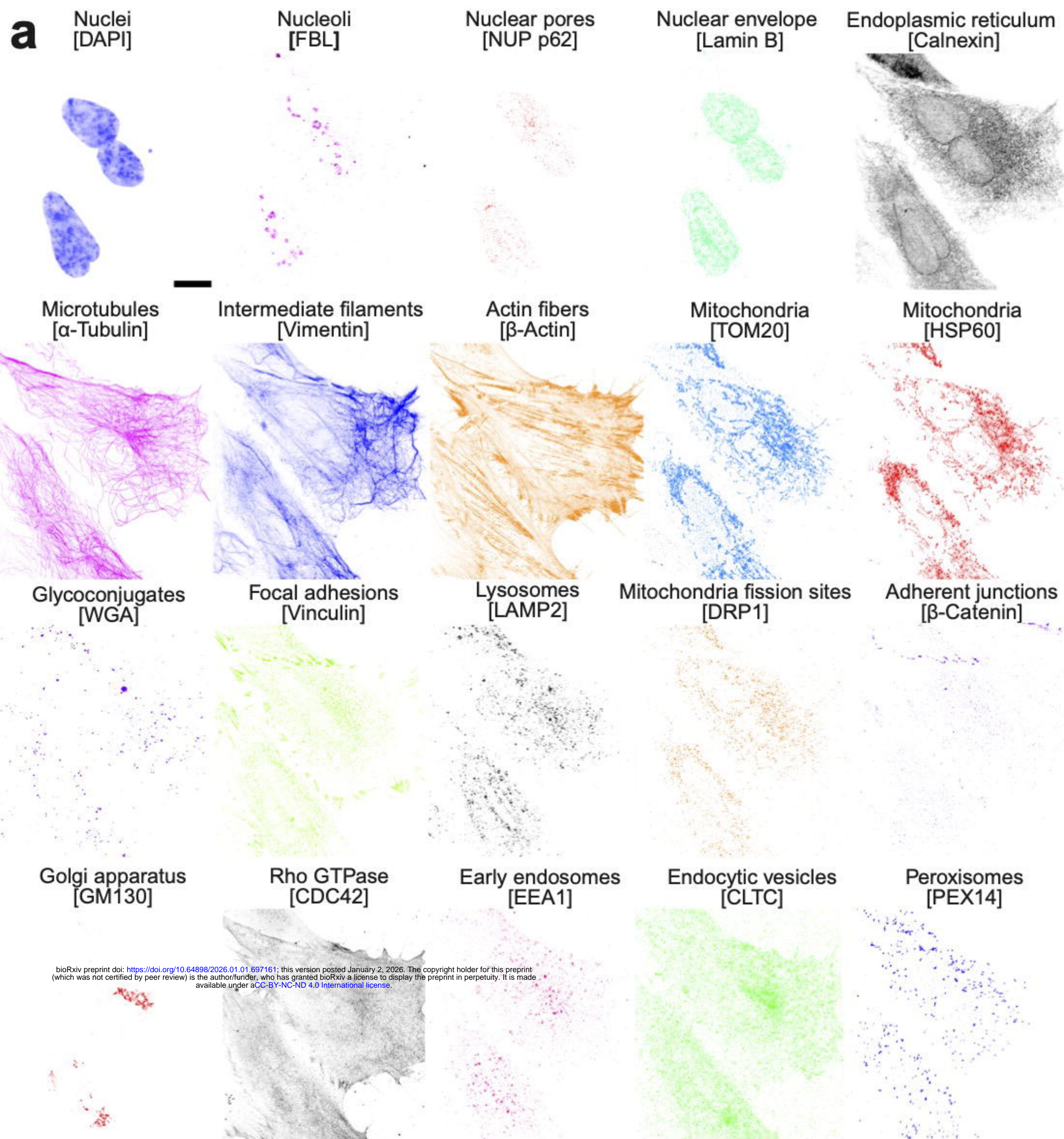
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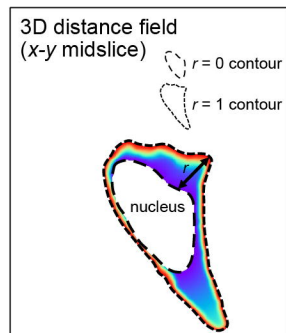
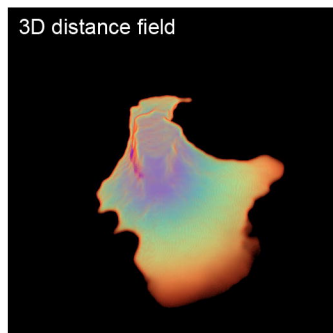
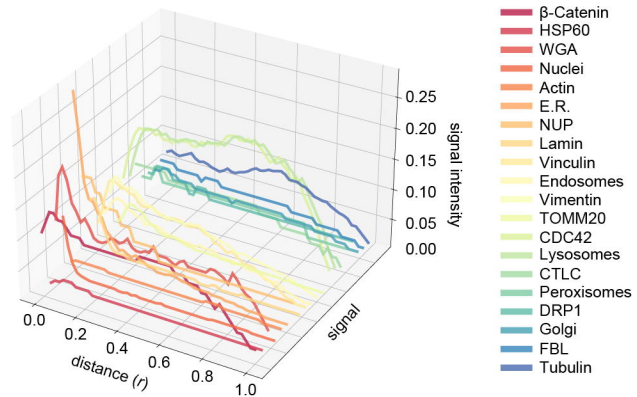
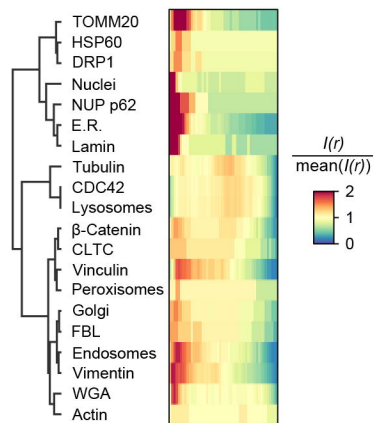


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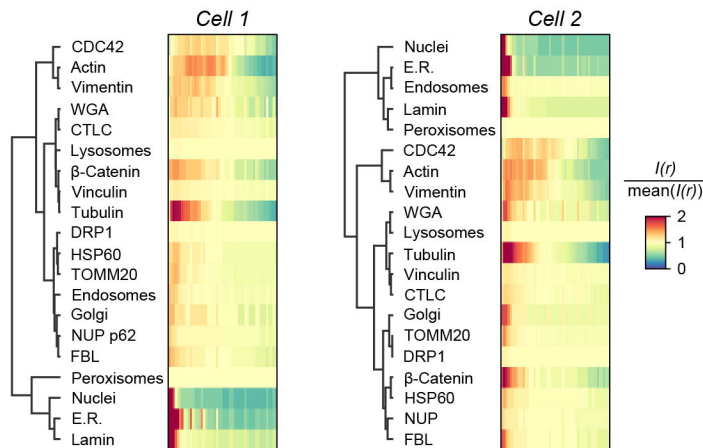
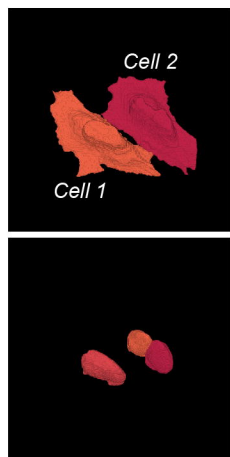
After Antibody Removal

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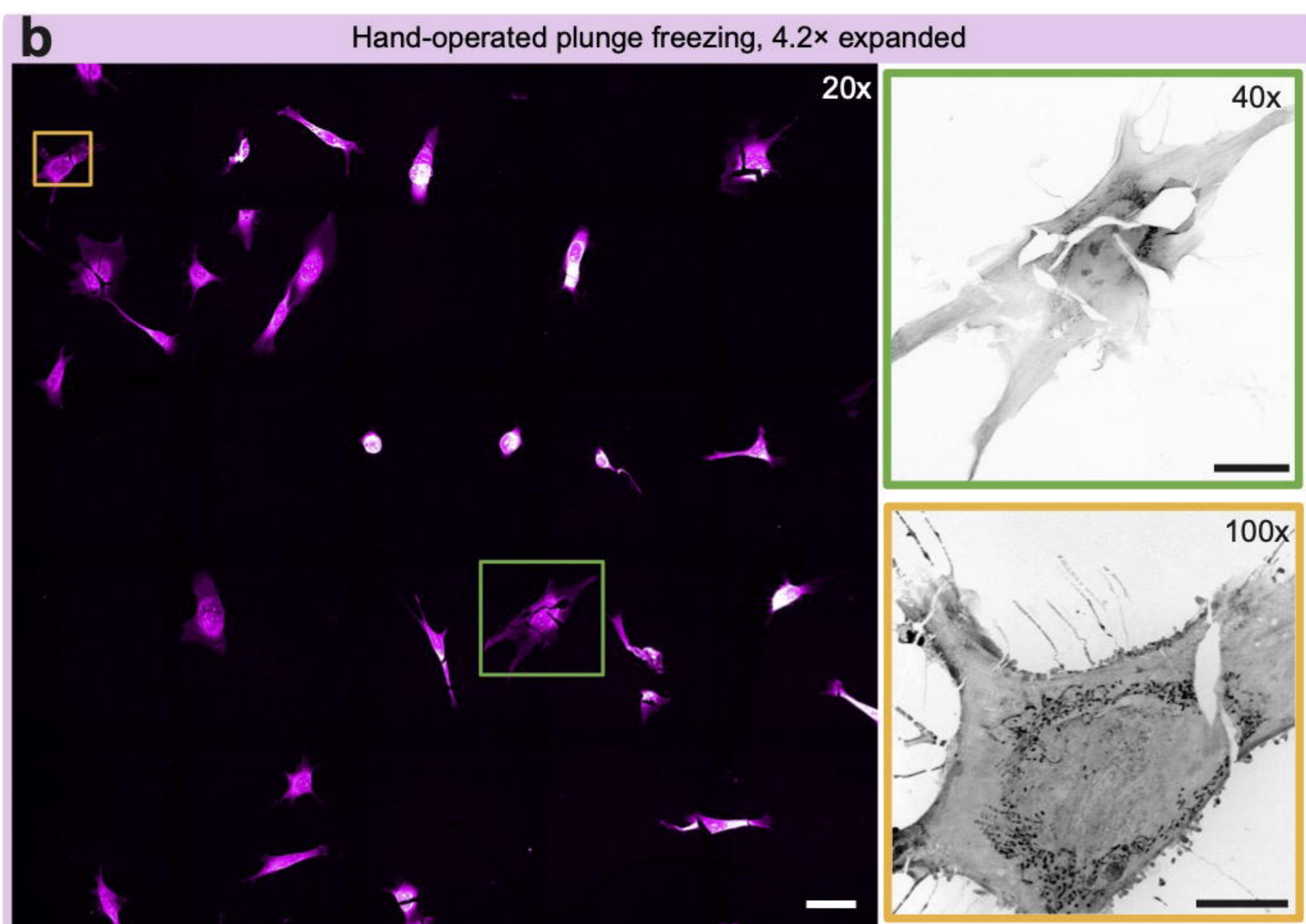
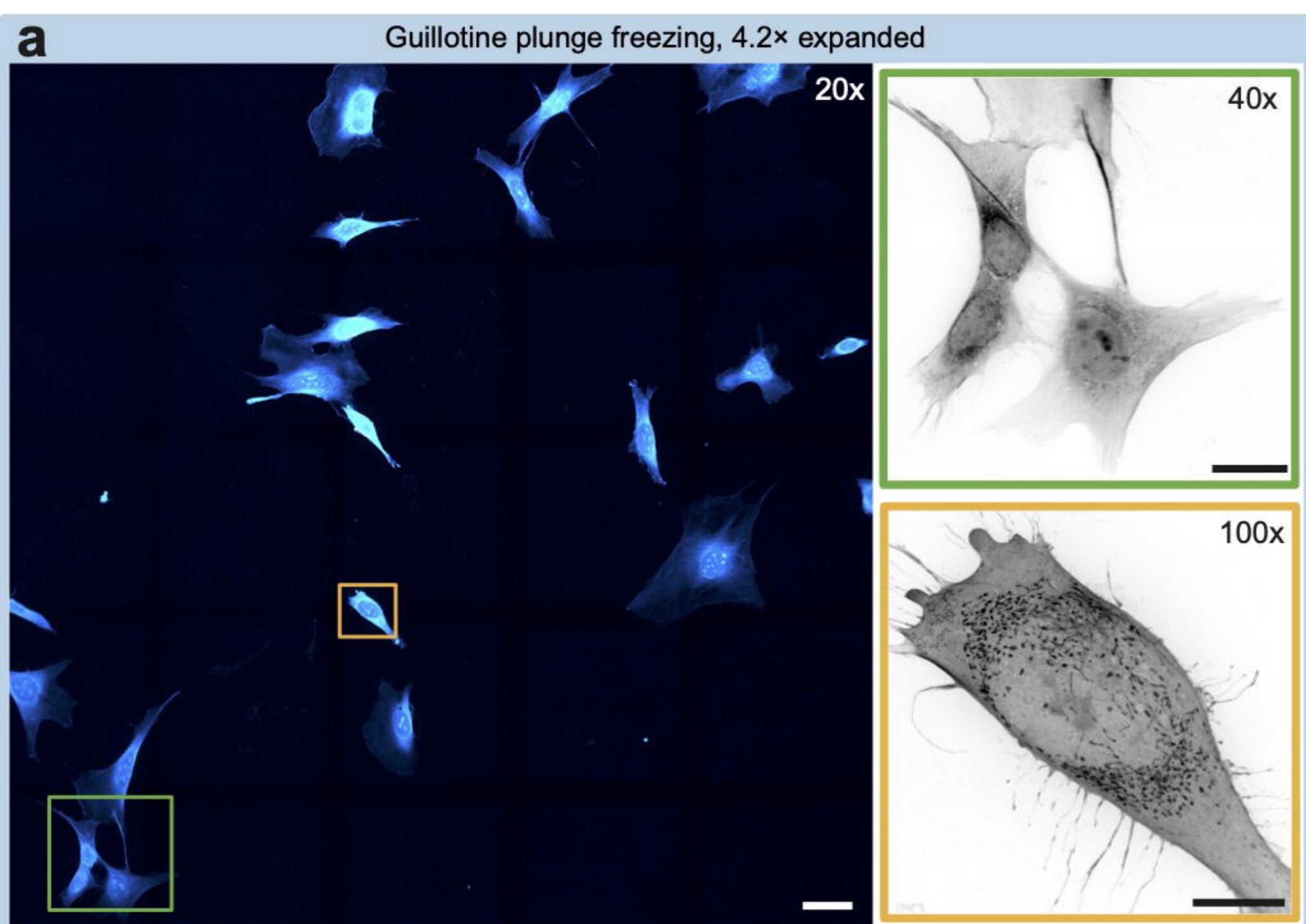


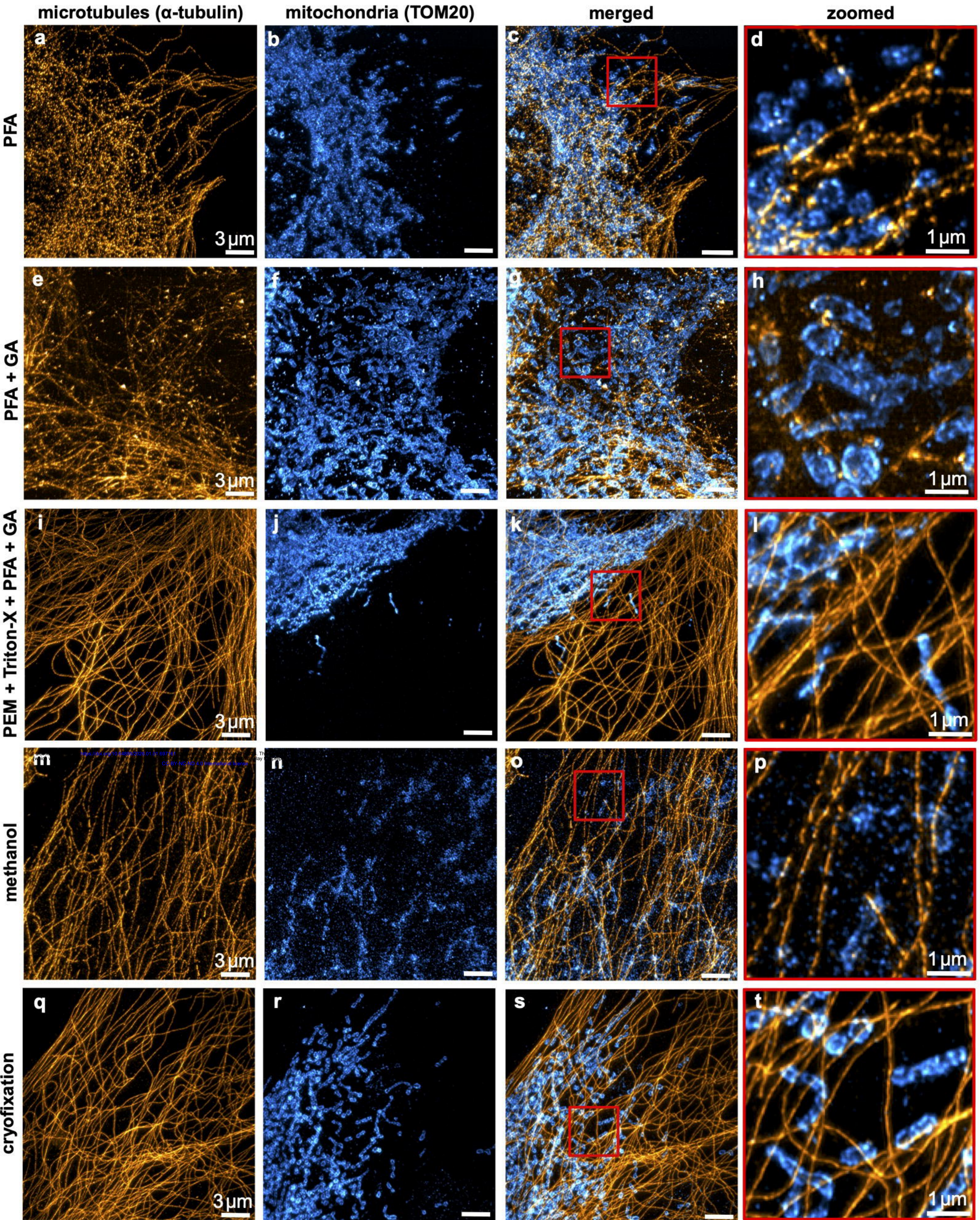
**a****b**signal distributions,  $I(r)$ **c**

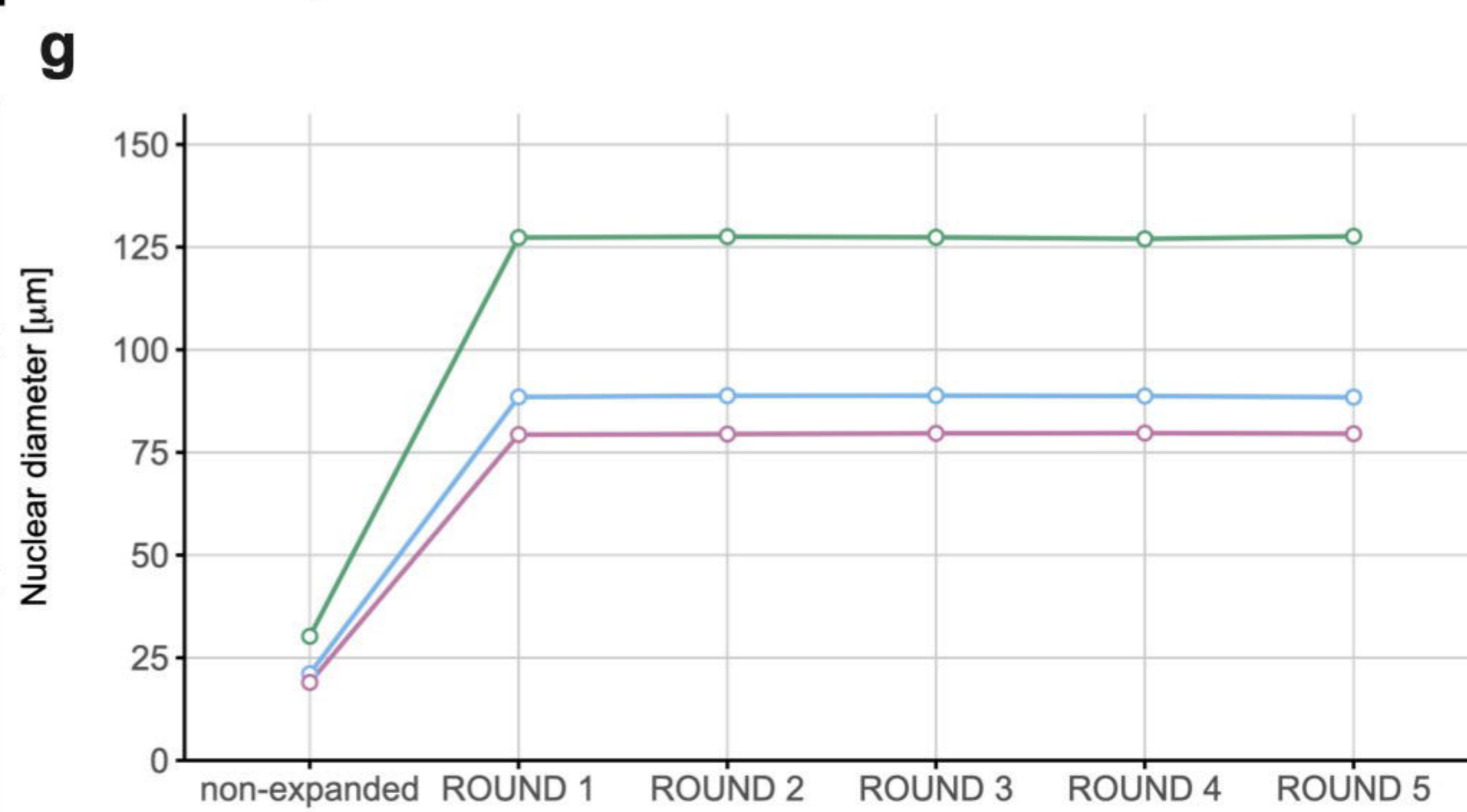
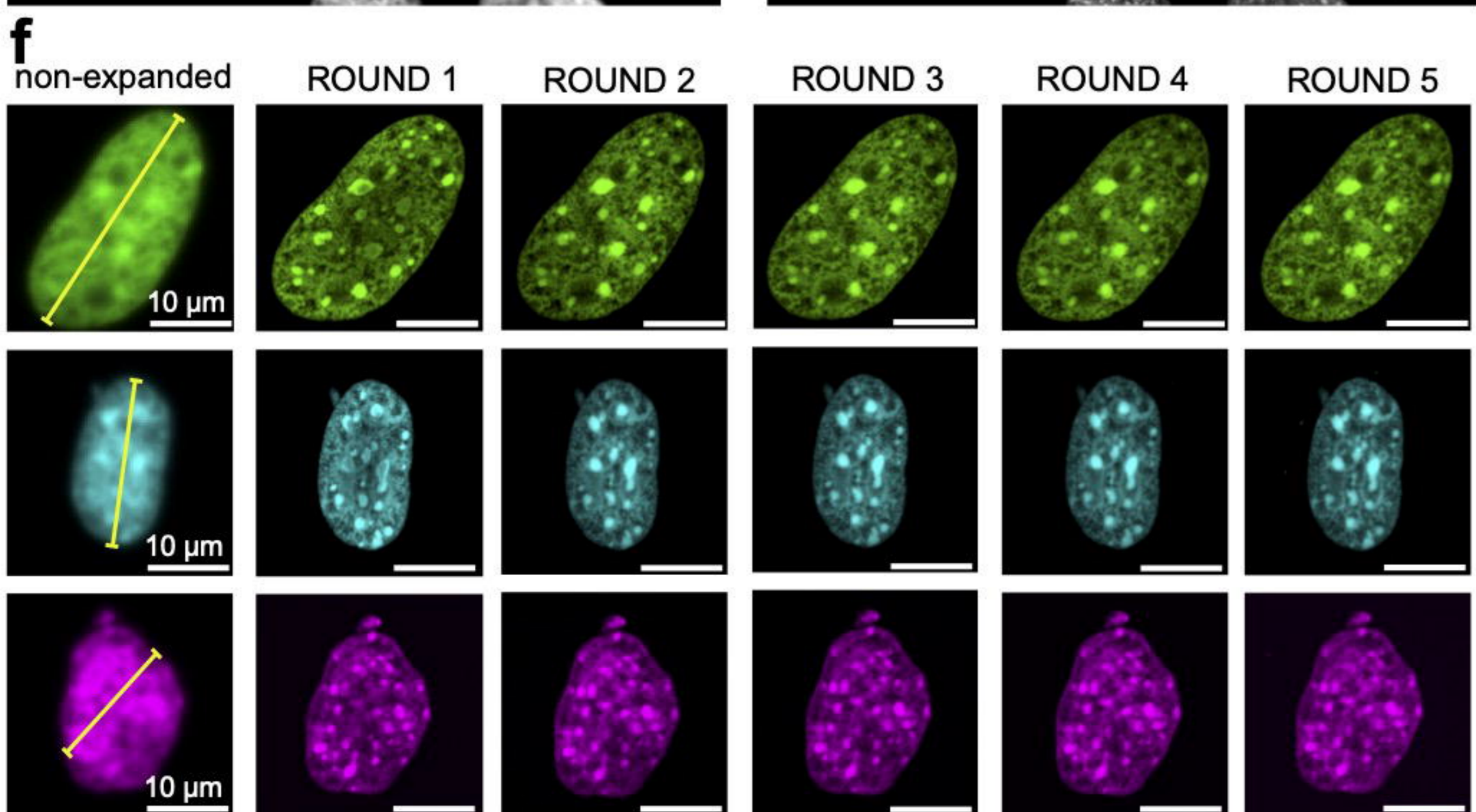
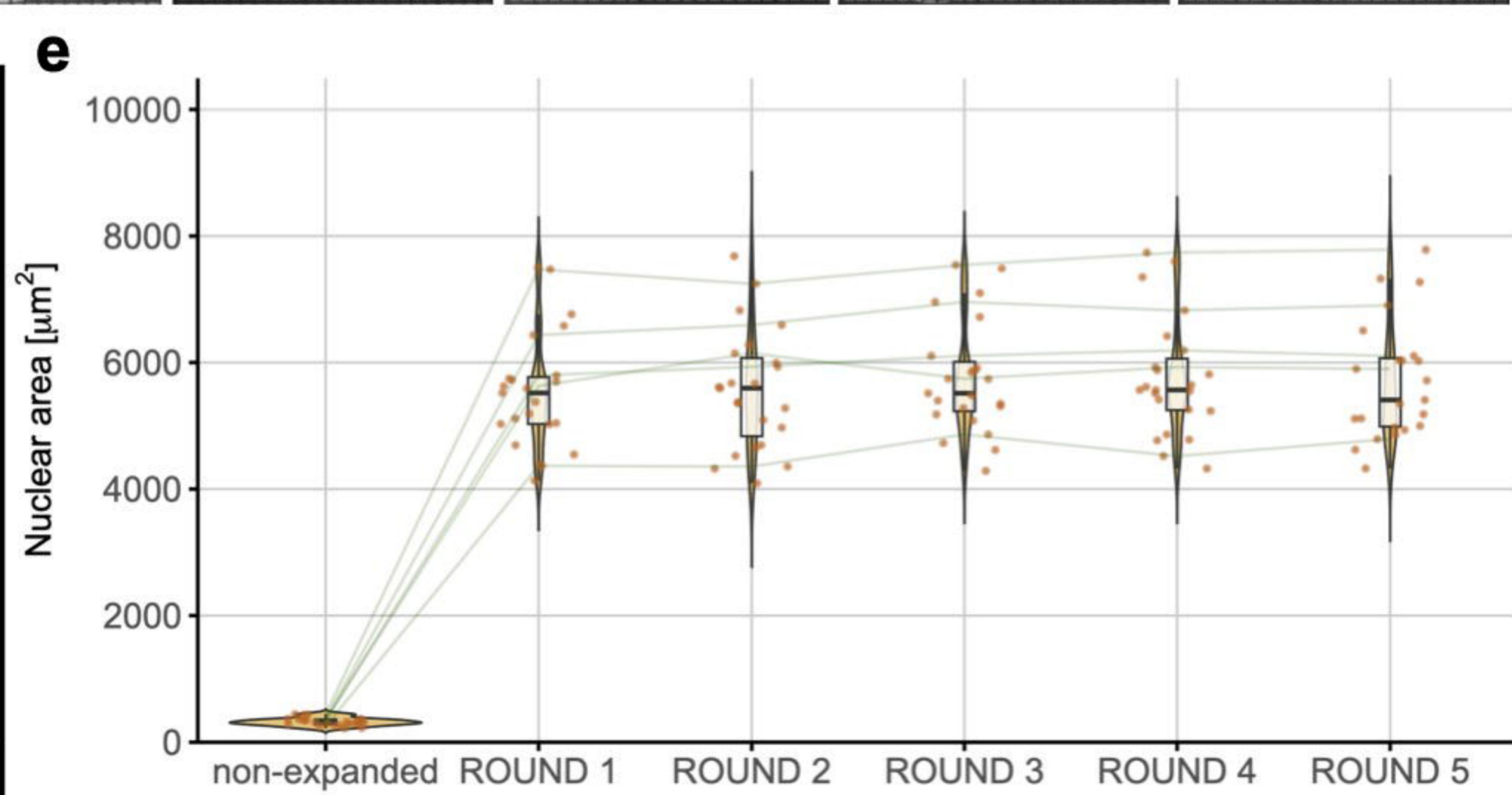
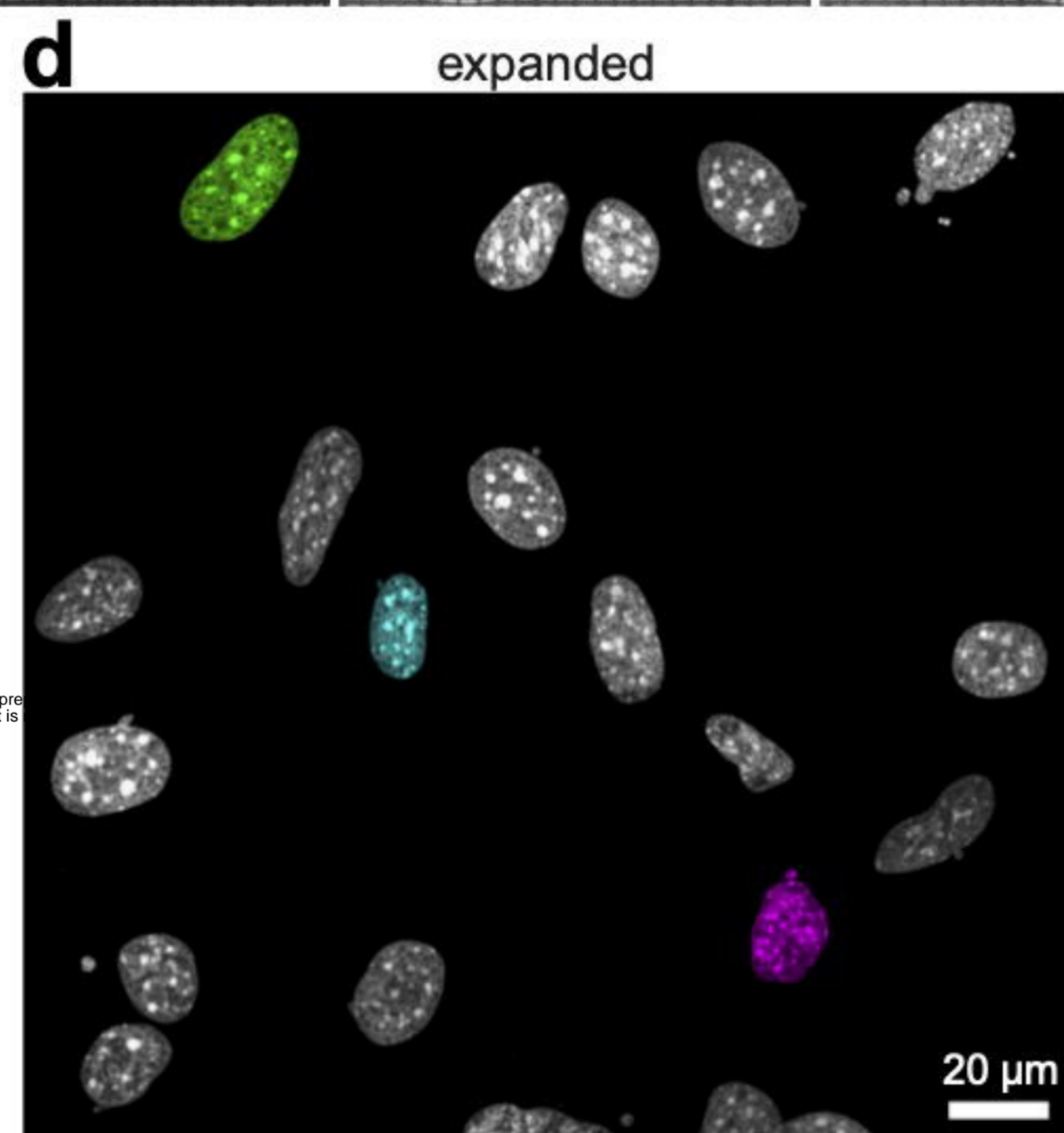
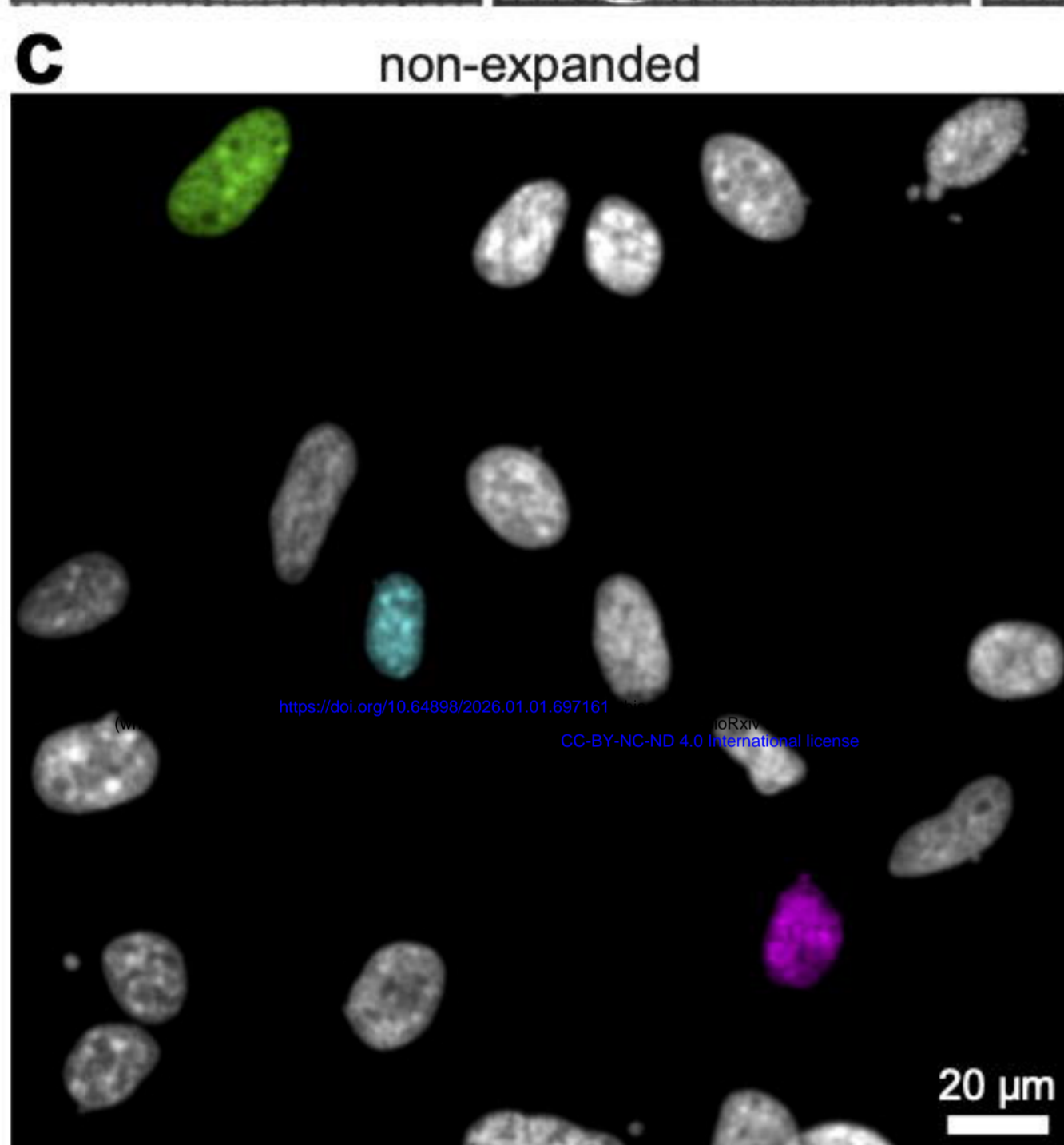
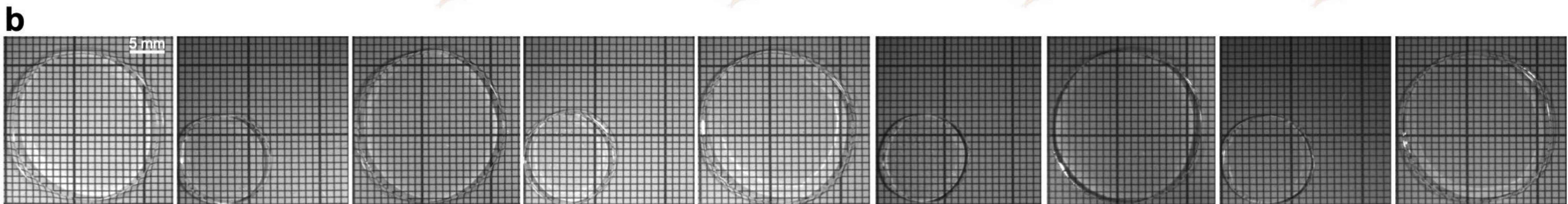
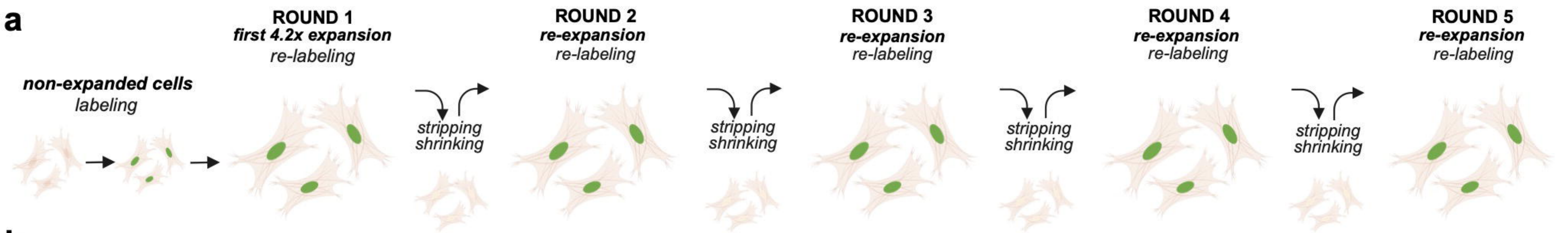
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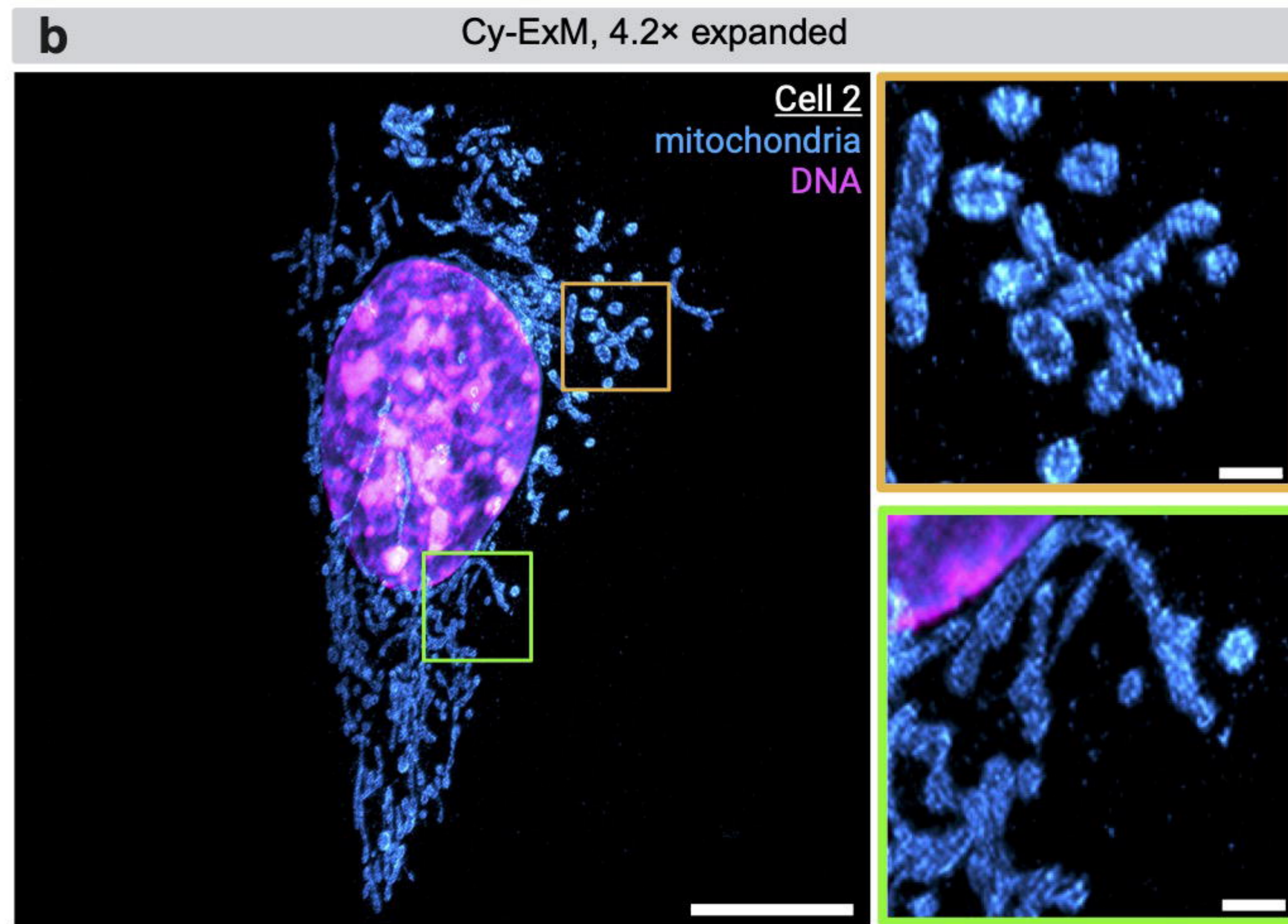
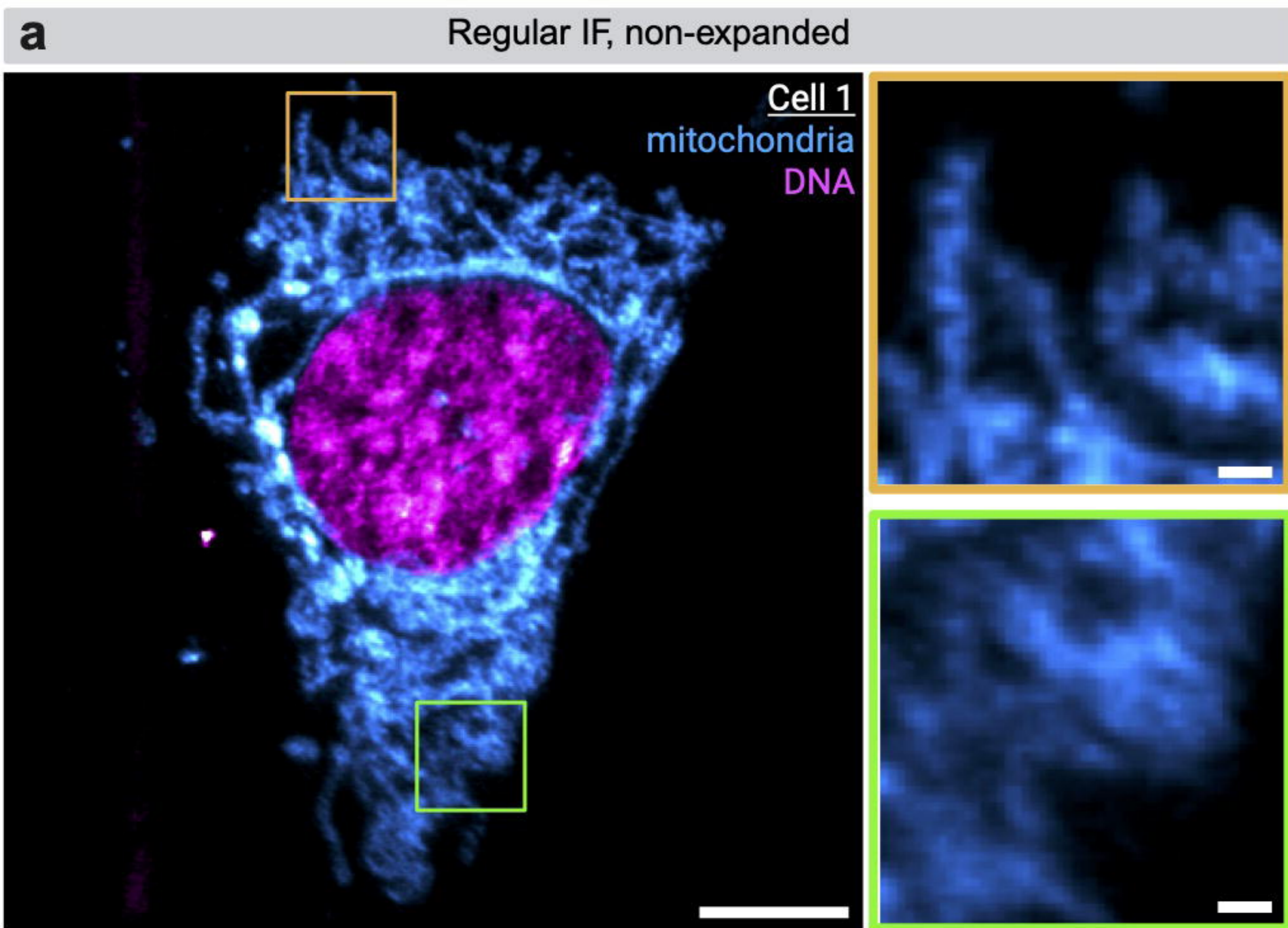
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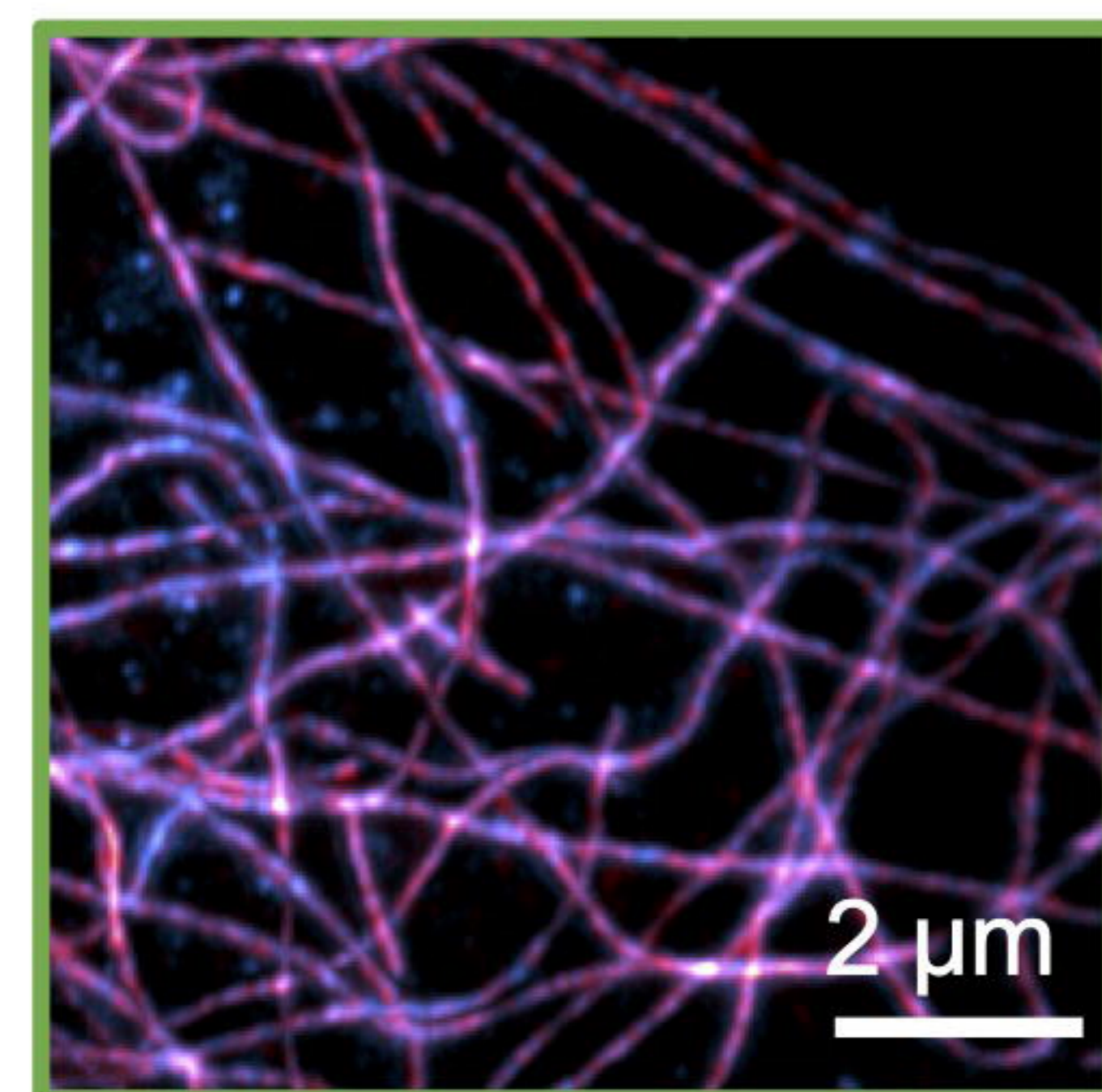
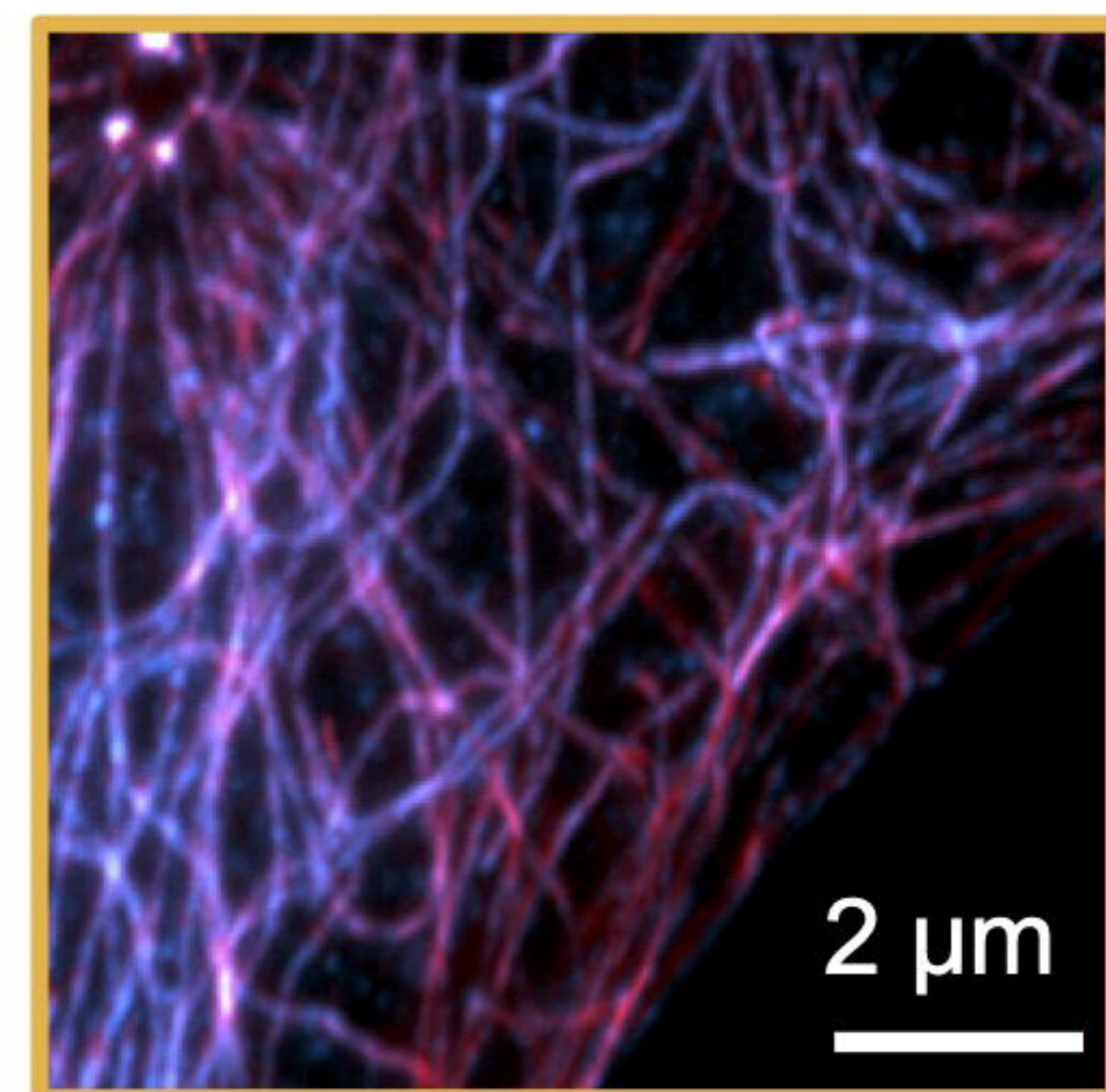
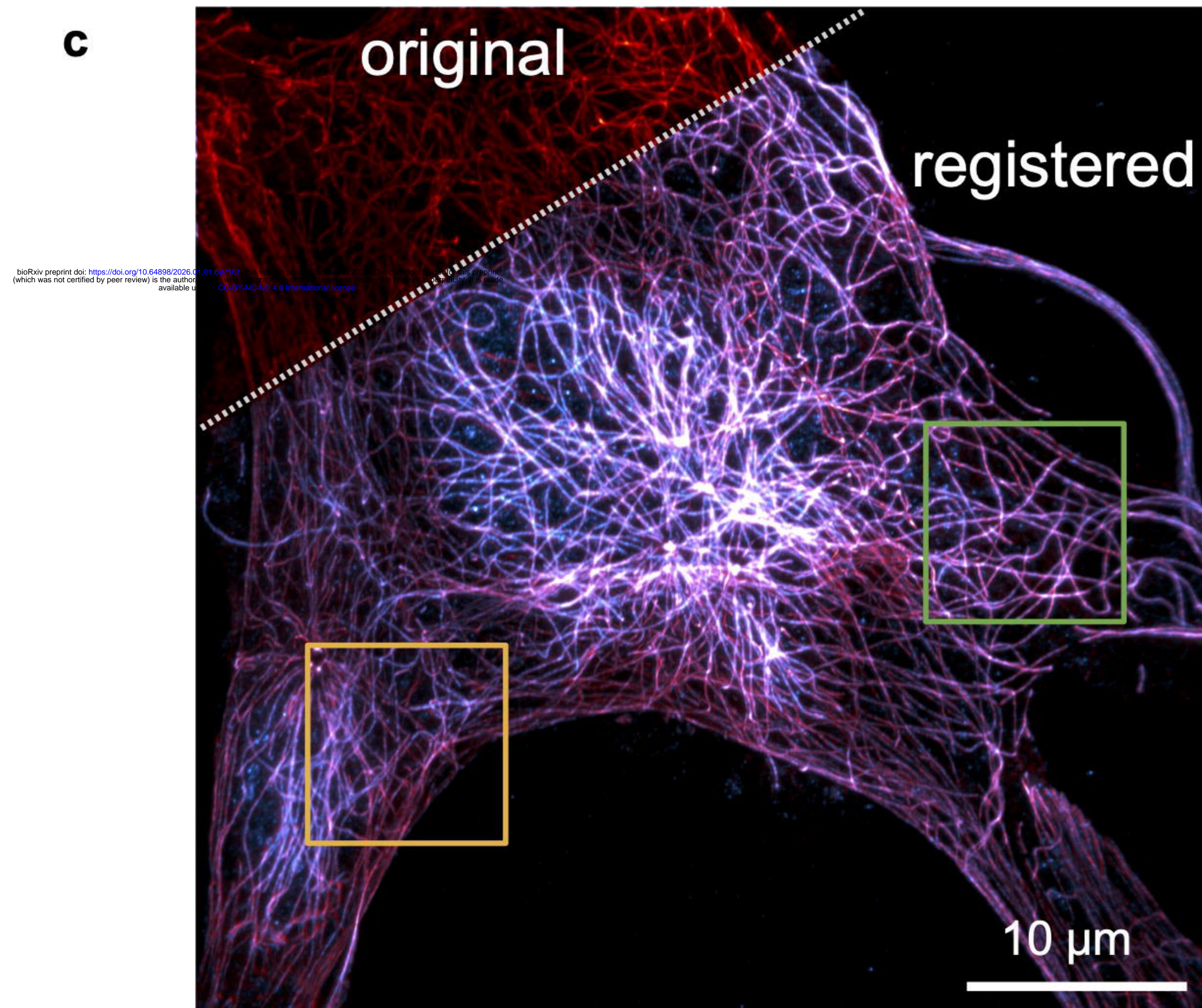
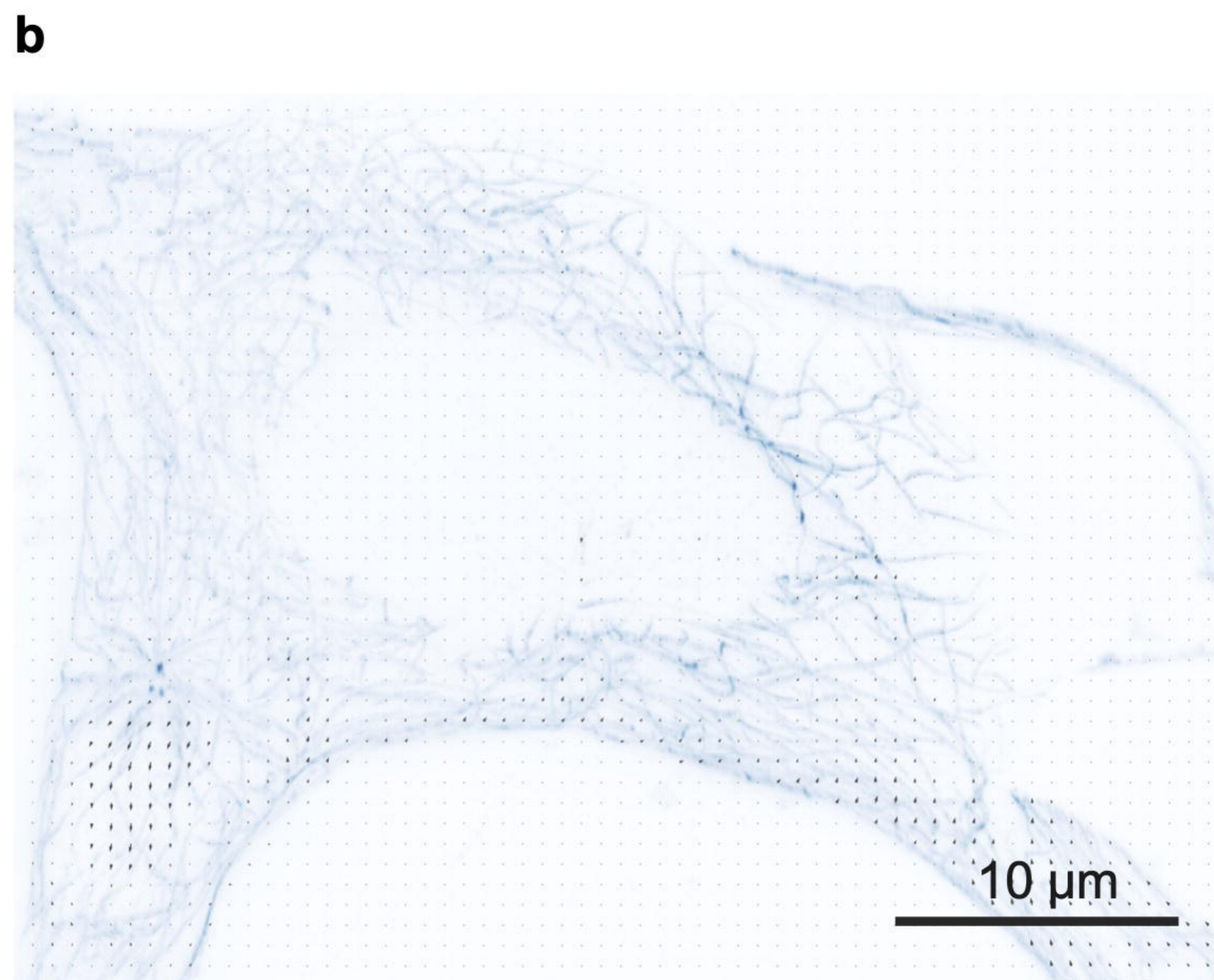
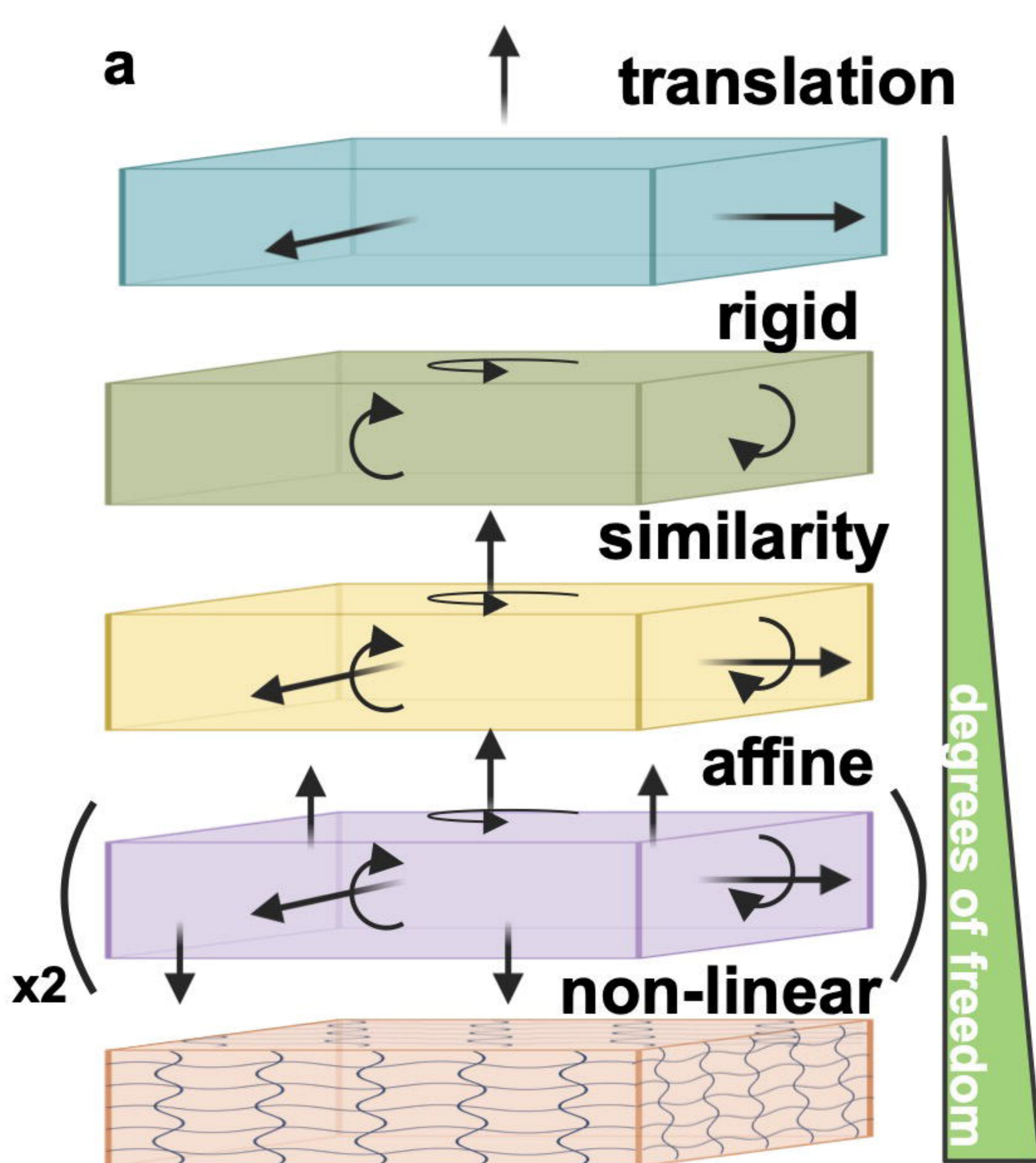
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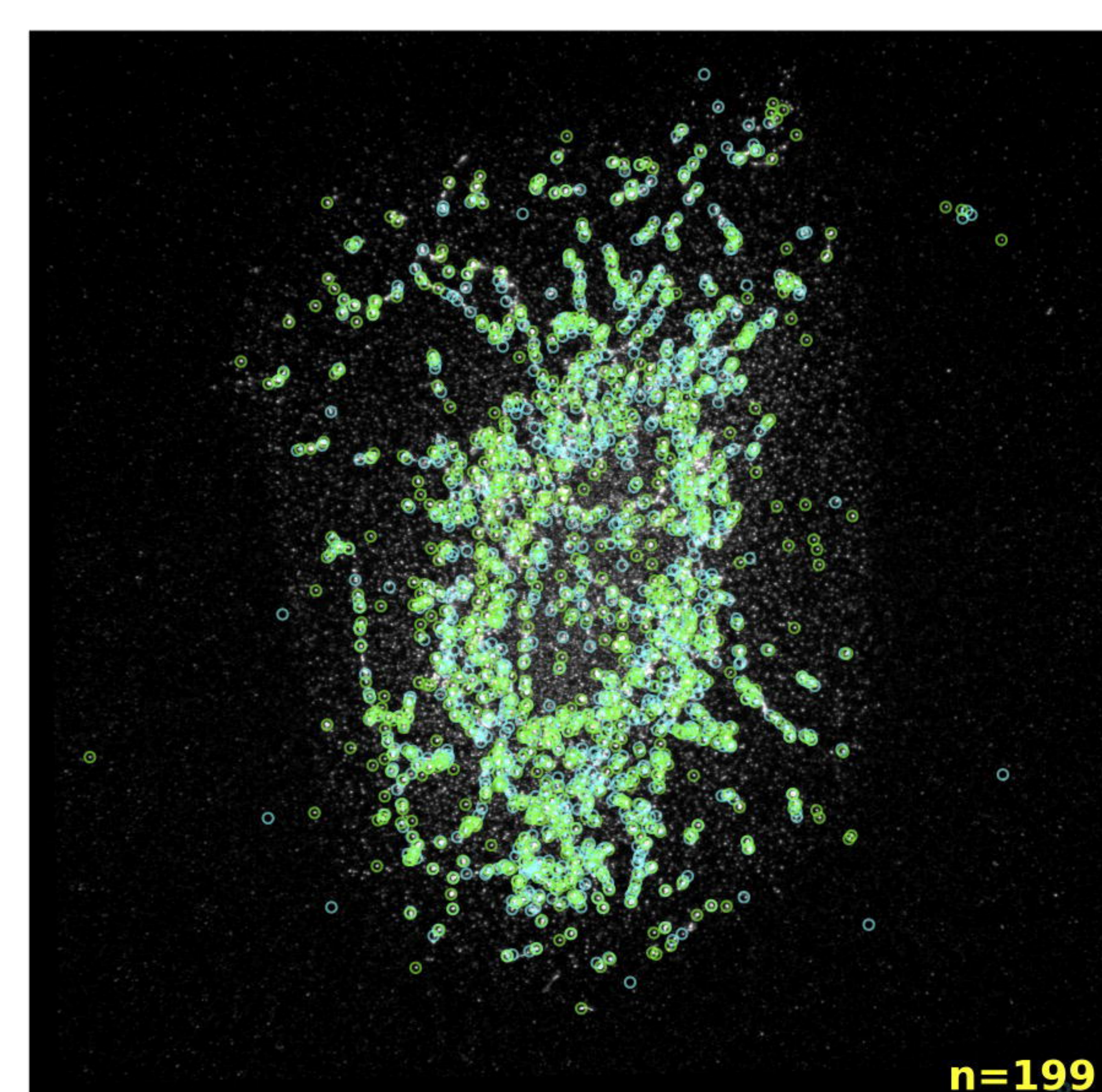
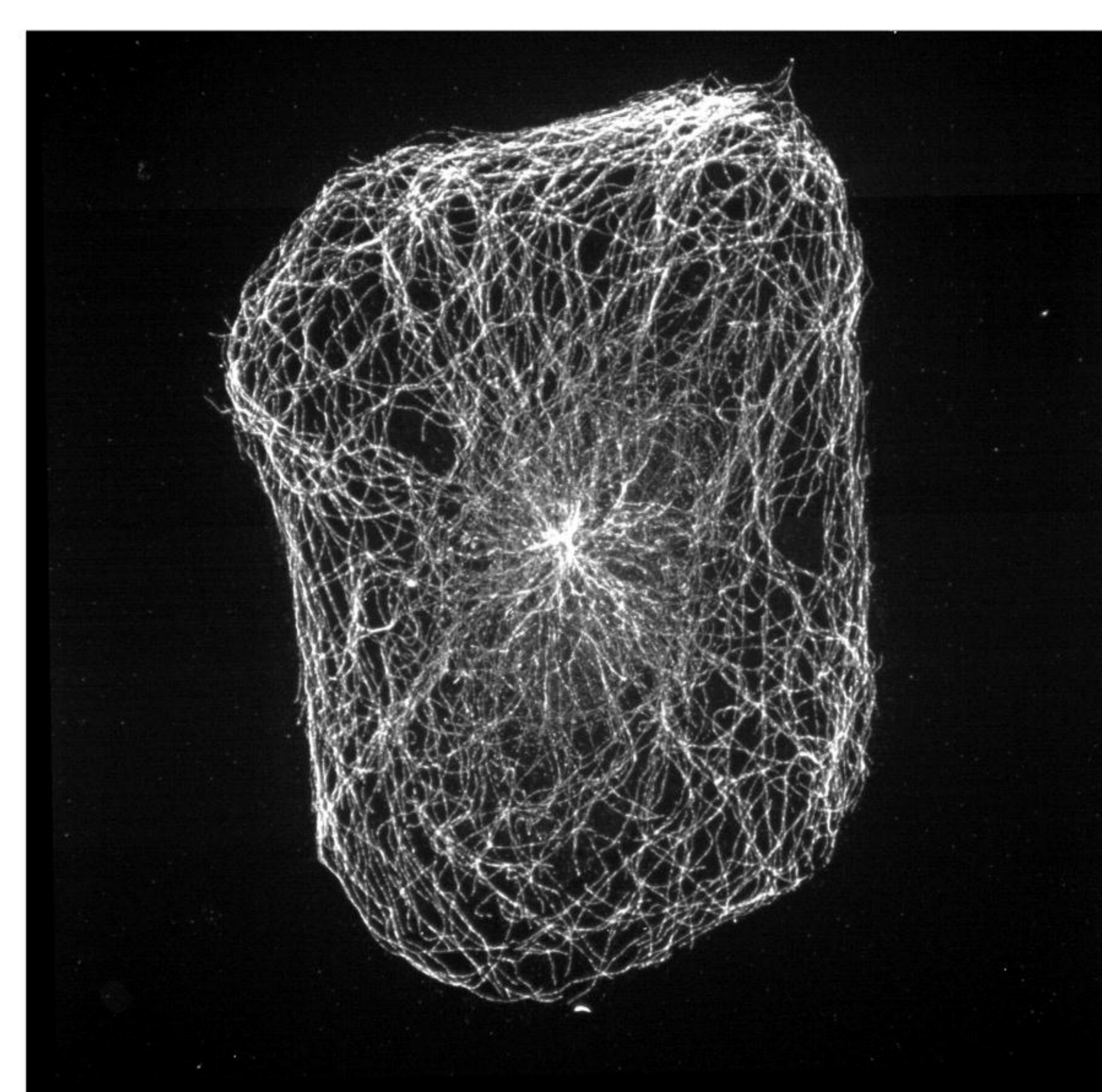
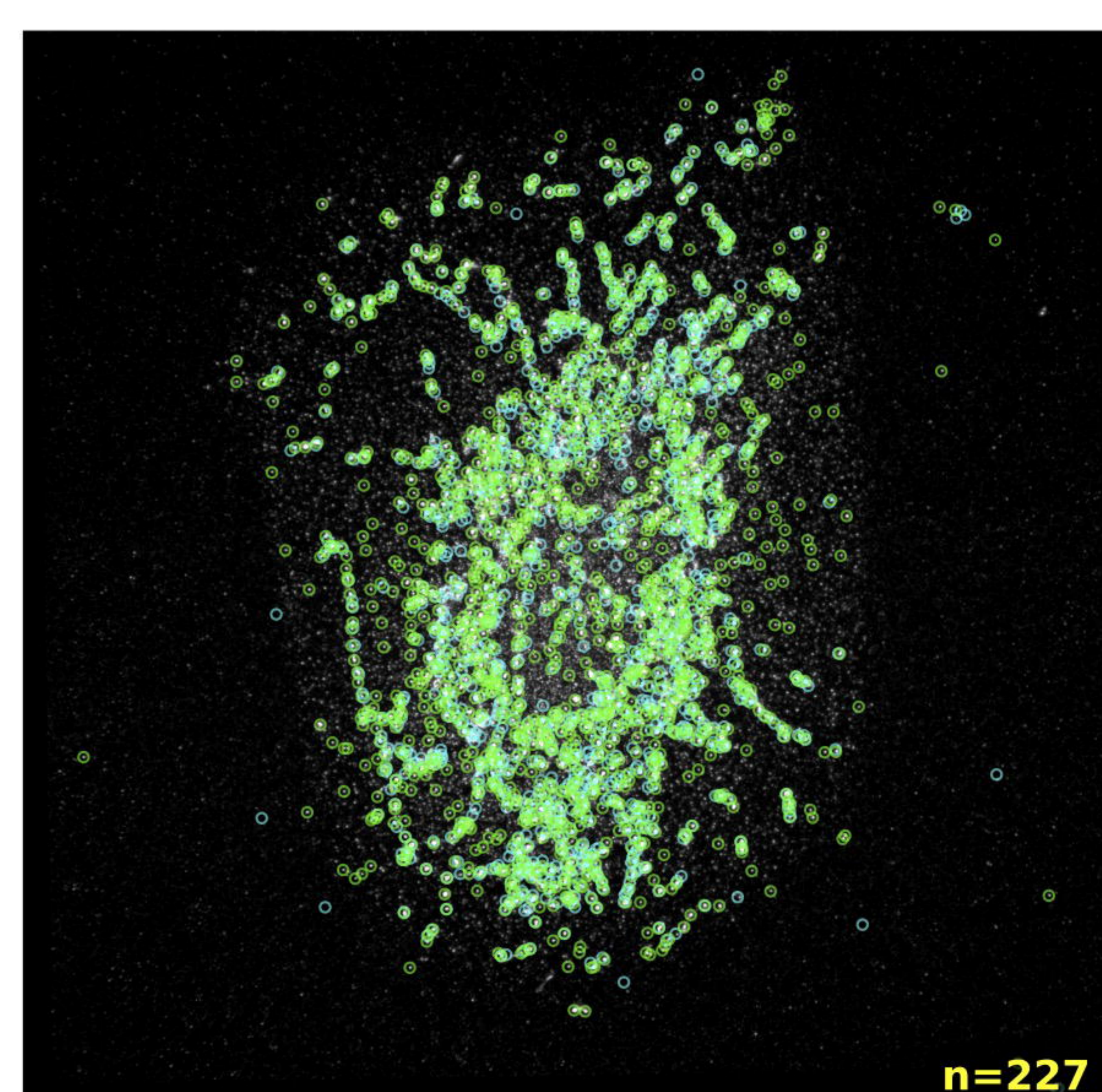
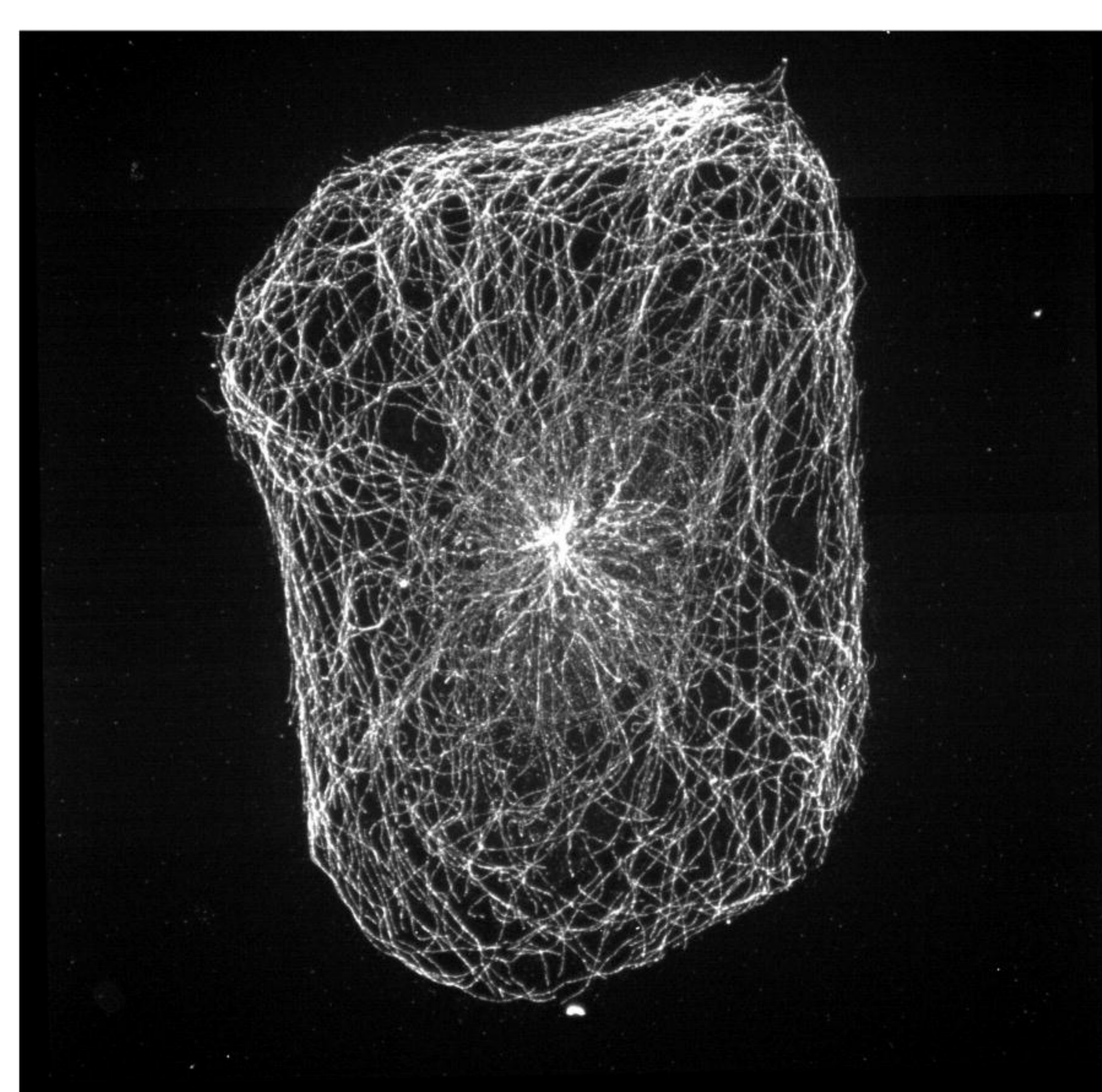
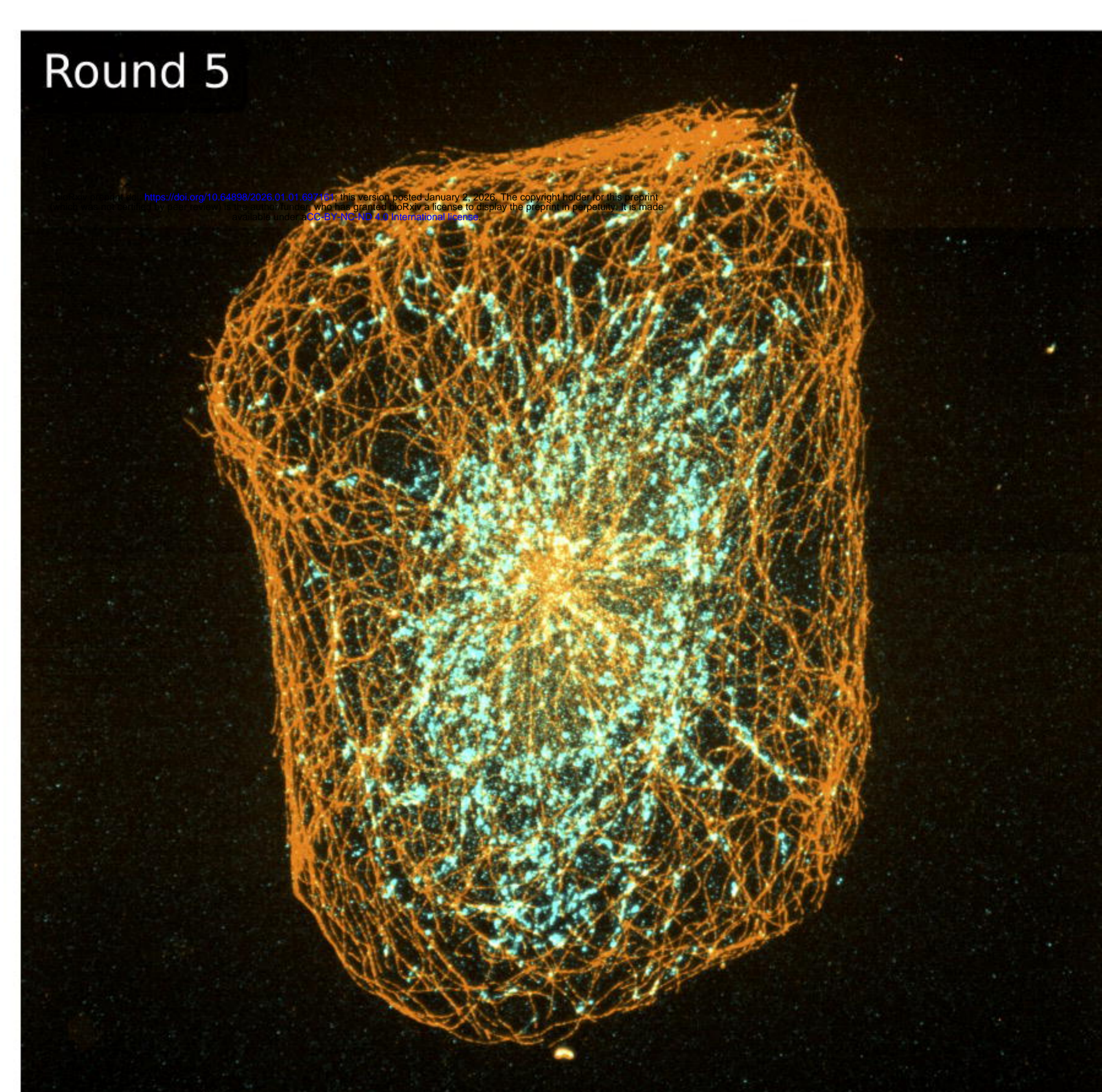
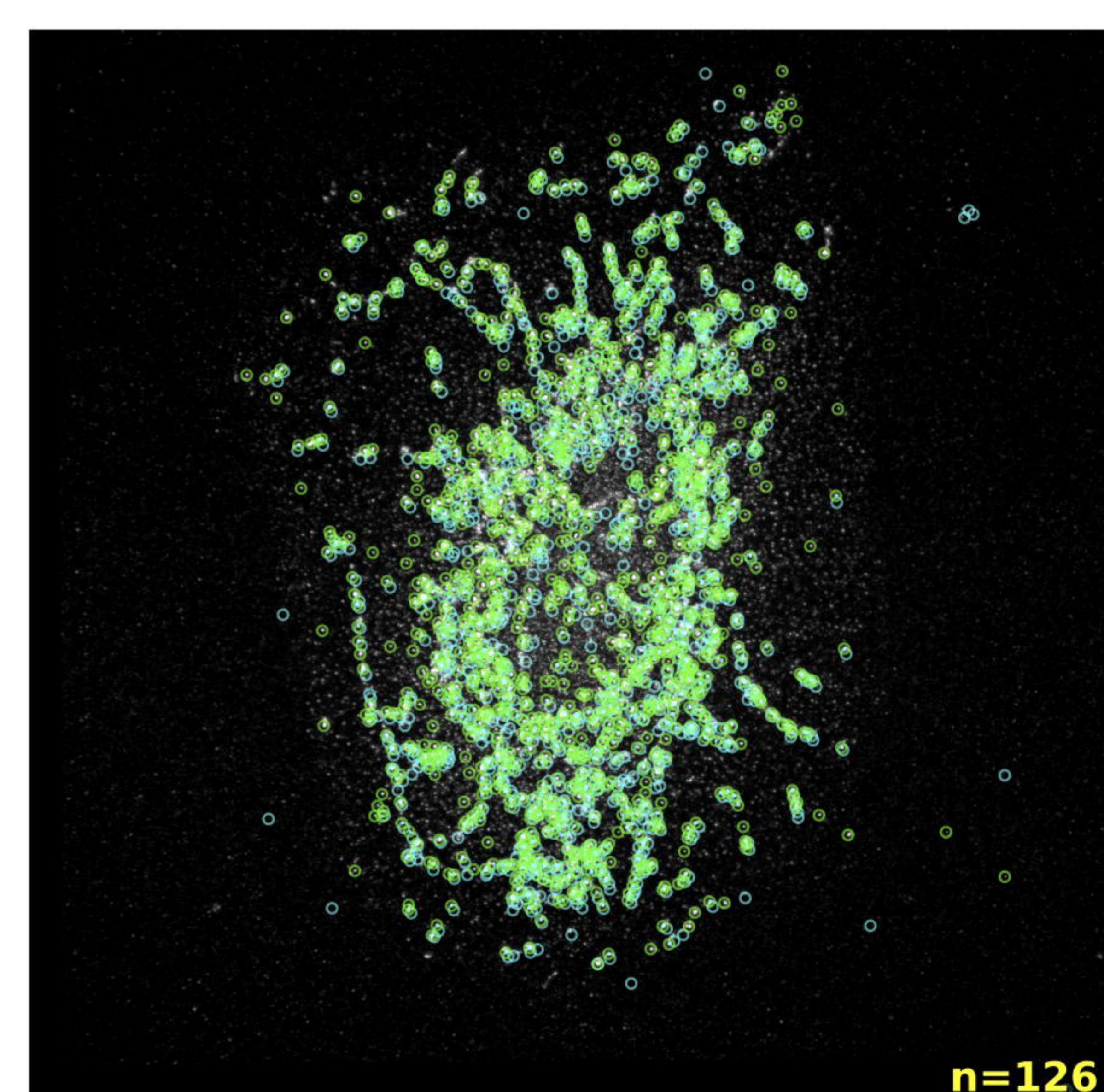
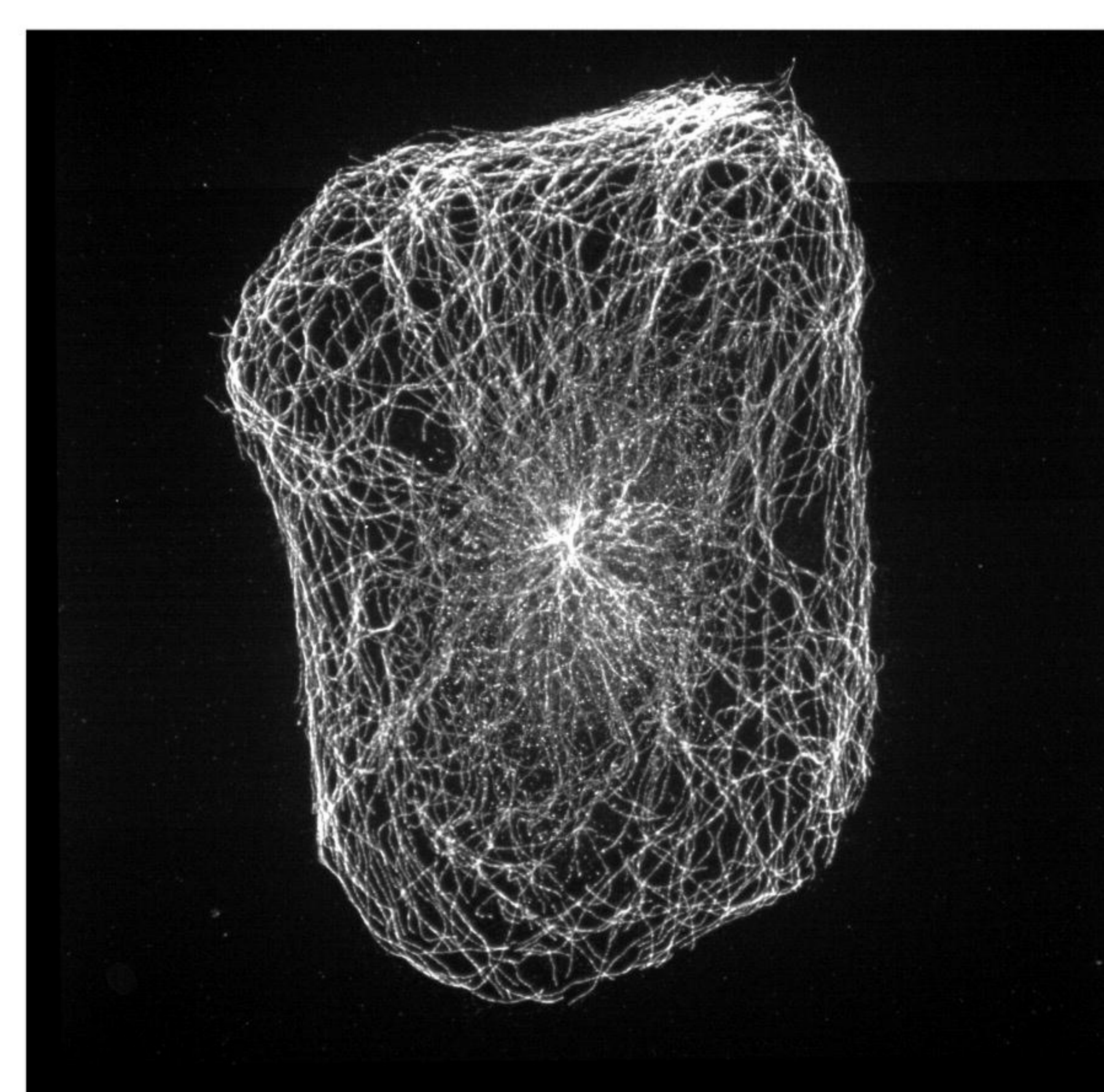
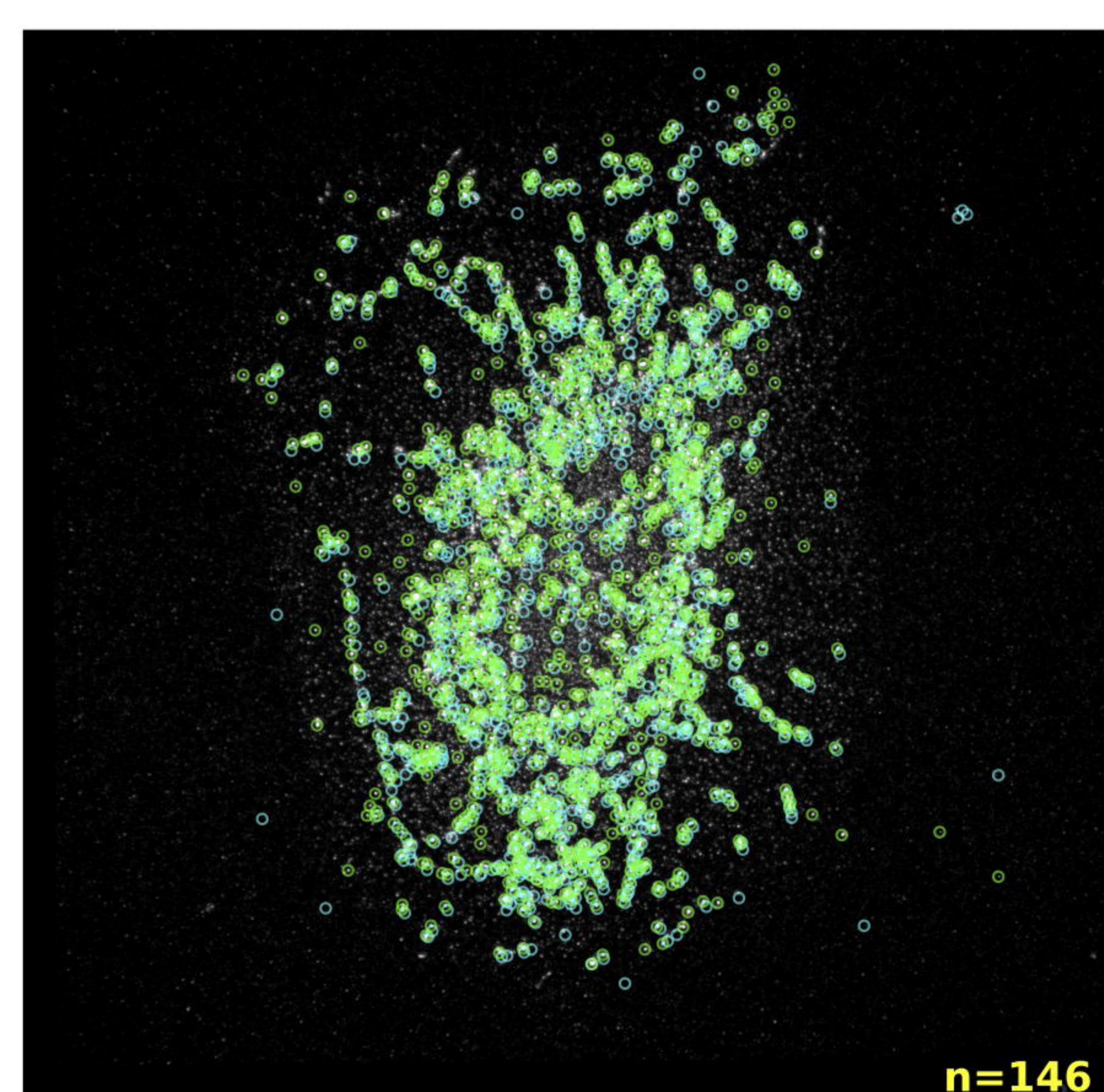
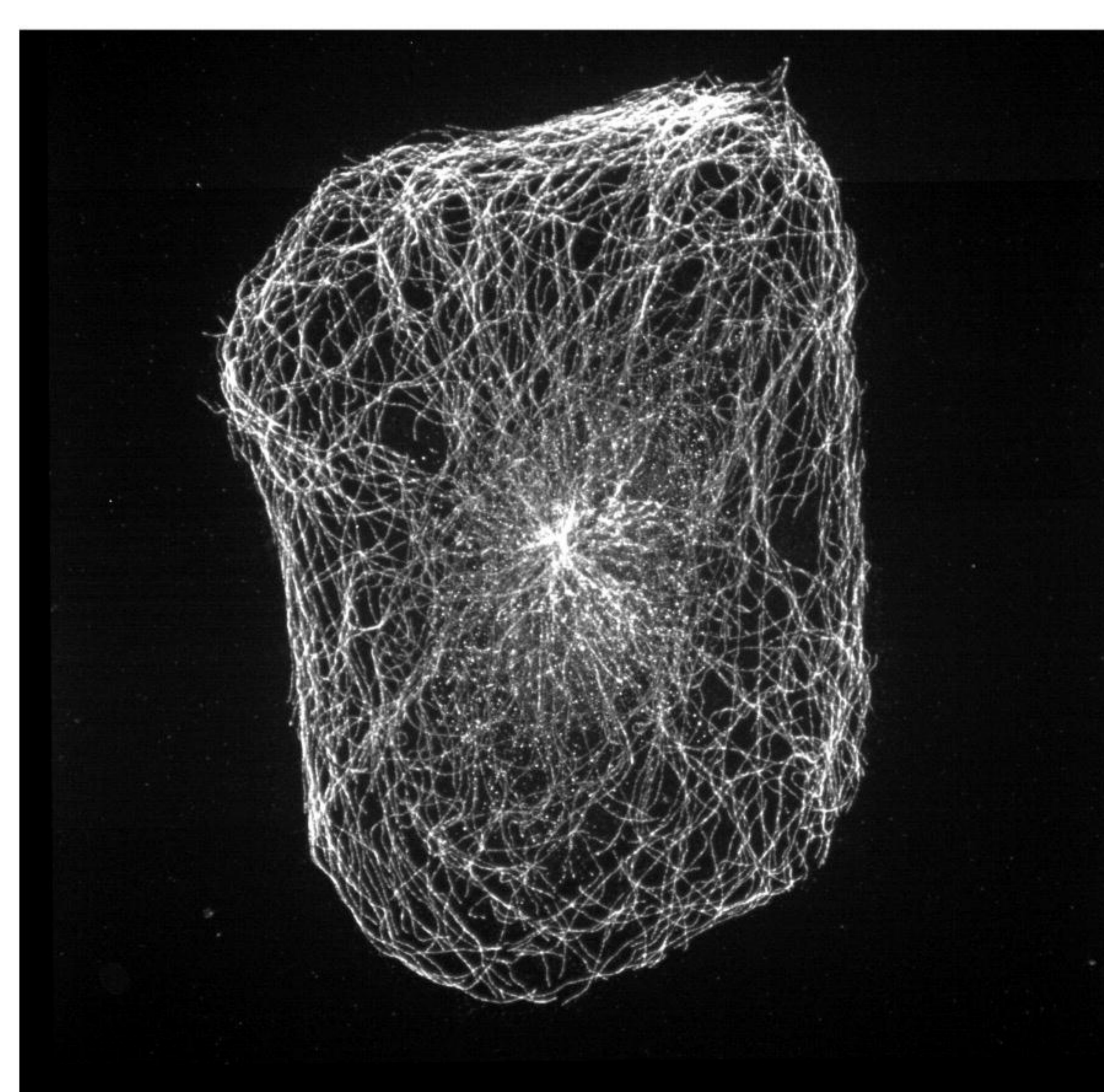
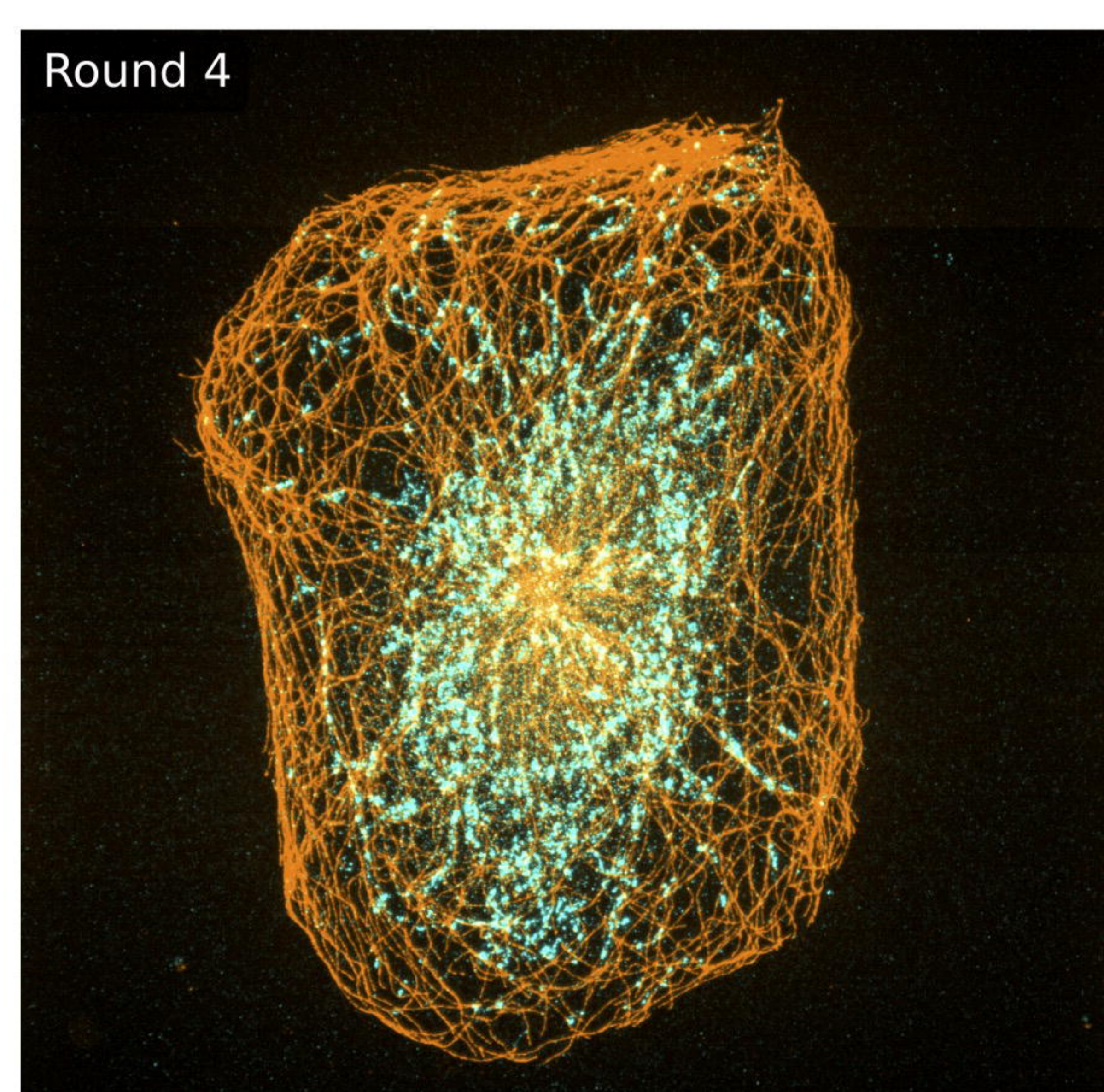
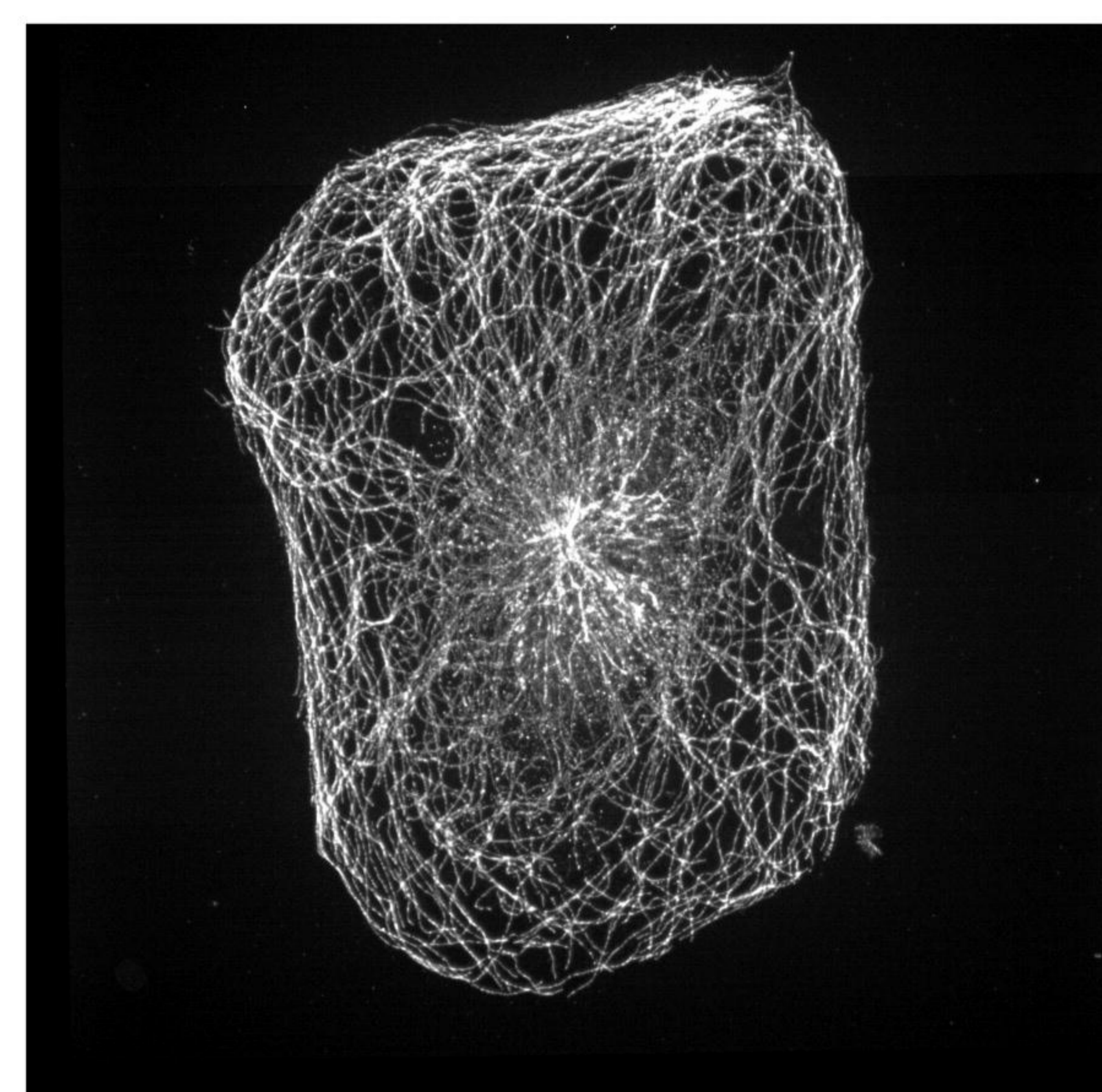
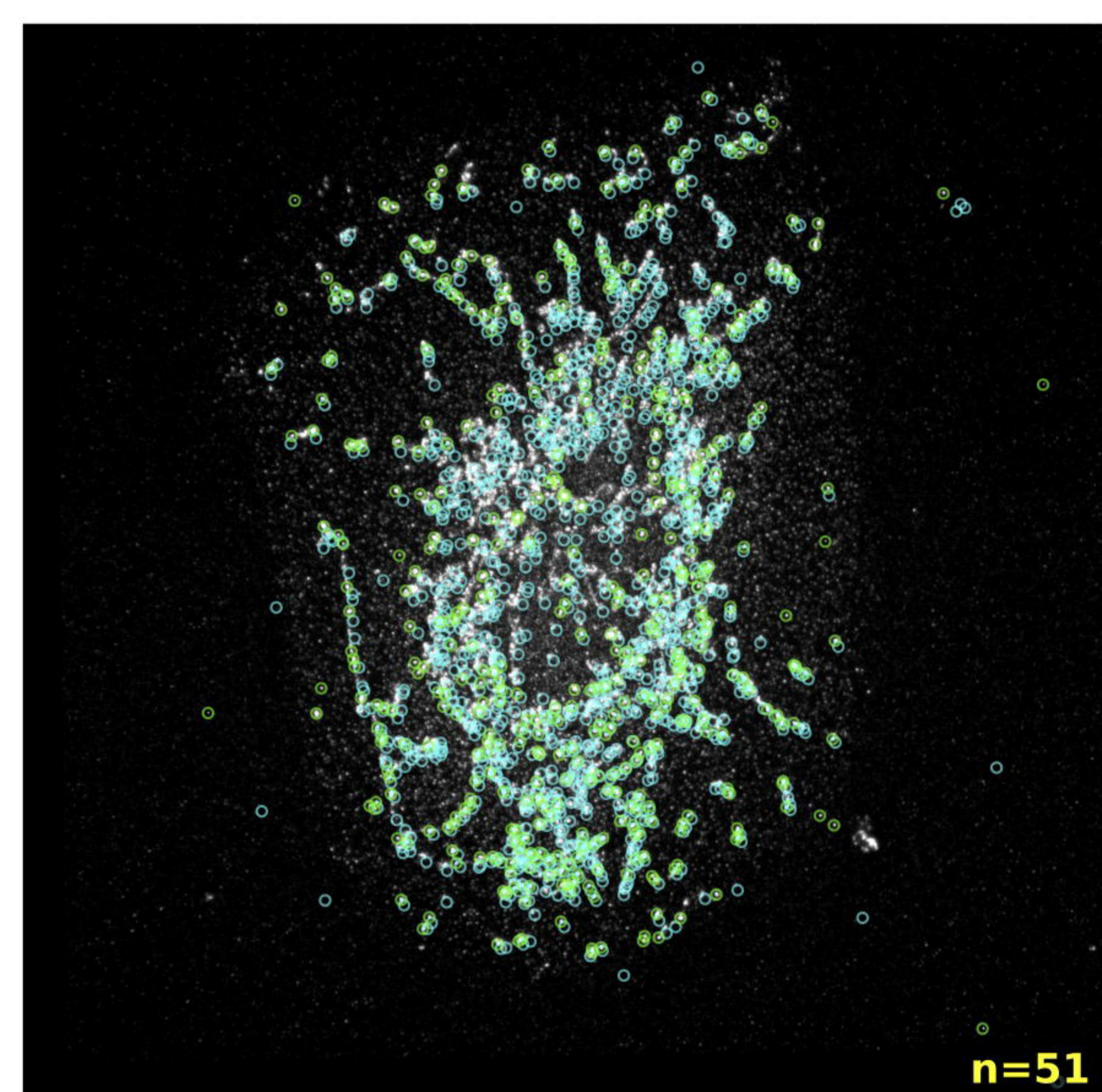
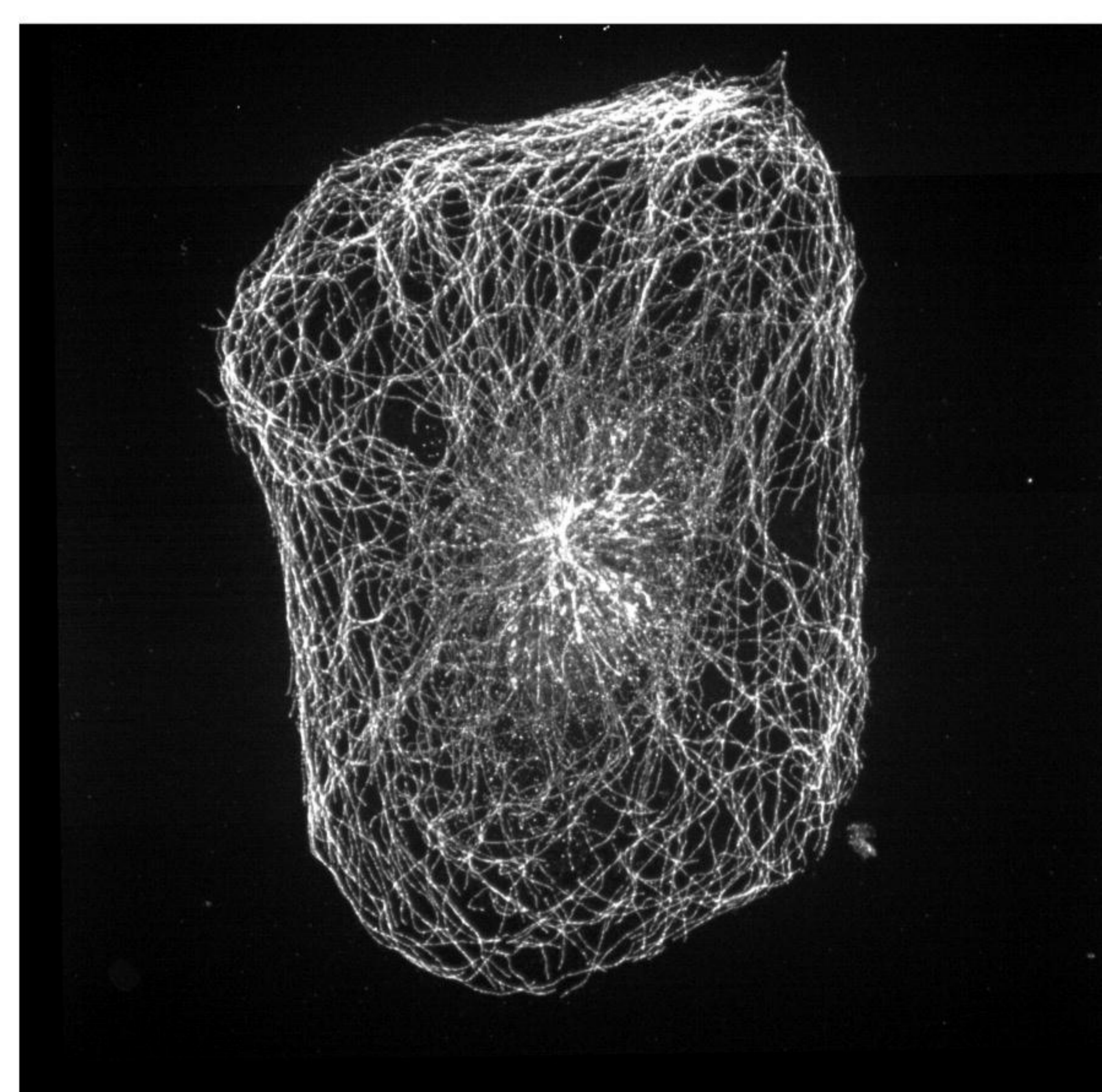
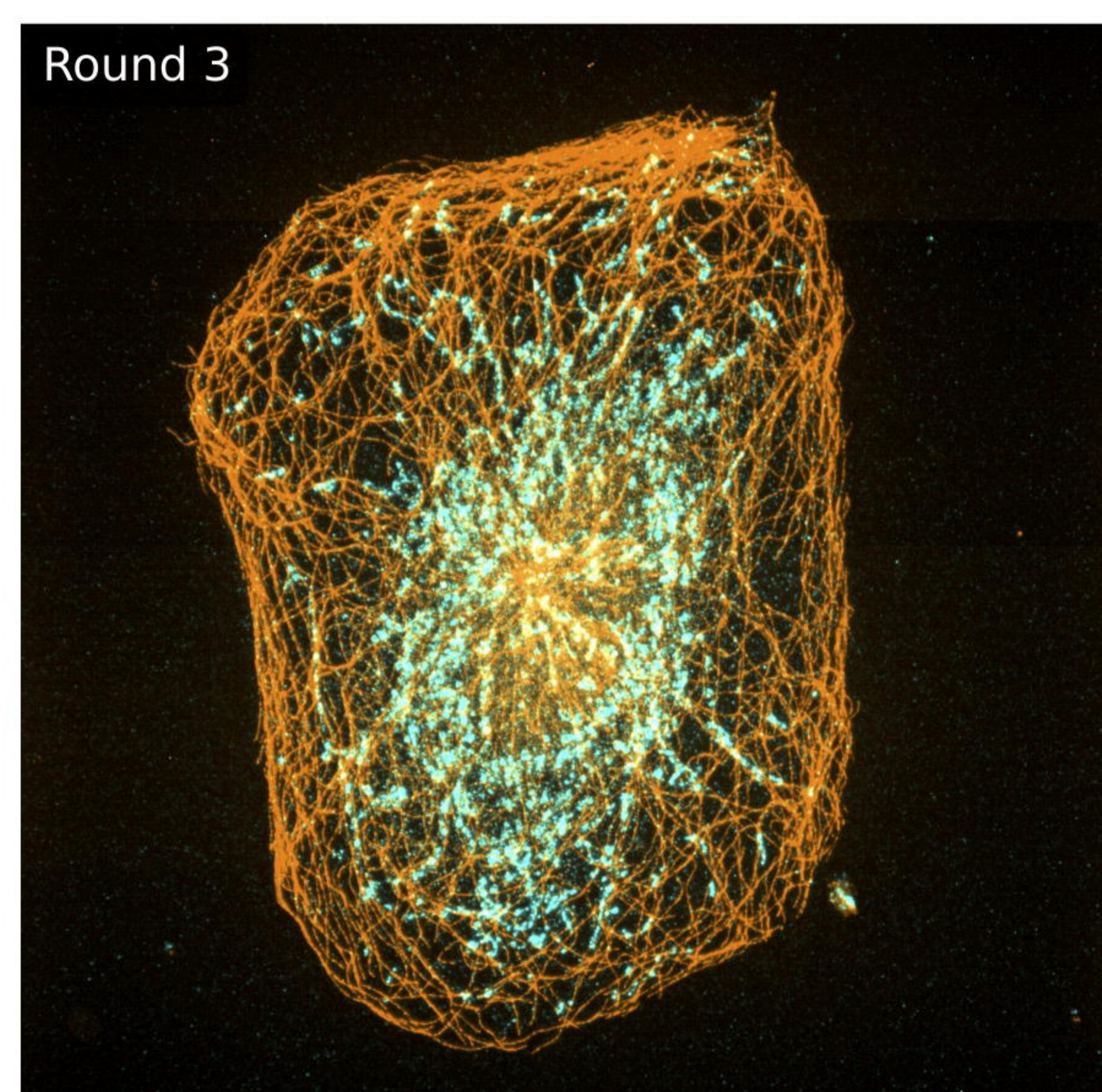
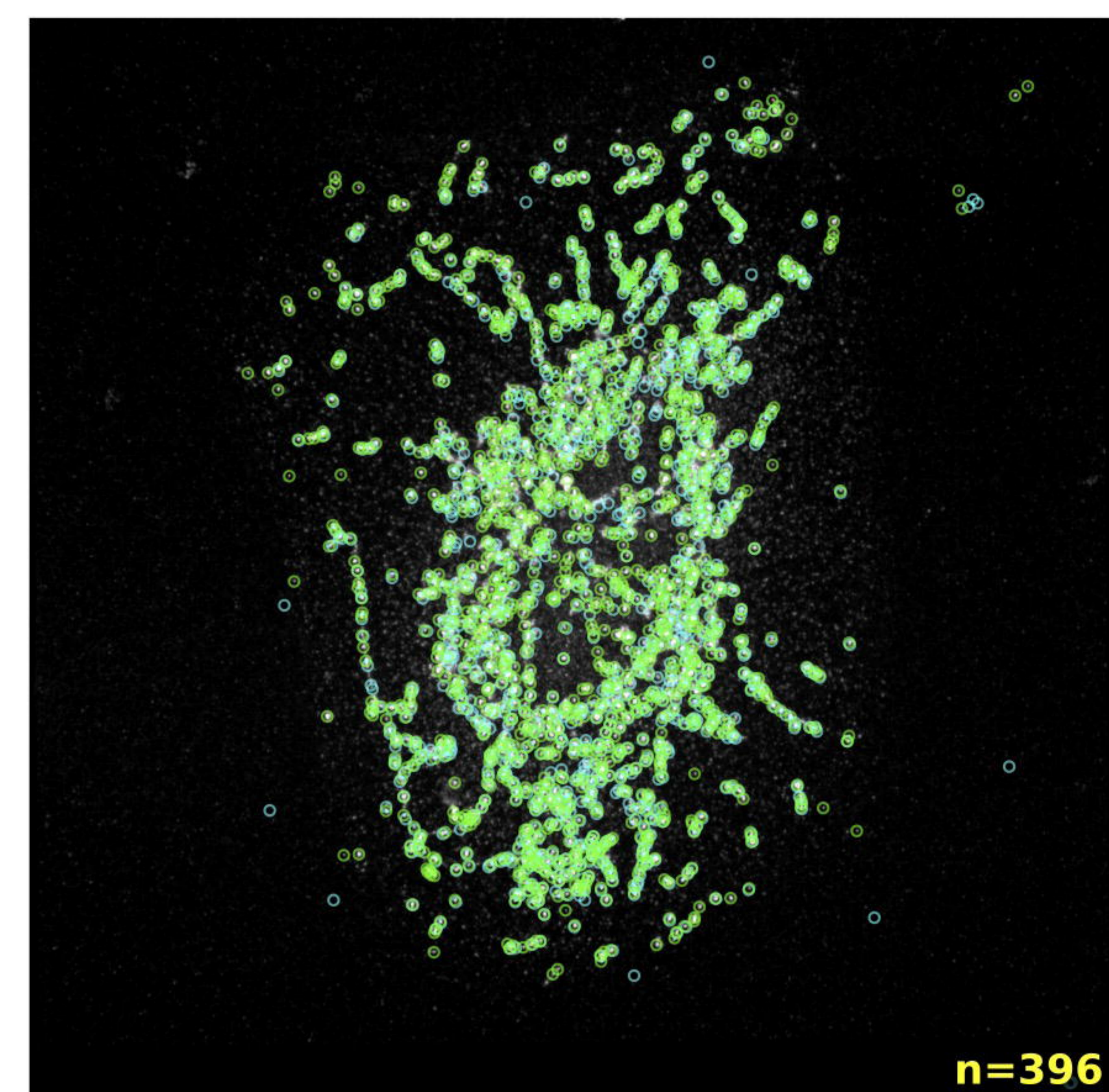
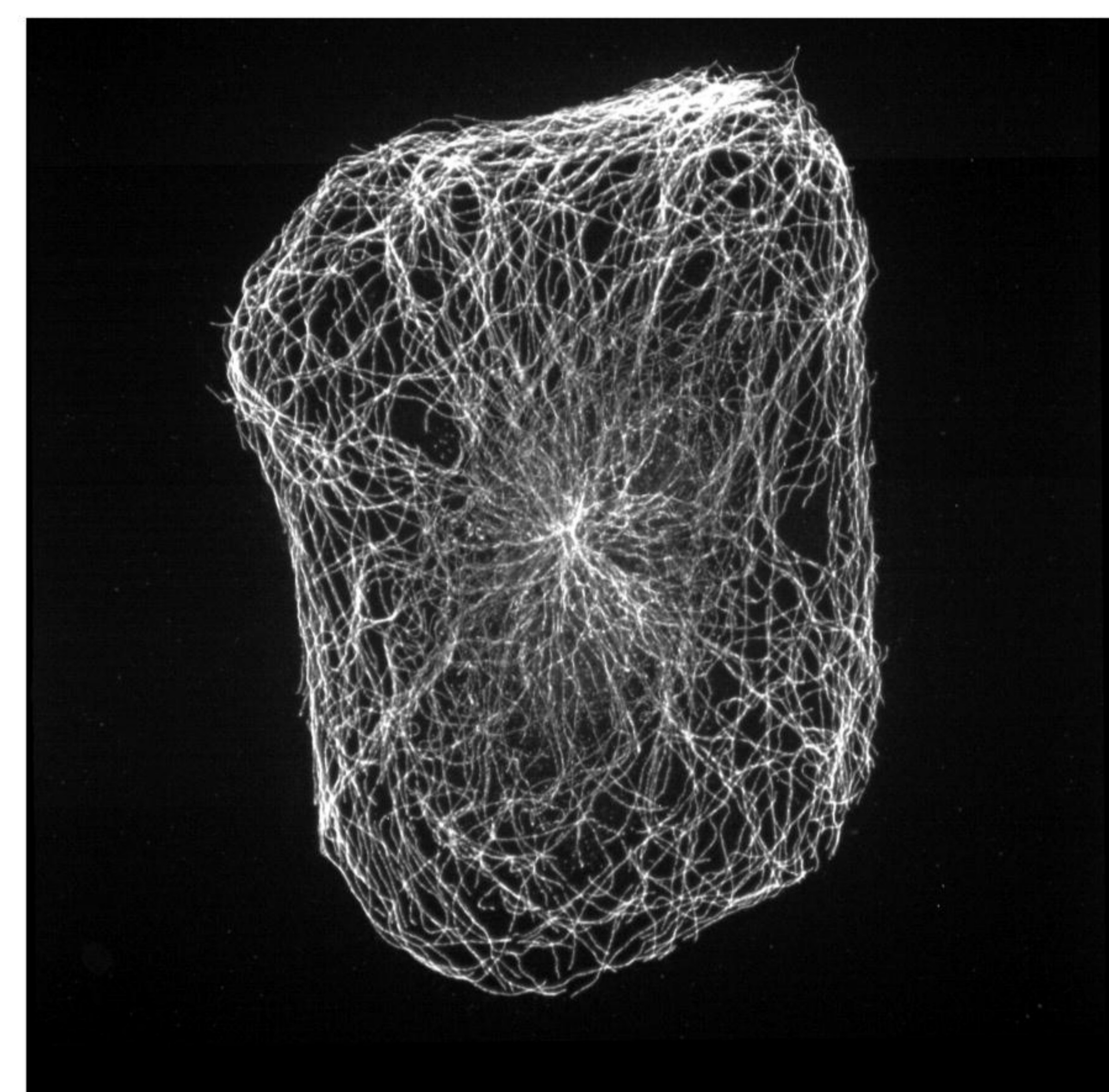
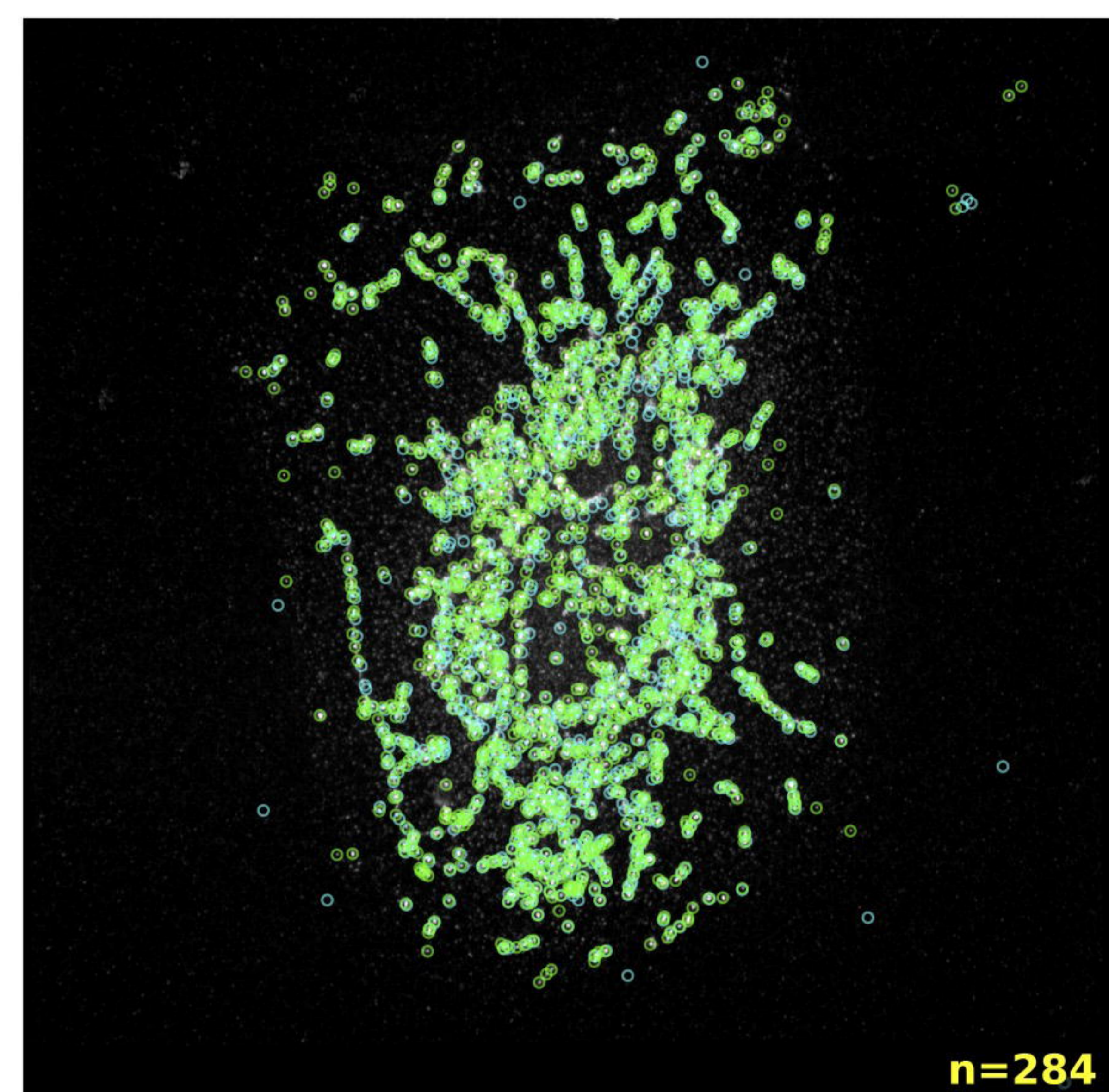
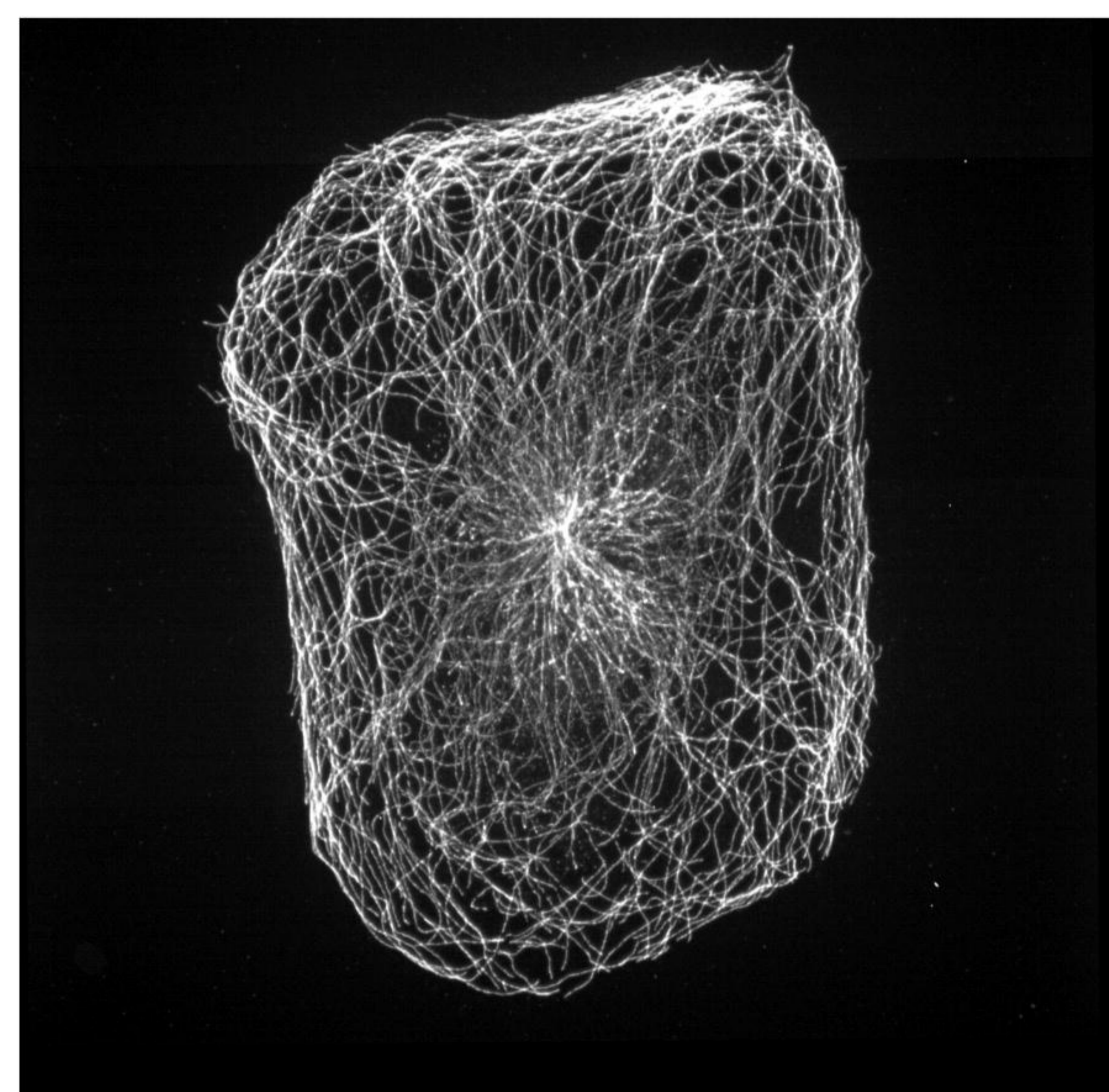
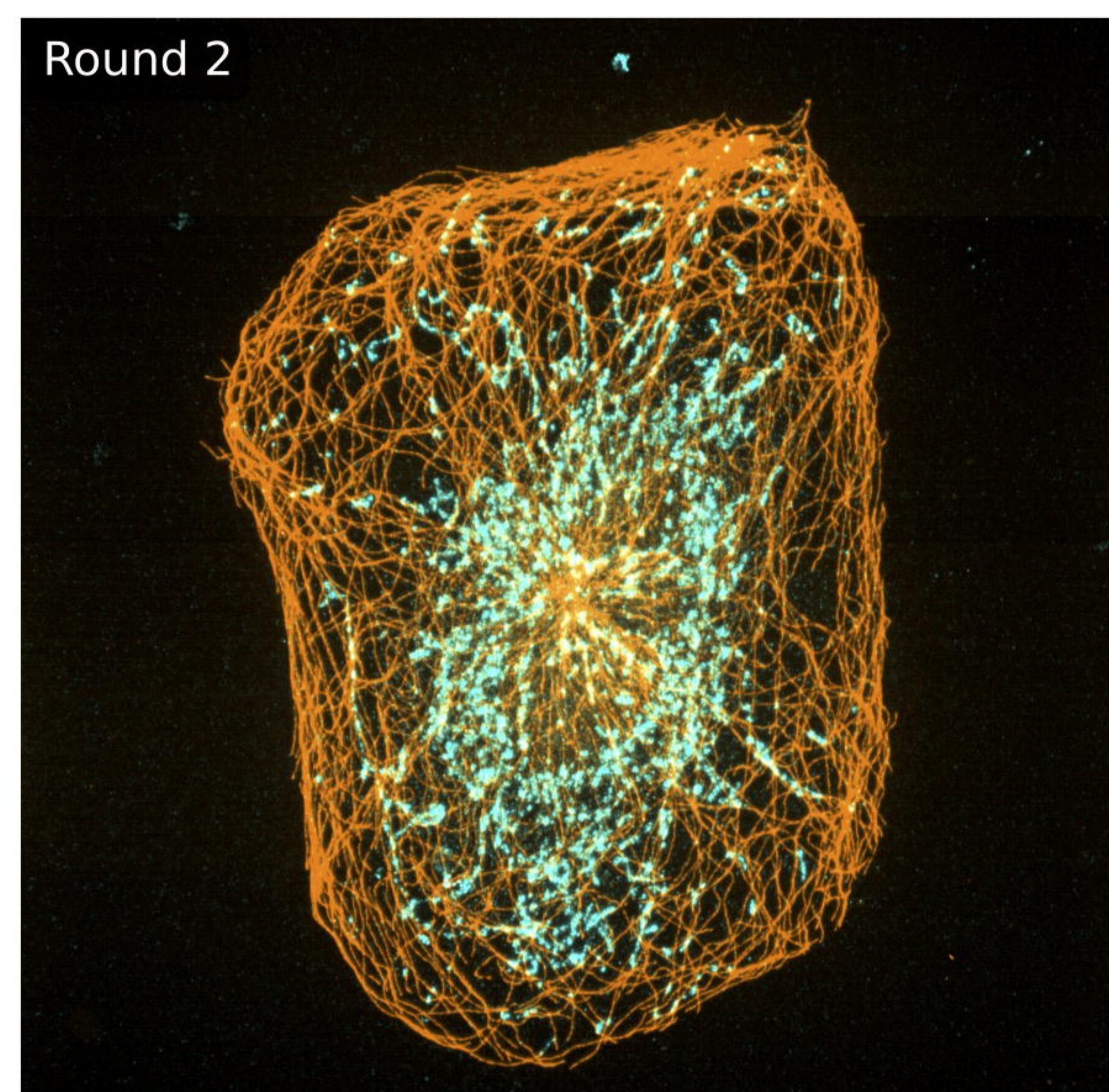
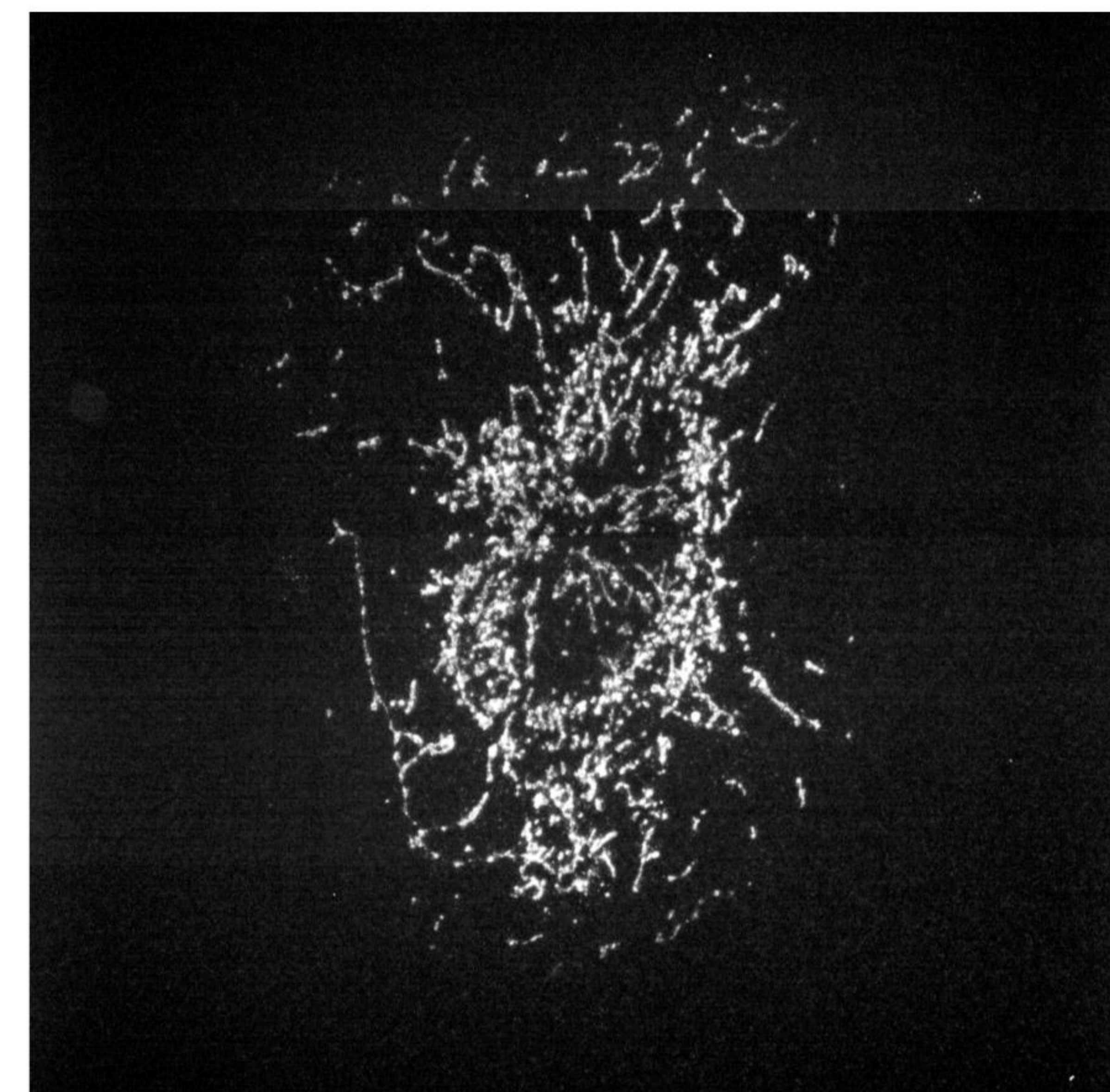
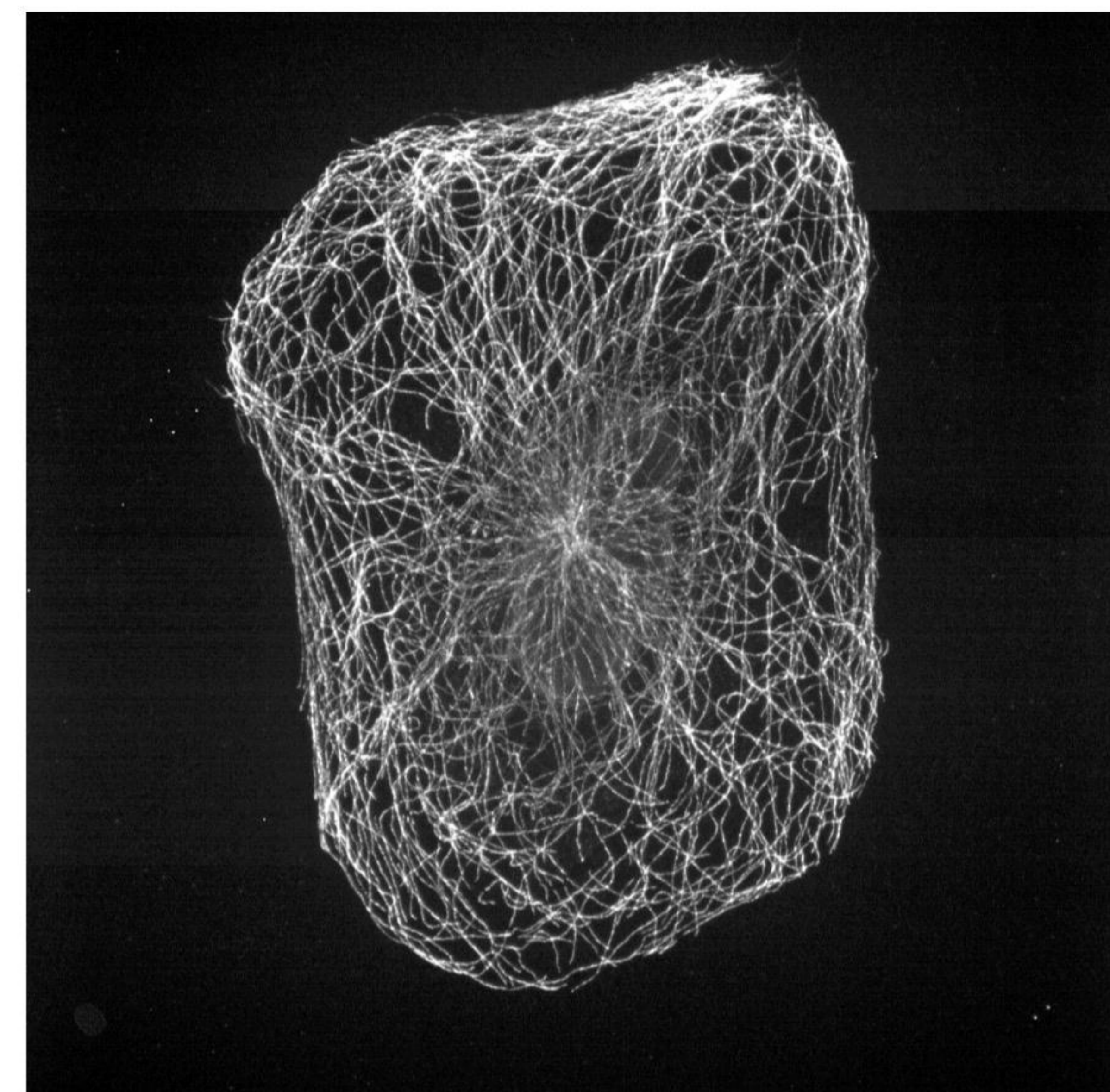
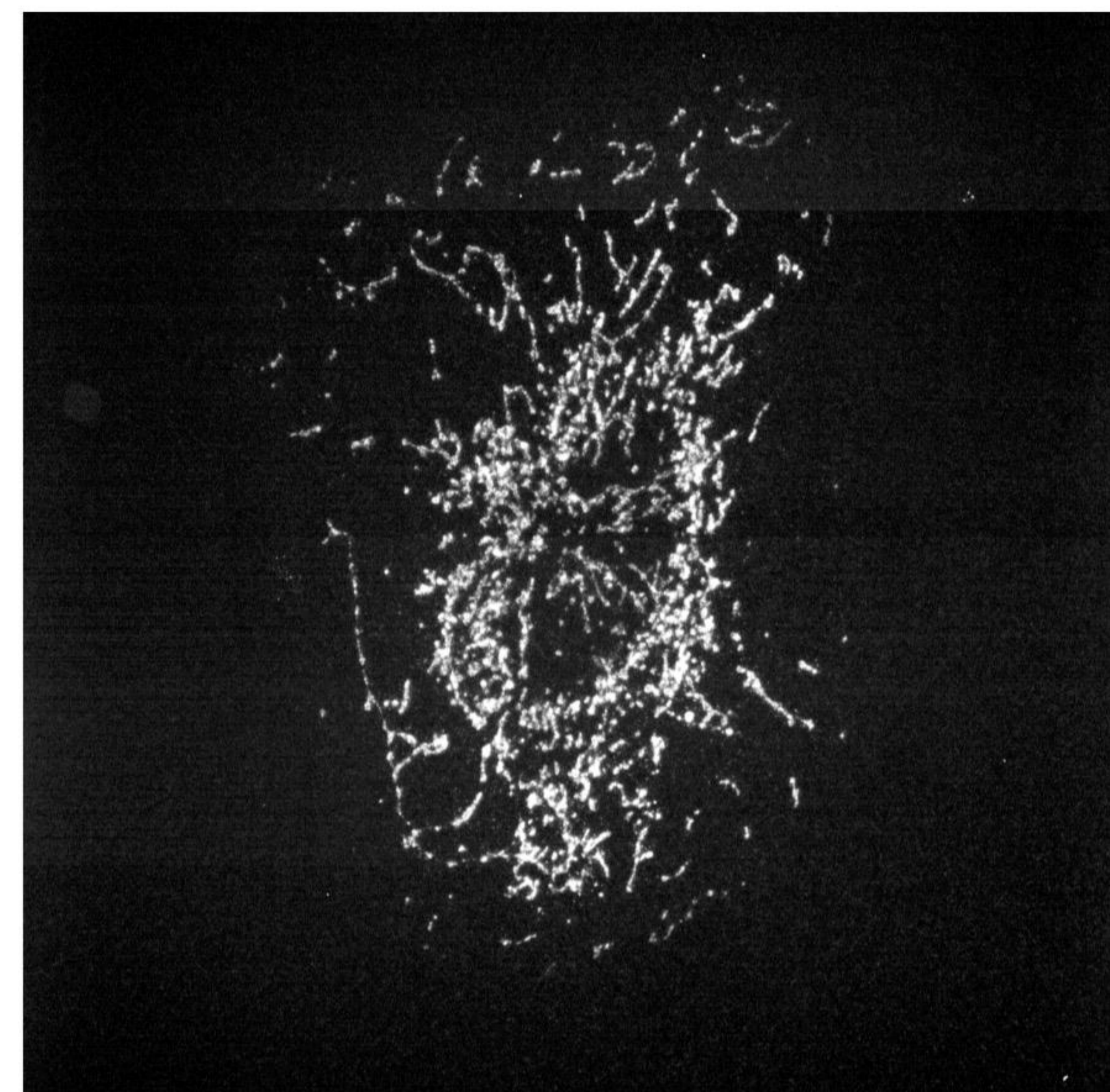
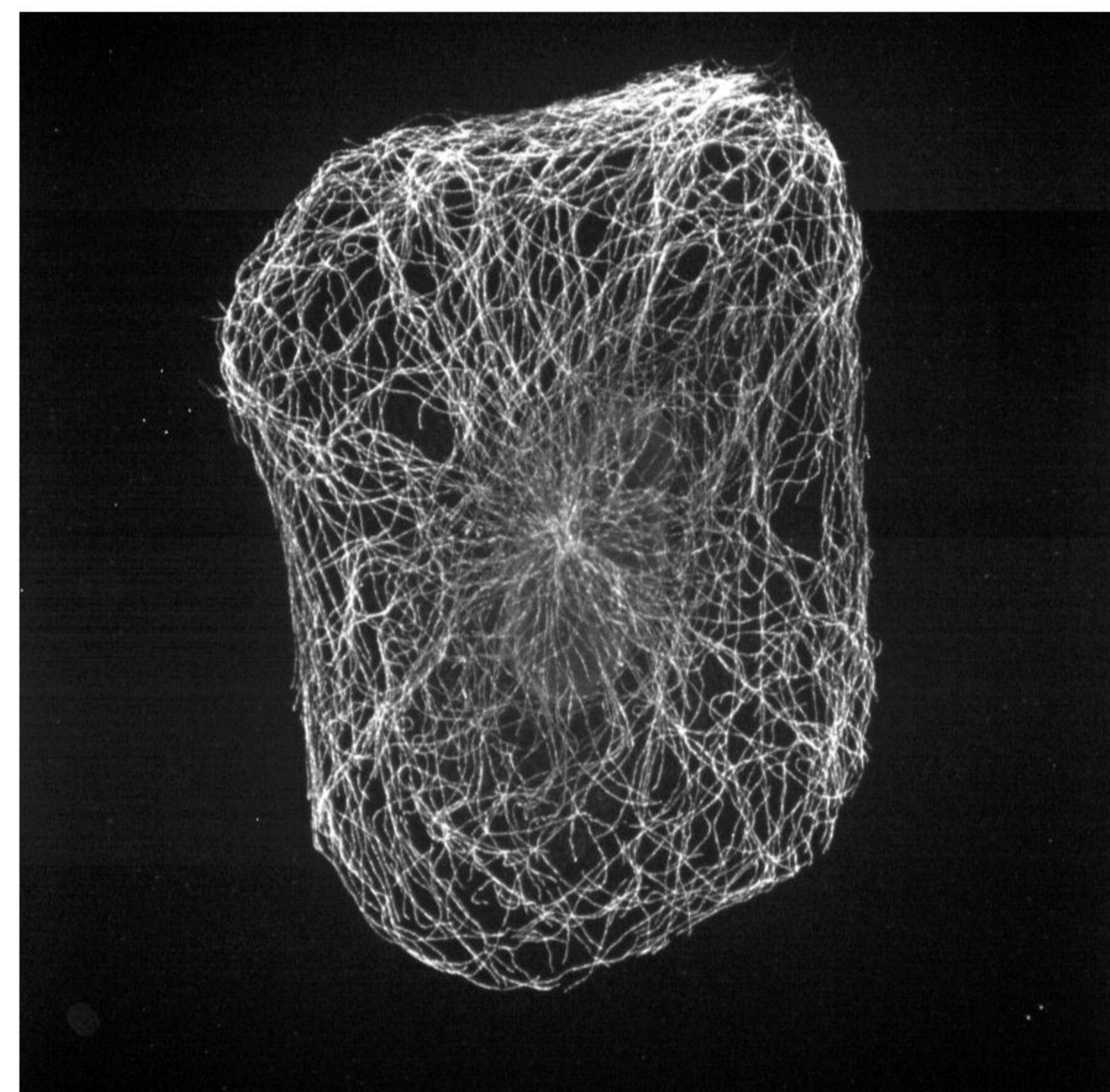
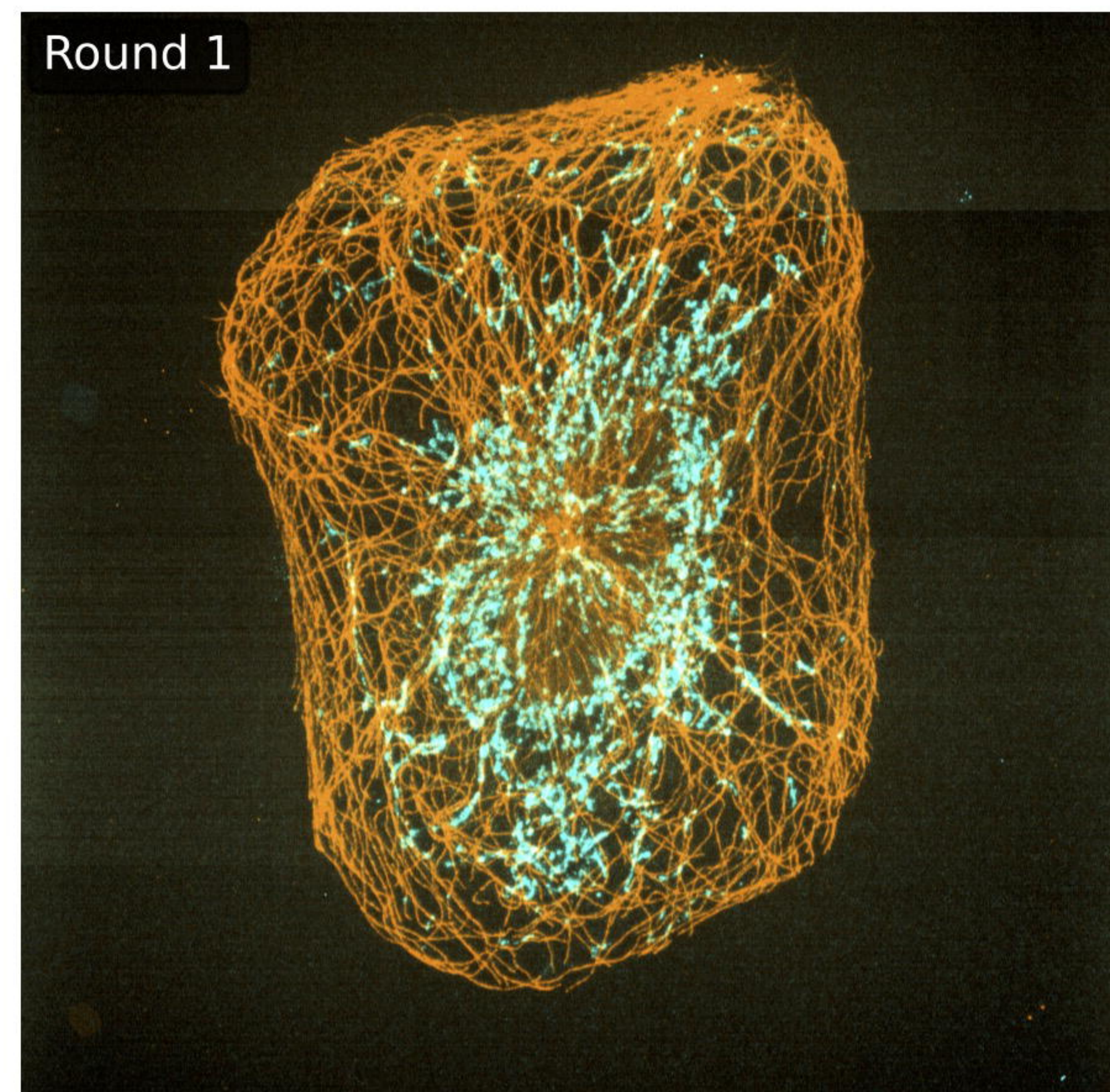


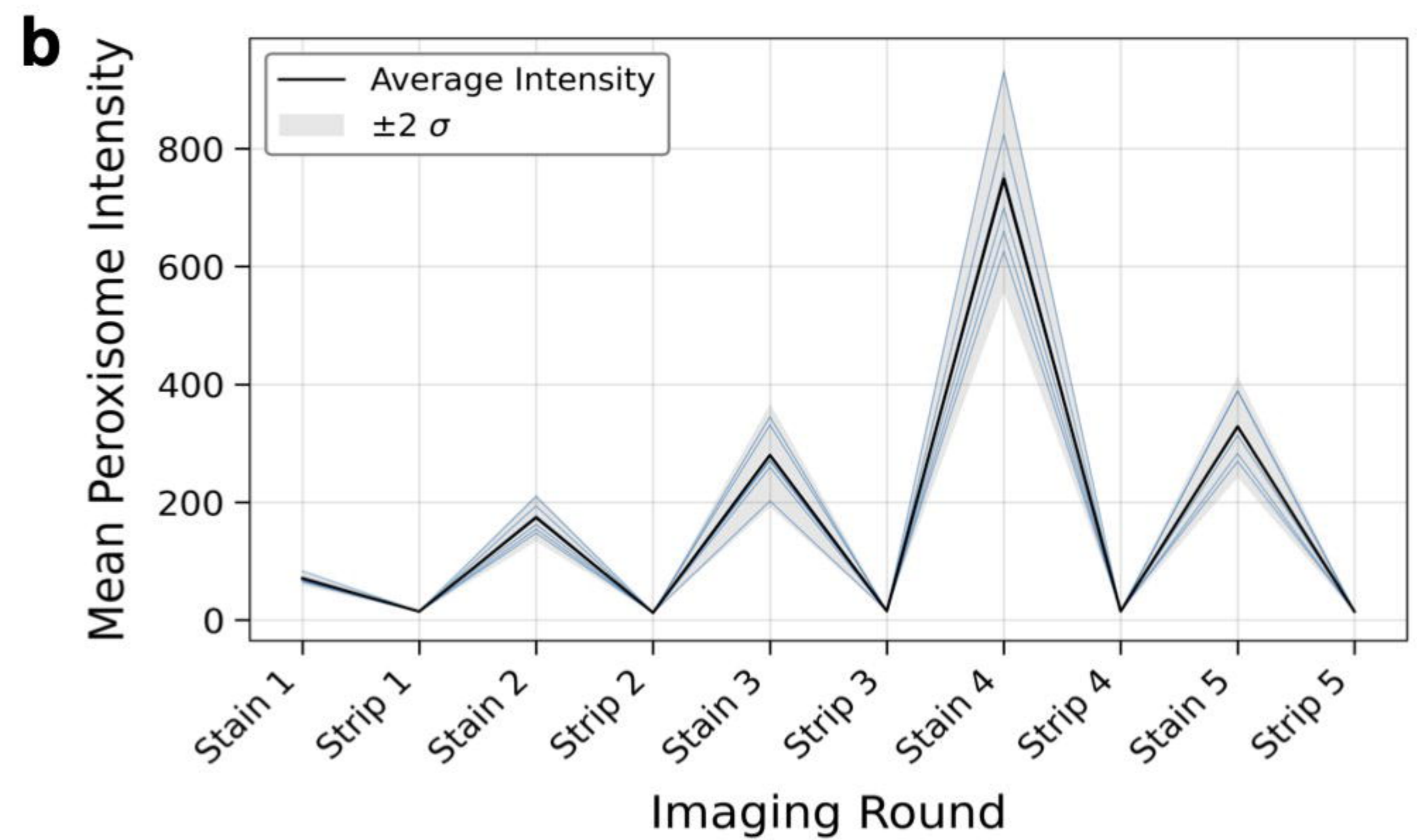
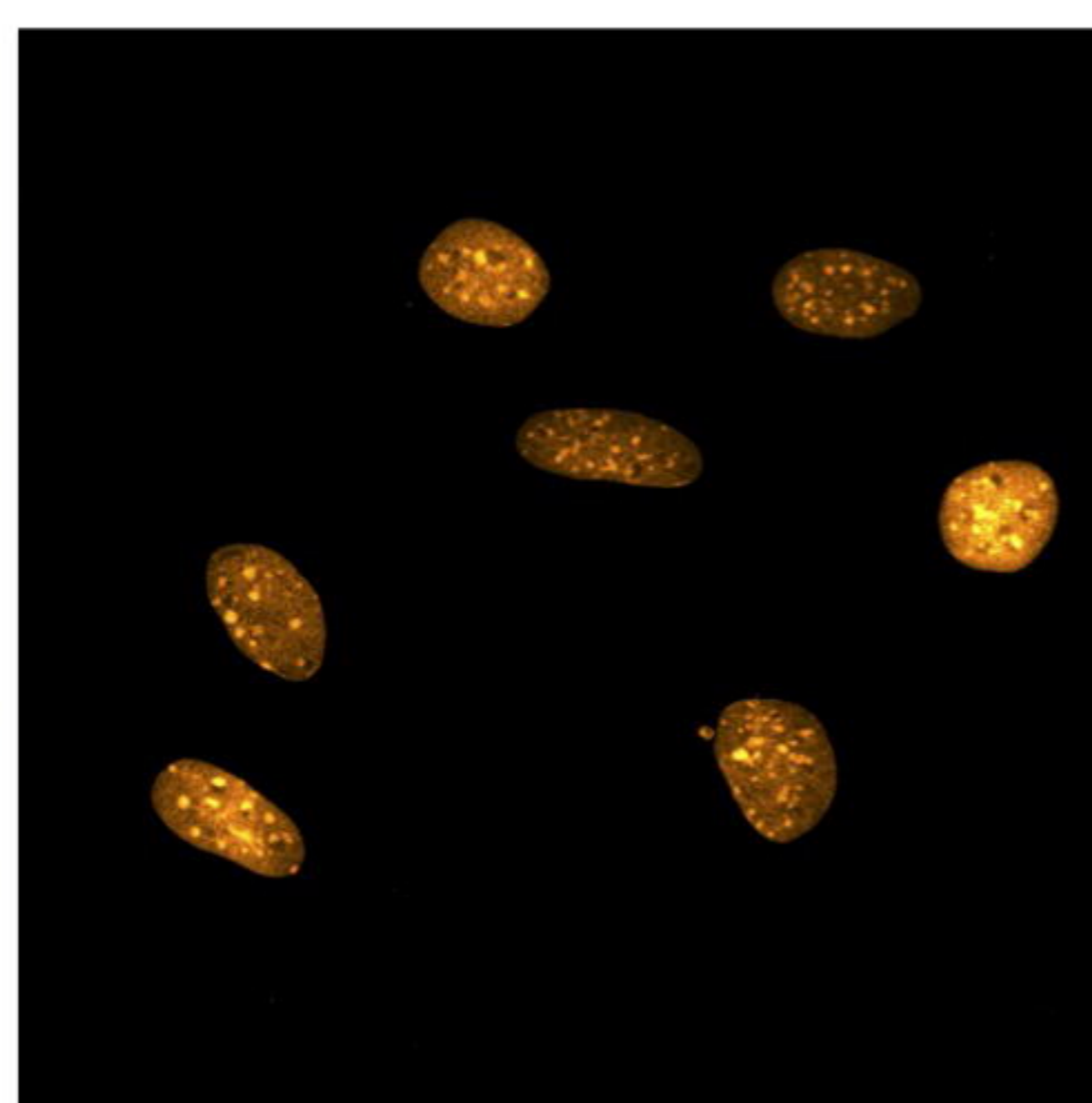
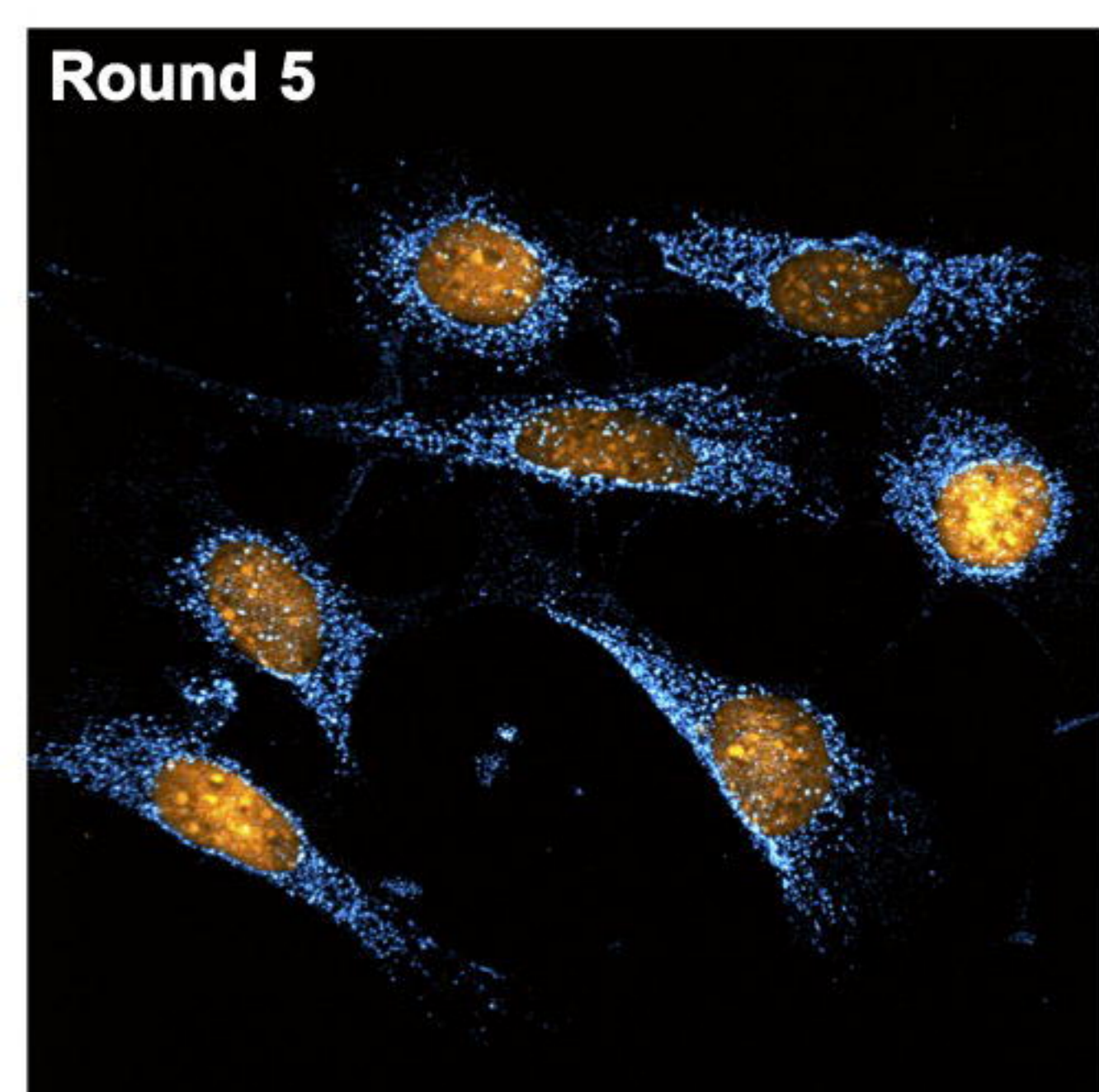
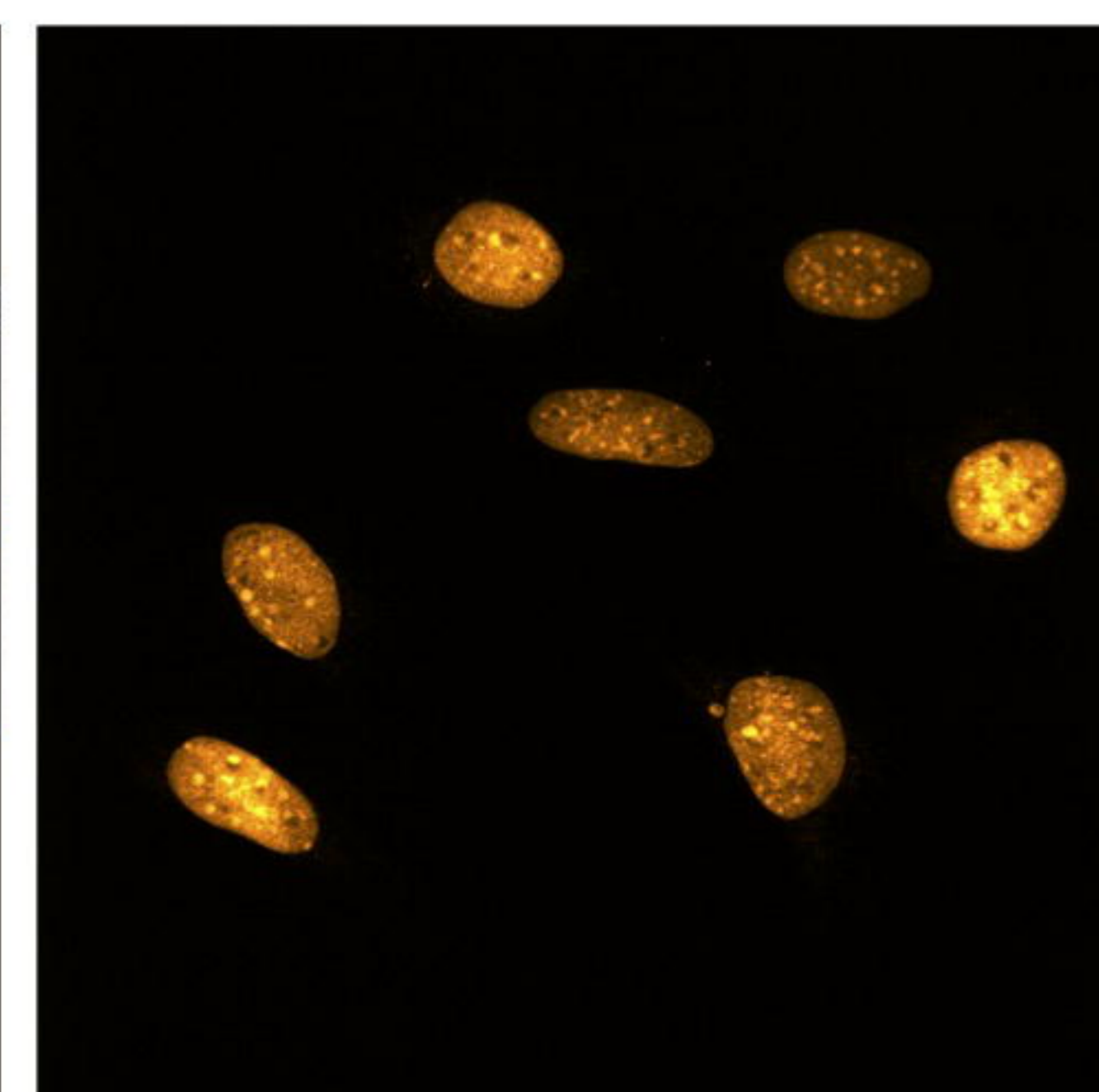
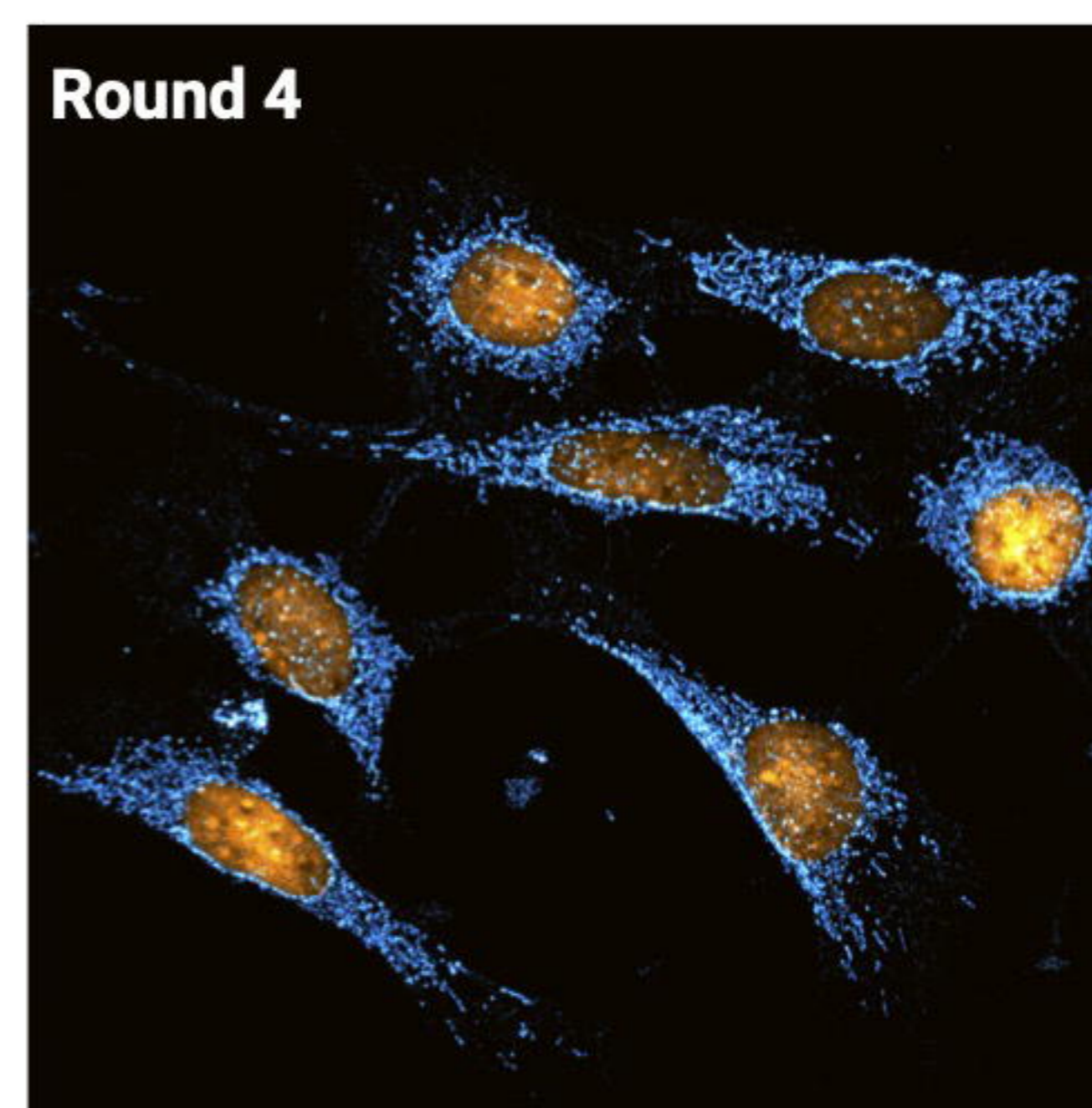
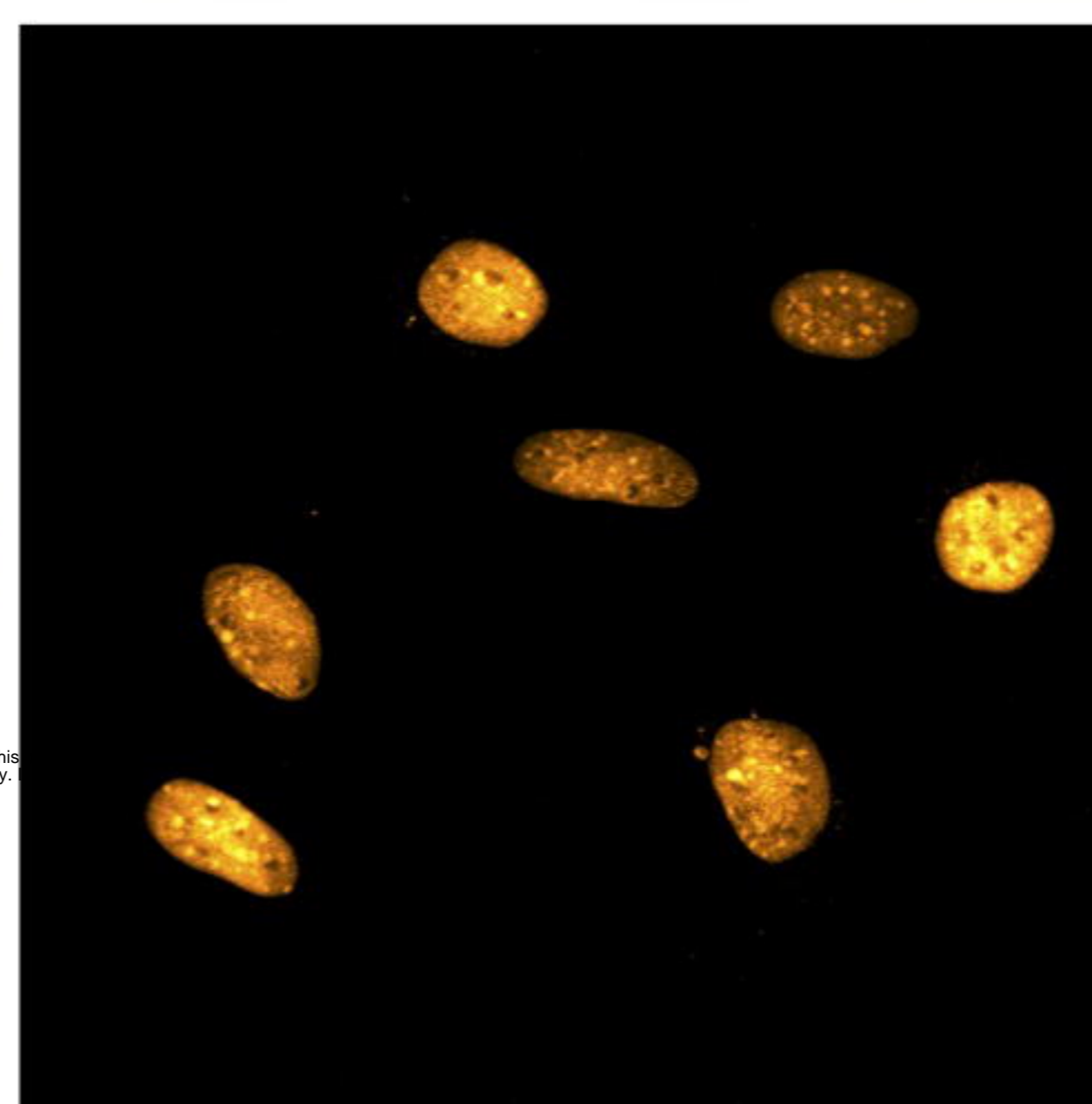
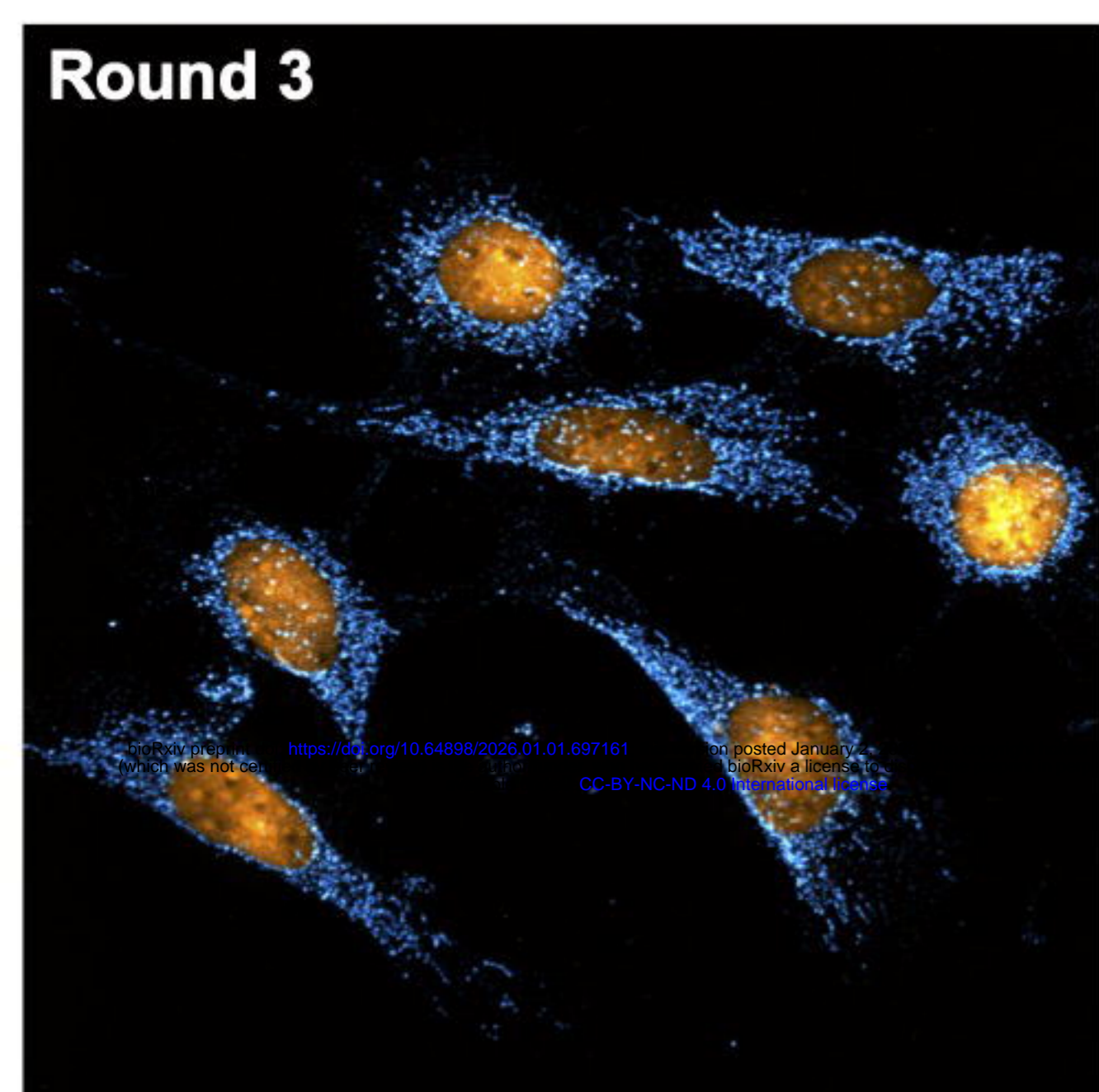
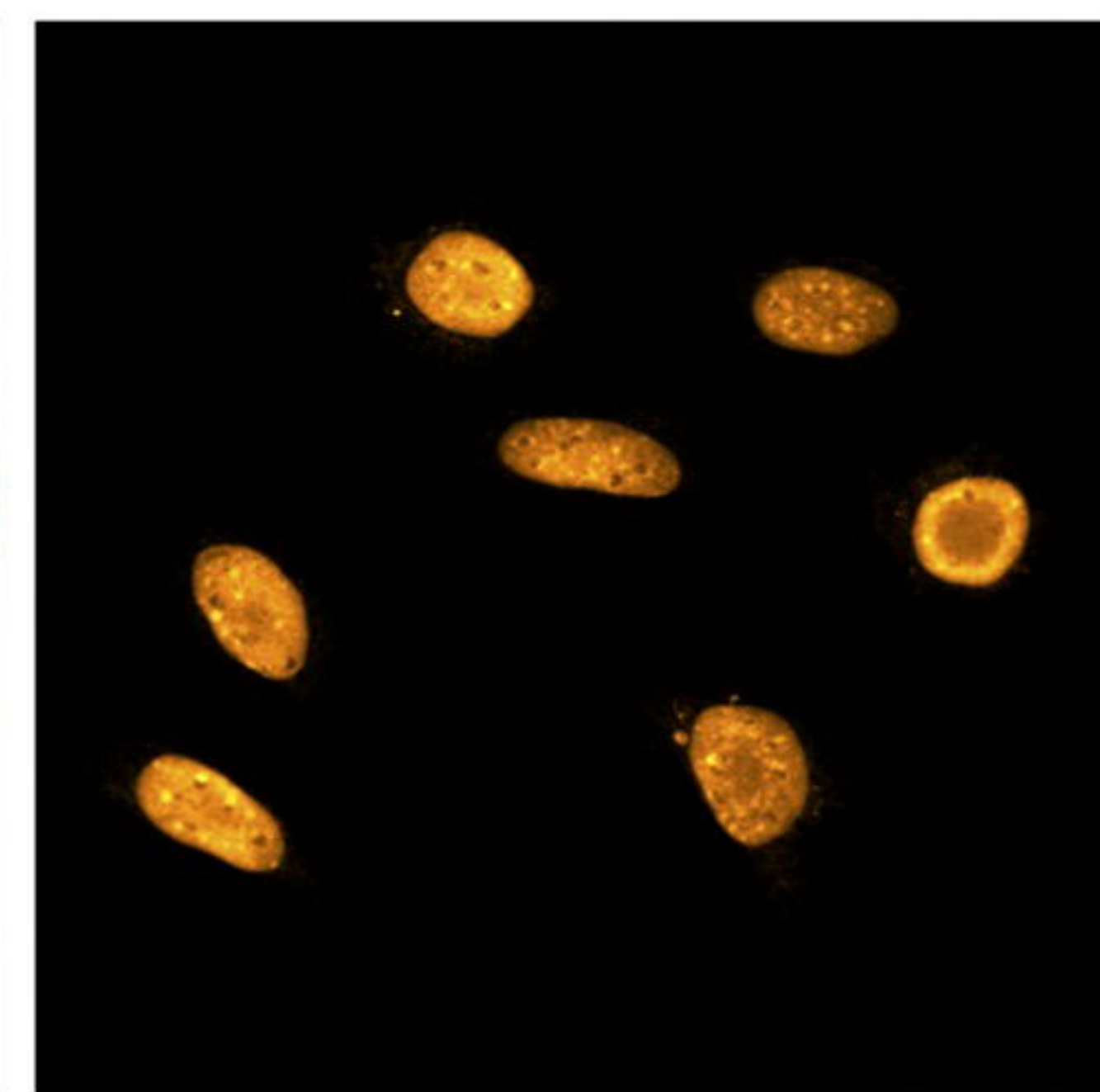
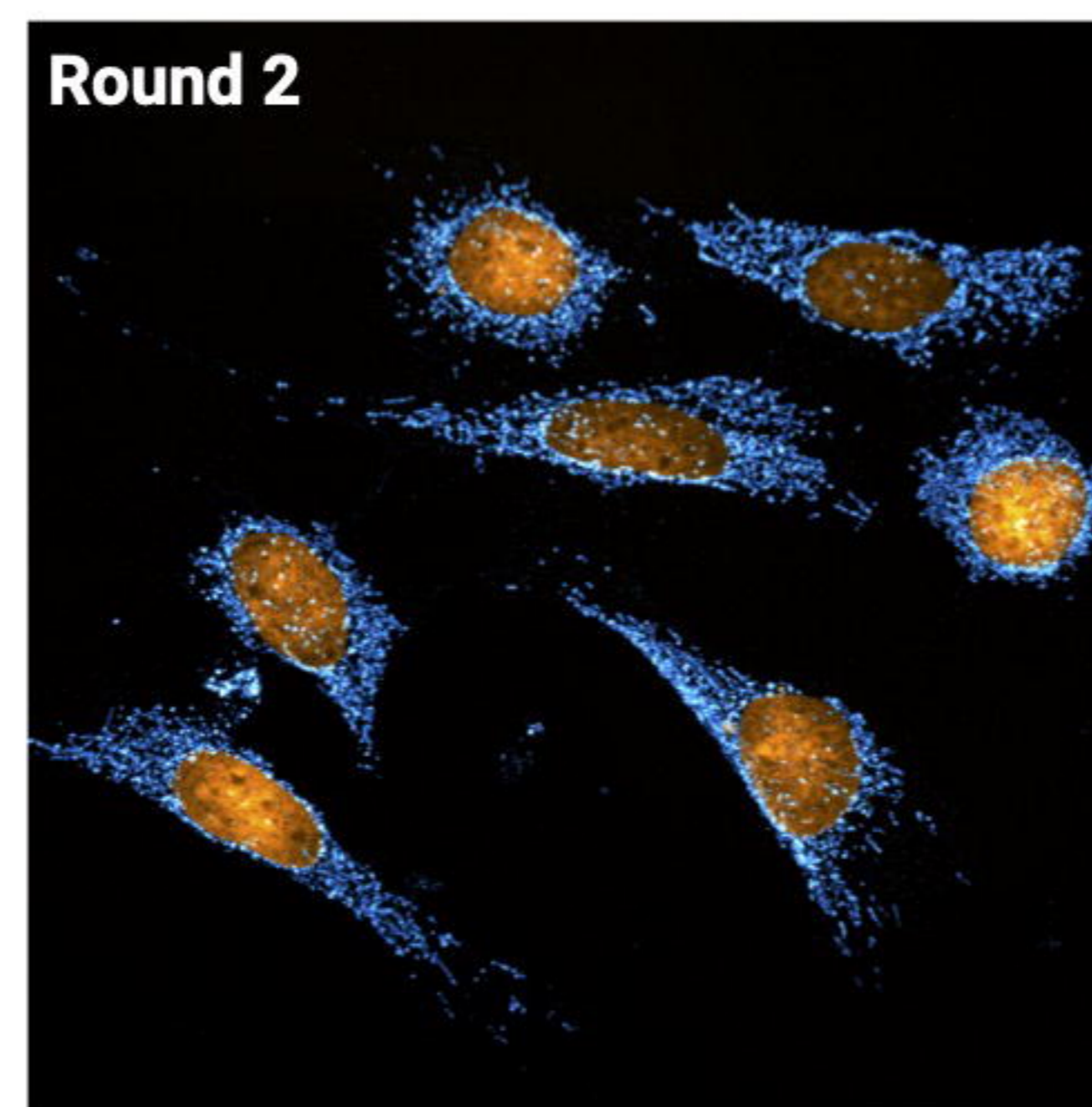
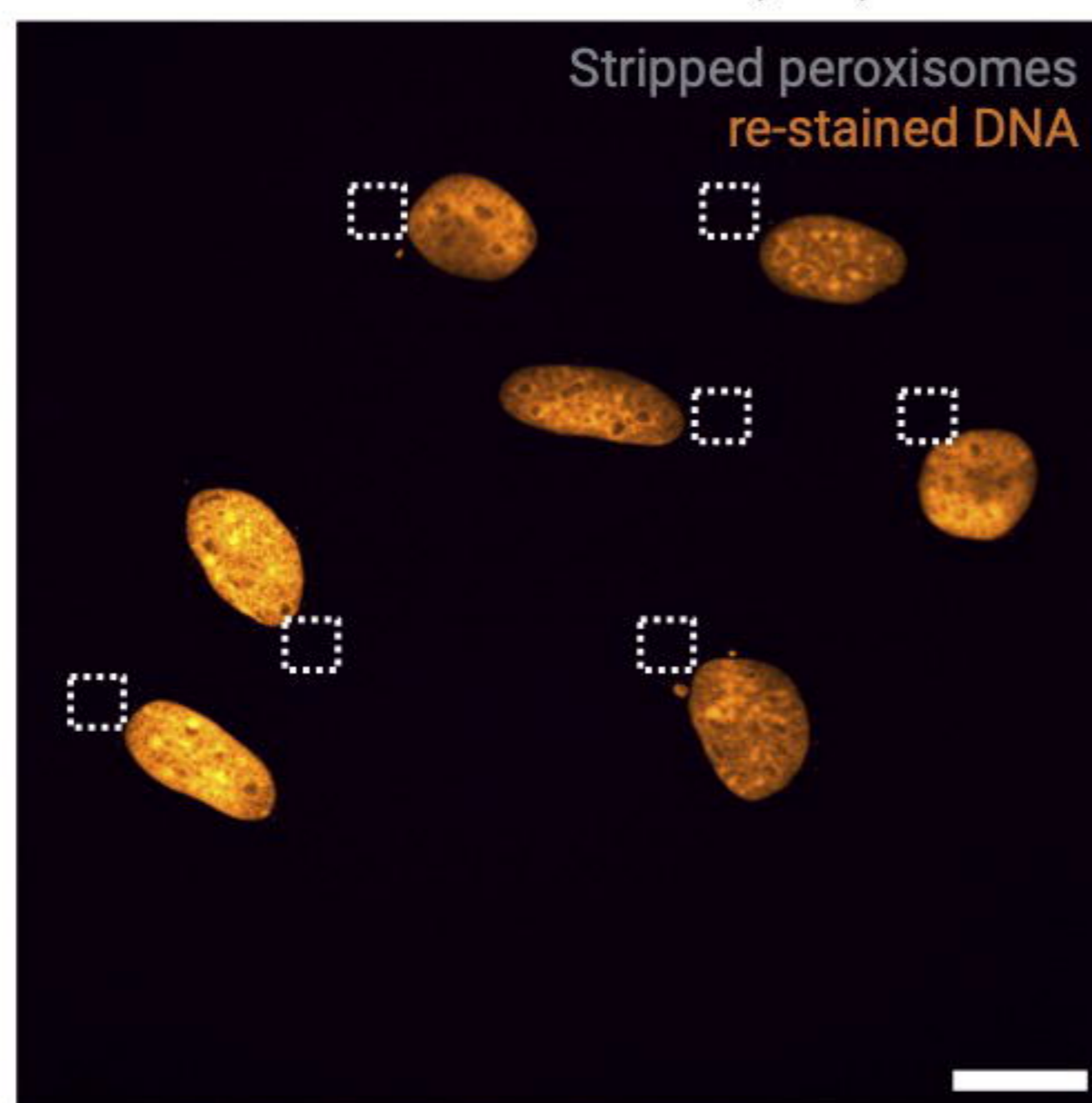
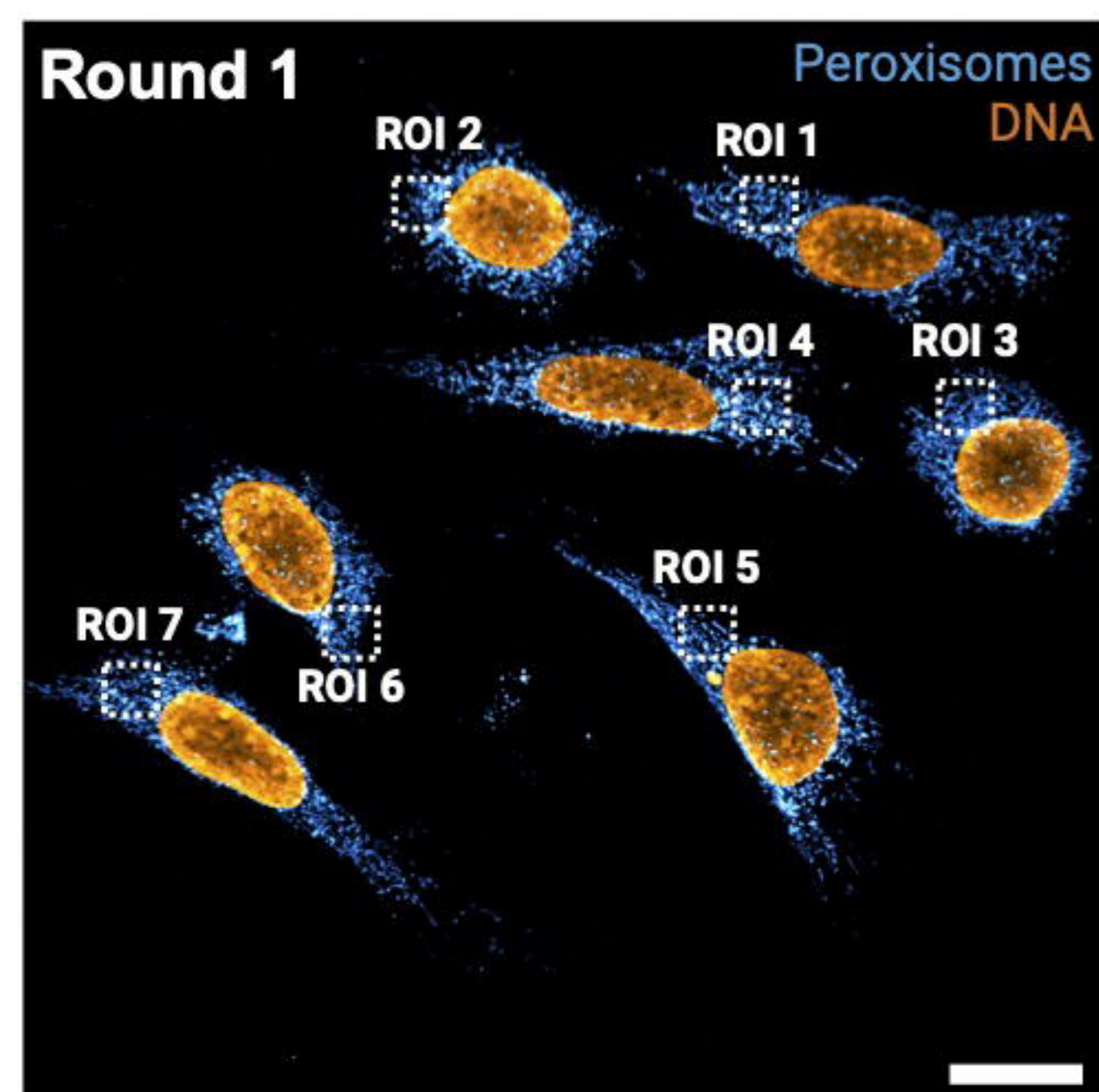


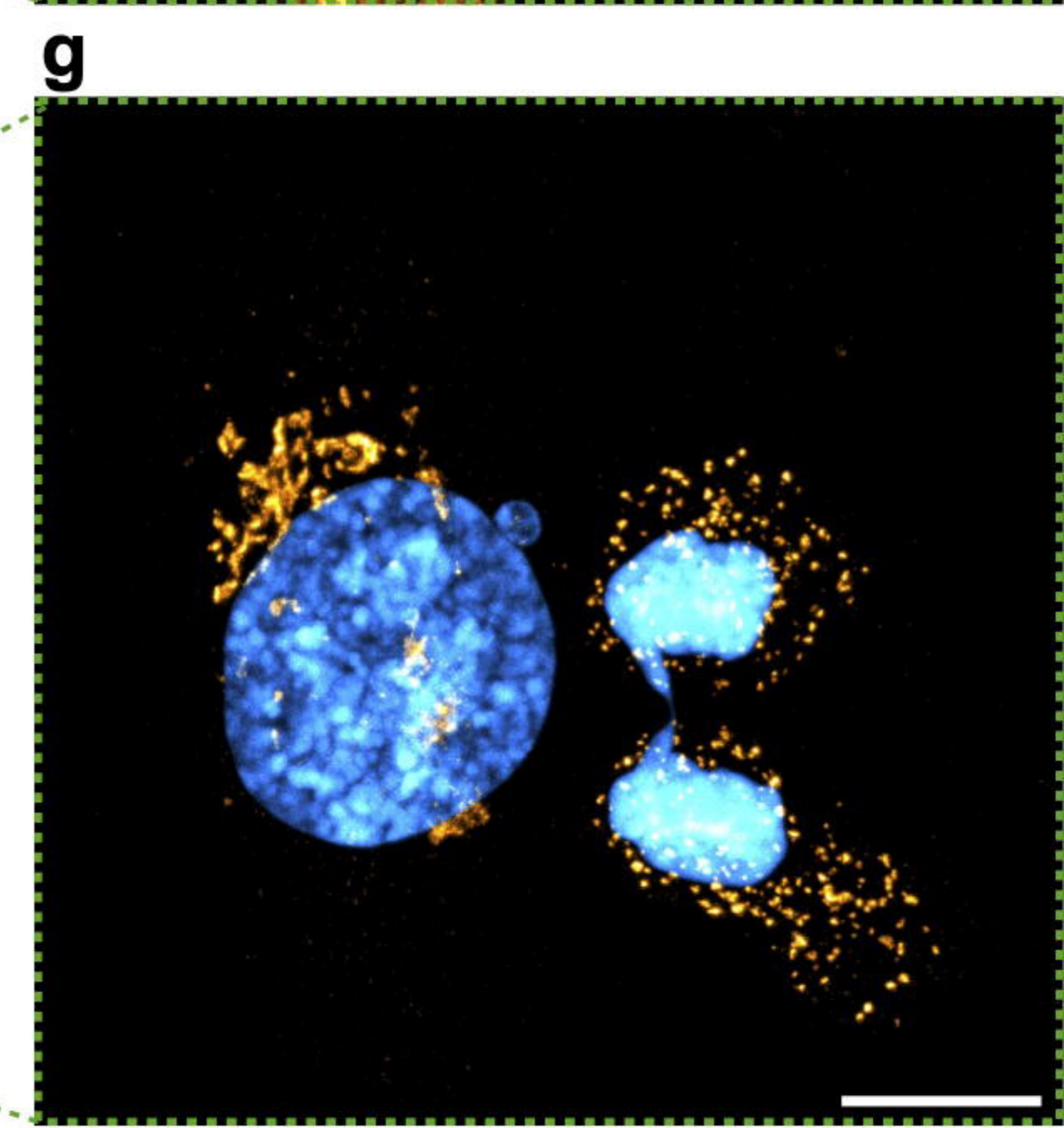
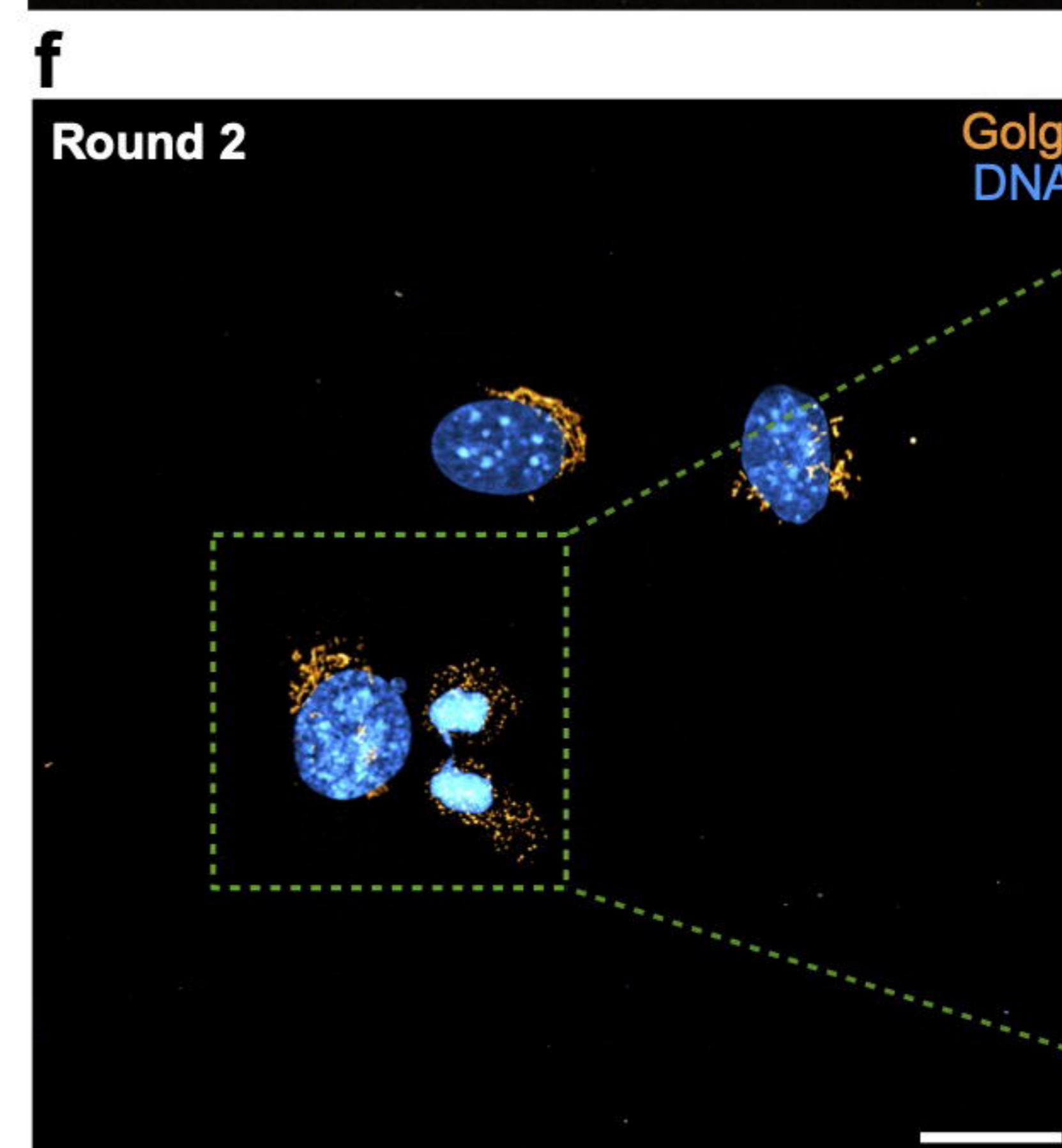
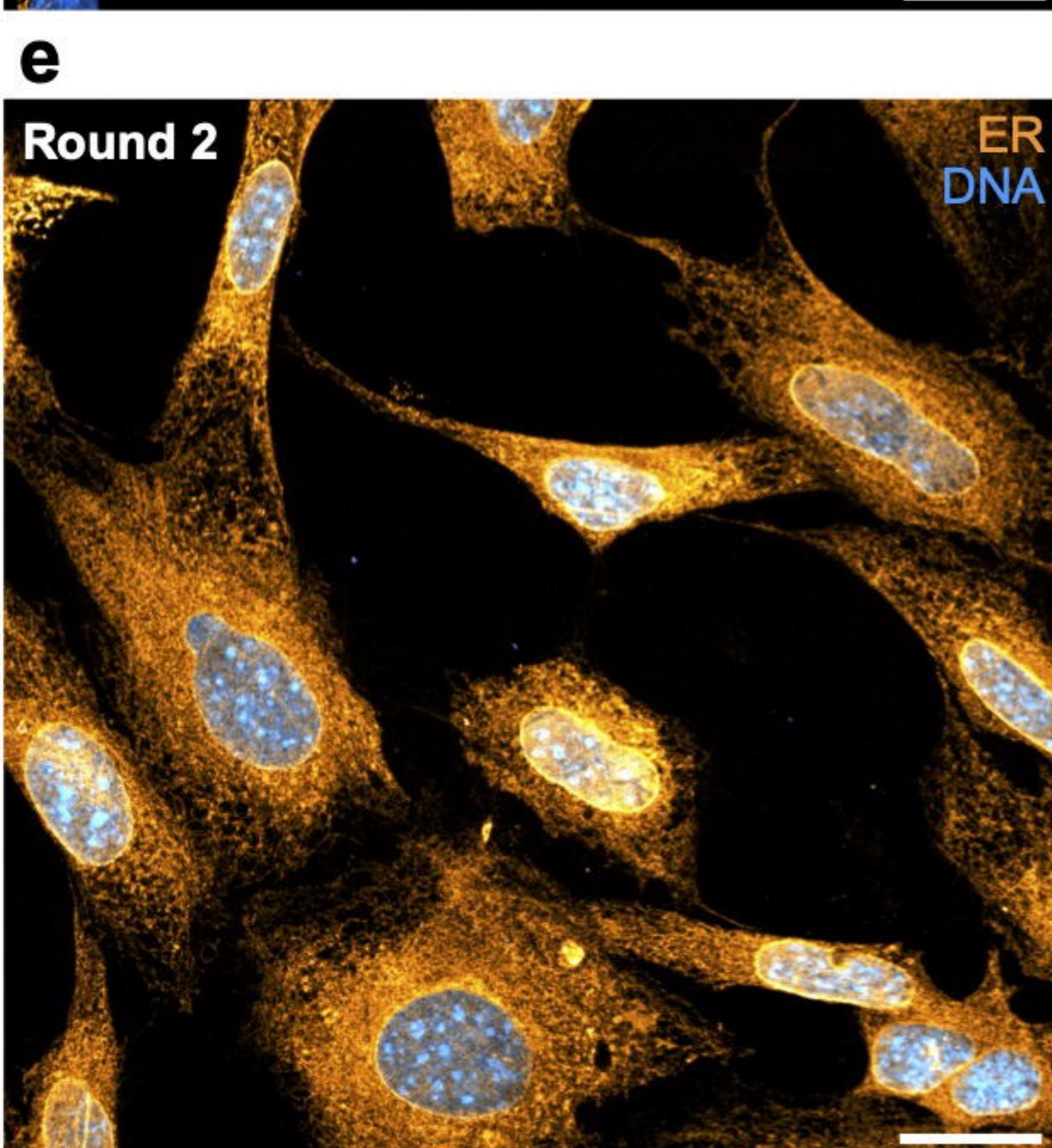
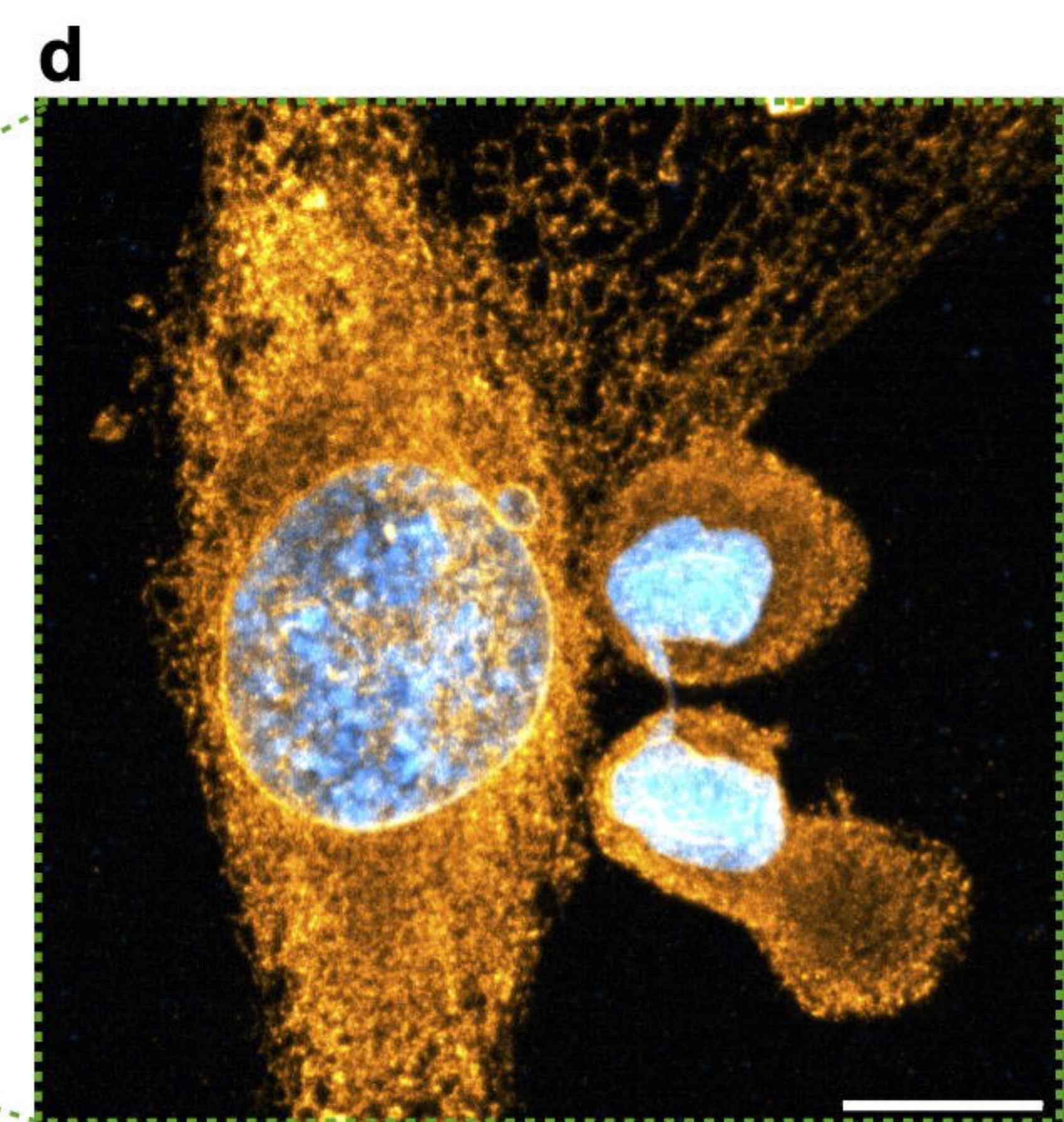
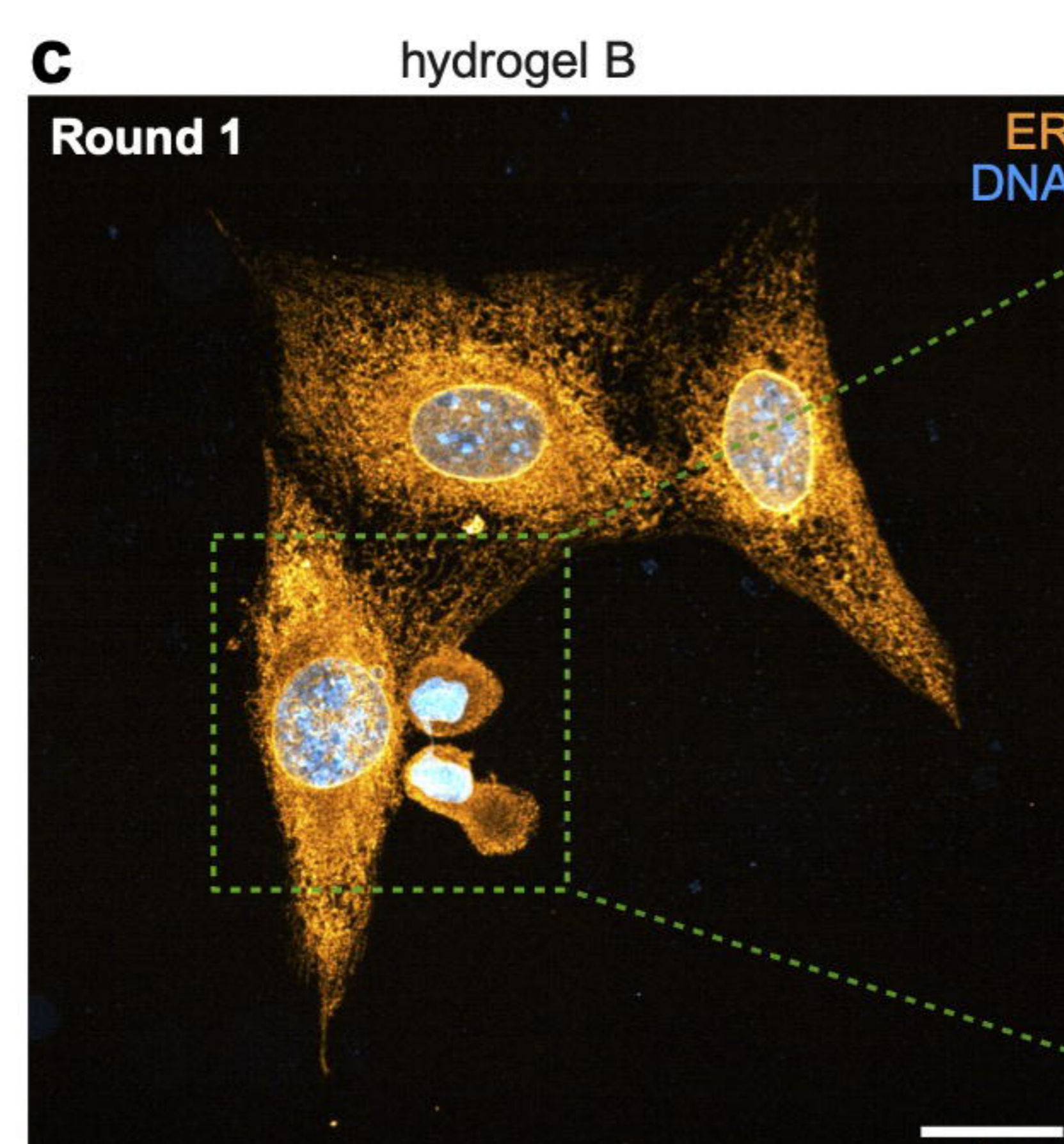
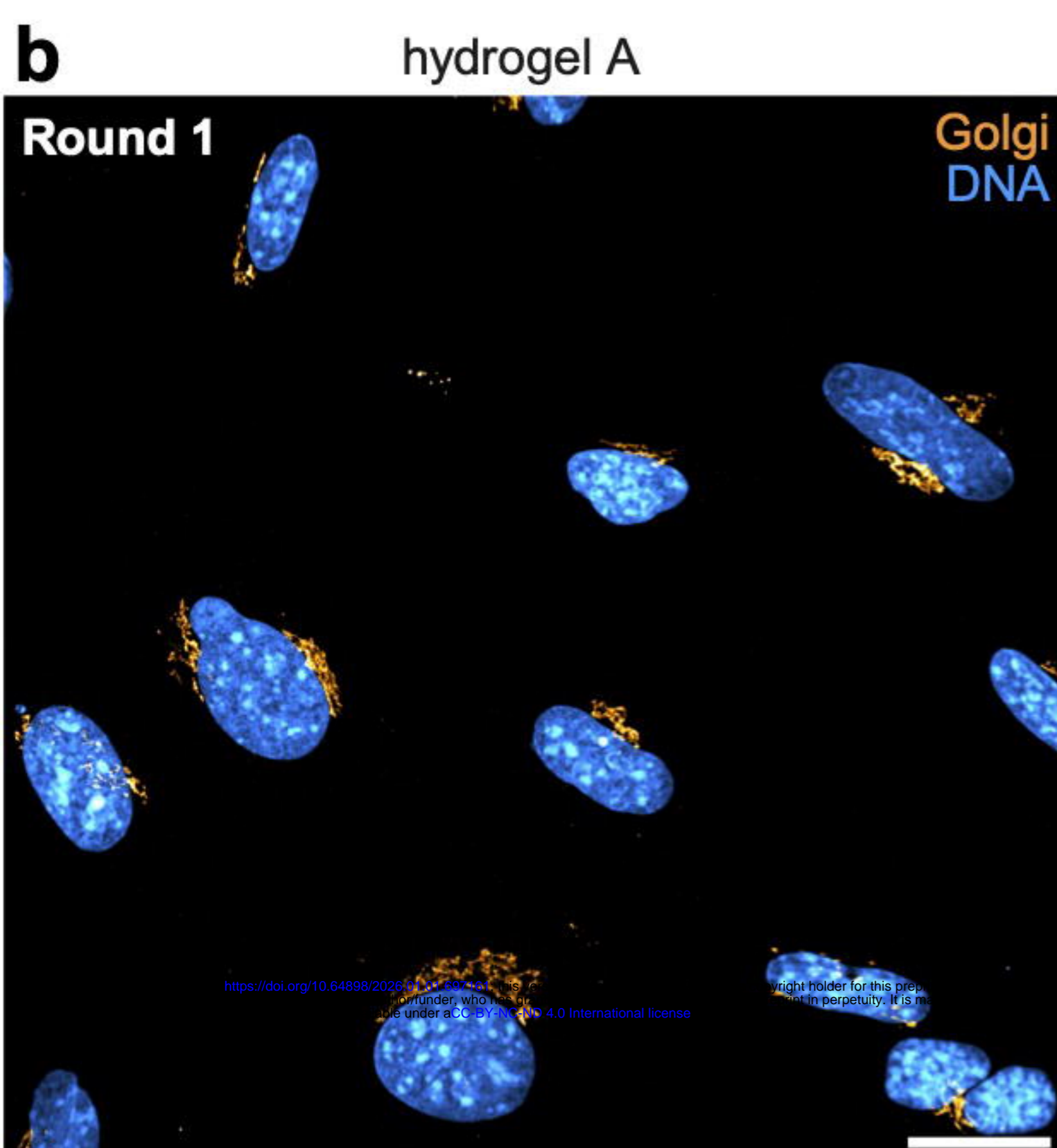
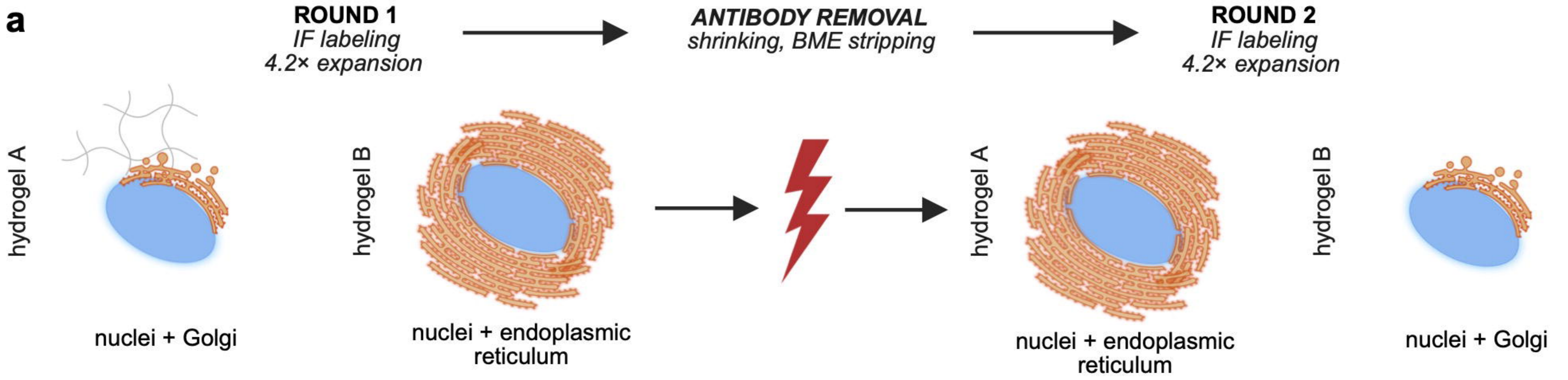


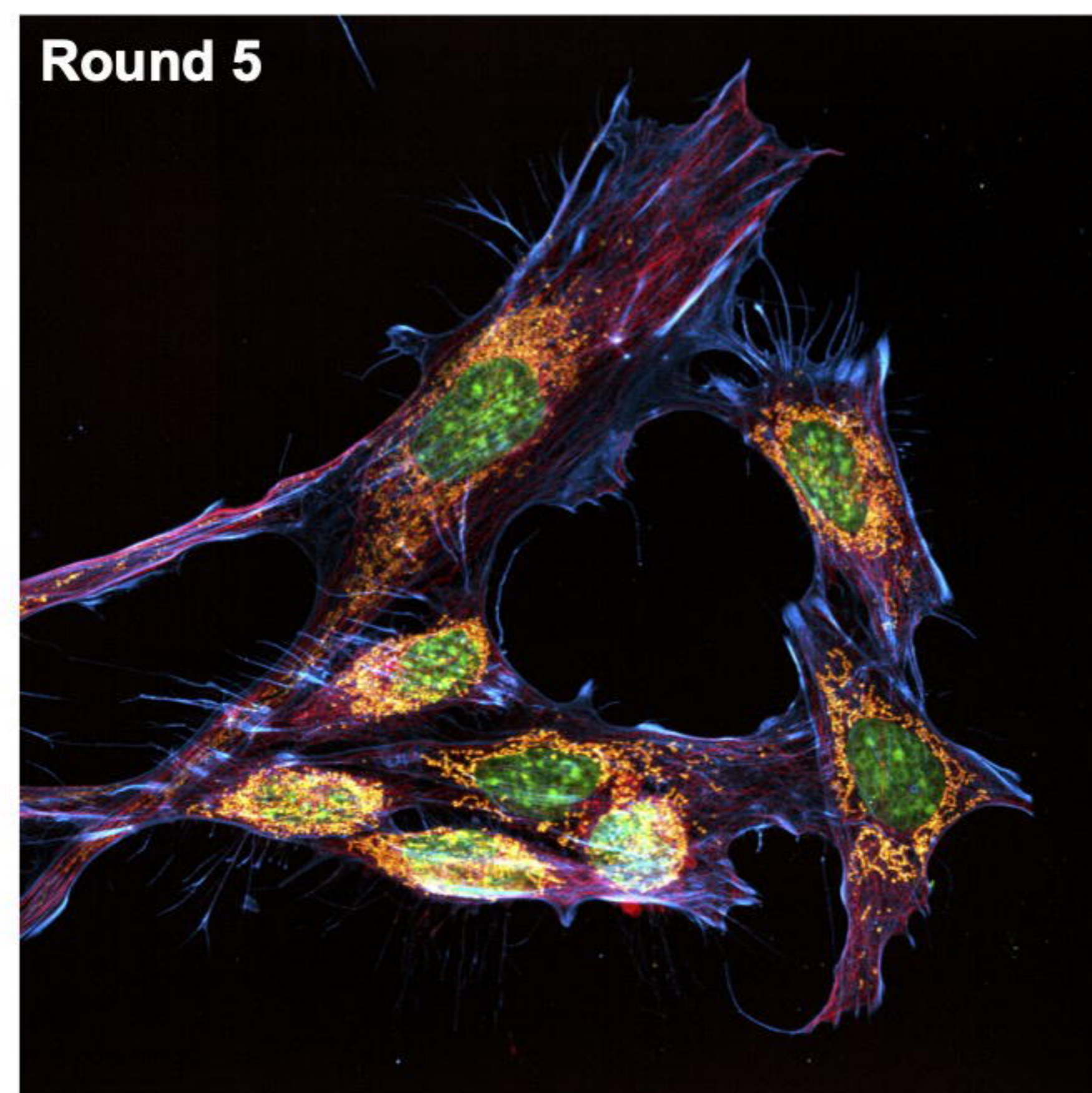
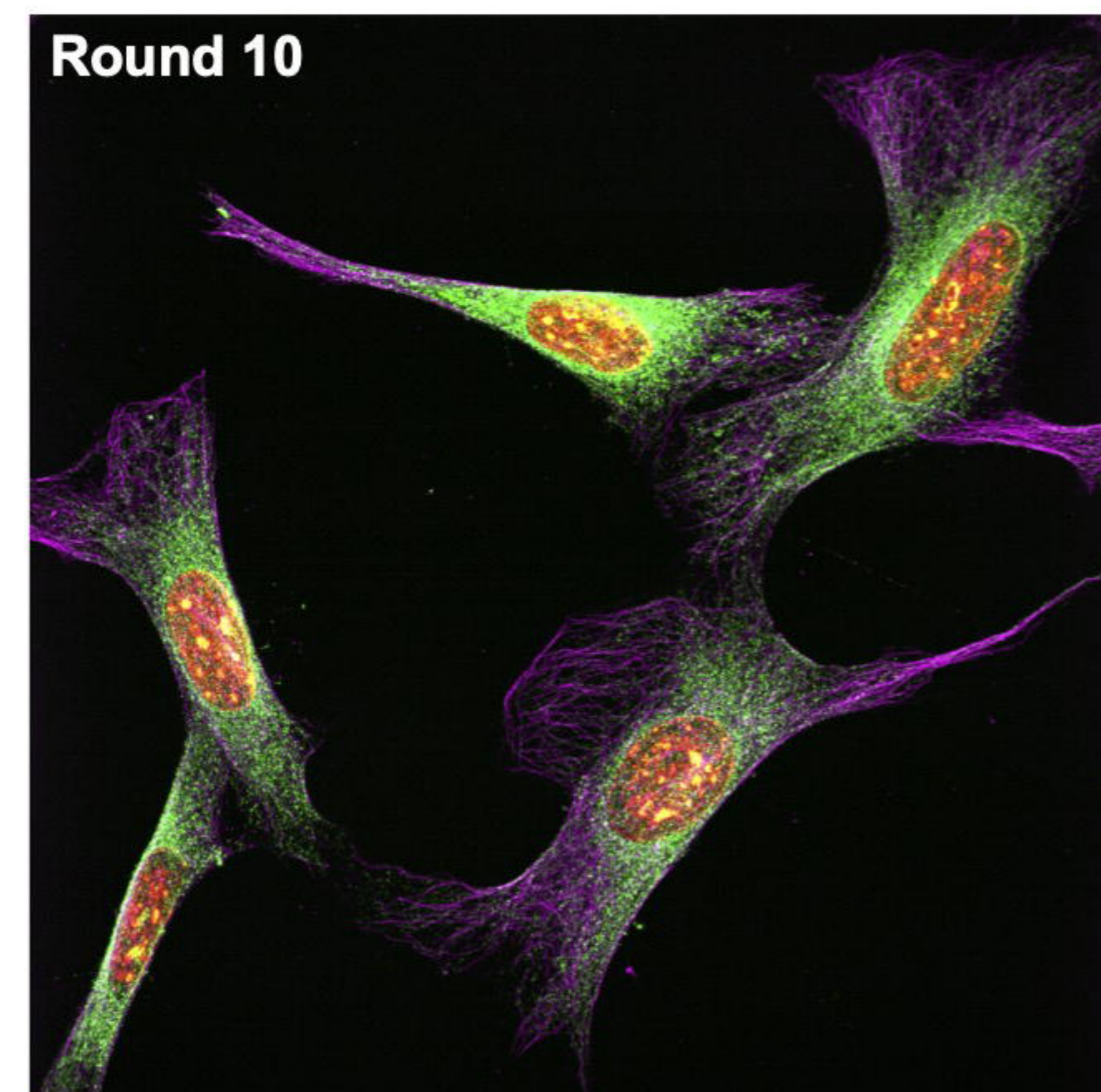
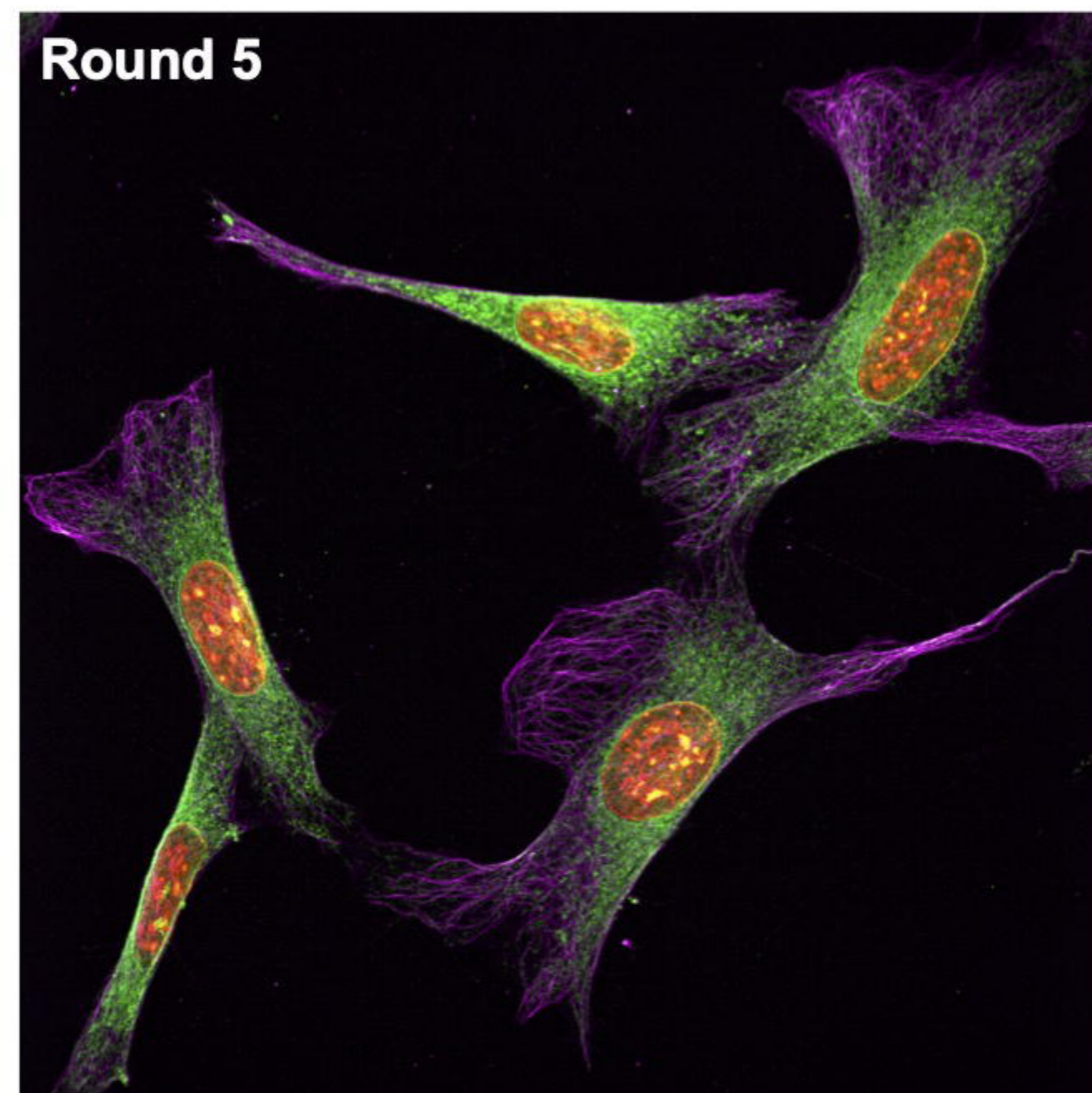
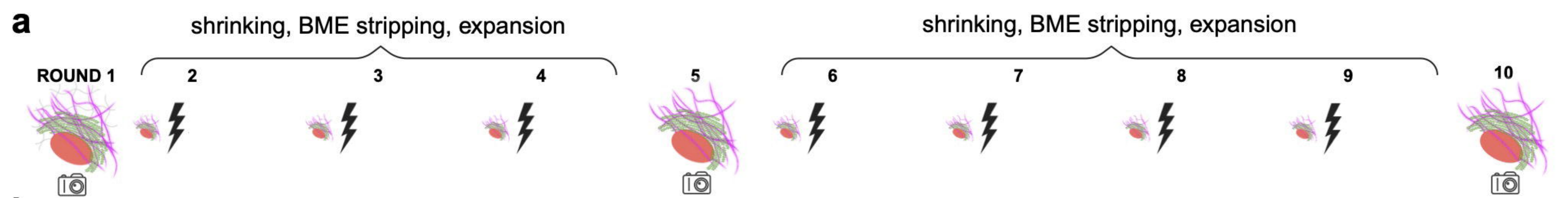




**Raw Data****Microtubules  
Linearly Registered****Mitochondria  
Linearly Registered****Microtubules  
Nonlinearly Registered****Mitochondria  
Nonlinearly Registered**







**Secretory pathway****Cytoskeletal components****Metabolic organelles network****Nuclei**